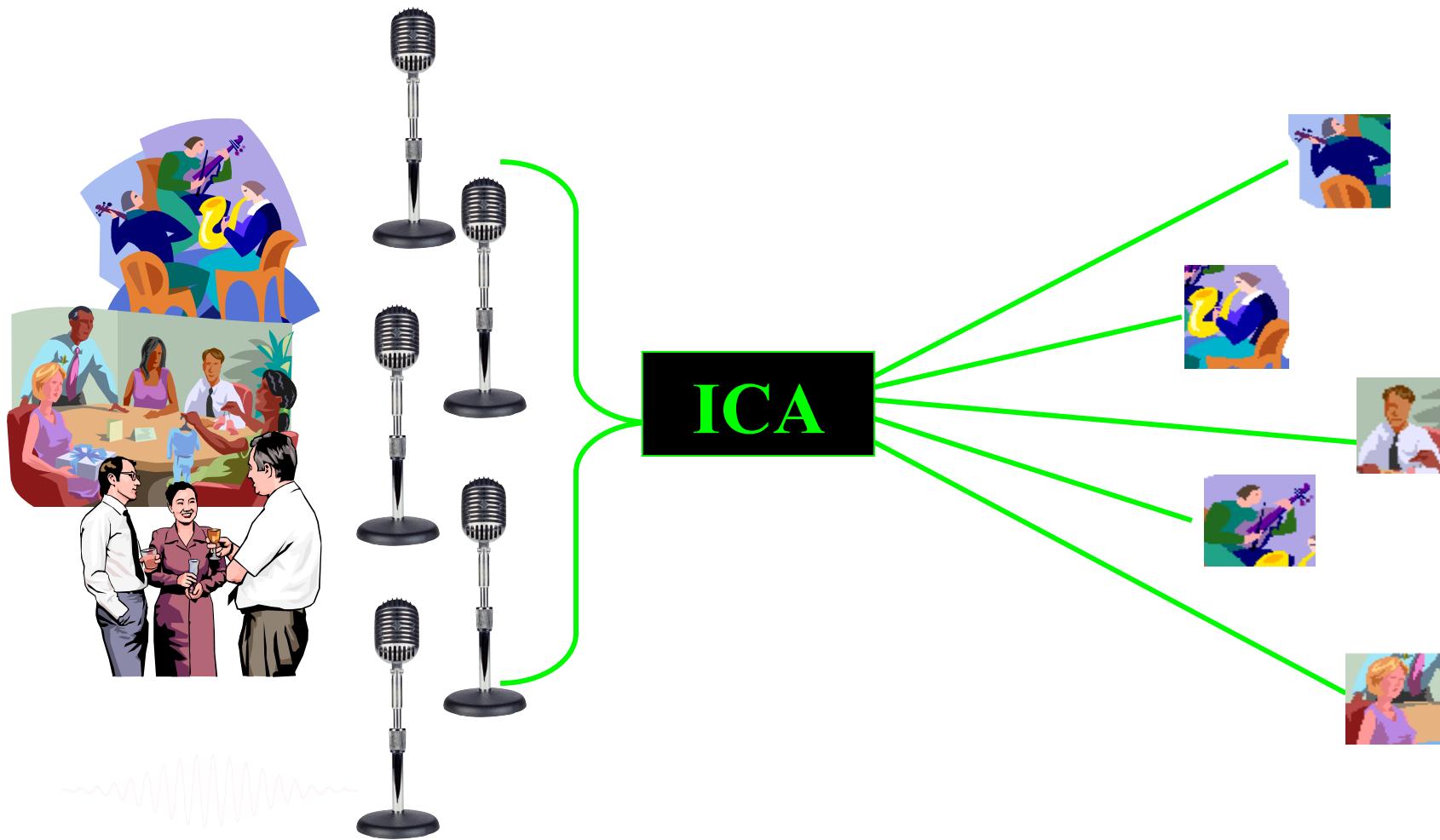


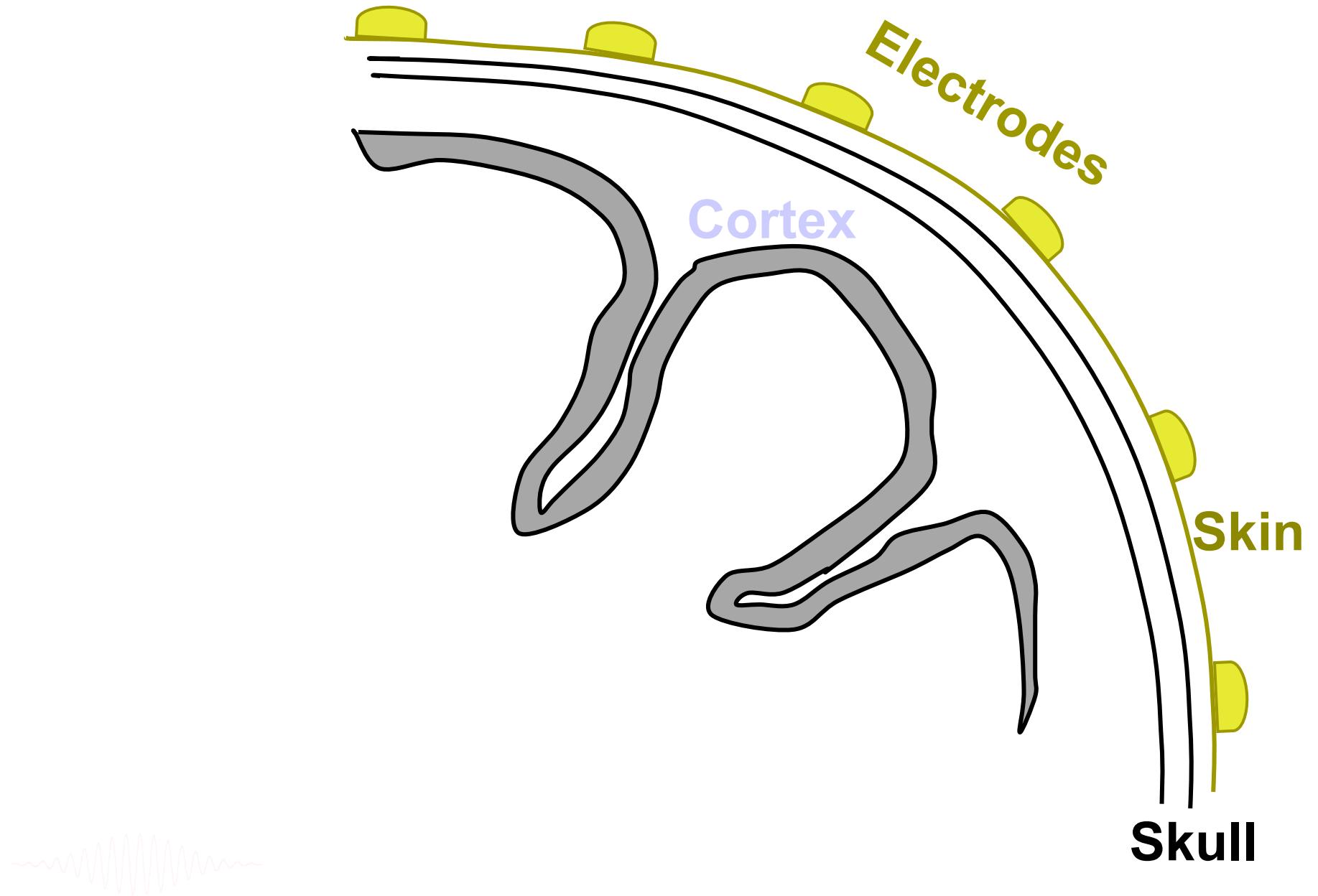
Independent component analysis applied to biophysical time series and EEG

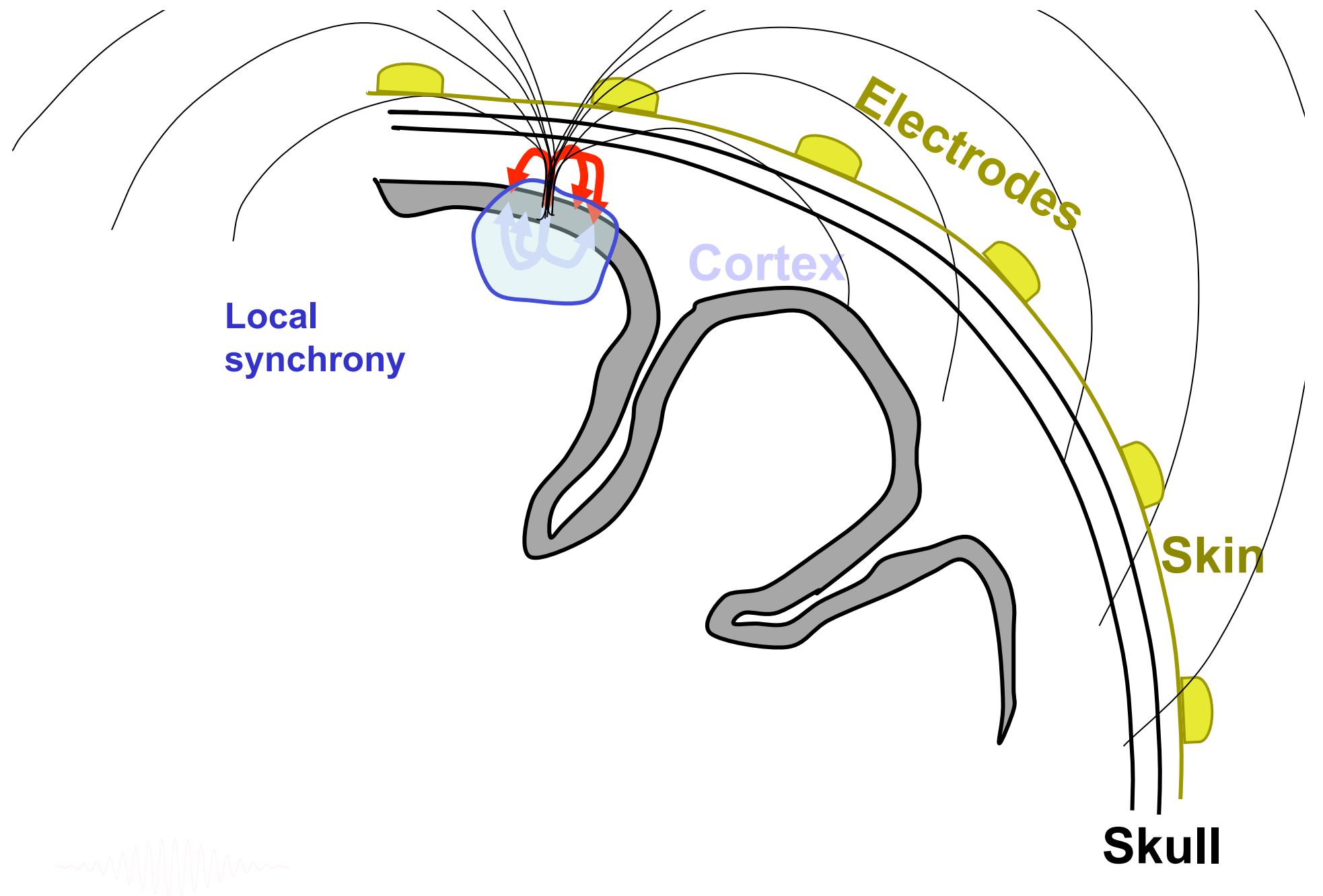
Arnaud Delorme

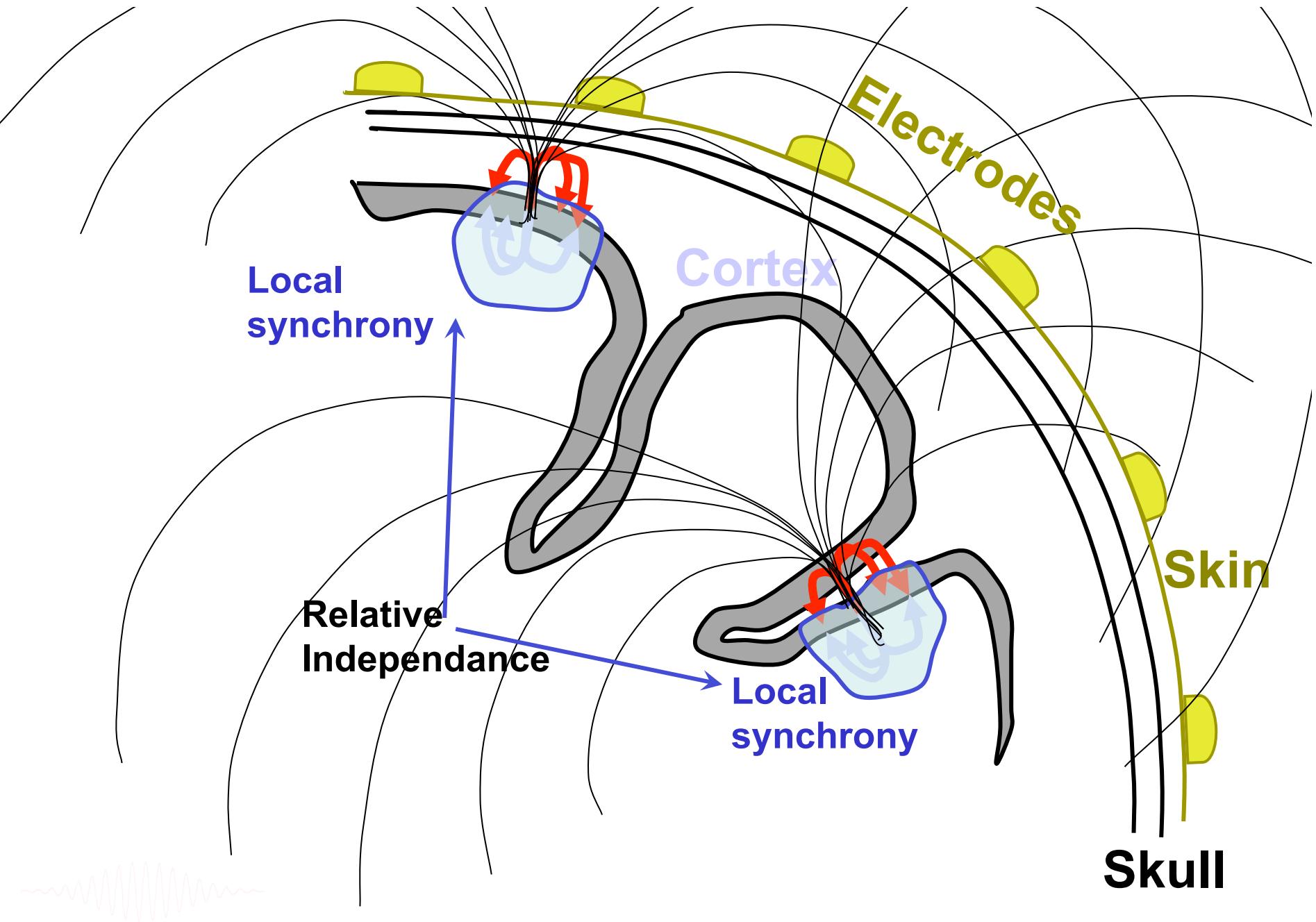


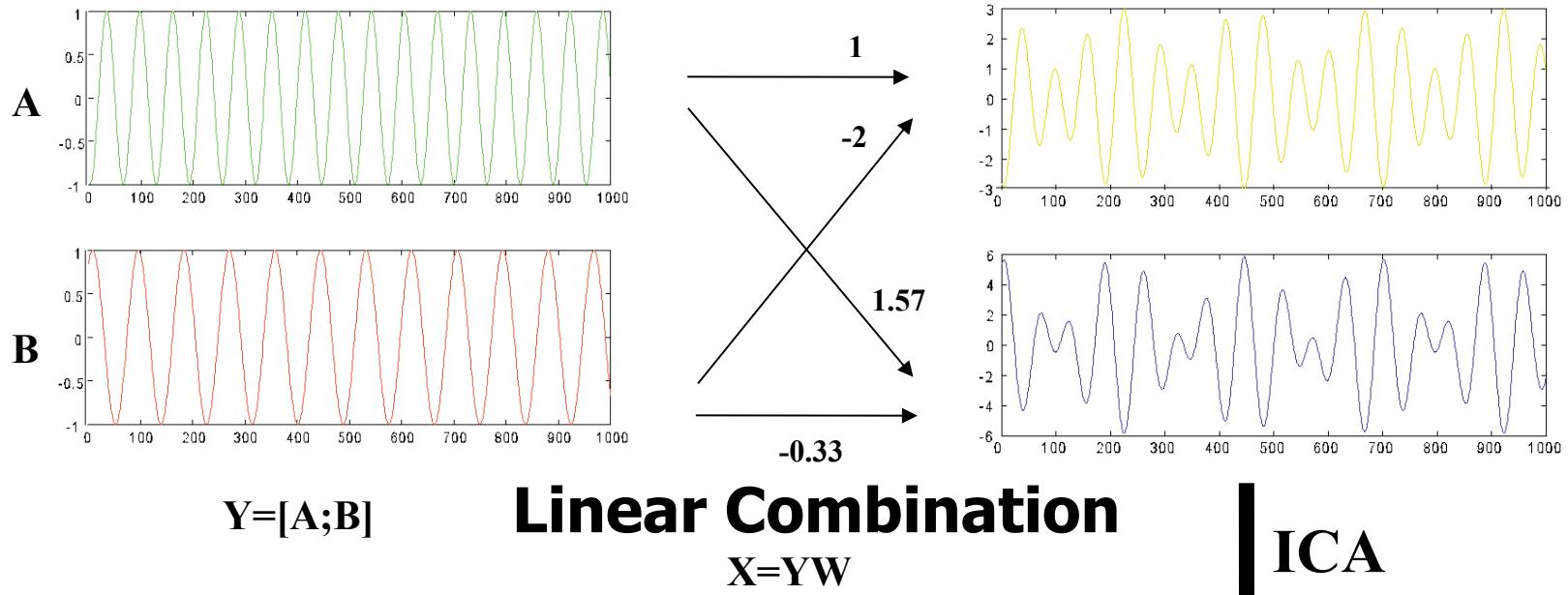
Example: Speech Separation



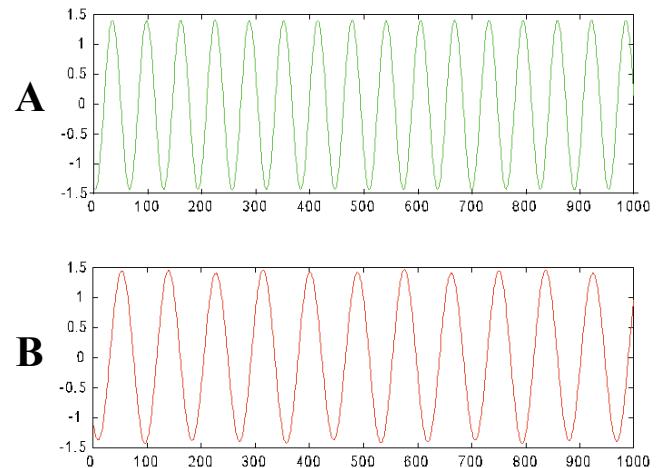






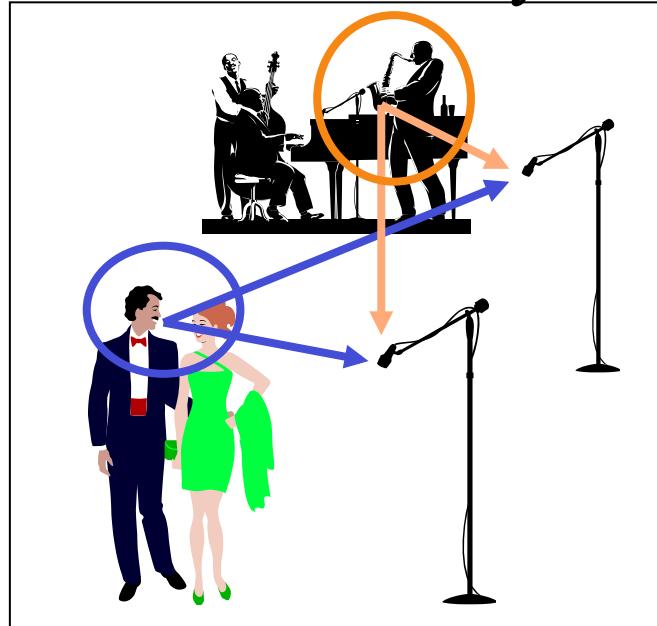


Infomax ICA

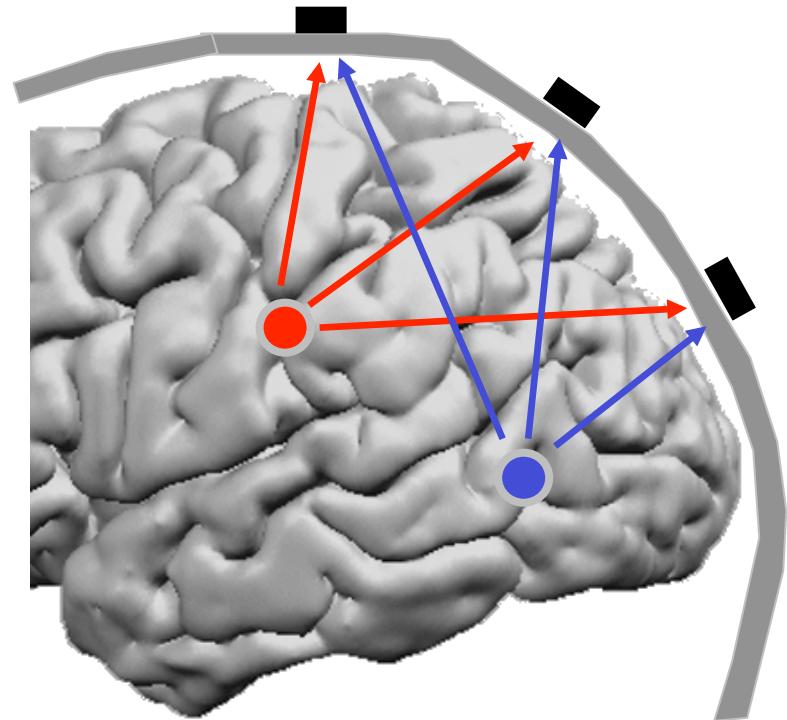


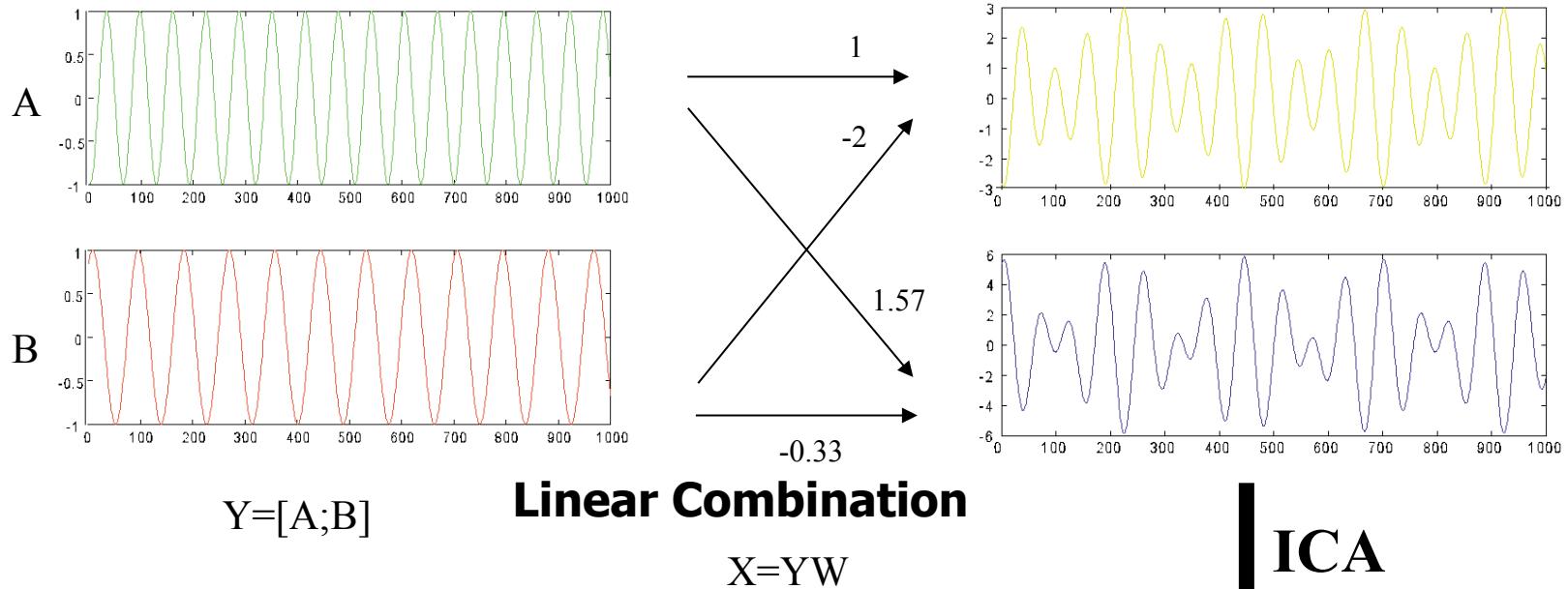
Independent component analysis

Cocktail Party

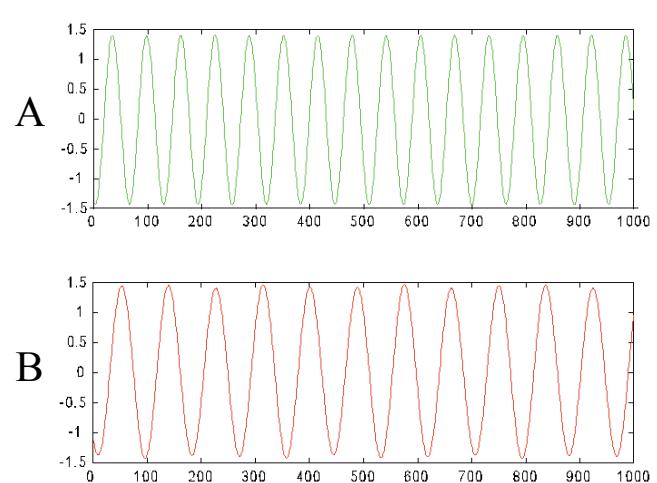


Mixture of Brain source activity





ICA is a method to recover a version, of the original sources by multiplying the data by a unmixing matrix



$$\text{ICA activity} \quad \text{Data}$$

Data X

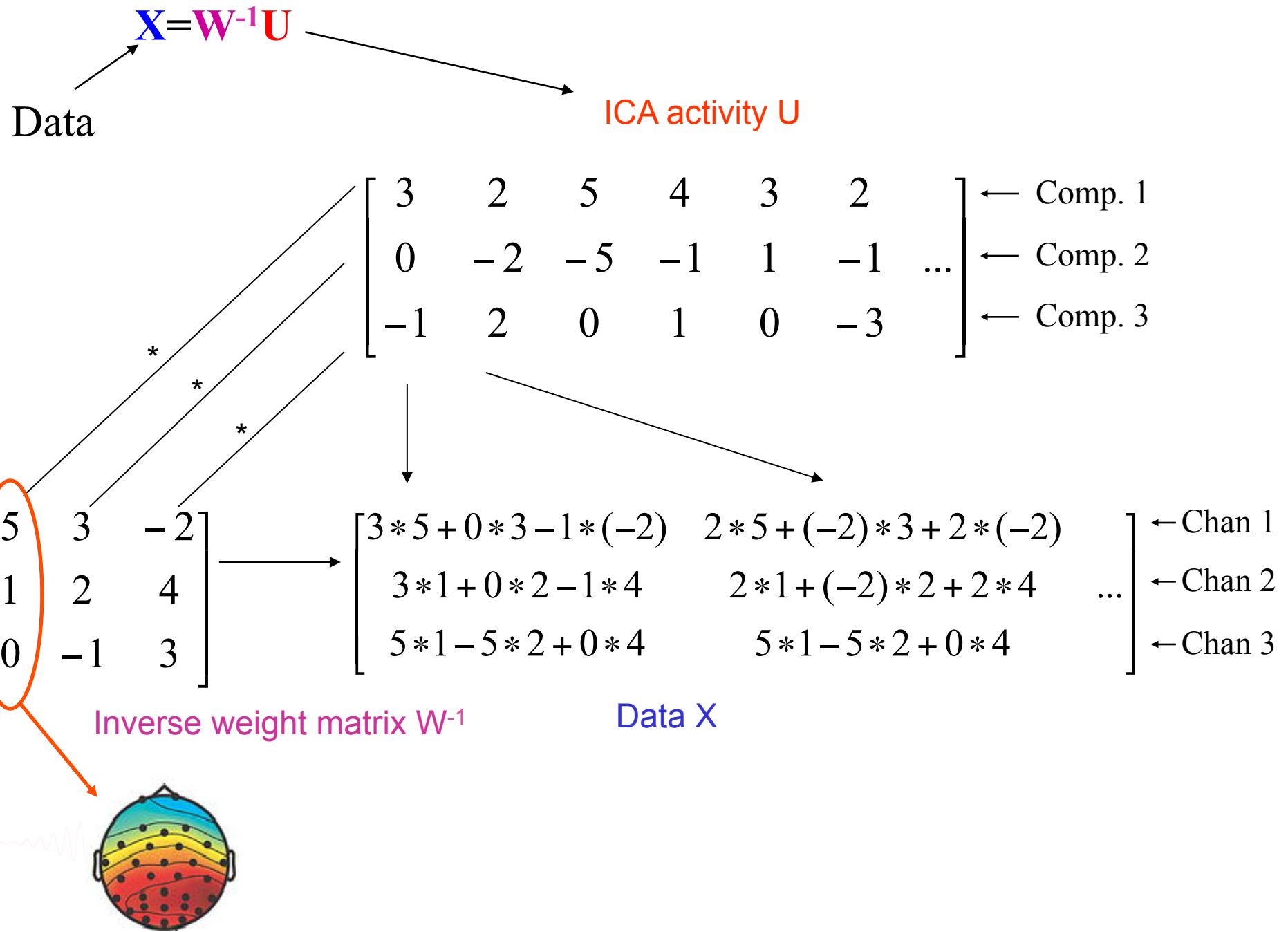
$$\begin{bmatrix} 3 & 2 & 5 & 4 & 3 & 2 & \dots \\ 0 & -2 & -5 & -1 & 1 & -1 & \dots \\ -1 & 2 & 0 & 1 & 0 & -3 & \dots \end{bmatrix} \leftarrow \begin{array}{l} \text{Channel 1} \\ \text{Channel 2} \\ \text{Channel 3} \end{array}$$

$$\begin{bmatrix} 5 & 3 & -2 \\ 1 & 2 & 4 \\ 0 & -1 & 3 \end{bmatrix}$$

Weight matrix W

$$\begin{bmatrix} 3*5 + 0*3 - 1*(-2) & 2*5 + (-2)*3 + 2*(-2) \\ 3*1 + 0*2 - 1*4 & 2*1 + (-2)*2 + 2*4 \\ 5*1 - 5*2 + 0*4 & 5*1 - 5*2 + 0*4 \end{bmatrix} \leftarrow \begin{array}{l} \text{Comp. 1} \\ \text{Comp. 2} \\ \text{Comp. 3} \end{array}$$

ICA activity U



Historical Remarks

- Herault & Jutten ("Space or time adaptive signal processing by neural network models", *Neural Nets for Computing Meeting*, Snowbird, Utah, 1986): **Seminal paper, neural network**
- Bell & Sejnowski (1995): Information Maximization
- Amari et al. (1996): Natural Gradient Learning
- Cardoso (1996): JADE
- **Applications of ICA to biomedical signals**
 - EEG/ERP analysis (Makeig, Bell, Jung & Sejnowski, 1996).
 - fMRI analysis (McKeown et al. 1998)



ICA Theory – Cost Functions

Family of BSS algorithms

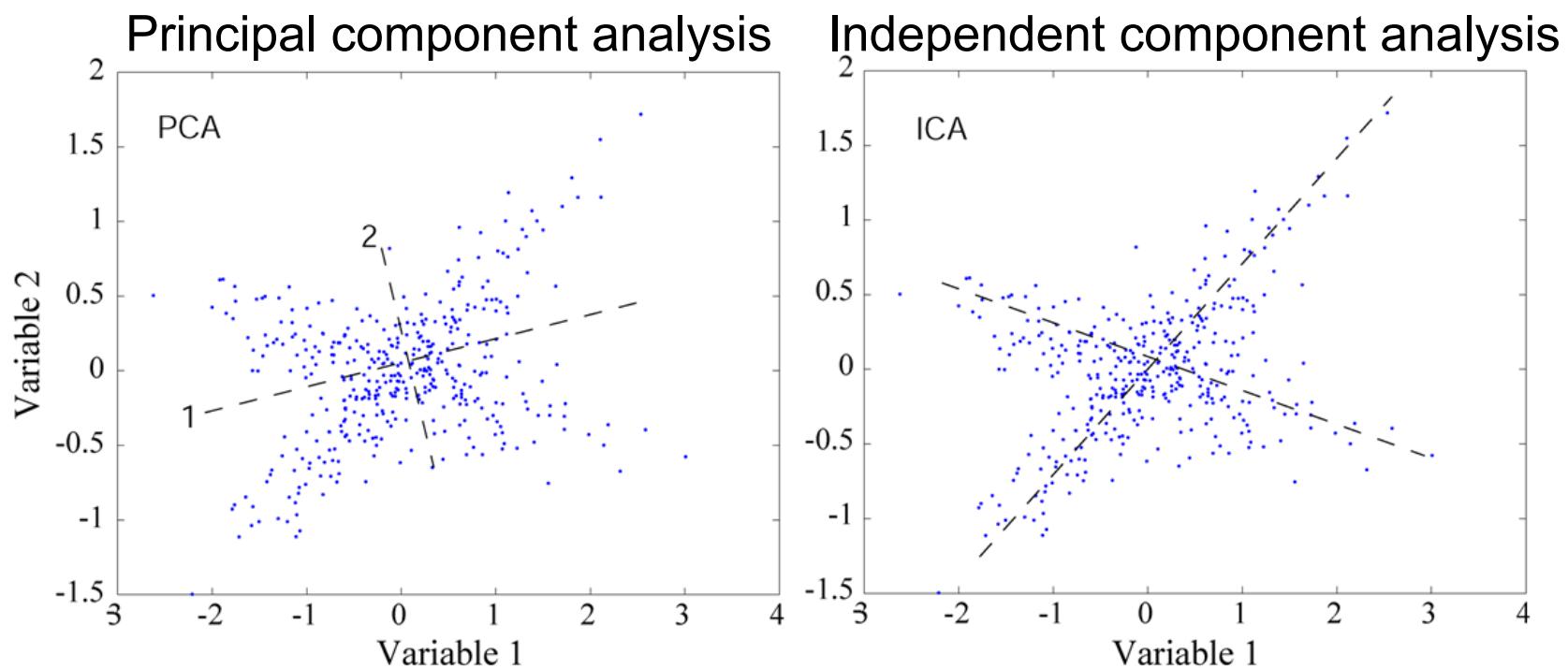
- Information theory (Infomax)
- Bayesian probability theory (Maximum likelihood estimation)
- Negentropy maximization
- Nonlinear PCA
- Statistical signal processing (cumulant maximization, JADE)

A unifying Information-theoretic framework for ICA

- Pearlmutter & Parra showed that InfoMax, ML estimation are equivalent.
- Lee et al. (1999) showed negentropy has the equivalent property to InfoMax.
- Girolami & Fyfe showed nonlinear PCA can be viewed from information-theoretic principle.

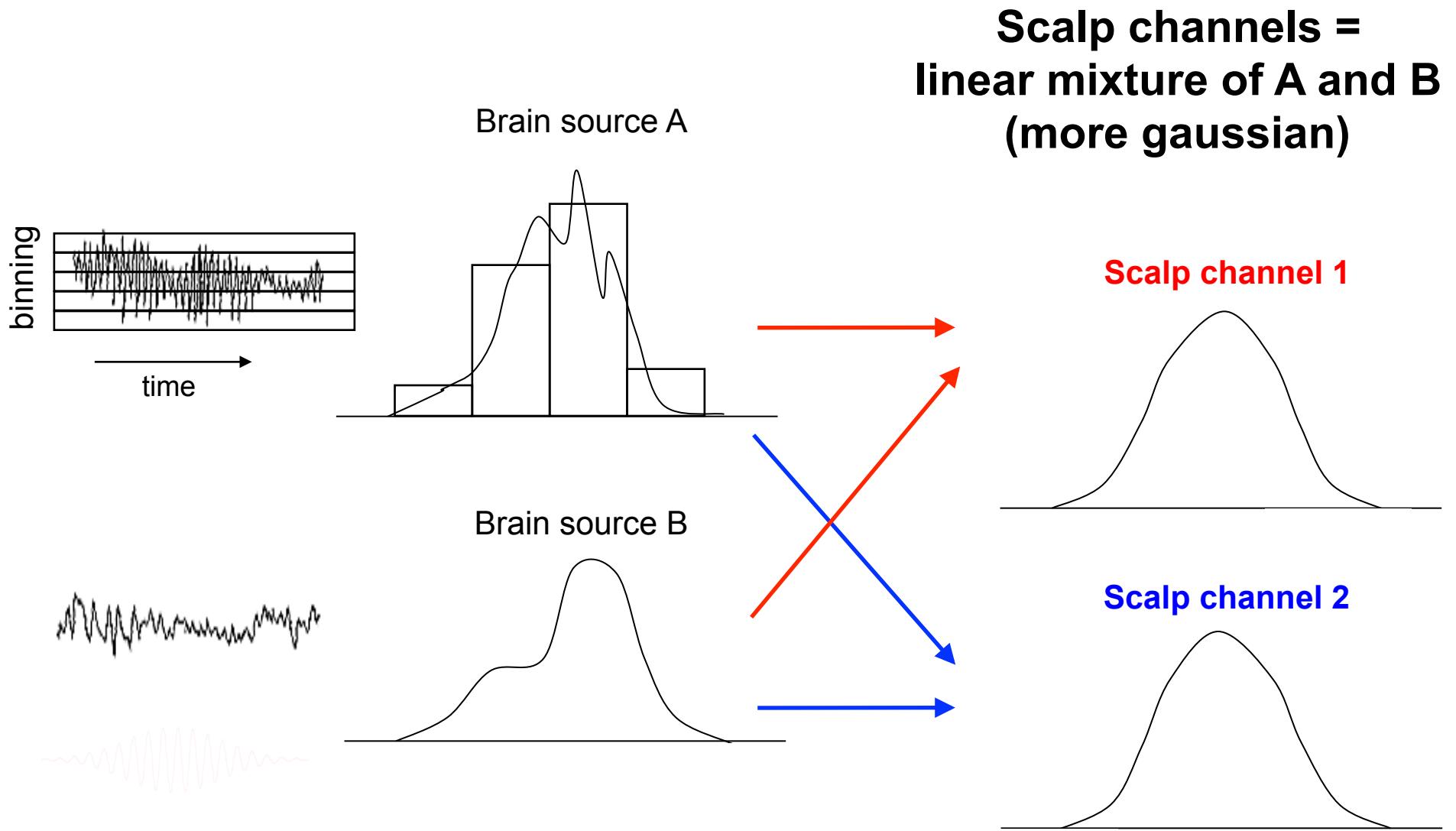
ICA and PCA

ICA is a method to recover a version, of the original sources by multiplying the data by a unmixing matrix,



While PCA simply decorrelates the outputs (using an orthogonal mixing matrix), ICA attempts to make the outputs **statistically independent**, while placing no constraints on the mixing matrix.

Central limit theorem

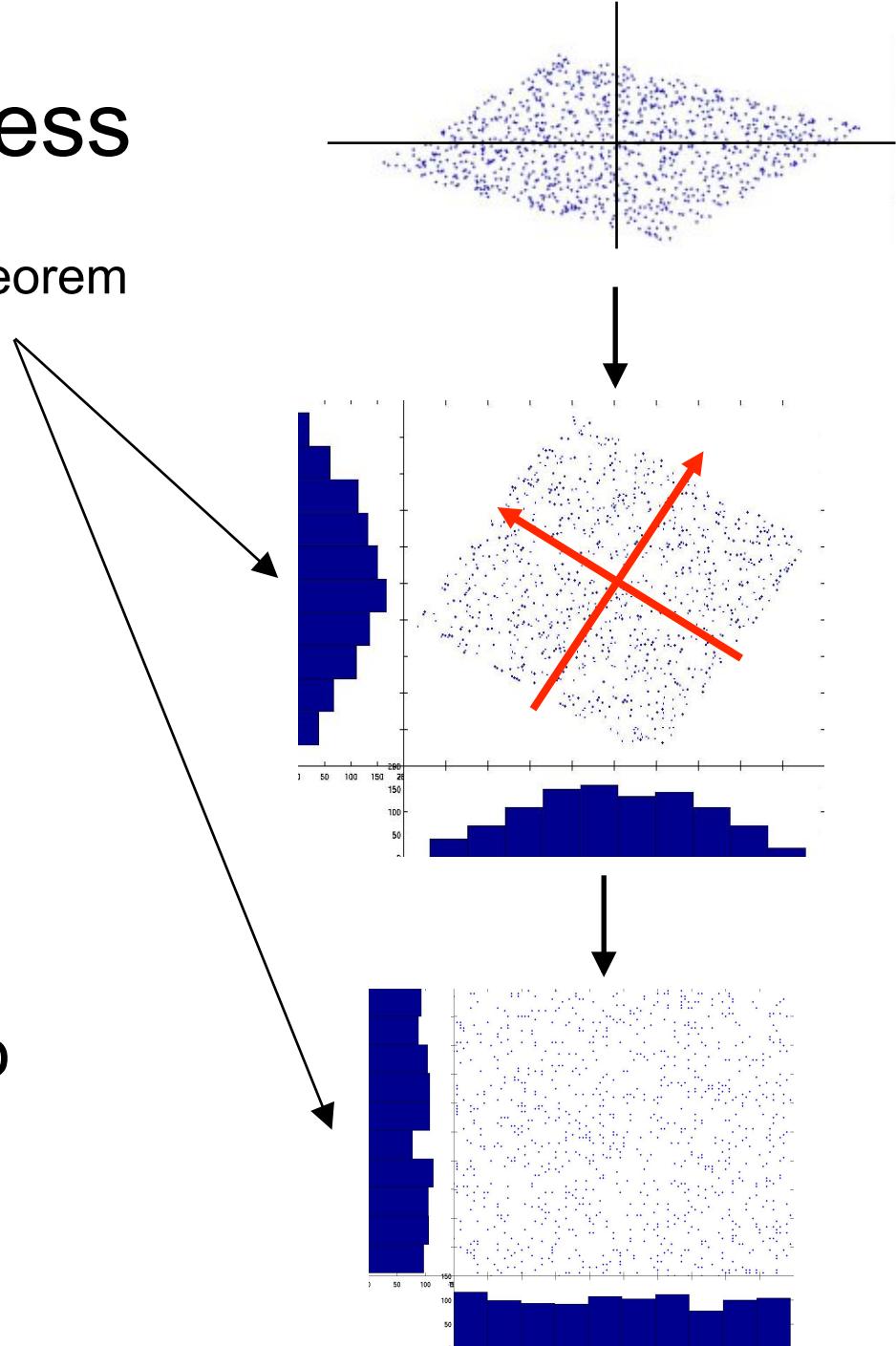


ICA Training Process

Central limit theorem

- Remove the mean
 $x = x - \langle x \rangle$
- ‘Sphere’ the data by diagonalizing its covariance matrix,
 $x = \langle xx^T \rangle^{-1/2} (x - \langle x \rangle)$.
- Update W according to

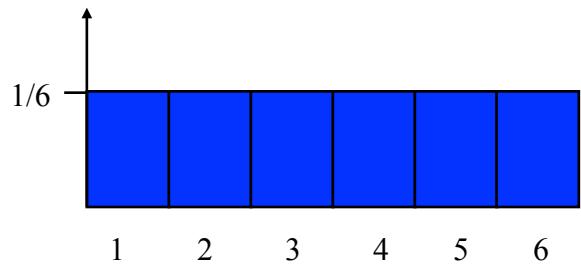
$$\Delta W \propto \frac{\partial H(y)}{\partial W} W^T w$$



Entropy

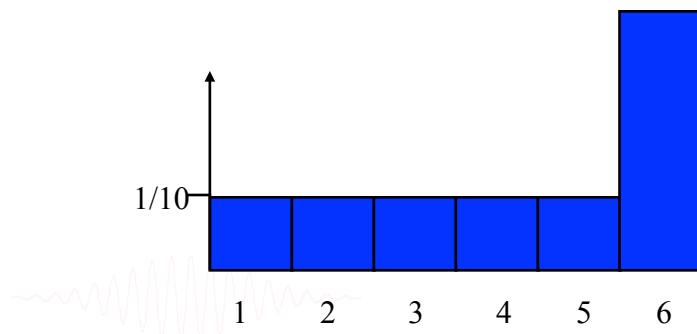
$$H(X) = - \sum_{x \in \mathcal{X}} p(x) \log_b p(x).$$

Dice: 1/6



$$H = 6 \left(-\frac{1}{6} \log_2 \left(\frac{1}{6} \right) \right) = 2.58$$

Fake dice (make a 6 half of the time): entropy 2.16 (base 2)



$$H = 5 \left(-\frac{1}{10} \log_2 \left(\frac{1}{10} \right) \right) - \frac{1}{2} \log_2 \left(\frac{1}{2} \right) = 2.16$$

Entropy

$$H(X) = - \sum_{x \in \mathcal{X}} p(x) \log_b p(x)$$

Joint entropy

$$H(X, Y) = - \sum_{(x, y) \in \mathcal{X} \times \mathcal{Y}} p(x, y) \log_b p(x, y).$$

Mutual Information

$$H(y_1, y_2) = H(y_1) + H(y_2) - I(y_1, y_2).$$



Shannon in his landmark 1948 paper ``A Mathematical Theory of Communication.''

From <http://planetmath.org/encyclopedia/ShannonsTheoremEntropy.html>

Contingency table for stress and emotionality

		STRE						
		1	2	3	4	5	6	Total
EMOT =	1	19	4					23
	2	11	63	64	3	1		142
	3	2	16	18	20	2	2	60
	4	1	4	1	9	6	2	23
	5			1	2	4	3	10
	6				1	1	1	3
Total		33	87	84	35	13	8	



From <http://tecfa.unige.ch/~lemay/thesis/THX-Doctorat/node149.html>

Contingency frequencies for stress and emotionality

	STRE					
	1	2	3	4	5	6
EMOT= 1	0.07	0.02				
2	0.04	0.24	0.25	0.01		
3	0.01	0.06	0.07	0.08	0.01	0.01
4		0.02		0.03	0.02	0.01
5				0.01	0.02	0.01
6						

Joint entropy 3.46; exercise: compute mutual information



$$H(X, Y) = - \sum_{(x,y) \in \mathcal{X} \times \mathcal{Y}} p(x, y) \log_b p(x, y)$$

ICA learning rule

How to make the outputs statistical independent?

Minimize their redundancy or mutual information.

Consider the joint entropy of two components,

$$H(y_1, y_2) = H(y_1) + H(y_2) - I(y_1, y_2).$$

Maximizing $H(y_1, y_2) \Rightarrow$ minimizing $I(y_1, y_2)$.



The learning rule:

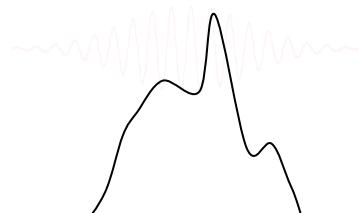


=0 if the two variables
are independent

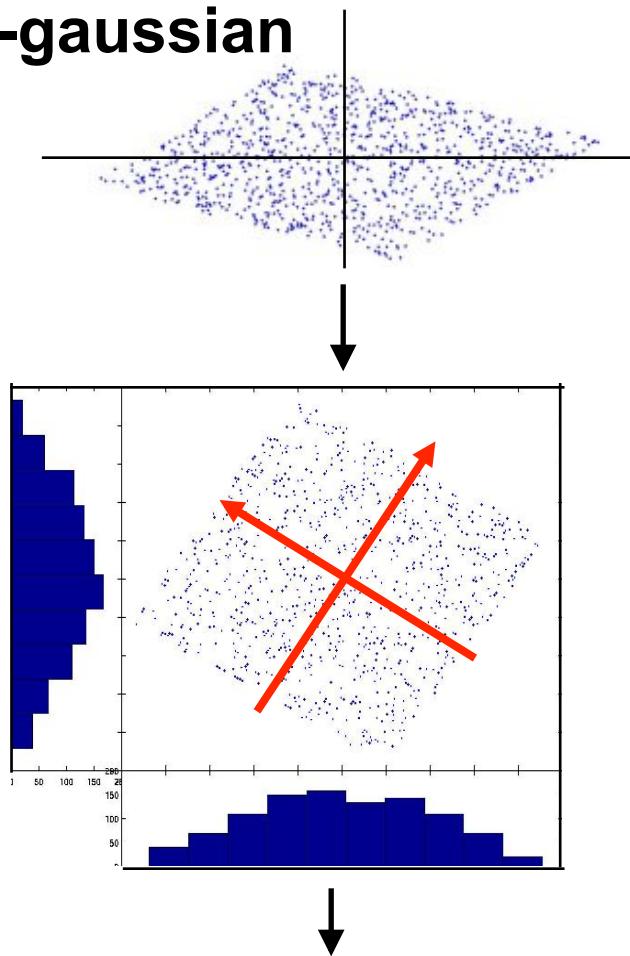
$$\Delta \mathbf{W} \propto \frac{\partial H(\mathbf{y})}{\partial \mathbf{W}} \underbrace{\mathbf{W}^T \mathbf{W}}$$

Entropy
extremum

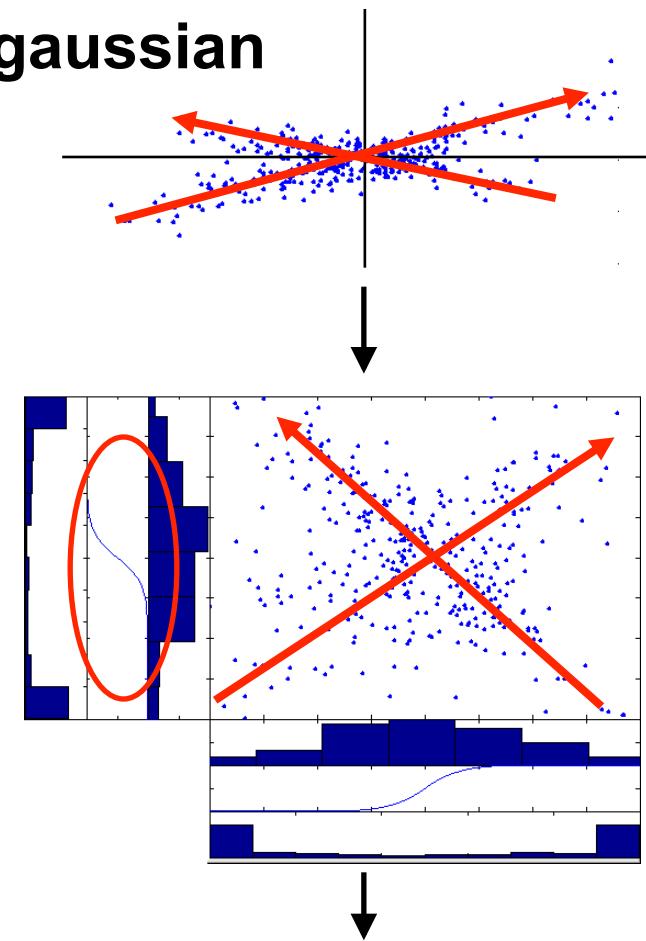
Natural gradient (Amari)



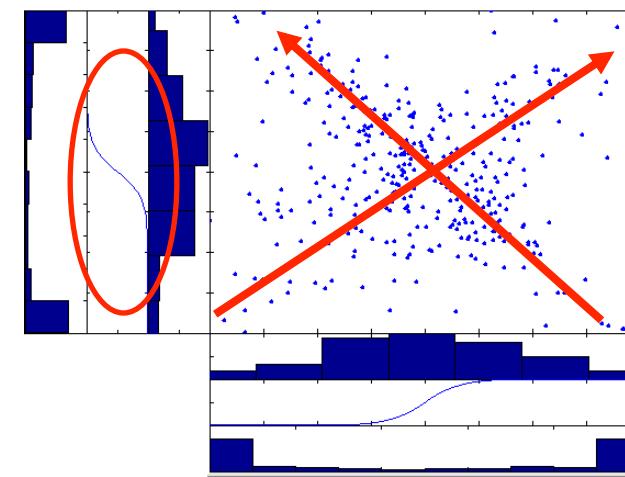
Sub-gaussian



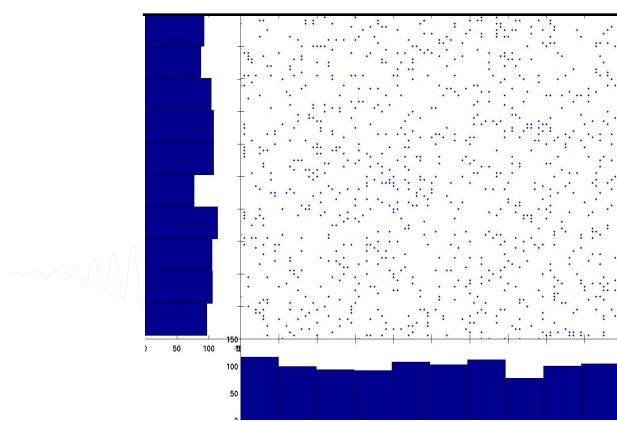
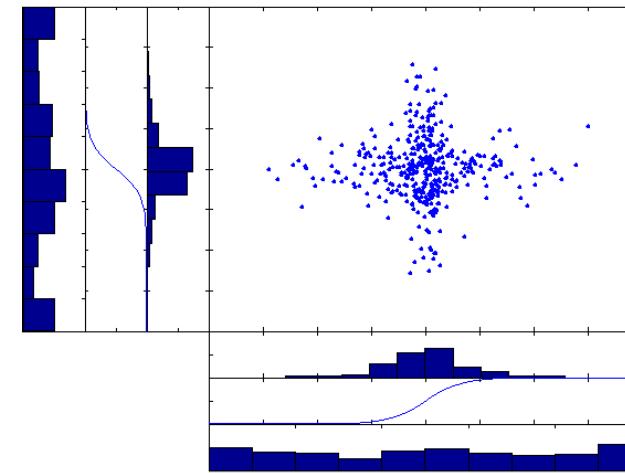
Super-gaussian



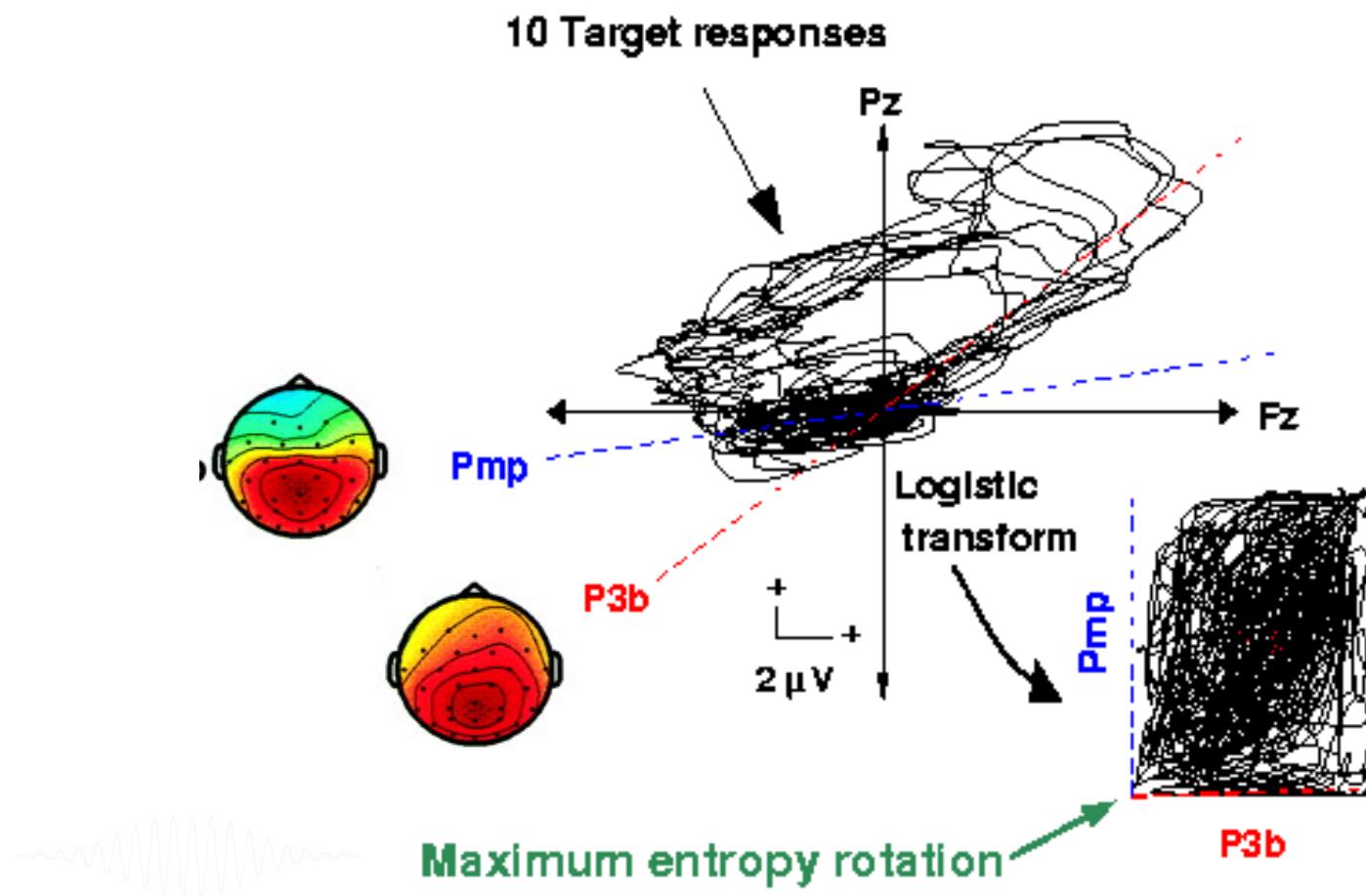
Spherering



ICA

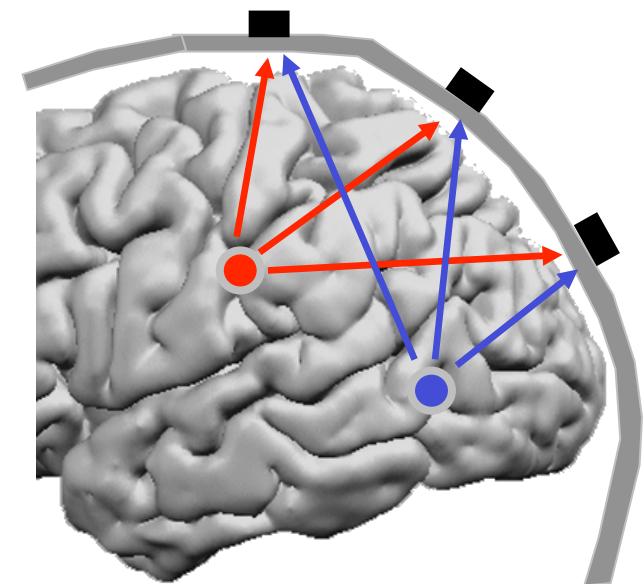
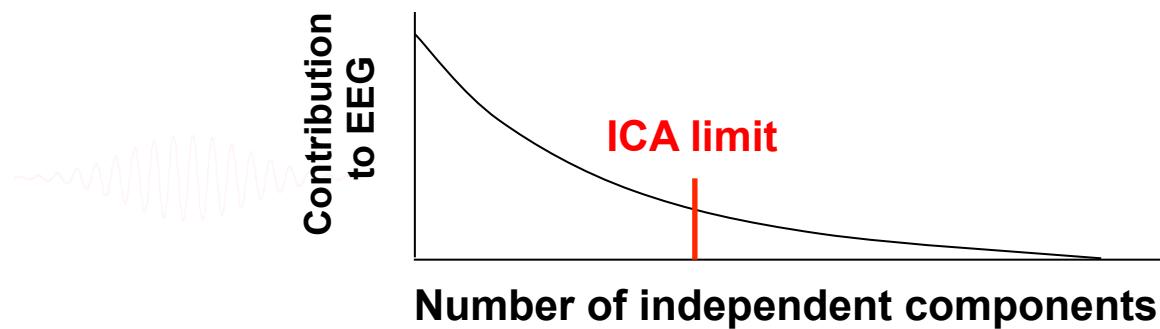


Independent components of EEG/ERP



ICA/EEG Assumptions

- Mixing is linear at electrodes **OK**
- Propagation delays are negligible **OK**
- Component time courses are independent **~**
- Number of components less than the number of channels.



Independent Component Categories

- Artifacts
- Stimulus-locked activity
- Response-locked activity
- Non-phase locked activity
- Event-modulated oscillatory activity

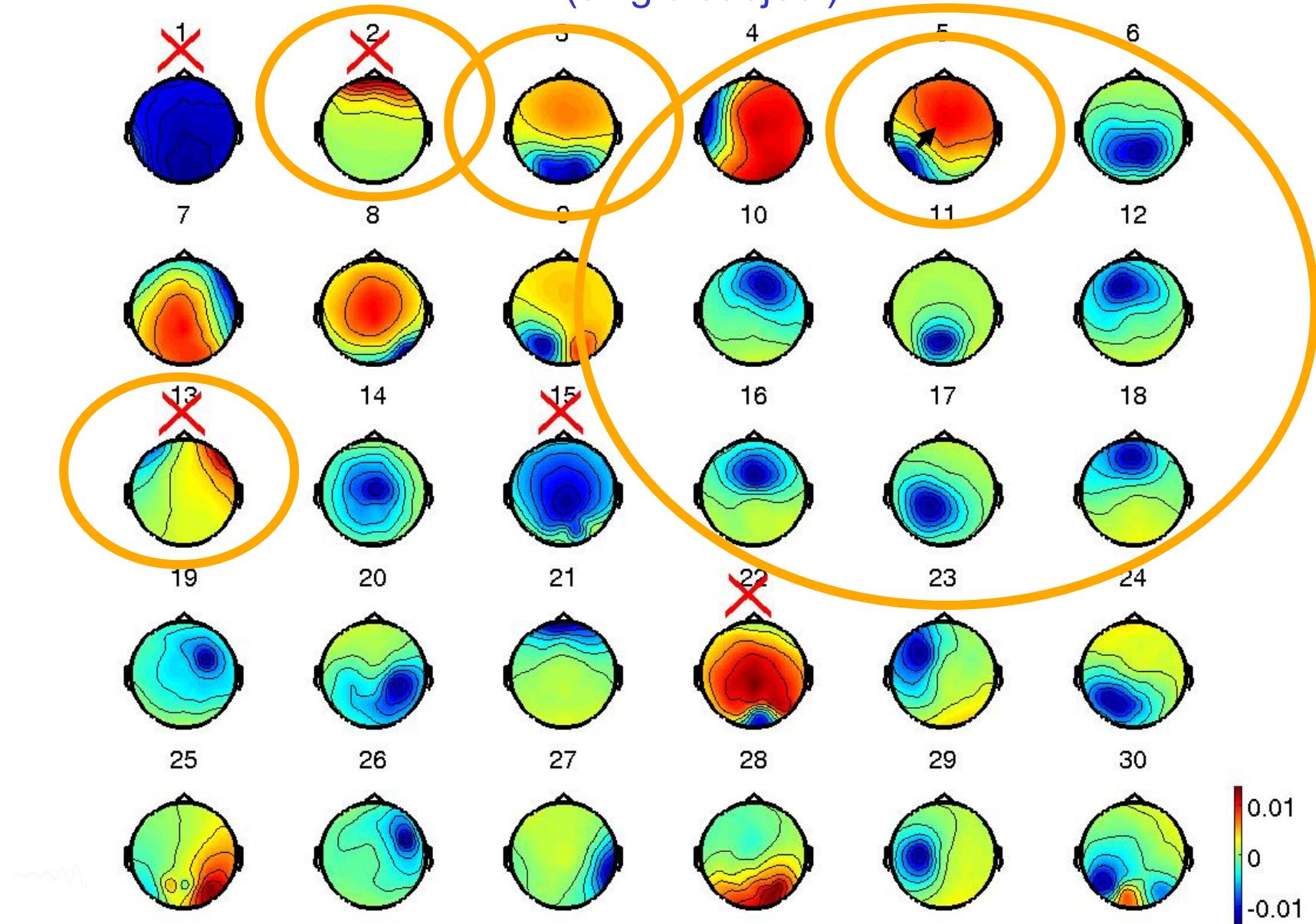


Characteristics of Independent Component of the EEG

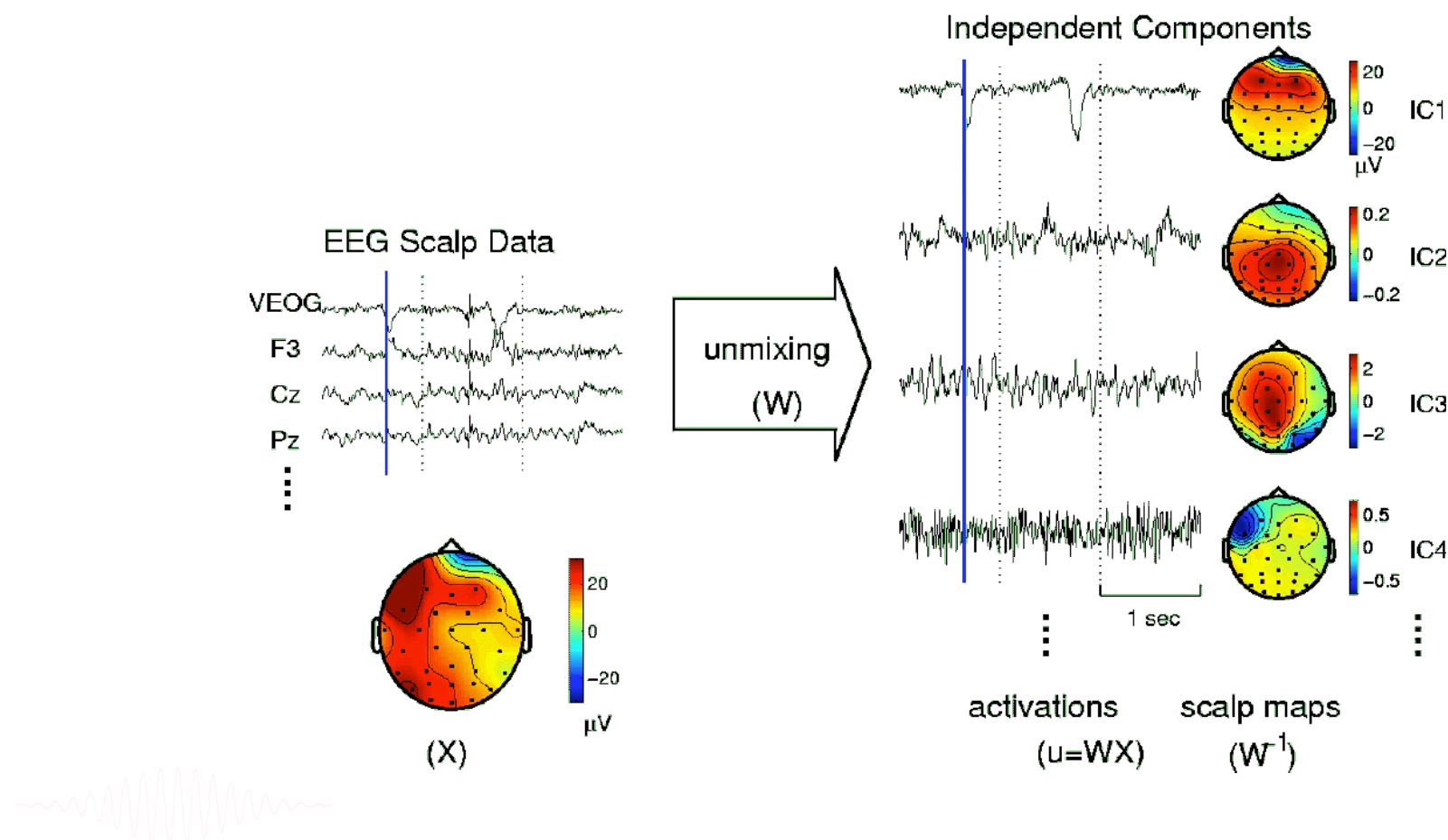
- Concurrent Activity
- Maximally Temporally Independent
- Overlapping Maps and Spectra
- Dipolar Scalp Maps
- Functionally Independent
- Between-Subject Regularity



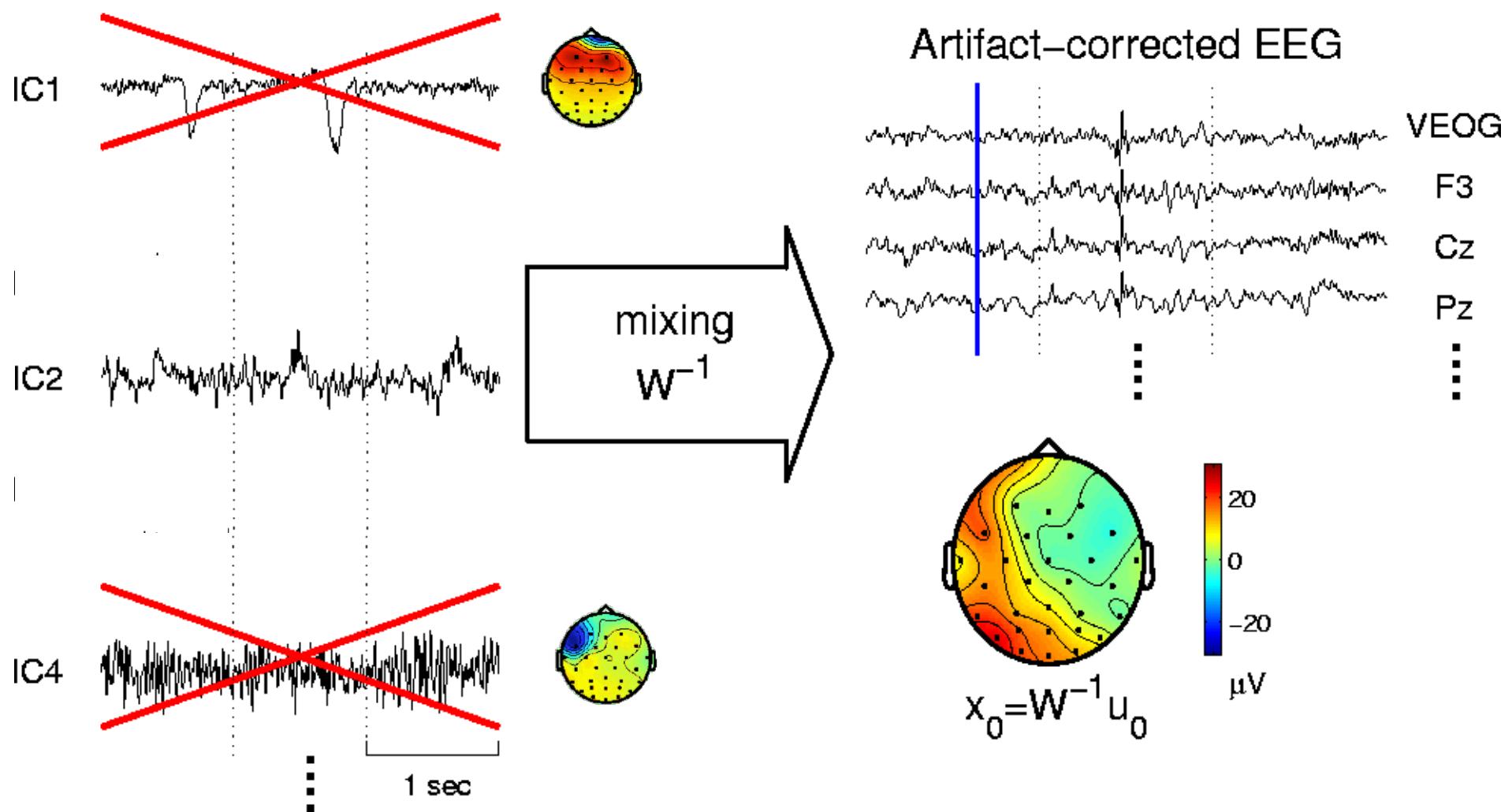
Largest 30 Independent Components (single subject)



ICA Decomposition into Independent Components



Selective Projection onto Scalp Channels



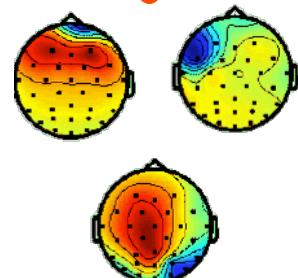
$$\mathbf{X} = \mathbf{W}^{-1} \mathbf{U}$$

Data

$$\begin{bmatrix} 5 \\ 1 \\ 0 \\ \dots \end{bmatrix} \quad \begin{bmatrix} 3 \\ 2 \\ -1 \\ \dots \end{bmatrix} \quad \begin{bmatrix} -2 \\ 4 \\ 3 \\ \dots \end{bmatrix}$$

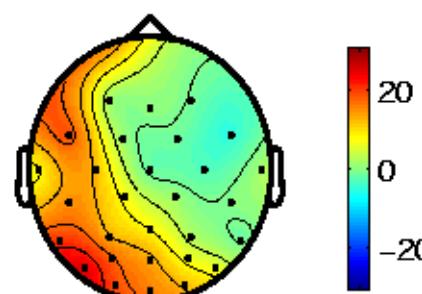
ICA activity \mathbf{U}

$$\begin{bmatrix} 0 & 0 & 0 & 0 & 0 & 0 & \dots \\ 0 & -2 & -5 & -1 & 1 & -1 & \dots \\ 0 & 0 & 0 & 0 & 0 & 0 & \dots \\ \dots & & & & & & \end{bmatrix} \leftarrow \begin{array}{l} \text{Comp. 1} \\ \text{Comp. 2} \\ \text{Comp. 3} \end{array}$$

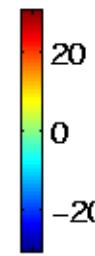


$$\begin{bmatrix} 3*5 + 0*3 - 1*(-2) & 2*5 + (-2)*3 + 2*(-2) & \dots \\ 3*1 + 0*2 - 1*4 & 2*1 + (-2)*2 + 2*4 & \dots \\ 5*1 - 5*2 + 0*4 & 5*1 - 5*2 + 0*4 & \dots \\ \dots & & \end{bmatrix} \leftarrow \begin{array}{l} \text{Chan 1} \\ \text{Chan 2} \\ \text{Chan 3} \end{array}$$

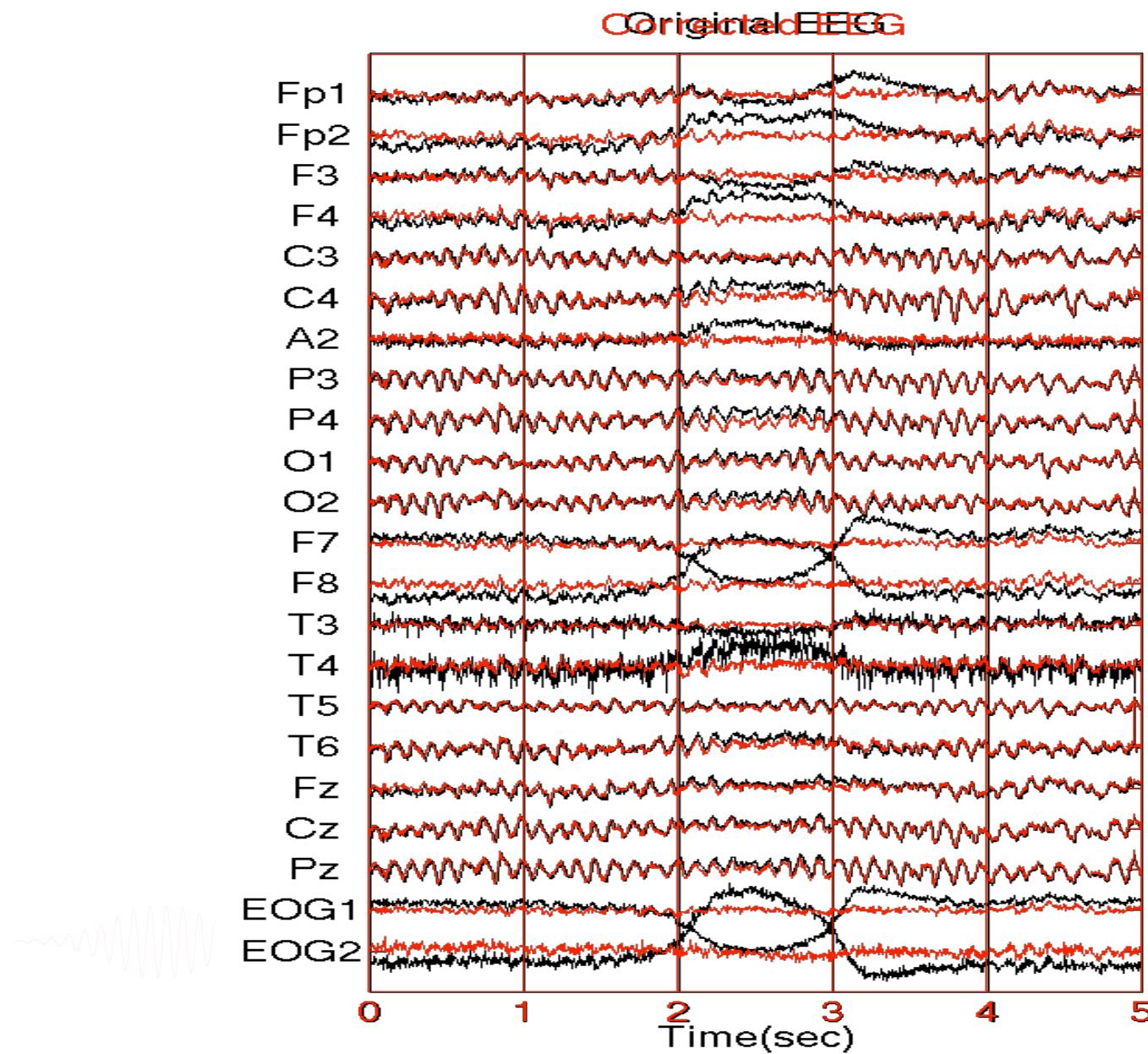
Data \mathbf{X}



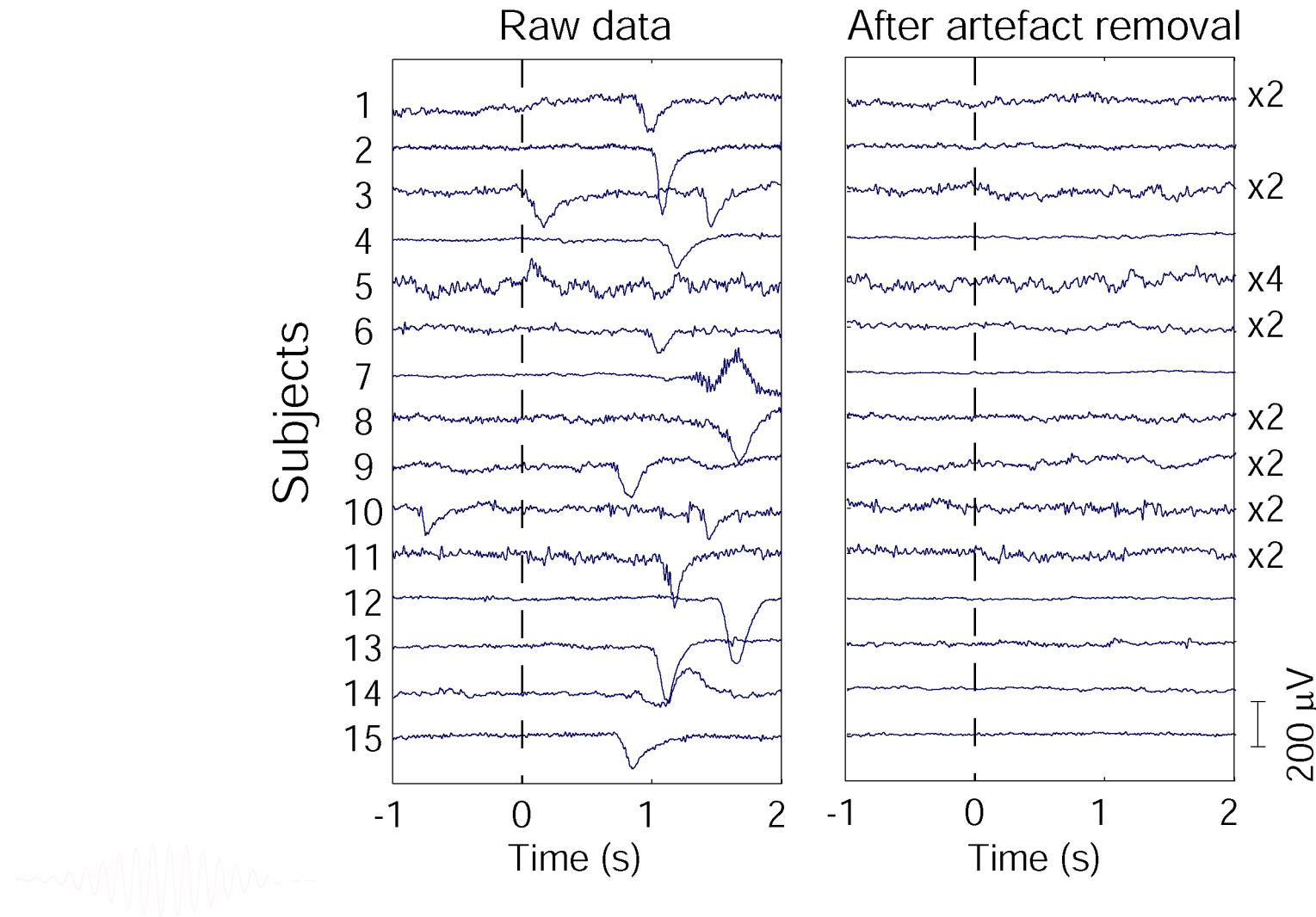
Inverse weight matrix \mathbf{W}^{-1}

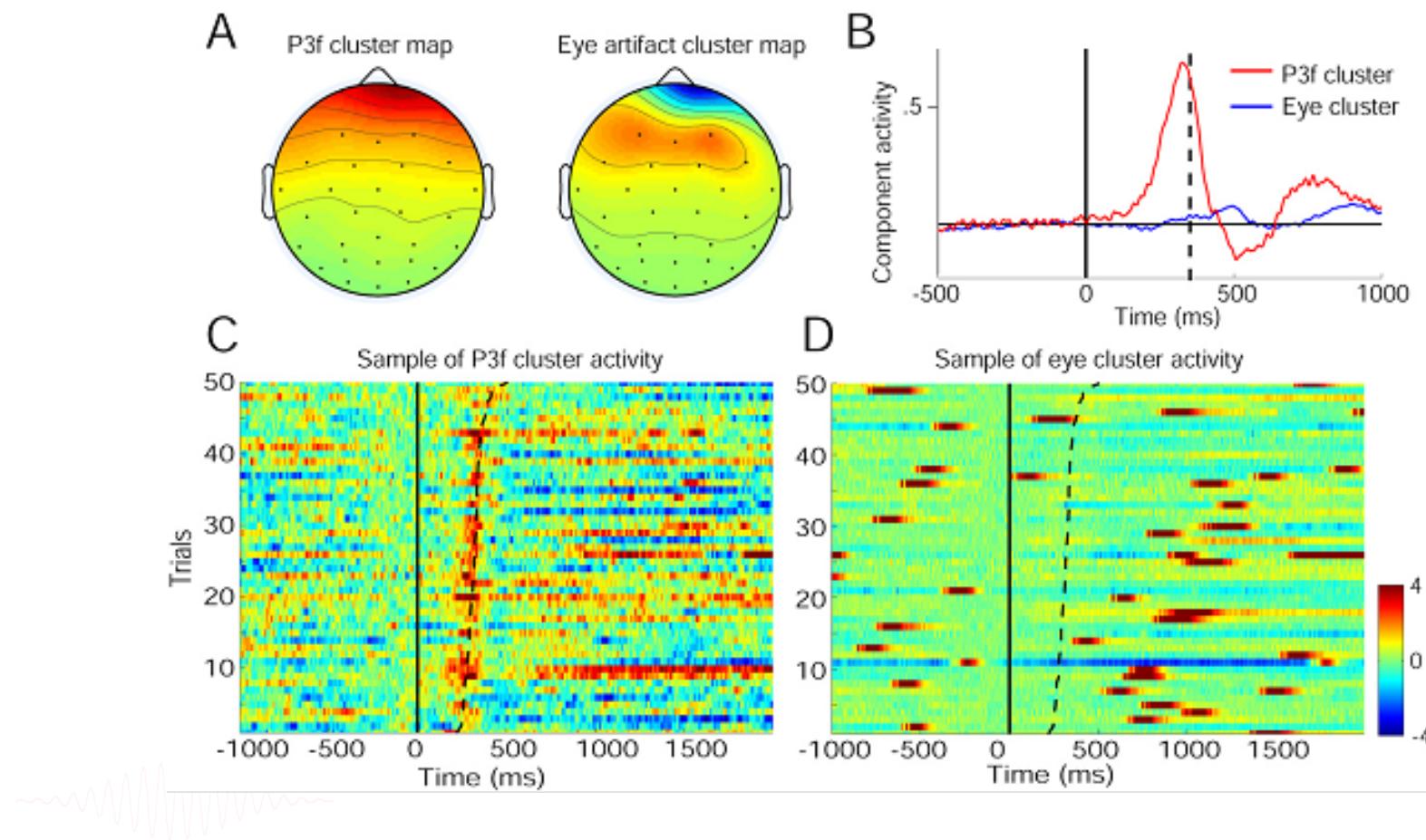


ICA-based Artifact Removal

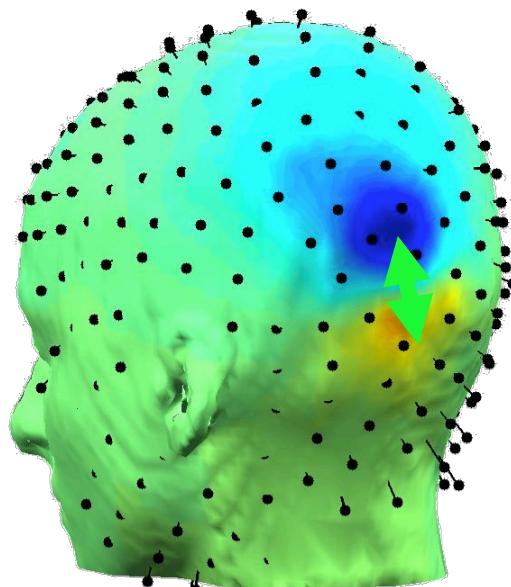


Artifact removal using ICA

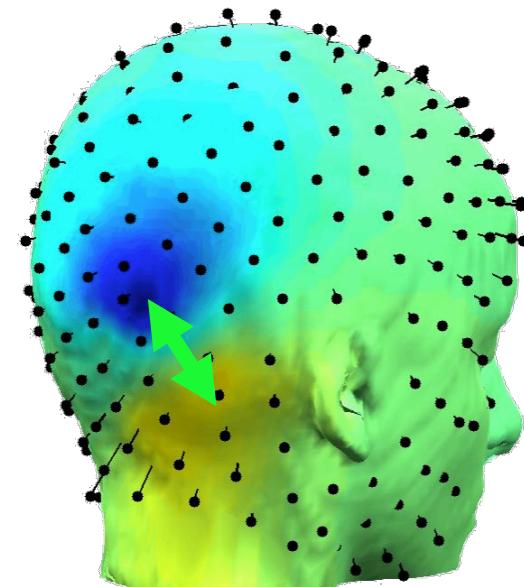




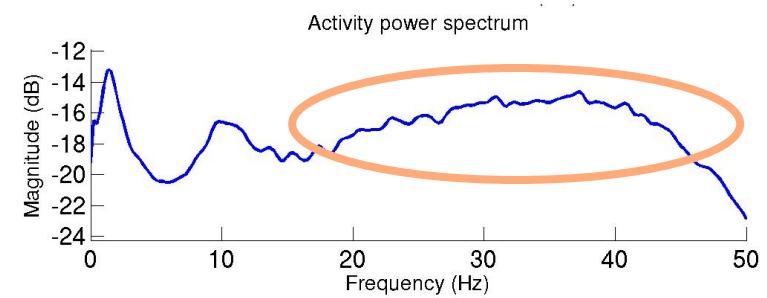
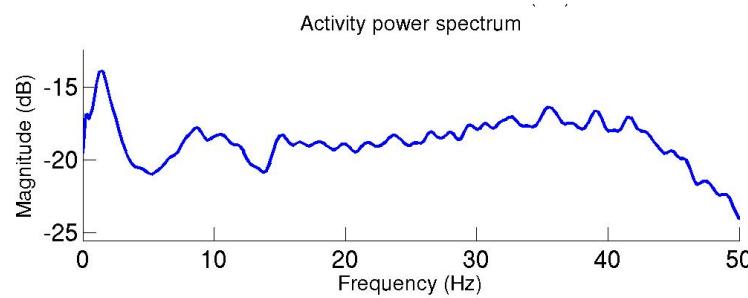
IC39



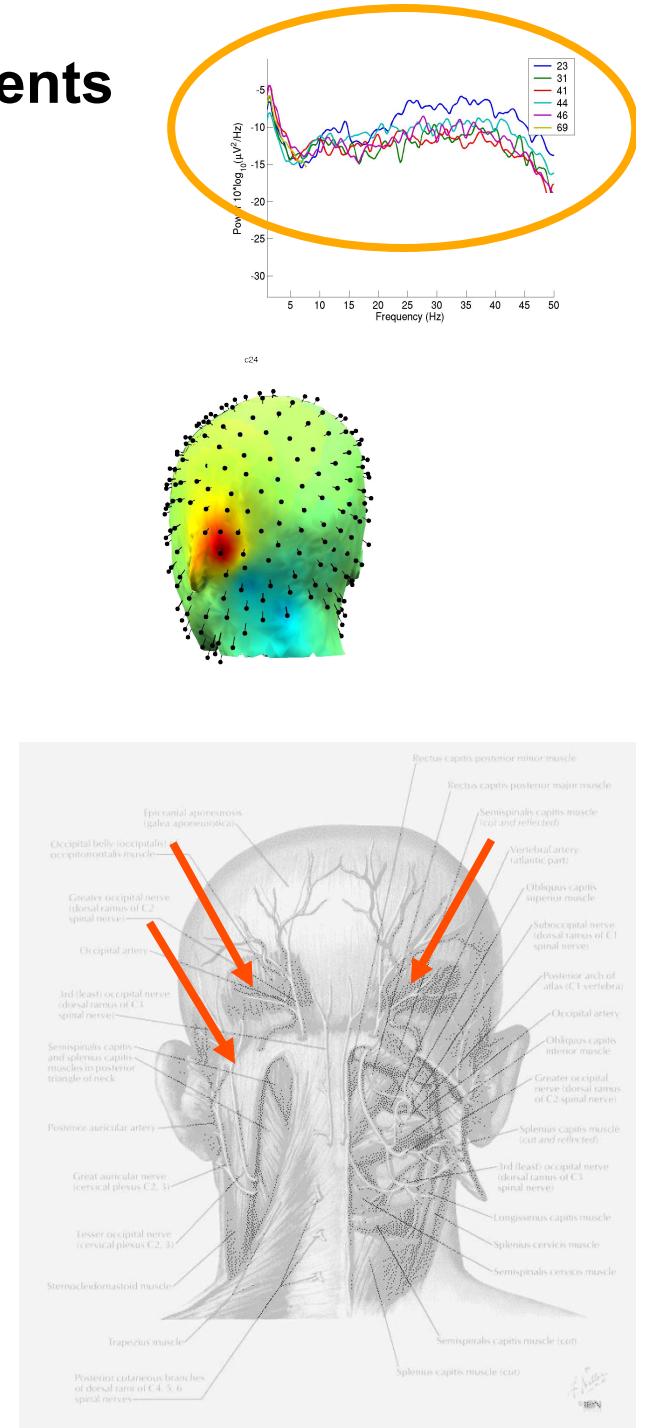
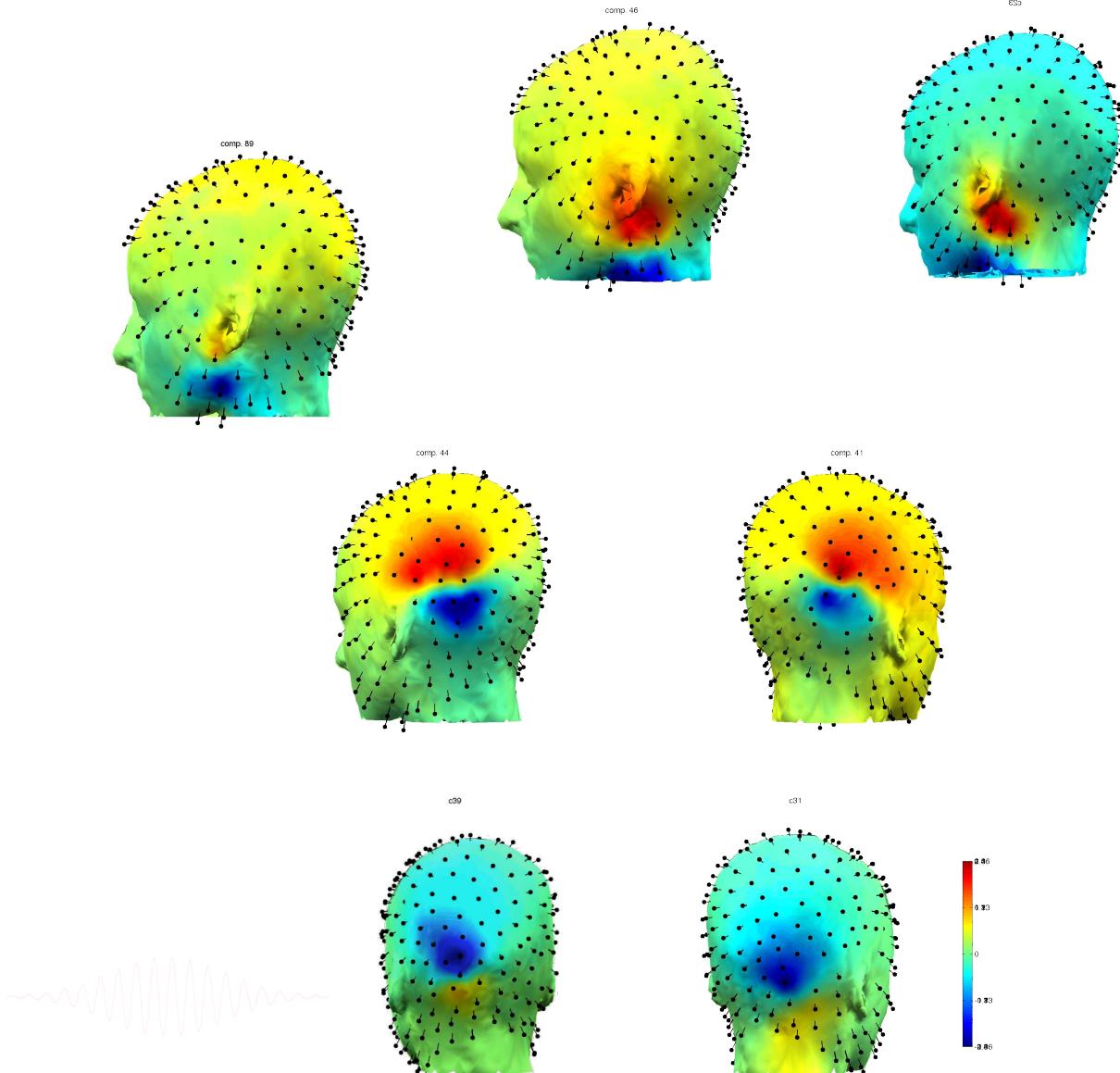
IC31



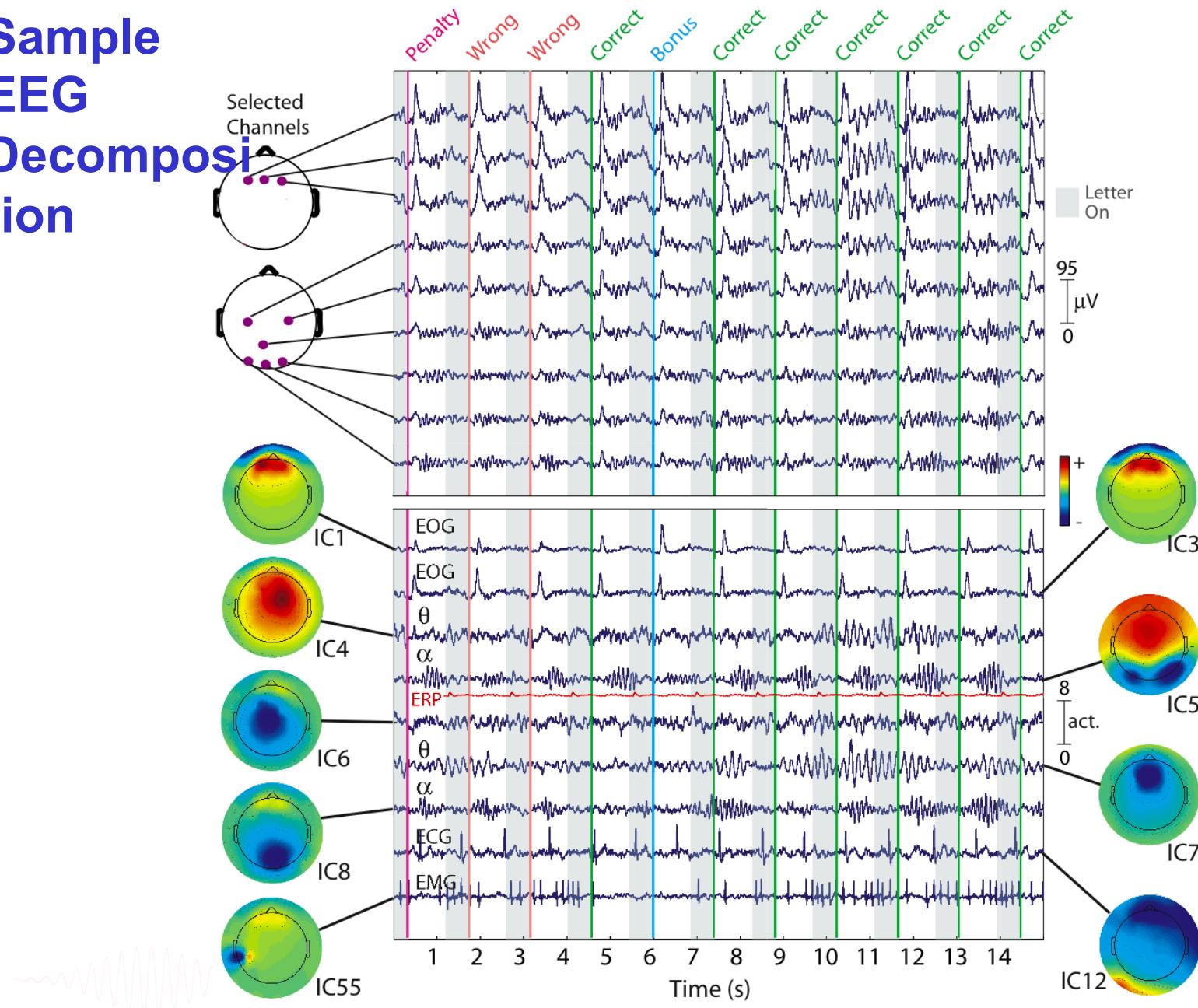
Two Neck Muscle Processes



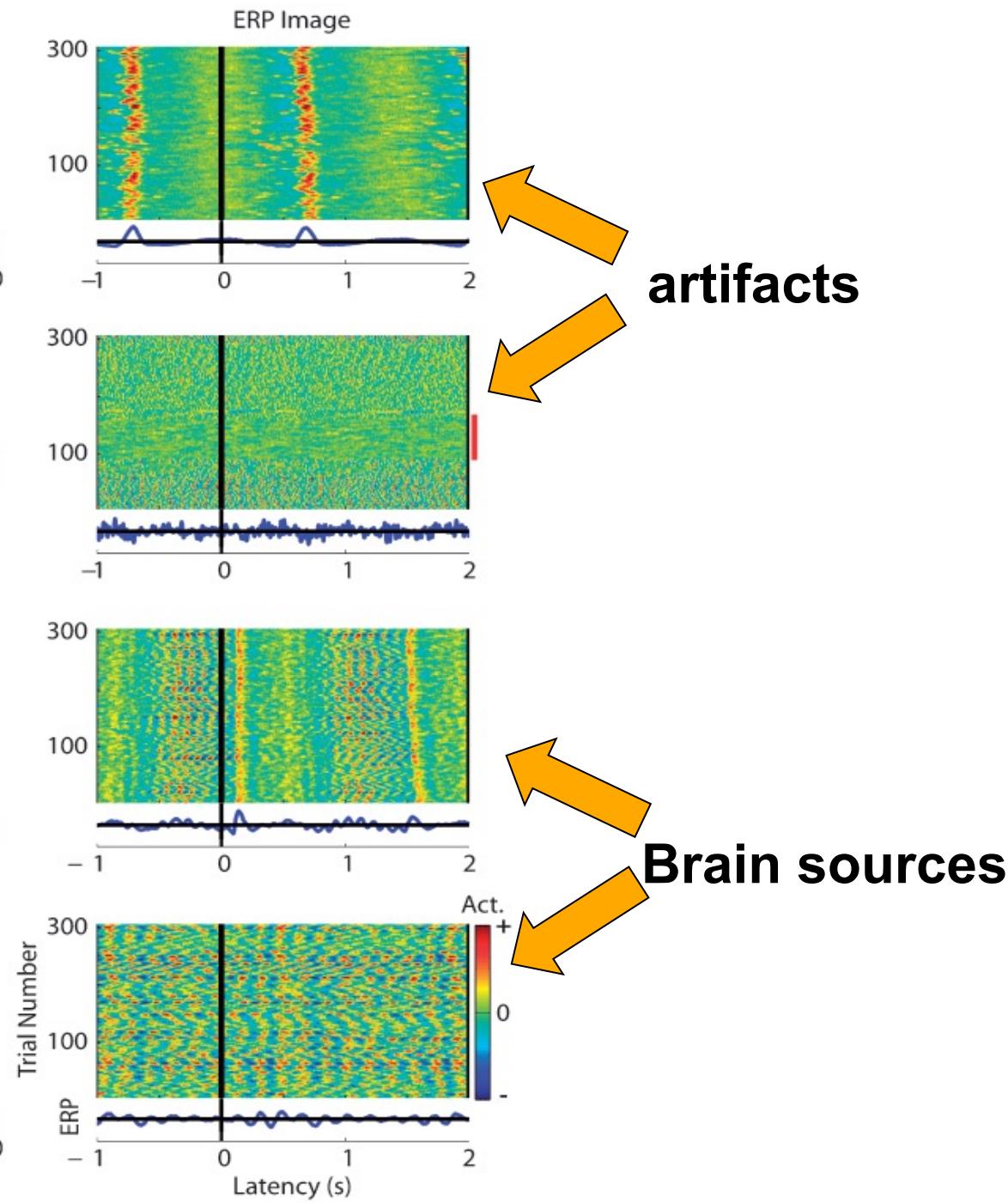
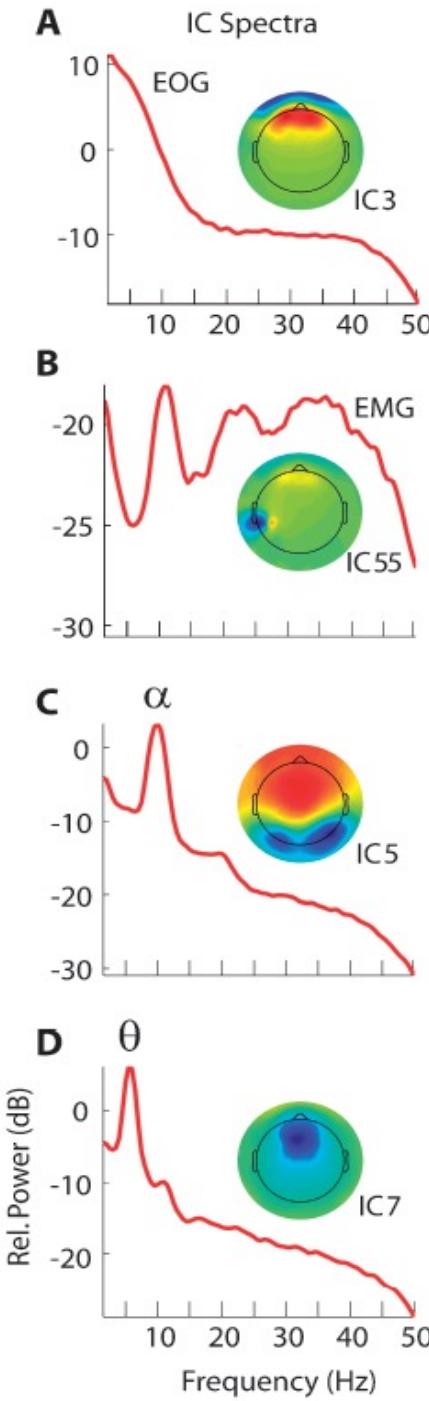
Some Independent EMG Components



Sample EEG Decompositi on

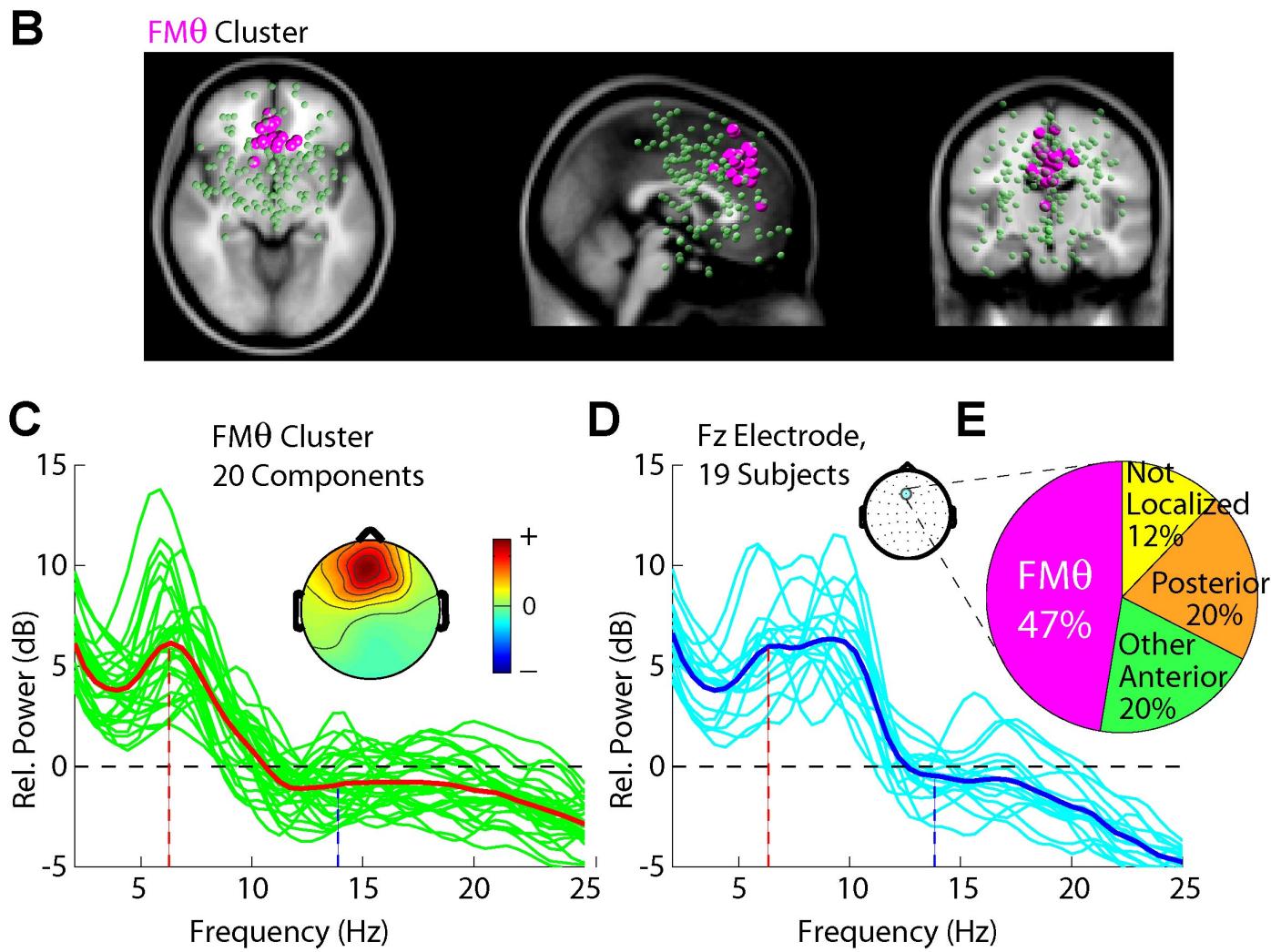


Credit: J. Onton

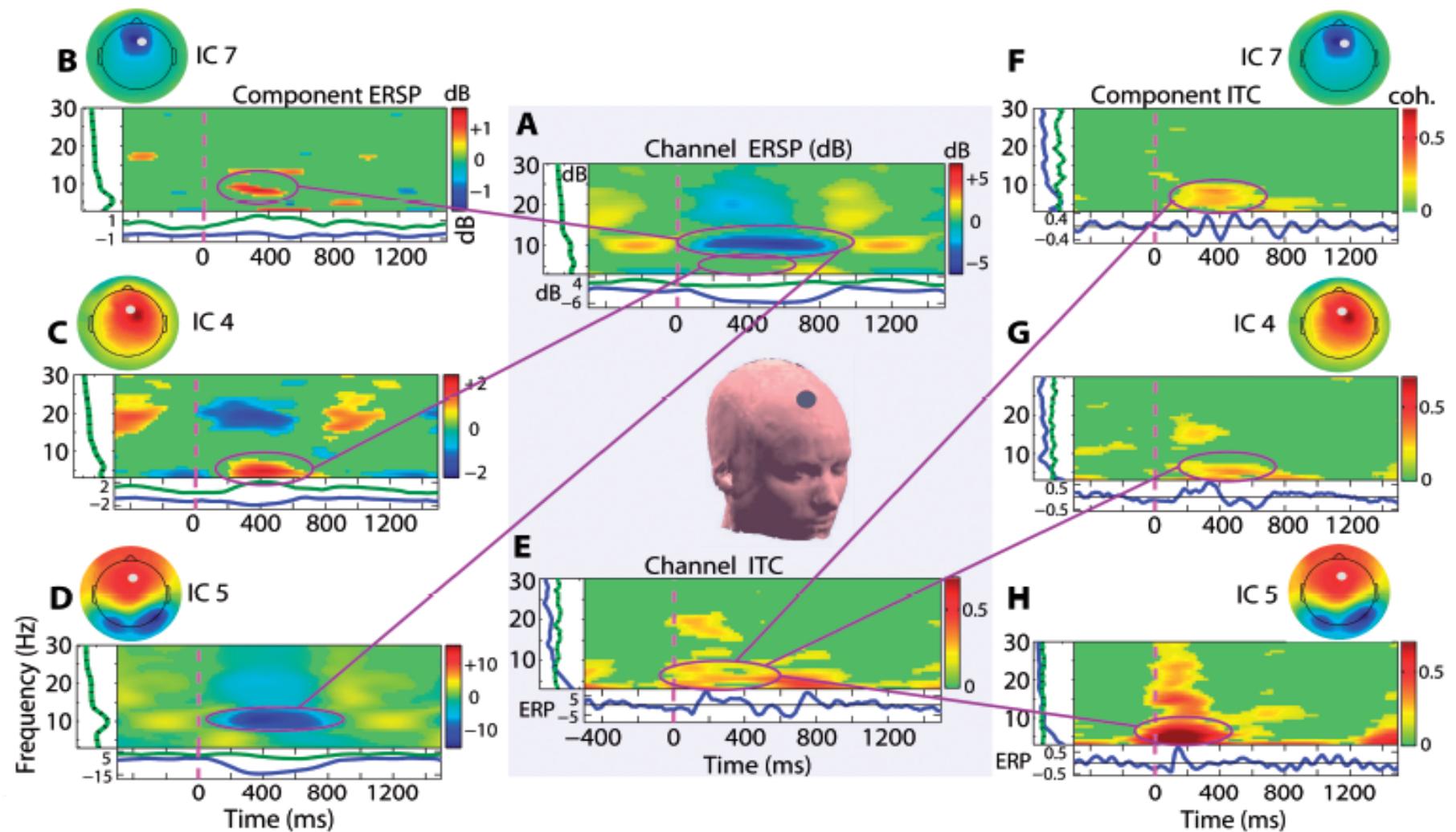


Credit: J. Onton

For example: frontal midline theta cluster

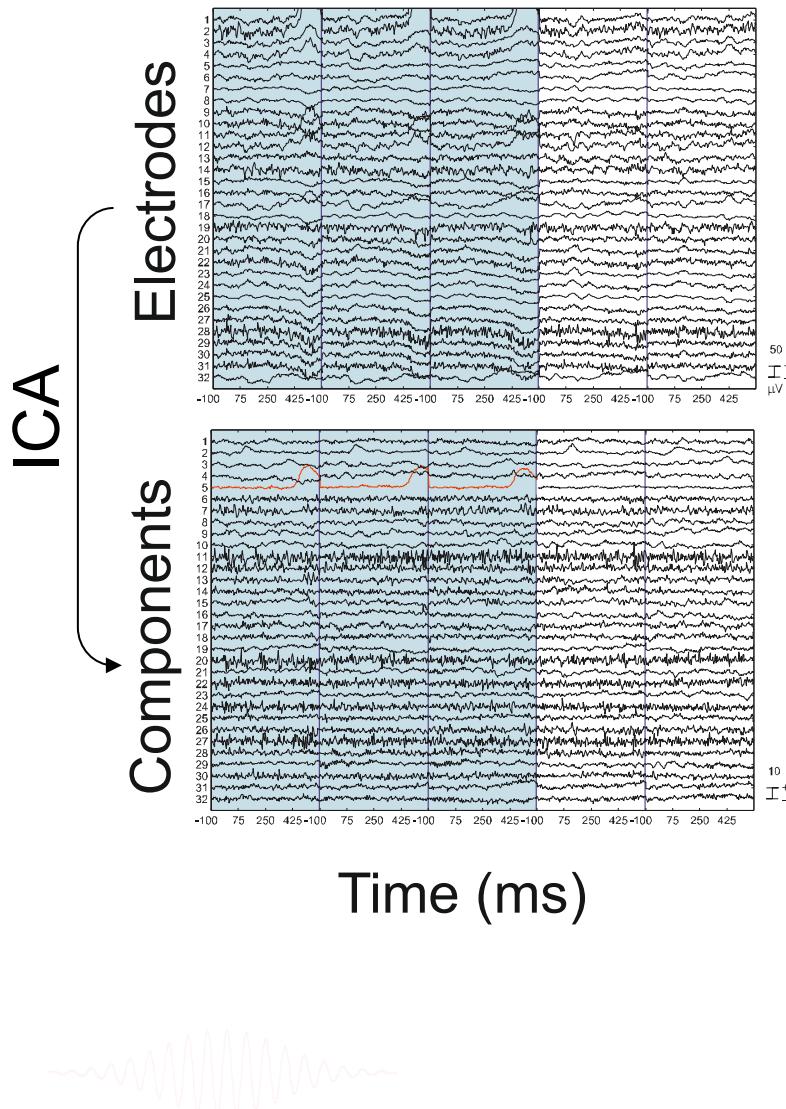


Why analyze source activity instead of channels?

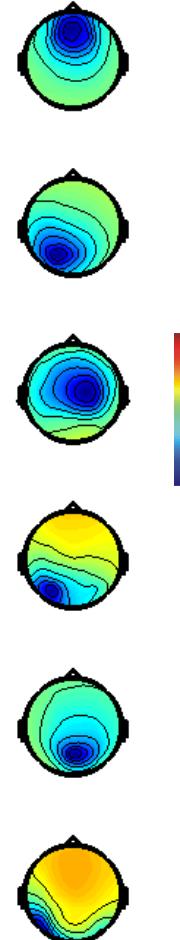


Credit: J. Onton

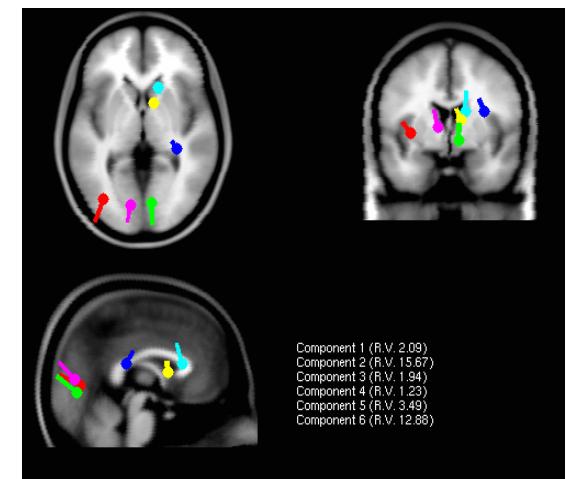
Localization



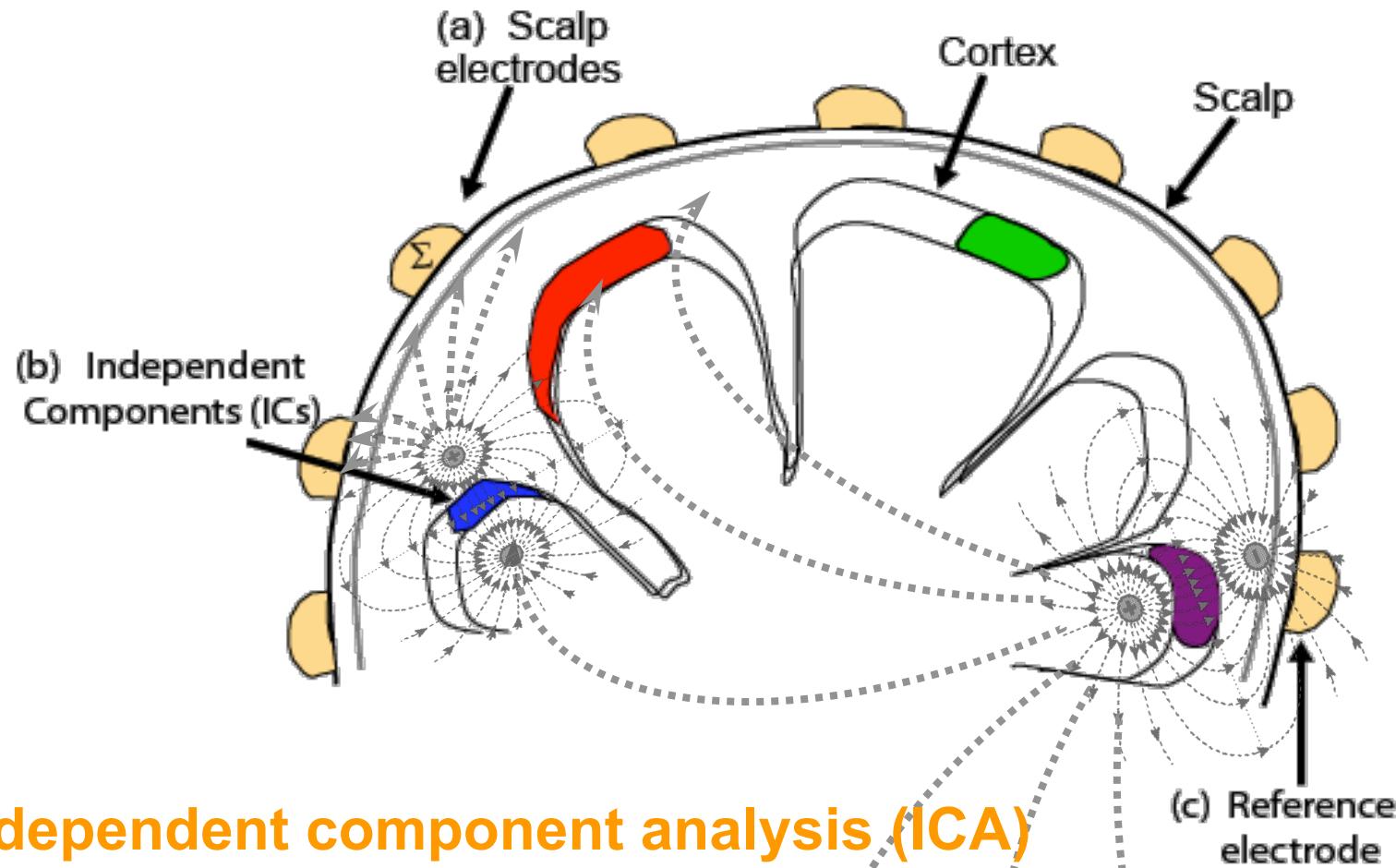
ICA component
scalp maps



Localization

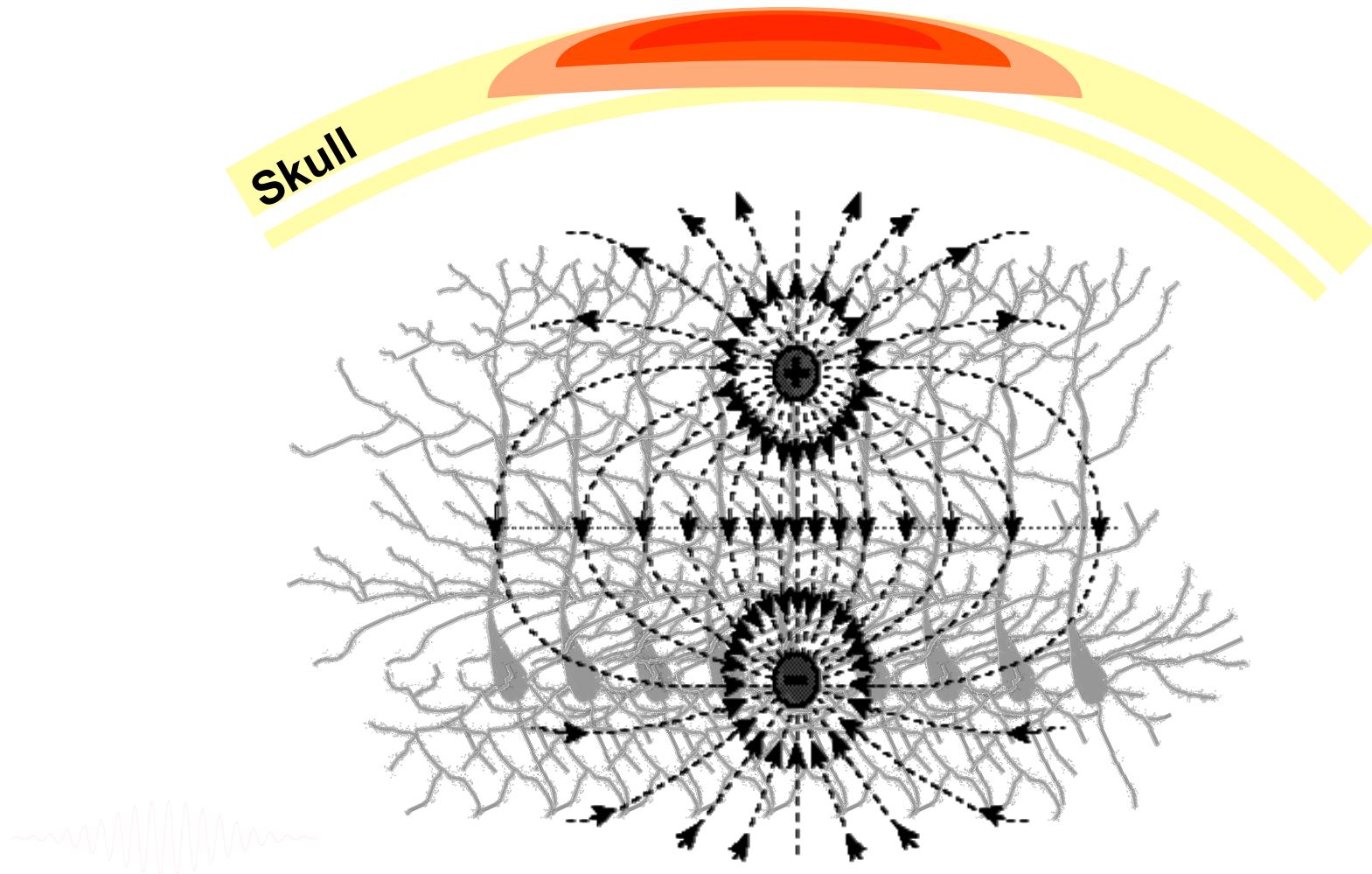


Separating EEG source activities



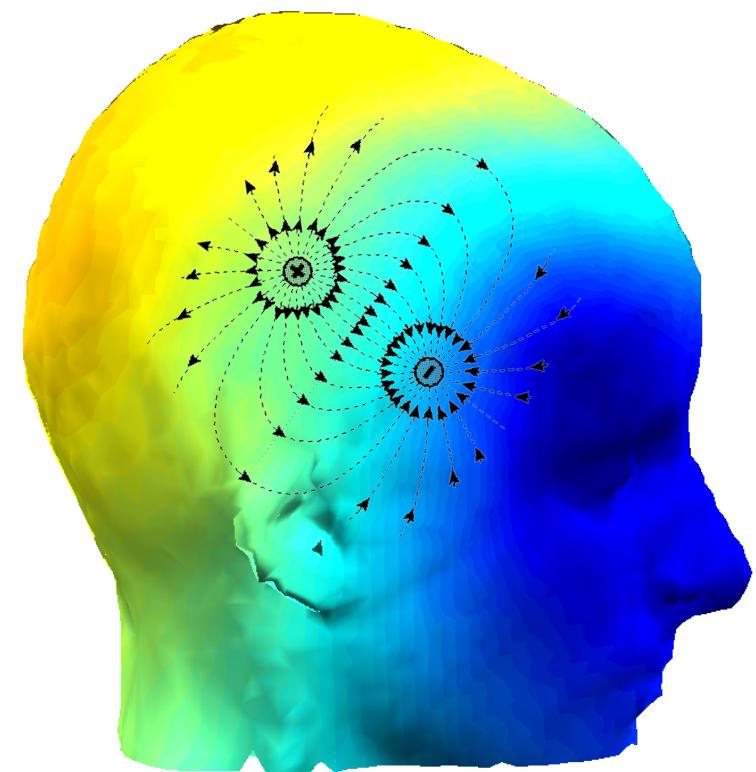
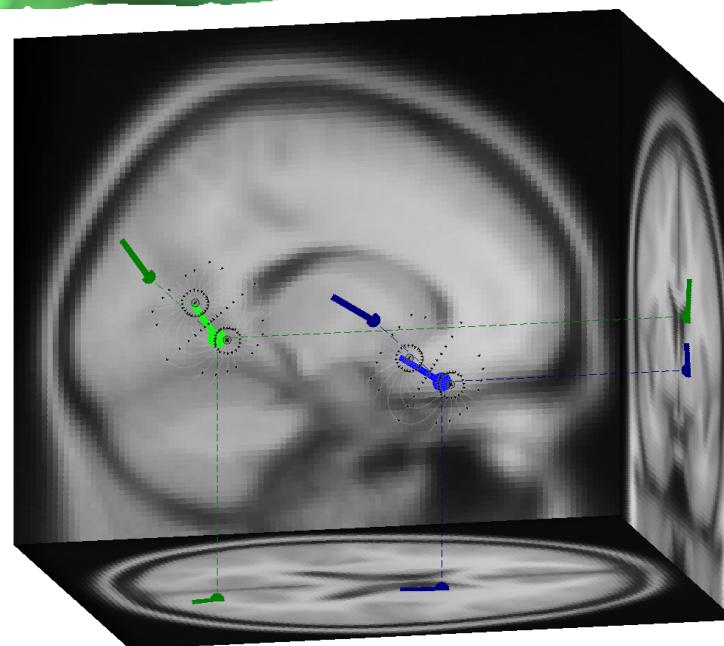
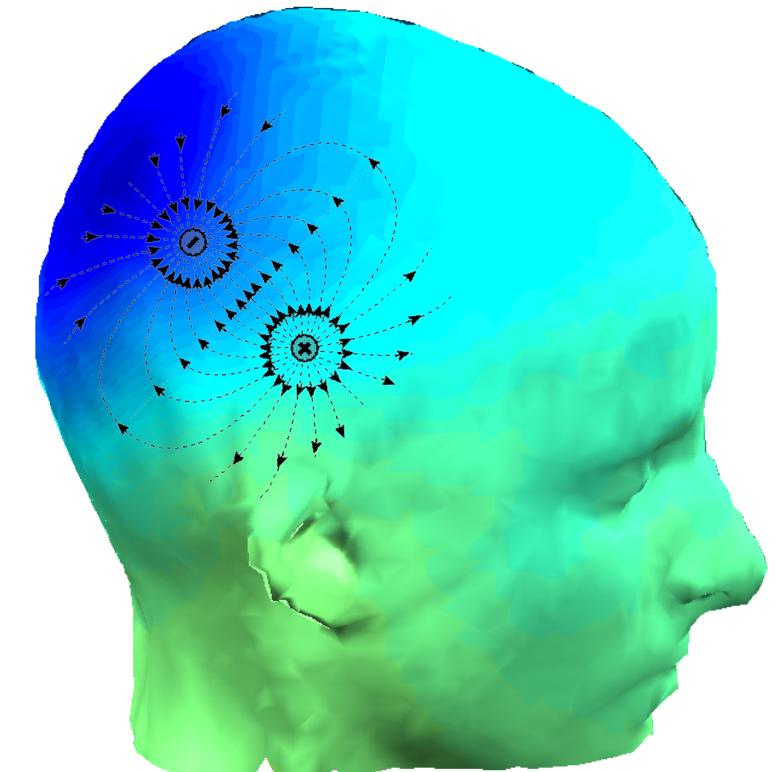
Independent component analysis (ICA)
separates mixed EEG signals at the scalp
into temporally independent time courses

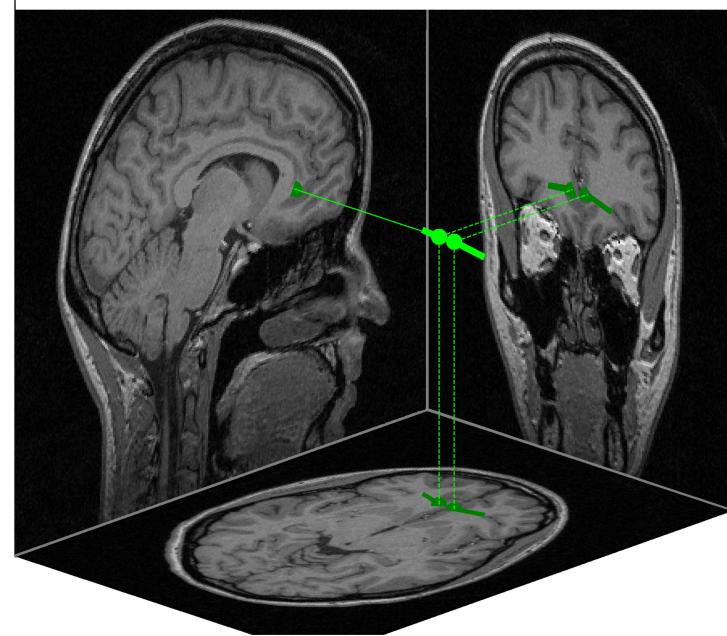
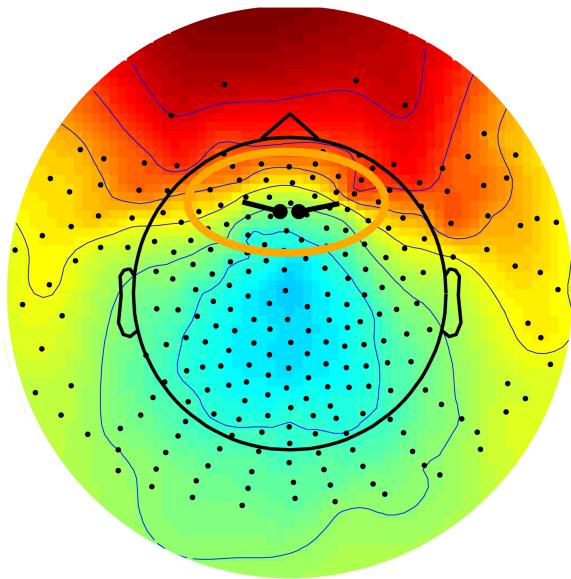
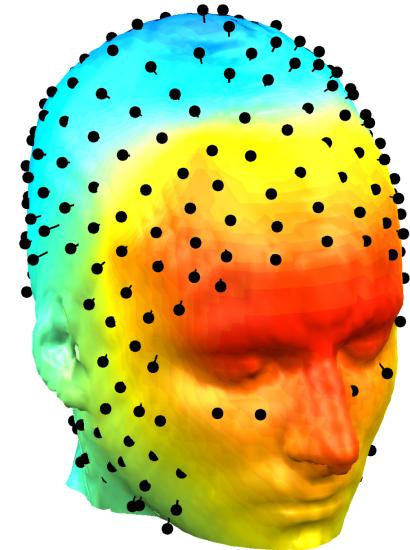
Patch of Cortex Acting as a Dipole



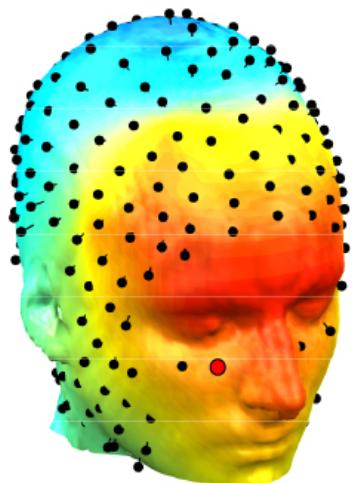
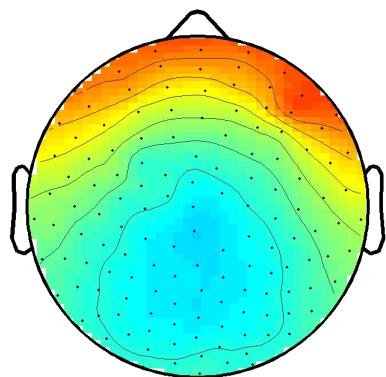
Dipolar Scalp Projections

ICA creates a spatial filter for each temporally independent source

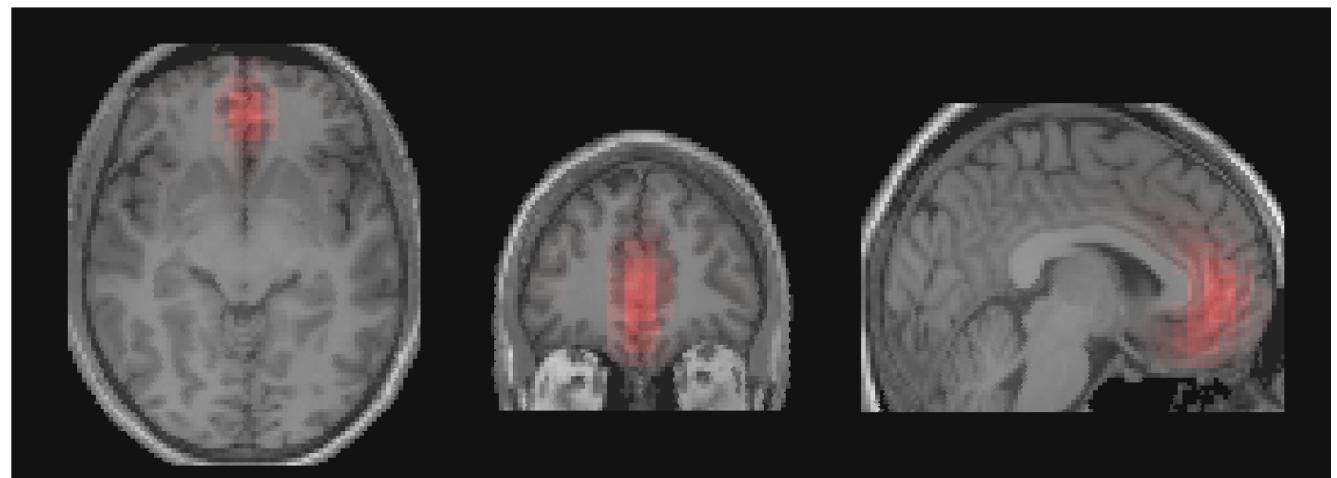
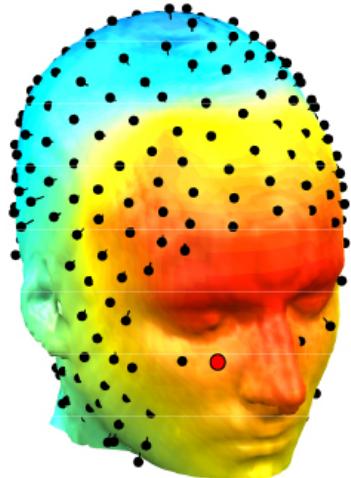
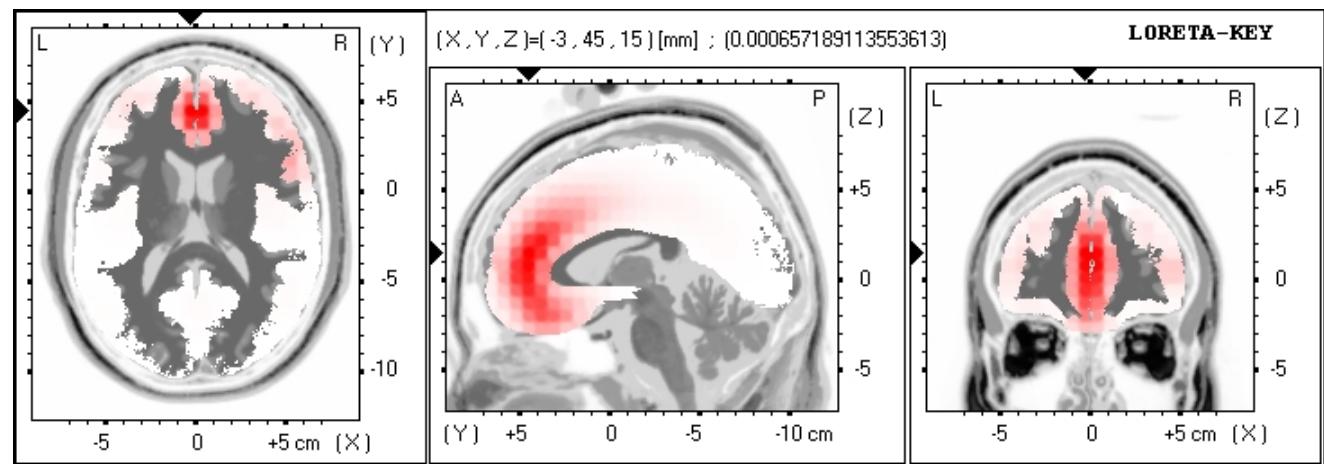
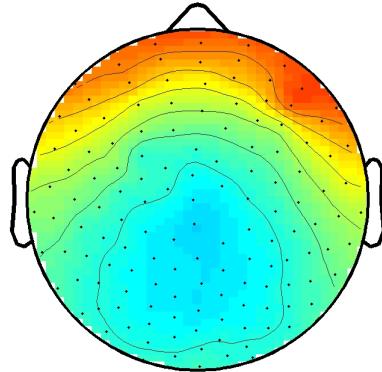




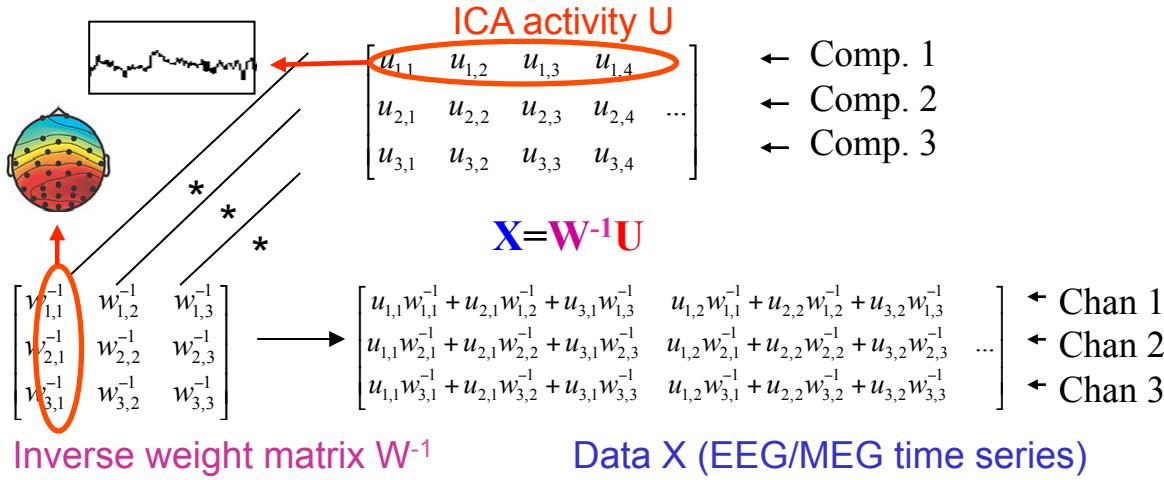
Localization of activity



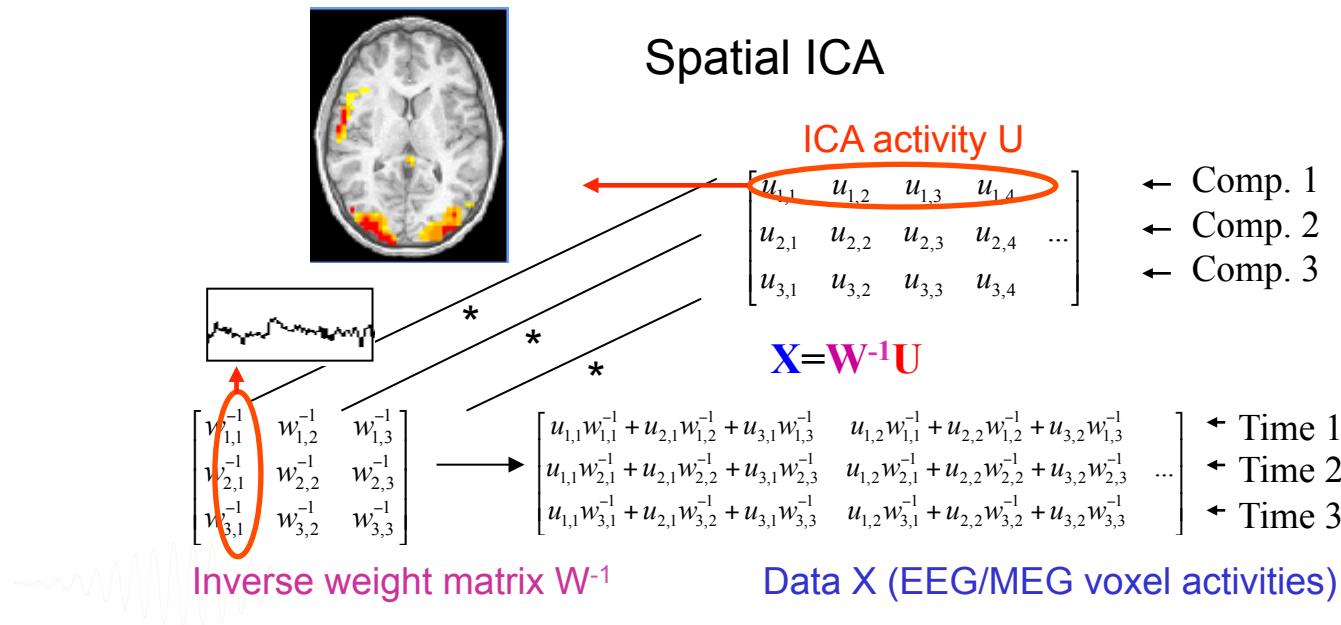
Localization of activity



Temporal ICA

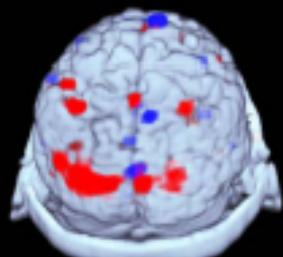


Spatial ICA

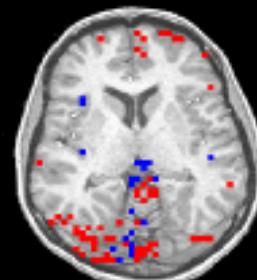


Independent fMRI Components

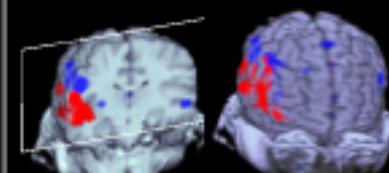
Consistently
task-related



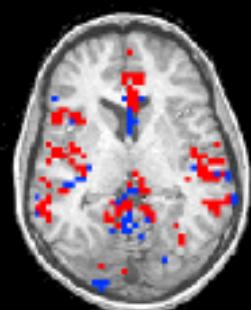
Transiently
task-related



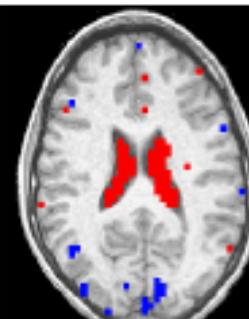
Abrupt head
movement



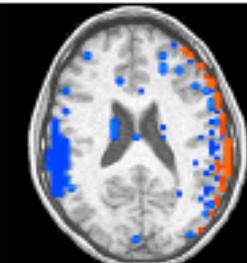
Quasi-periodic



Slowly-varying



Slow head
movement



■ Activated
■ Suppressed

The end

