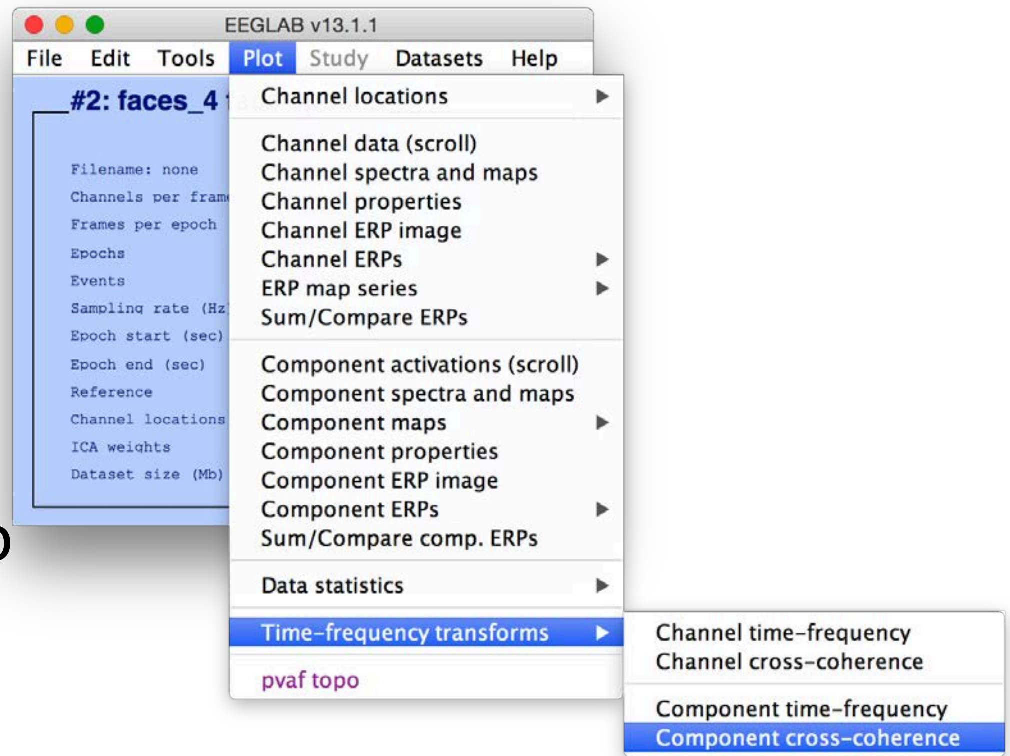
Source information flow and Granger-Causal modeling tools

EEGLAB Workshop XXVI
Ben-Gurion University, Be'er-Sheva, Israel
Day 3

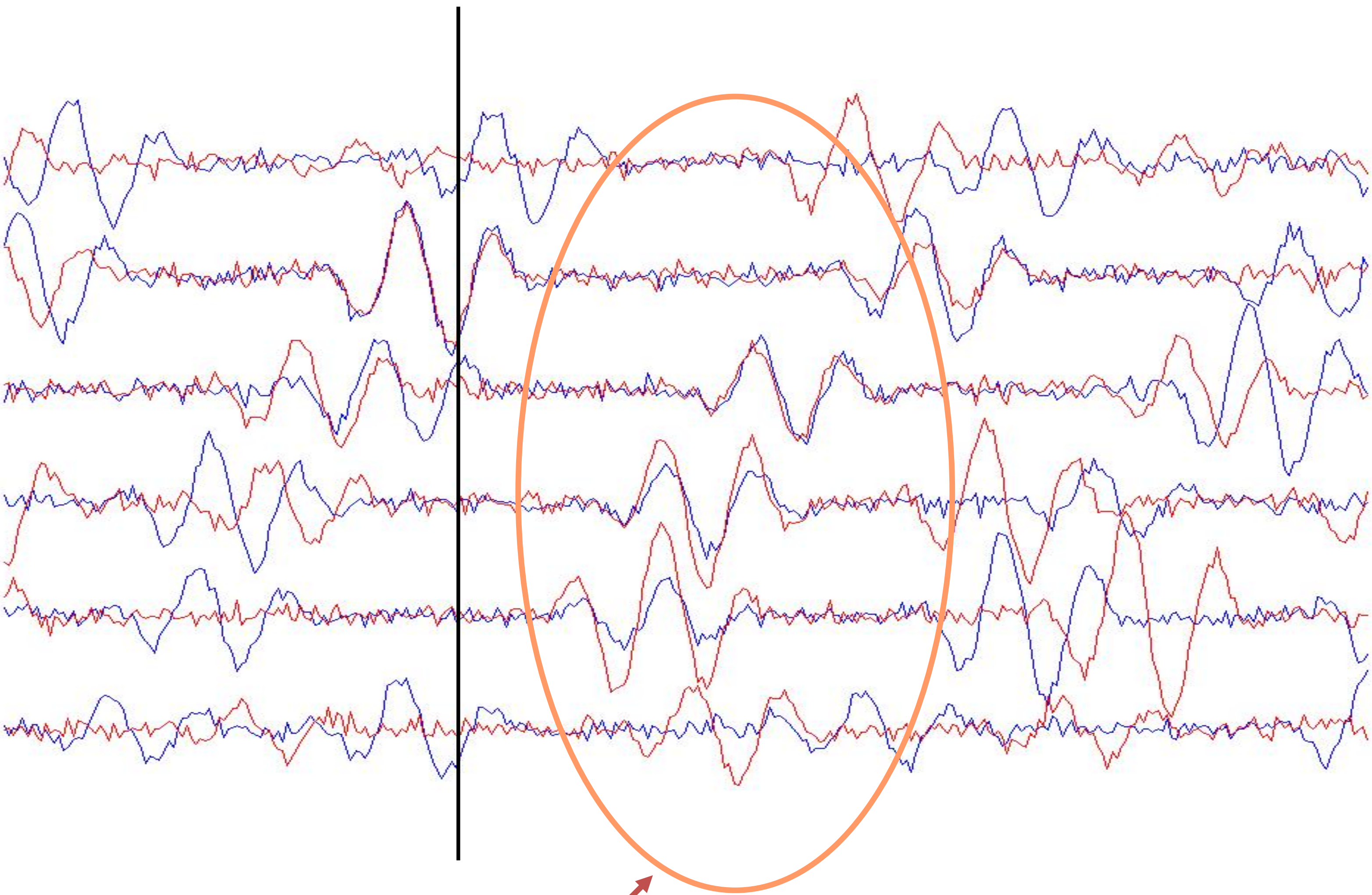
John Iversen

Part 3b: Event Related Coherence

- Goal: How similar is the event-related response of two signals?
  - Between channels (problematic due to volume conduction)
  - Between ICs
  - Useful to quickly begin to understand relationships between components

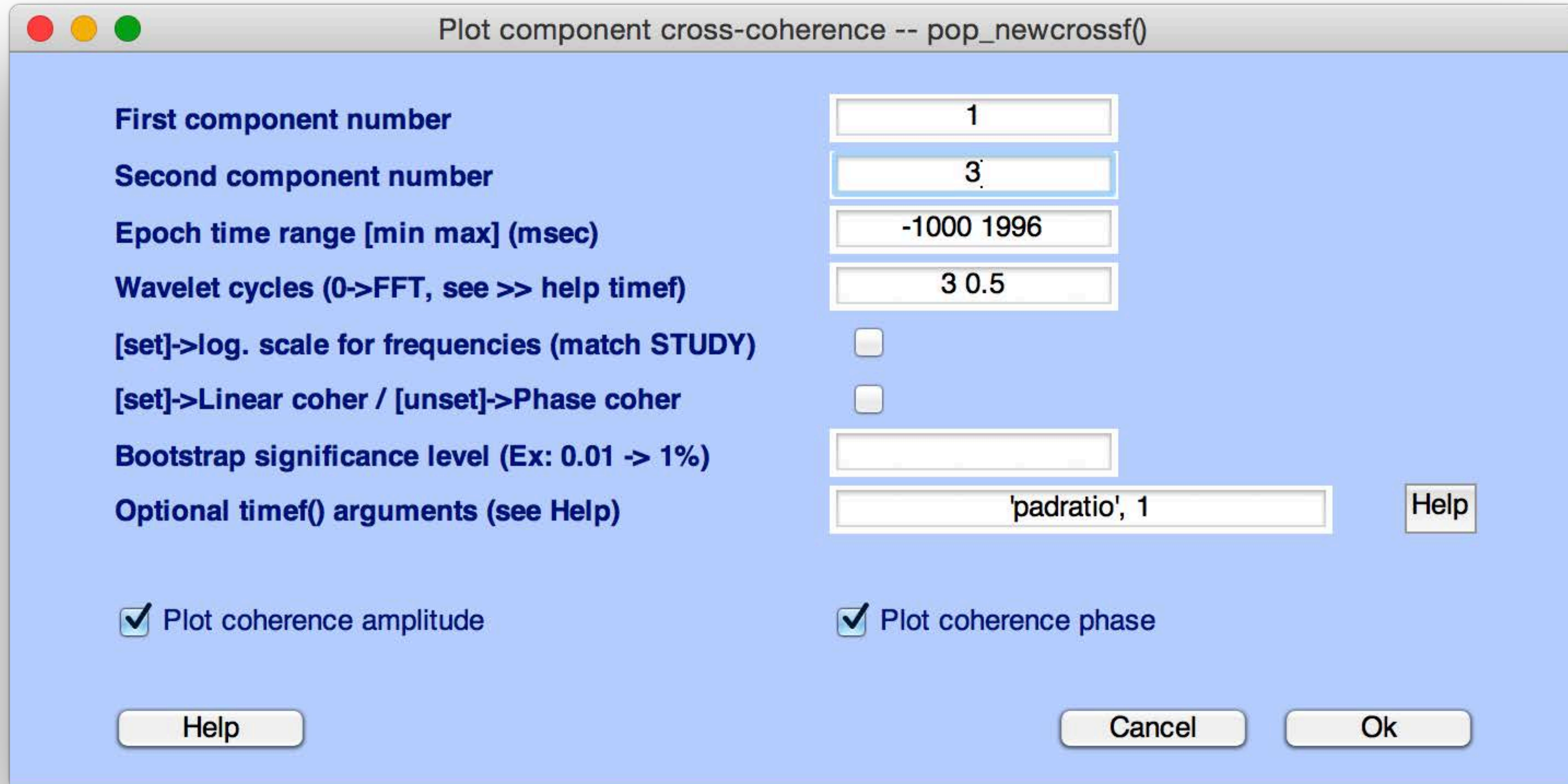


TWO SIMULATED THETA PROCESSES



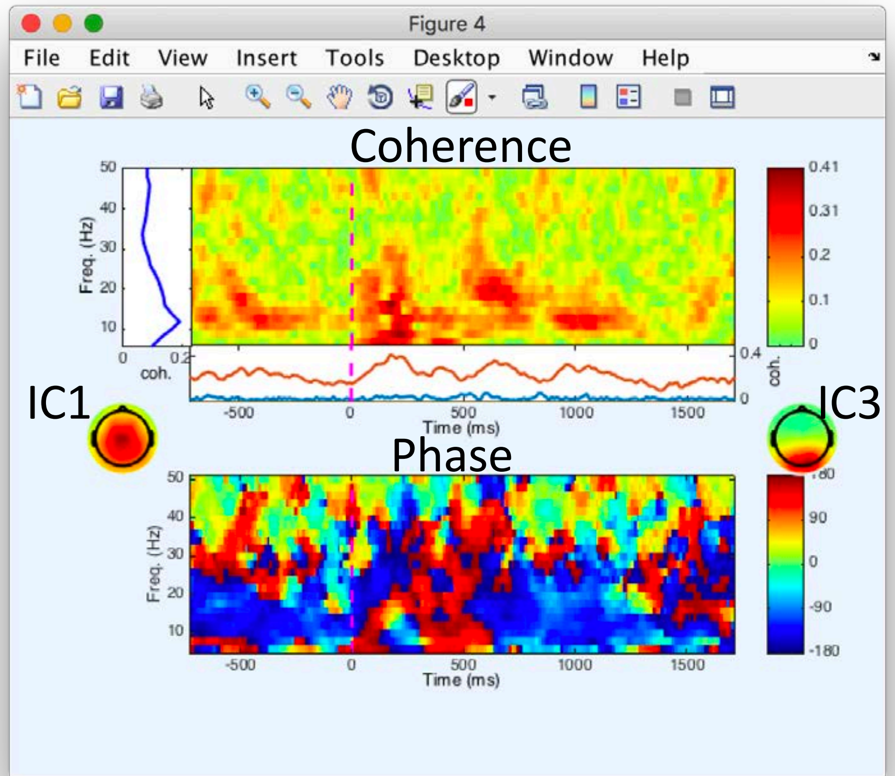
Event-related Coherence

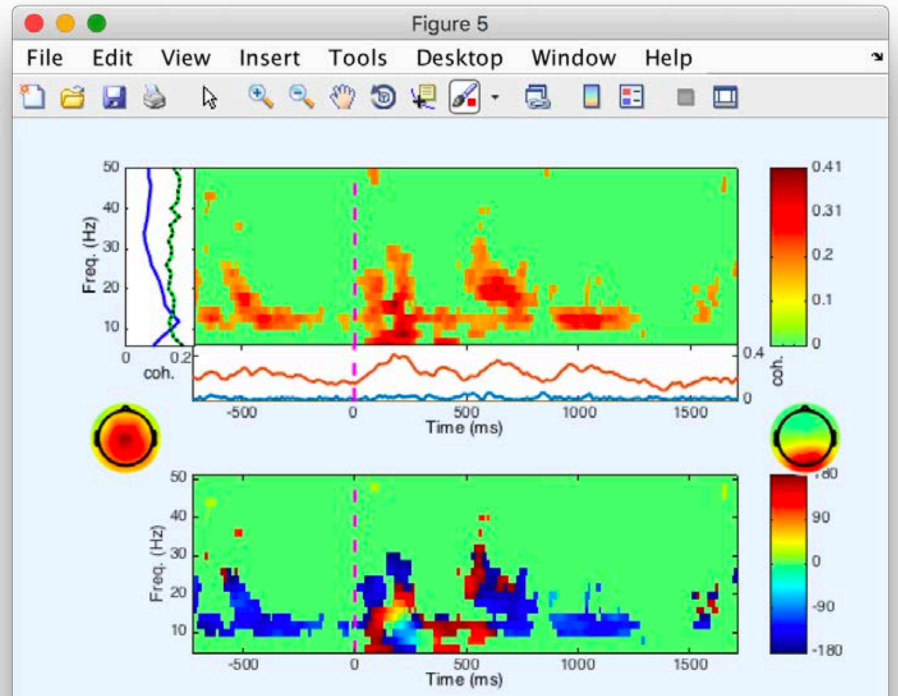
Try it!


Plot component cross-coherence -- pop_newcrossf()
First component number
1
Second component number
3
Epoch time range [min max] (msec)
-1000 1996
Wavelet cycles (0->FFT, see >> help timef)
3 0.5
[set]->log. scale for frequencies (match STUDY)
[set]->Linear coher / [unset]->Phase coher
Bootstrap significance level (Ex: 0.01 -> 1%)
Optional timef() arguments (see Help)
'padratio', 1
Help
Plot coherence amplitude
Plot coherence phase
Help
Cancel
Ok

Cross coherence between IC 1 and IC 3

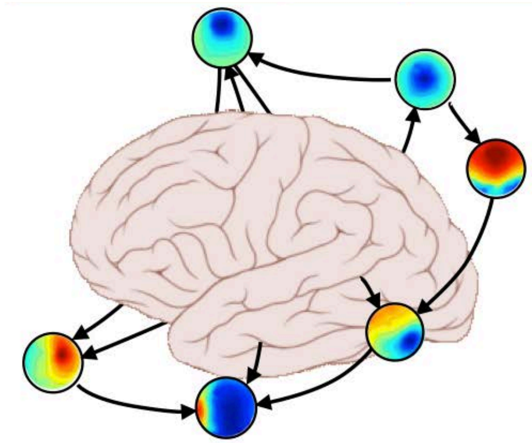
$\alpha = 0.01$





Significant event-related coherence (as well as tonic coherence) in alpha/beta bands
IC 1 tonically leads IC 3 (negative phase), but phase relationships are changed post-stimulus

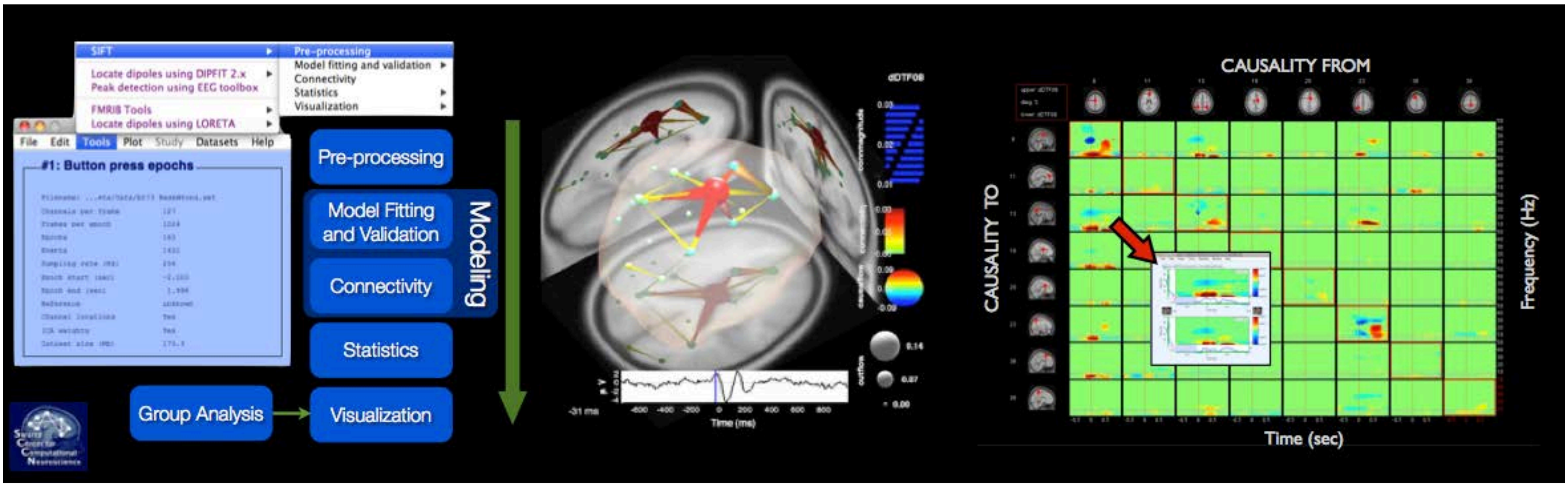
Directional measures of effective connectivity are present in the SIFT toolbox.



SIFT

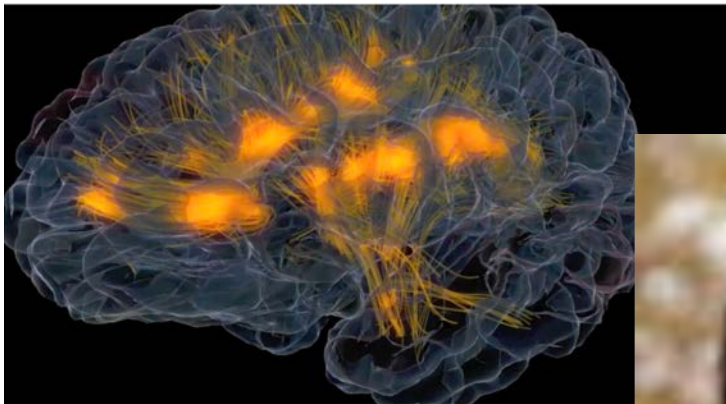
Source Information Flow Toolbox

http://sccn.ucsd.edu/wiki/SIFT
Mullen, et al, *Journal of Neuroscience Methods* (in prep, 2012)
Mullen, et al, *Society for Neuroscience*, 2010
Delorme, Mullen, Kothe et al, *Computational Intelligence and Neuroscience*, vol 12, 2011



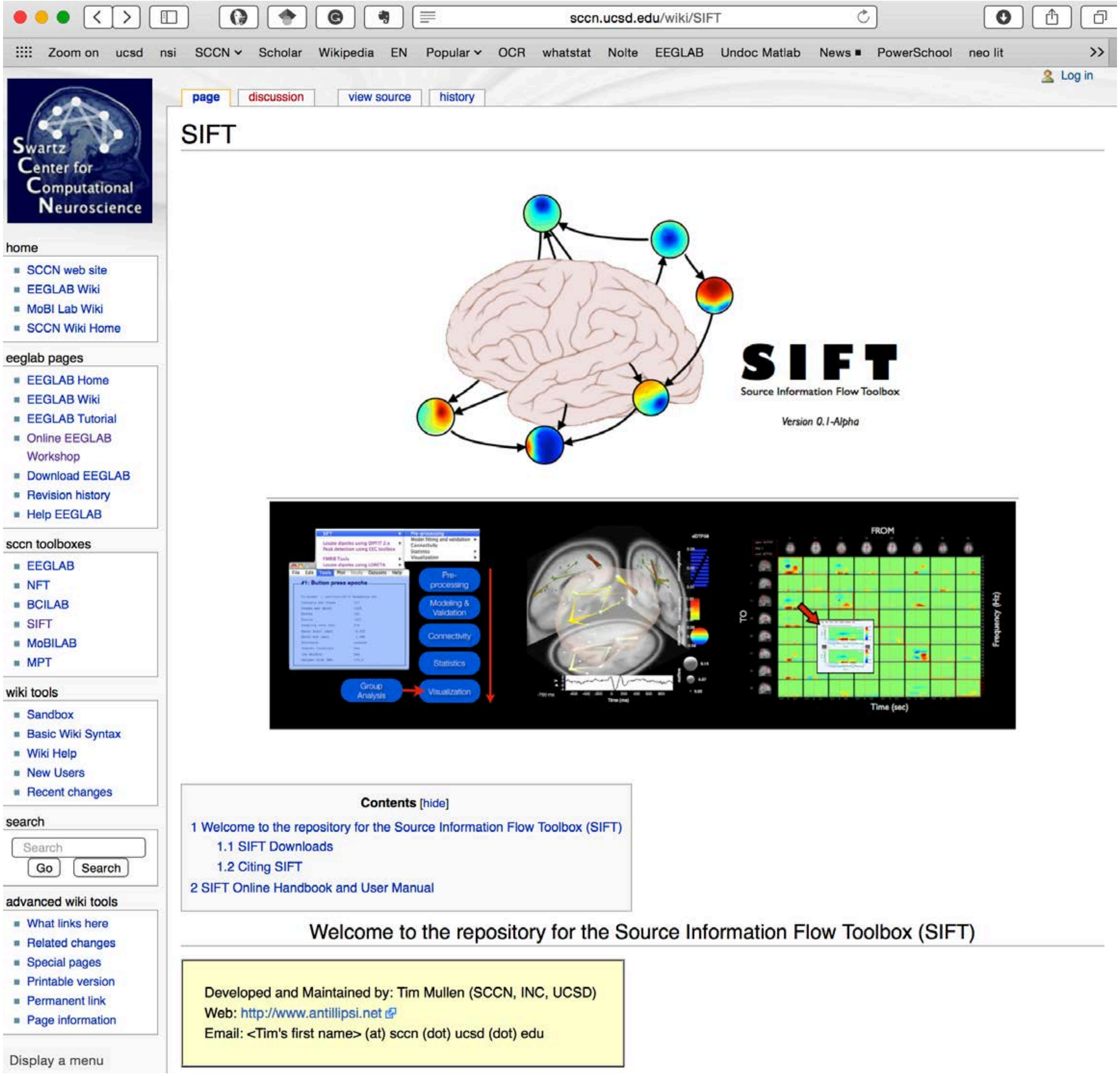
- A toolbox for (source-space) electrophysiological information flow and causality analysis (single- or multi-subject) integrated into the EEGLAB software environment.
- Emphasis on vector autoregression and time-frequency domain approaches
- Standard and novel interactive visualization methods for exploratory analysis of connectivity across time, frequency, and spatial location

Tim Mullen



QUSP is now

intheon



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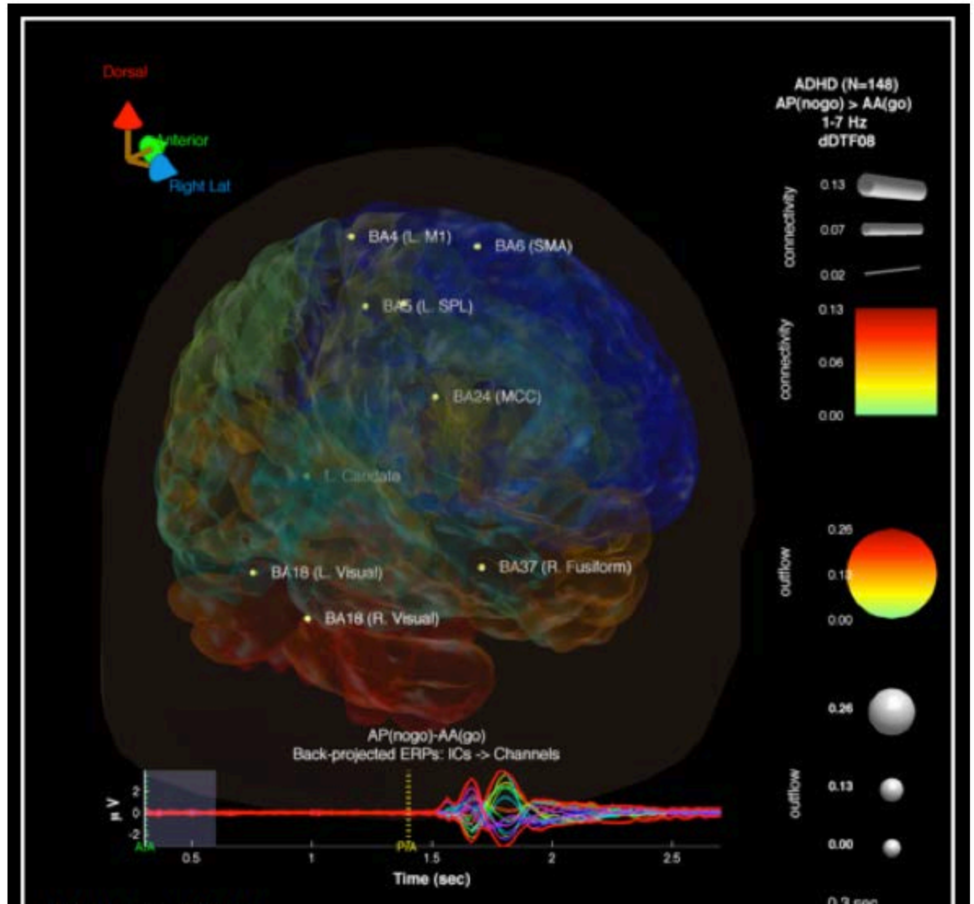
1.2 Citing SIFT
2 SIFT Online Handbook and User Manual
Welcome to the repository for the Source Information Flow Toolbox (SIFT)
Developed and Maintained by: Tim Mullen (SCCN, INC, UCSD)
Web: http://www.antillipsi.net
Email: <Tim's first name> (at) sccn (dot) ucsd (dot) edu

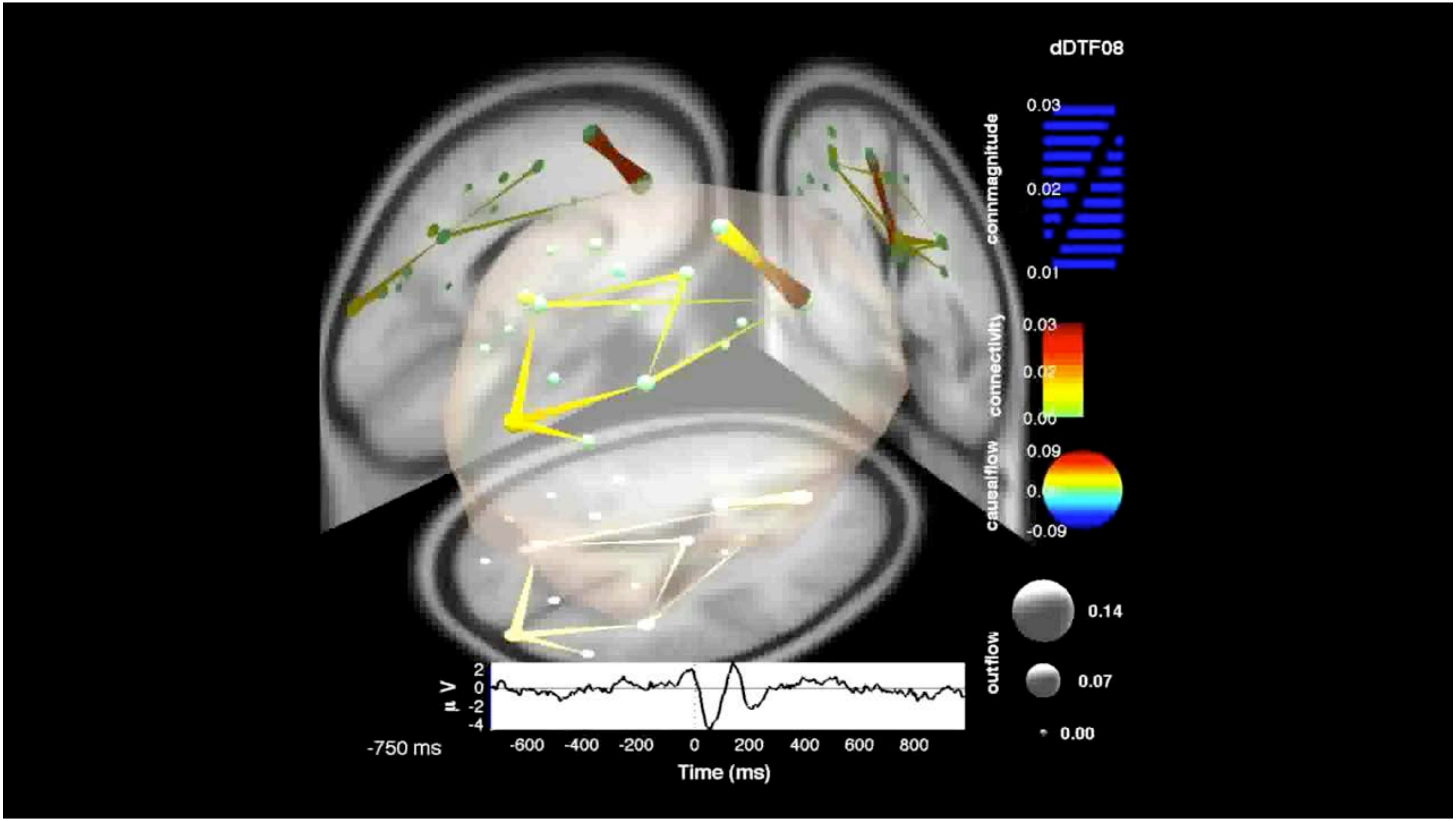
The Dynamic Brain

- A key goal: To model temporal changes in neural dynamics and information flow that index and predict task-relevant changes in cognitive state and behavior

- **Open Challenges:**
  - Non-invasive measures (source inference)
  - Robustness and Validity (constraints & statistics)
  - Scalability (multivariate)
  - Temporal Specificity / Non-stationarity / Single-trial (dynamics)
  - Multi-subject Inference
  - Usability and Data Visualization (software)



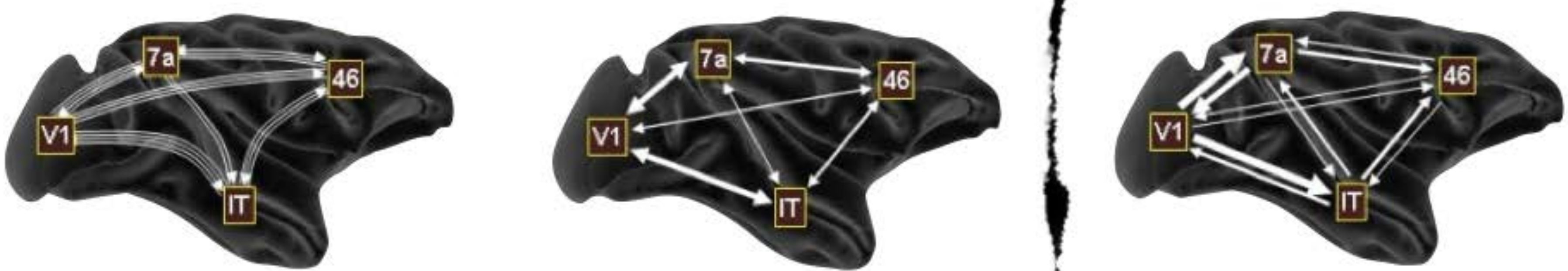
Mullen, 2011


dDTF08
0.03
connmagnitude
0.02
0.01
0.03
connectivity
0.00
0.09
causalflow
-0.09
0.14
outflow
0.07
0.00
μV
2
0
-2
-4
-750 ms
-600
-400
-200
0
200
400
600
800
Time (ms)

Large-scale brain connectivity

(Bullmore and Sporns, *Nature*, 2009)

Structural | **Functional** | **Effective**



state-invariant, anatomical

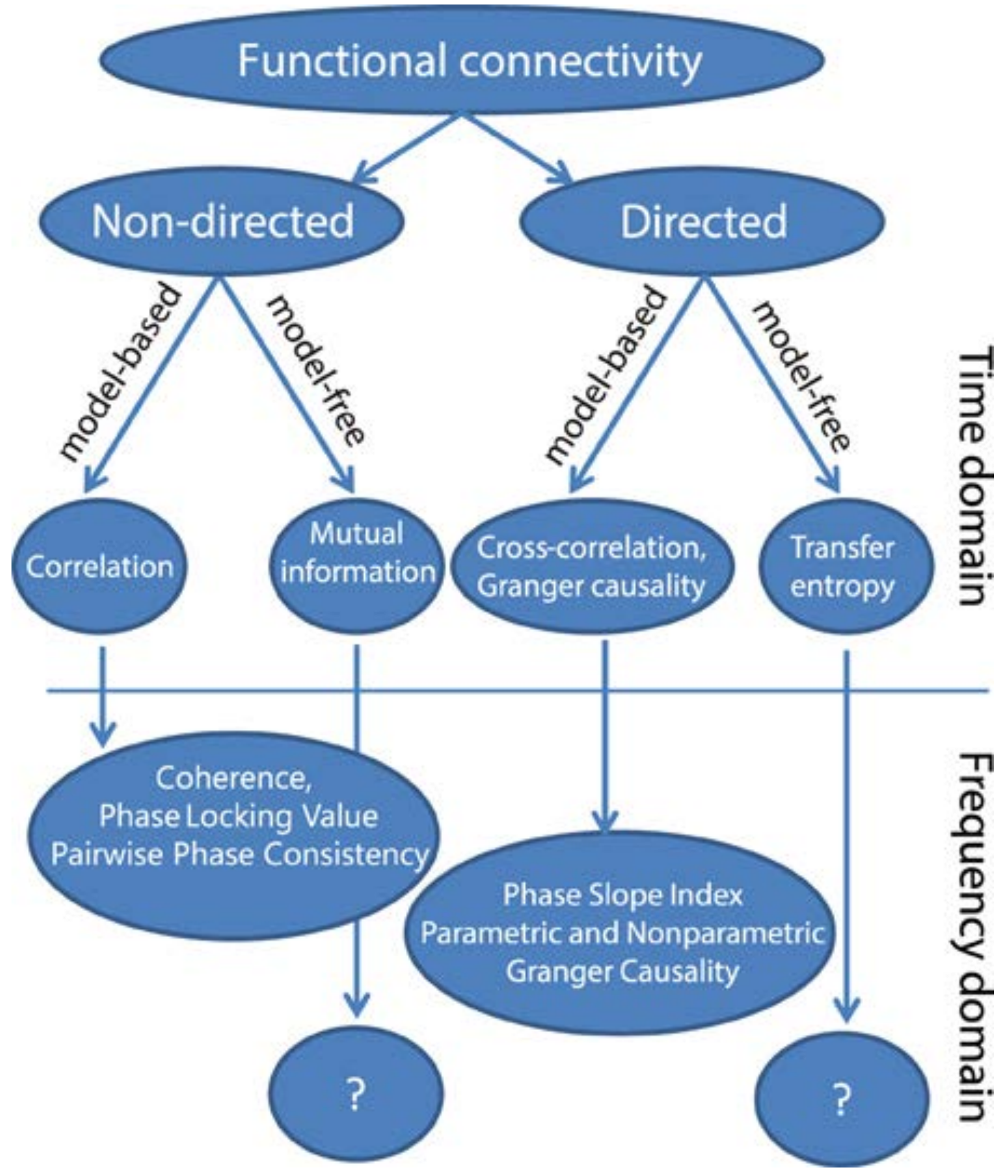
dynamic, state-dependent, correlative, symmetric

dynamic, state-dependent, asymmetric, causal, information flow

Hours-Years — **milliseconds-seconds**

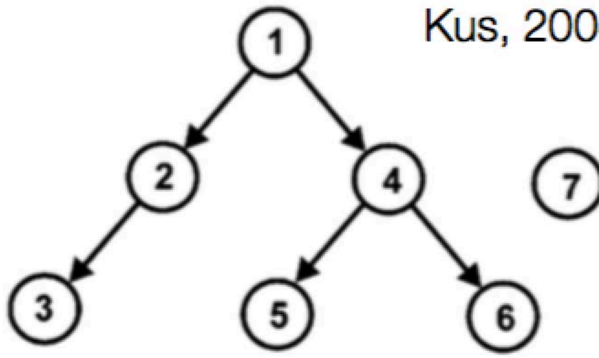
Temporal Scale

A taxonomy of connectivity measures



Bastos AM, Schoffelen J-M: **A Tutorial Review of Functional Connectivity Analysis Methods and Their Interpretational Pitfalls**. *Front Sys Neurosci* 2016, **9**:413.

The problem of spurious connectivity

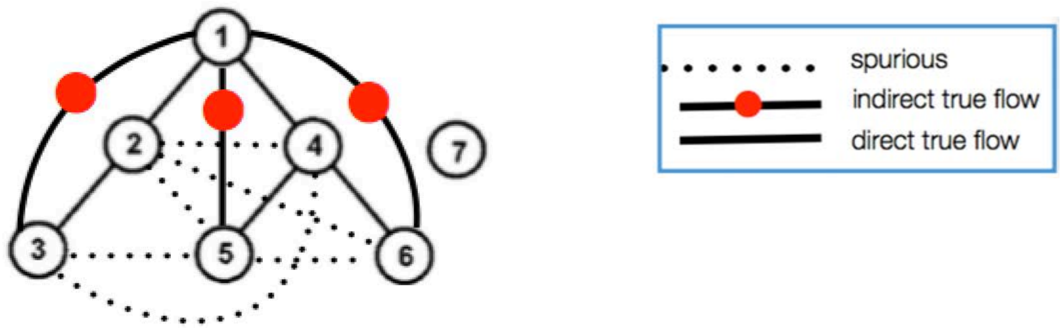


Kus, 2004

Coherency

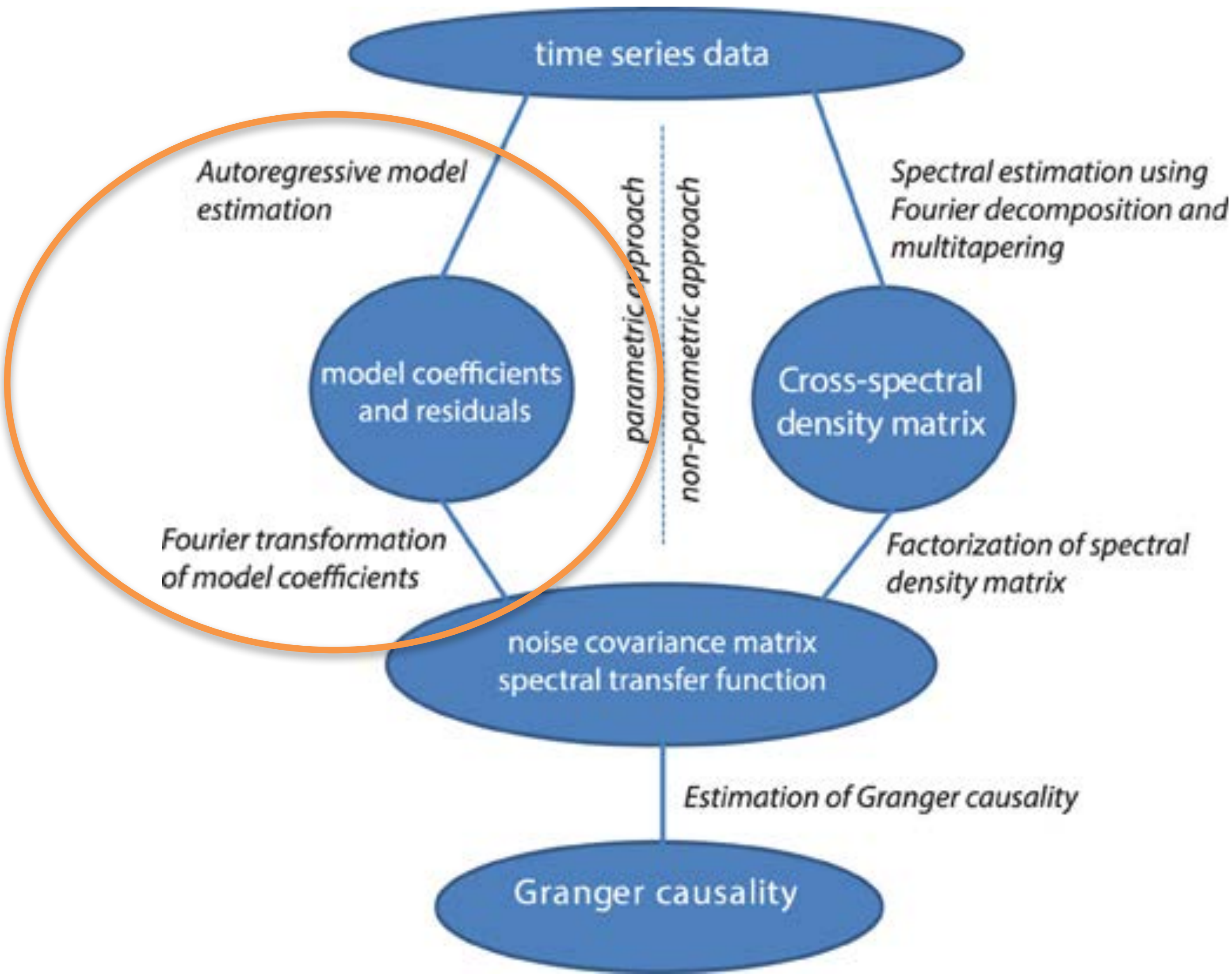
$$C_{ij}(f) = \frac{S_{ij}(f)}{\sqrt{S_{ii}(f)S_{jj}(f)}}$$

(Bendat and Piersol, 1986)



Bivariate measures, such as coherence (but also original GC), find spurious connections between nodes if they share a **common input**.

Calculation of GC



Granger Causality

- A measure of *statistical* causality based on prediction.
- Widely used in time-series econometrics.
- Nobel Prize in economics, 2003.

If a signal A causes a signal B, then knowledge of the past of both A and B should improve the predictability of B, as compared to knowledge of B alone.

Granger Causality

- Granger (1969) quantified this definition for **bivariate** processes in the form of an F-ratio:

$$F_{X_1 \leftarrow X_2} = \ln\left(\underbrace{\overbrace{\frac{var(\tilde{E}_1)}{var(E_1)}}^{\text{reduced model}}}_{\text{full model}}\right) = \ln\left(\frac{var(X_1(t) \mid X_1(\cdot))}{var(X_1(t) \mid X_1(\cdot), X_2(\cdot))}\right)$$

- Alternately, for a **multivariate interpretation** we can fit a single MVAR model to all channels and apply the following definition:

Definition 1

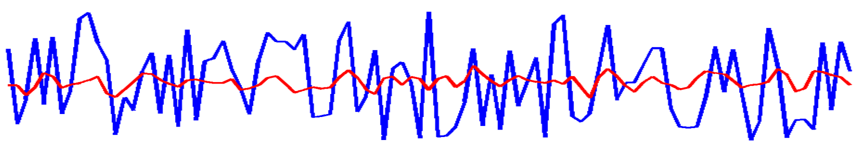
X_j granger-causes X_i conditioned on all other variables in $\mathbf{X}$

if and only if $\mathbf{A}_{ij}(k) >> 0$ for some lag $k \in \{1, \ldots, p\}$

Autoregressive Models

Goal: Predict future values of a data time series (EEG signal) from its past.

X



$$x(t) = \sum_{\tau=1}^{p} a(\tau)x(t-\tau) + e(t)$$

weighted sum of past values

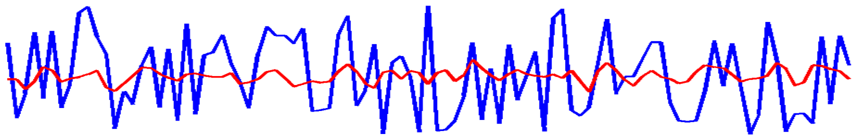
error

Example: order p = 2:

$$x(t) = a(1)x(t-1) + a(2)x(t-2) + e(t)$$

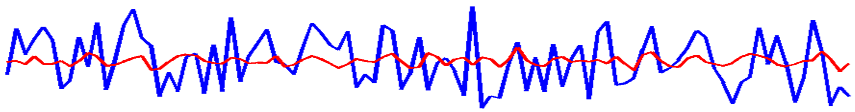
AR Models (prediction of future of a signal by its past)

x₁



$$x_1(t) = \sum_{\tau=1}^{p} a(\tau)x_1(t-\tau) + e_1(t)$$

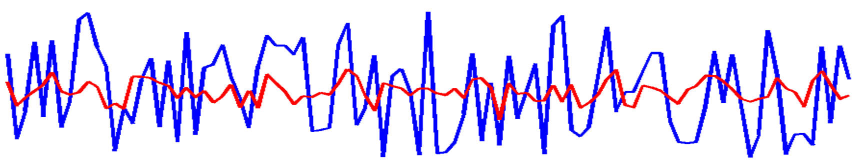
x₂



$$x_2(t) = \sum_{\tau=1}^{p} b(\tau)x_2(t-\tau) + e_2(t)$$

VAR Models (prediction of future of a signal by its past + the other signal's past)

$X_1 \,|\, X_2$



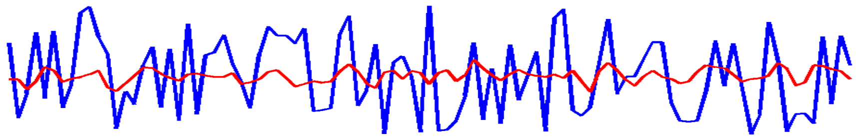
$$x_{1|2}(t) = \sum_{\tau=1}^{p} c(\tau)x_1(t-\tau) + \sum_{\tau=1}^{p} d(\tau)x_2(t-\tau) + e_{1|2}(t)$$

$$GC_{2\rightarrow 1} = ln\,\frac{var(e_1)}{var(e_{1|2})}$$

$$\approx \ln(1)=0$$

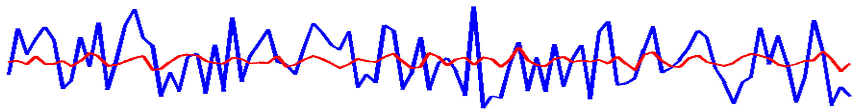
AR Models (prediction of future of a signal by its past)

X_1



$$x_1(t) = \sum_{\tau=1}^{p} a(\tau) x_1(t-\tau) + e_1(t)$$

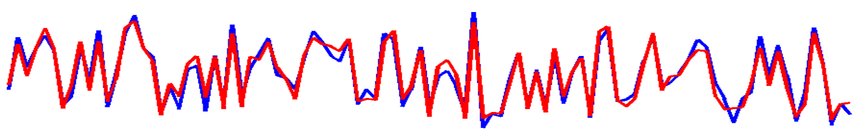
X_2



$$x_2(t) = \sum_{\tau=1}^{p} b(\tau) x_2(t-\tau) + e_2(t)$$

VAR Models (prediction of future of a signal by its past + the other signal's past)

$X_2 | X_1$



$$GC_{2\rightarrow1} = ln \frac{var(e_2)}{var(e_{2|1})}$$

$\boxed{\approx \ln(>1) = >1}$

$$x_{2|1}(t) = \sum_{\tau=1}^{p} u(\tau) x_2(t-\tau) + \sum_{\tau=1}^{p} v(\tau) x_1(t-\tau) + e_{2|1}(t)$$

Incorporating information about X_1 improves the prediction of X_2!

We say "X_1 granger-causes X_2"

Granger Causality

- Granger (1969) quantified this definition for **bivariate** processes in the form of an F-ratio:

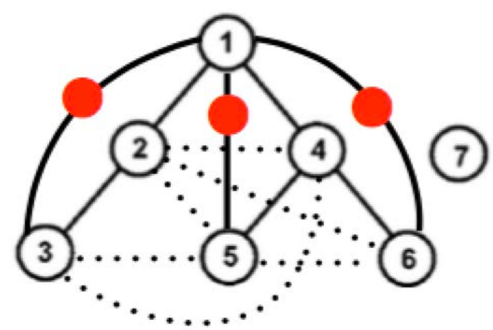
reduced model

$$F_{X_1 \leftarrow X_2} = \ln\left(\frac{var(\tilde{E}_1)}{var(E_1)}\right) = \ln\left(\frac{var(X_1(t) \mid X_1(\cdot))}{var(X_1(t) \mid X_1(\cdot), X_2(\cdot))}\right)$$

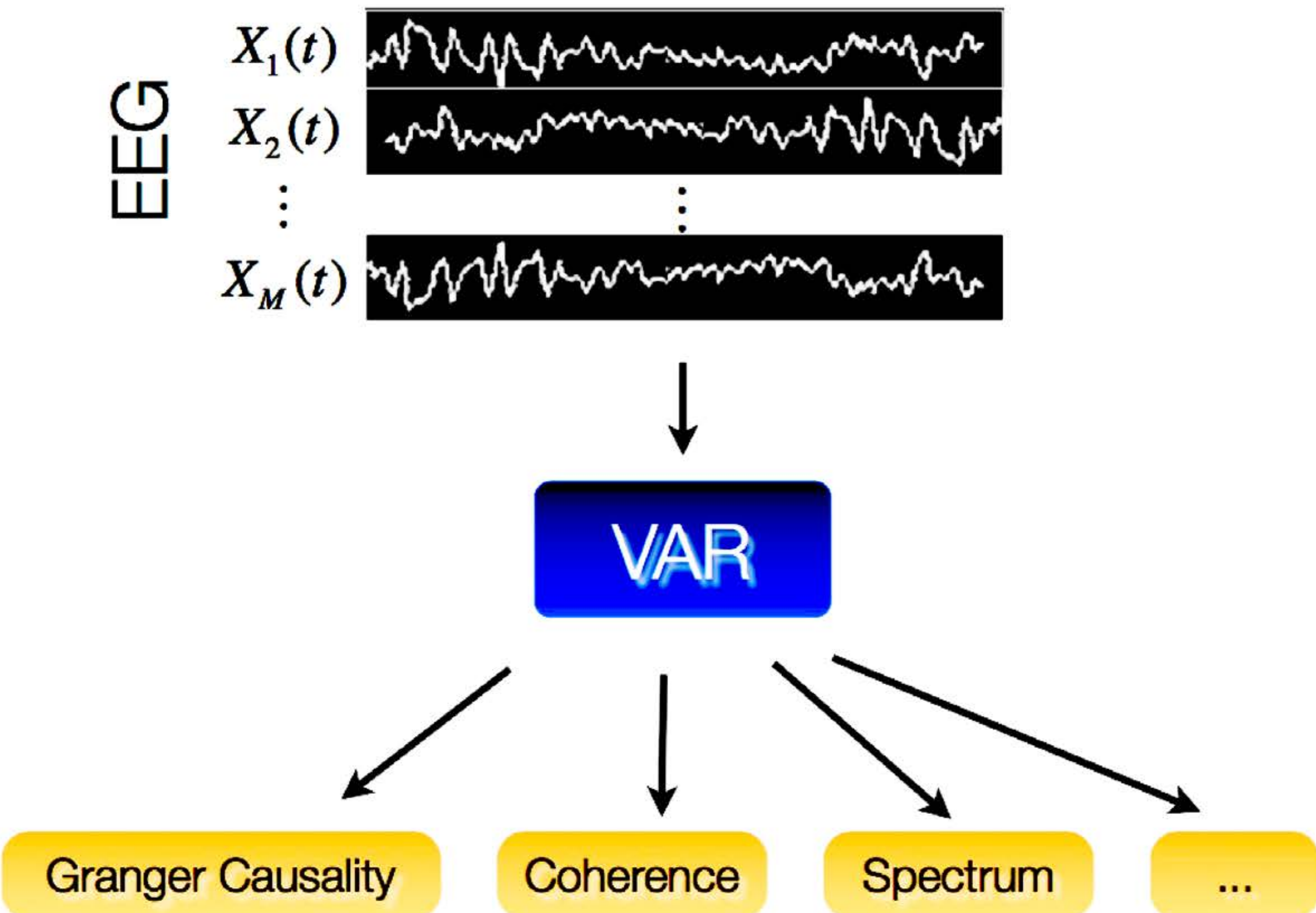
full model

Problem: Pairwise GC for multichannel data has problems of spurious connectivity due to common inputs

Solution: Multivariate VAR (MVAR)

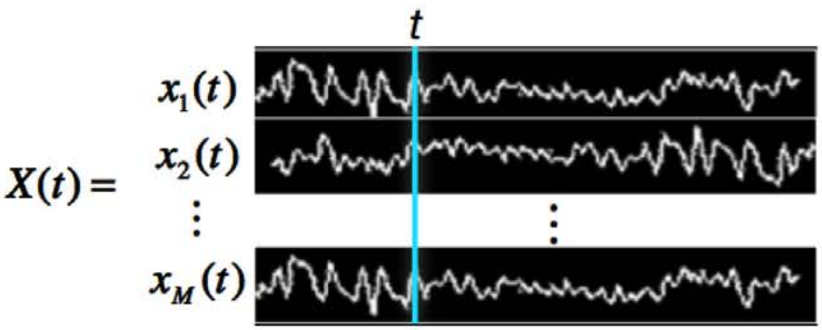


Vector Autoregressive (VAR / MAR / MVAR) Modeling



The Linear Vector Auto-regressive (VAR) Model

Ordinary Least-Squares



VAR[*p*] model

model order

random noise process

$$\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}^{(k)}(t)\mathbf{X}(t-k) + \mathbf{E}(t)$$

M-channel data vector at current time *t*

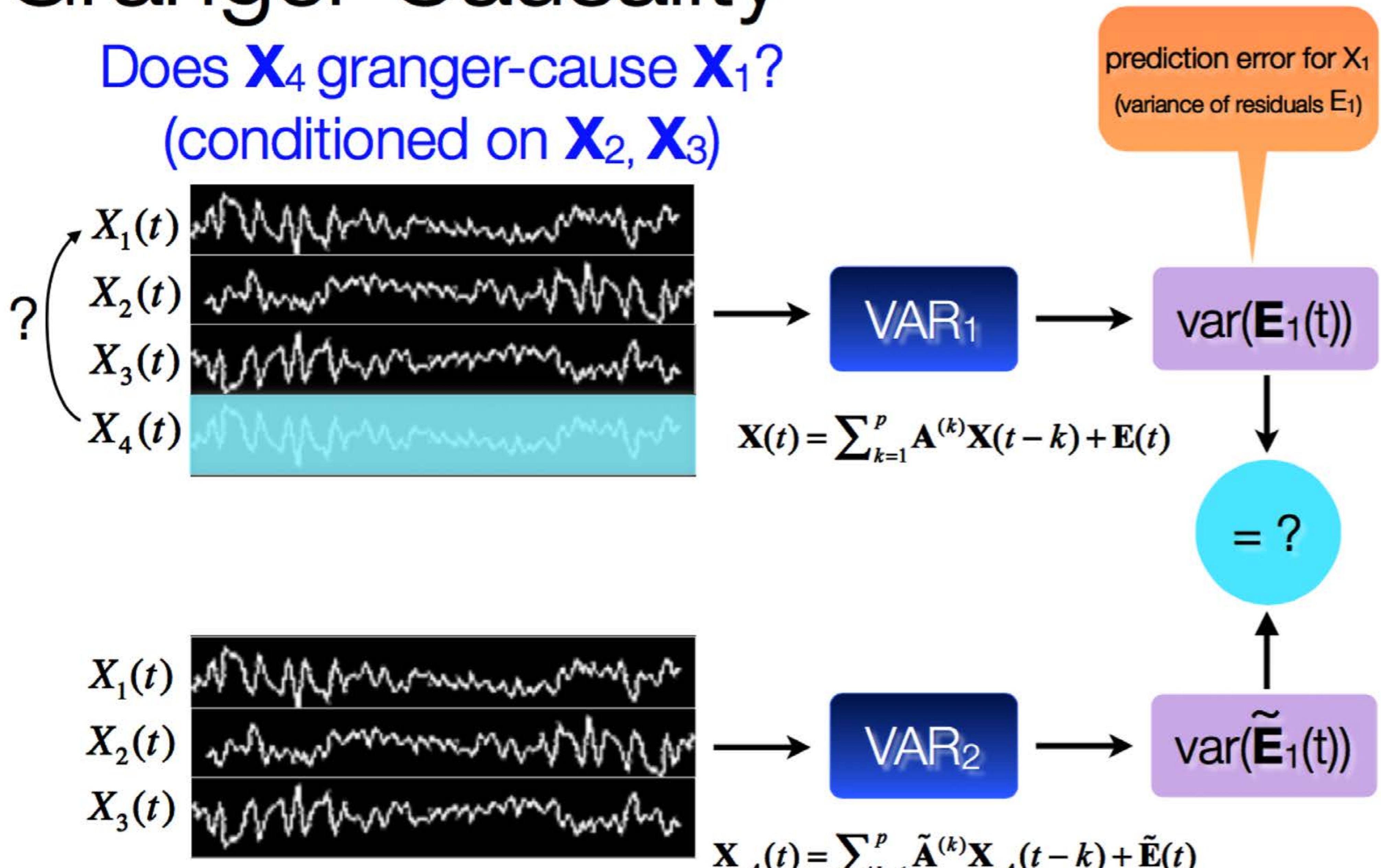
M x M matrix of (possibly time-varying) model coefficients indicating variable dependencies at lag *k*

multichannel data *k* samples in the past

$$\mathbf{A}^{(k)}(t) = \begin{pmatrix} a_{11}^{(k)}(t) & \cdots & a_{1M}^{(k)}(t) \\ \vdots & \ddots & \vdots \\ a_{M1}^{(k)}(t) & \cdots & a_{MM}^{(k)}(t) \end{pmatrix} \qquad \mathbf{E}(t) = N(0, \mathbf{V})$$

Granger Causality

Does $\mathbf{X}_4$ granger-cause $\mathbf{X}_1$? (conditioned on $\mathbf{X}_2$, $\mathbf{X}_3$)



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Definition 1

X_j granger-causes X_i conditioned on all other variables in $\mathbf{X}$

if and only if $\mathbf{A}_{ij}(k) >> 0$ for some lag $k \in \{1, \ldots, p\}$

Granger Causality – Frequency Domain

$$\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}^{(k)}\mathbf{X}(t-k) + \mathbf{E}(t)$$

Fourier-transforming $\mathbf{A}^{(k)}$ we obtain

Likewise, $\mathbf{X}(f)$ and $\mathbf{E}(f)$ correspond to the fourier transforms of the data and residuals, respectively

$$\mathbf{A}(f) = -\sum_{k=0}^{p} \mathbf{A}^{(k)} e^{-i2\pi fk}; \mathbf{A}^{(0)} = I$$

We can then define the spectral matrix $\mathbf{X}(f)$ as follows:

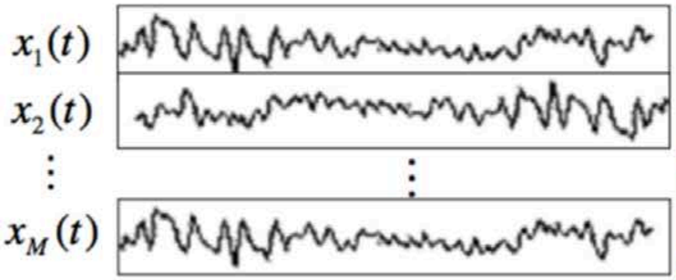
$$\mathbf{X}(f) = \mathbf{A}(f)^{-1}\mathbf{E}(f) = \mathbf{H}(f)\mathbf{E}(f)$$

Where $\mathbf{H}(f)$ is the *transfer matrix* of the system.

Definition 2

X_j granger-causes X_i conditioned on all other variables in $\mathbf{X}$ <u>if and only if</u> $|\mathbf{A}_{ij}(f)| \gg 0$ for some frequency f

leads to PDC

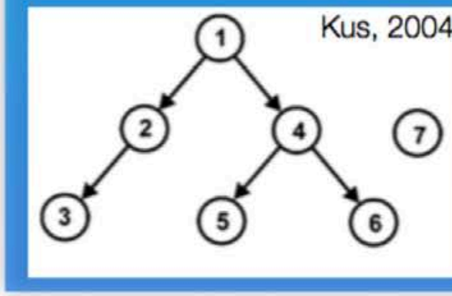


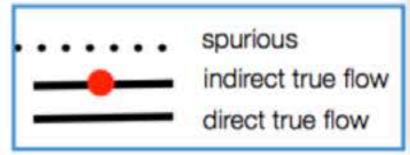
$$\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}^{(k)}(t)\mathbf{X}(t-k) + \mathbf{E}(t)$$

$$\mathbf{A}(f,t) = -\sum_{k=0}^{p} \mathbf{A}^{(k)}(t)e^{-i2\pi fk}; \quad \mathbf{A}^{(0)} = I$$

$$\mathbf{X}(f,t) = \mathbf{A}(f,t)^{-1}\mathbf{E}(f,t) = \mathbf{H}(f,t)\mathbf{E}(f,t)$$

Ground Truth

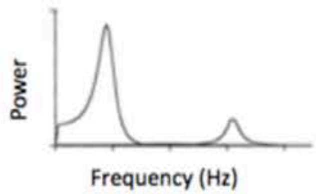




Spectrum

$$S(f) = \mathbf{X}(f)\mathbf{X}(f)^* = \mathbf{H}(f)\Sigma\mathbf{H}(f)^*$$

(Brillinger, 2001)



NOTE: time index (t) dropped for convenience

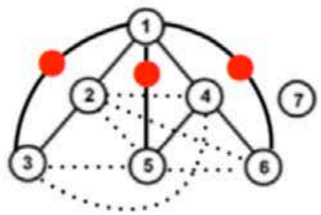
	Functional	Effective
Bivariate	Coherency	Granger-Geweke Causality
Multivariate	Partial Coherence	Partial Directed Coherence

Bivariate

Coherency

$$C_{ij}(f) = \frac{S_{ij}(f)}{\sqrt{S_{ii}(f)S_{jj}(f)}}$$

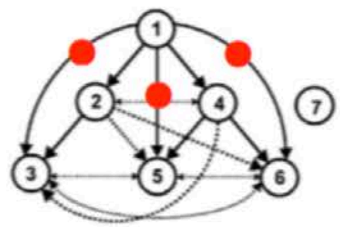
(Bendat and Piersol, 1986)



Granger-Geweke Causality

$$F_{ij}(f) = \frac{\Sigma_{jj} - (\Sigma_{ij}^2 / \Sigma_{ii}))\,|H_{ij}(f)|^2}{S_{ii}(f)}$$

(Geweke, 1982; Bressler et al., 2007)

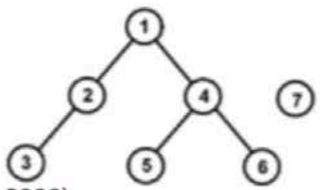


Multivariate

Partial Coherence

$$P_{ij}(f) = \frac{S_{ij}^{-1}(f)}{\sqrt{S_{ii}^{-1}(f)S_{jj}^{-1}(f)}}$$

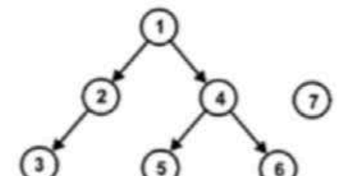
(Bendat and Piersol, 1986; Dalhaus, 2000)



Partial Directed Coherence

$$\pi_{ij}^2(f) = \frac{|A_{ij}(f)|^2}{\sum_{k=1}^{M}\left|A_{kj}(f)\right|^2}$$

(Baccalá and Sameshima, 2001)

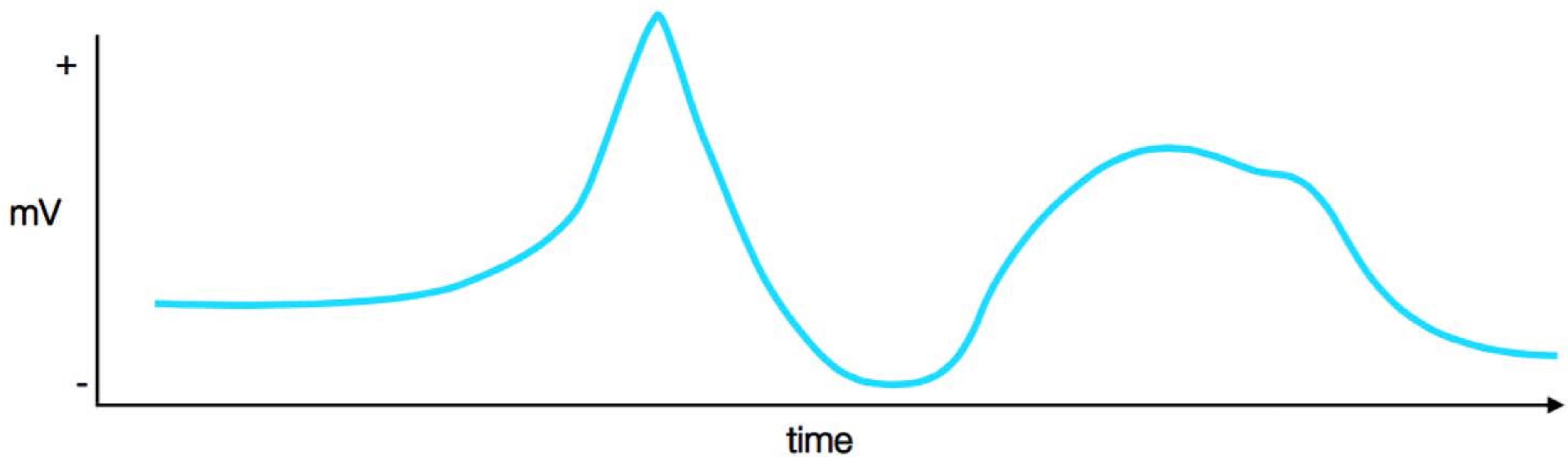


Time-Frequency GC

- Brain network dynamics often change rapidly with time
  - event-related responses
  - transient network changes during sequential information processing
- Electrophysiological processes often exhibit oscillatory phenomena, making them well-suited for frequency-domain analysis

Adapting to Non-Stationarity

- The brain is a **dynamic system** and measured brain activity and coupling can change rapidly with time (non-stationarity)
  - event-related perturbations (ERSP, ERP, etc)
  - structural changes due to learning/feedback
- How can we adapt to non-stationarity?

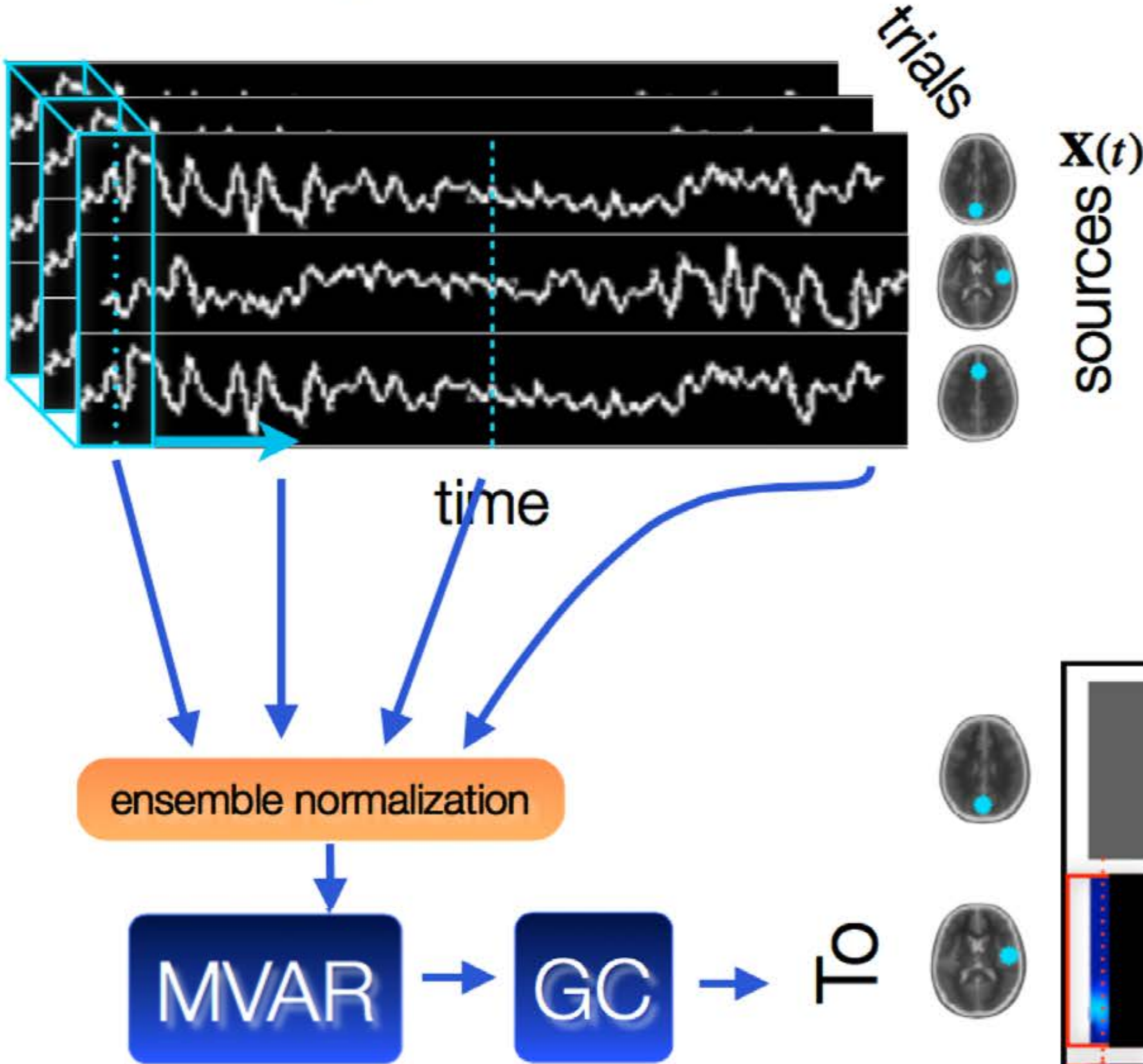


Adapting to Non-Stationarity

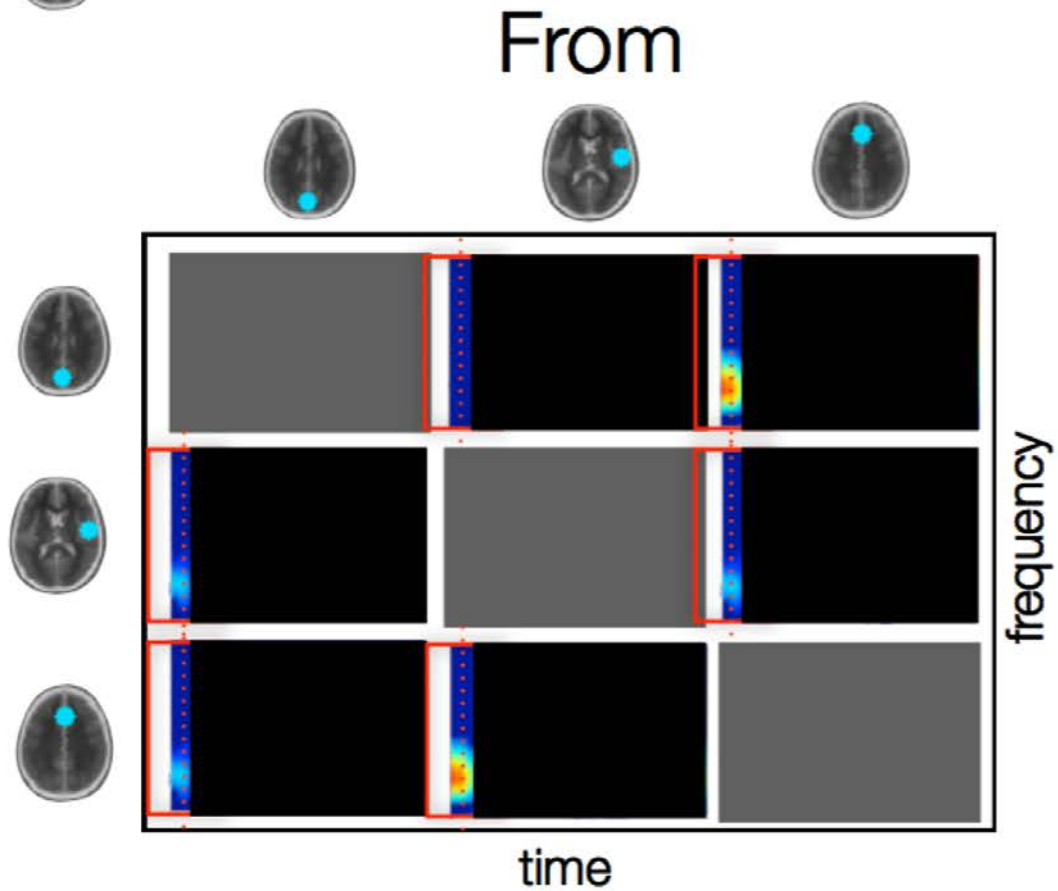
- **Many ways to do adaptive VAR estimation**
  - Segmentation-based adaptive VAR estimation
  - Factorization of time-varying spectral density matrices (e.g. from STFTs, Wavelets, etc)
  - State-Space Modeling
  - ...

Segmentation-based VAR

(Jansen et al., 1981; Florian and Pfurtscheller, 1995; Ding et al, 2000)

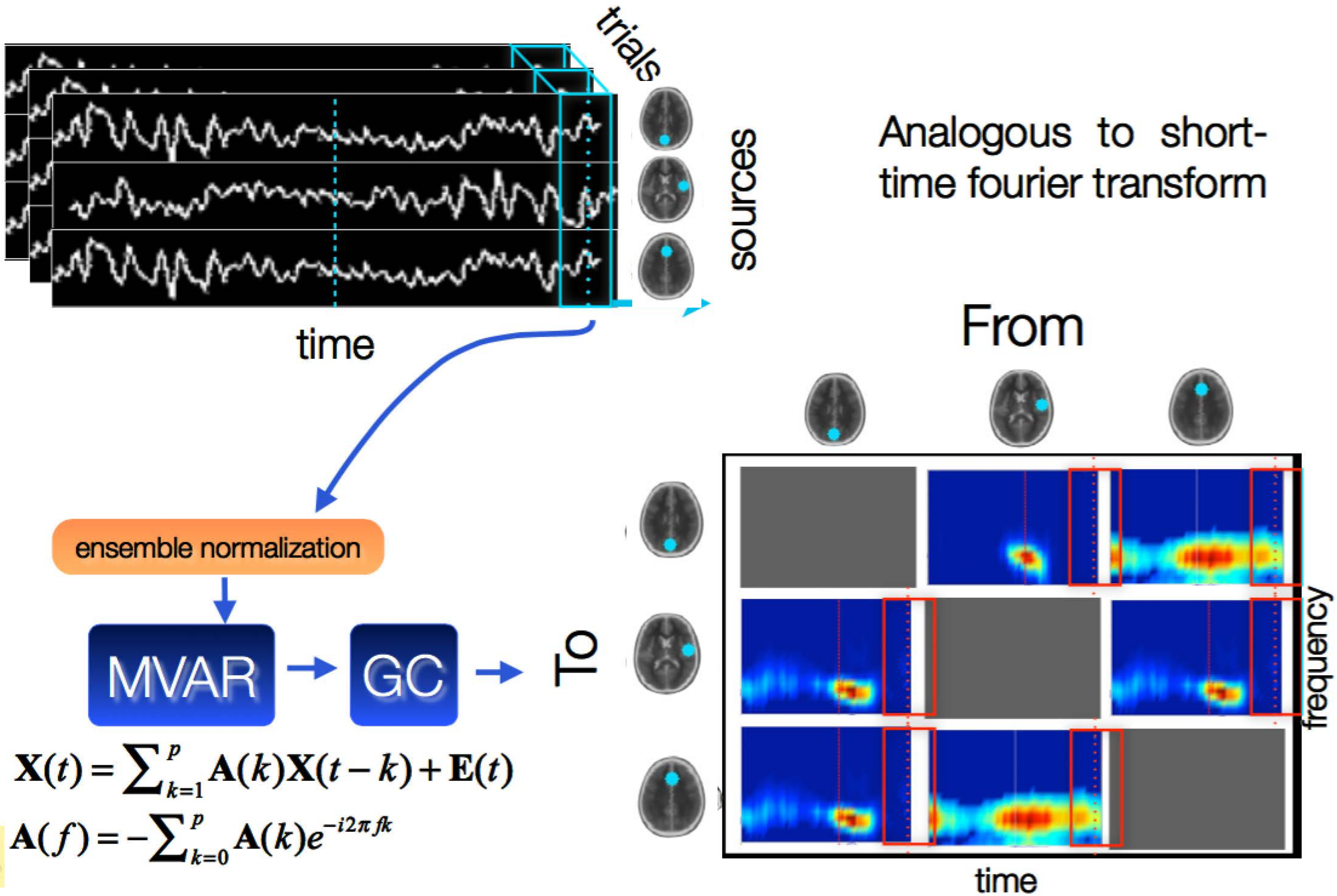


Analogous to short-time Fourier transform



$$\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}^{(k)}(t)\mathbf{X}(t-k) + \mathbf{E}(t)$$

$$\mathbf{A}(f,t) = -\sum_{k=0}^{p} \mathbf{A}^{(k)}(t)e^{-i2\pi fk}; \mathbf{A}^{(0)} = I$$



Analogous to short-time fourier transform

$$\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}(k)\mathbf{X}(t-k) + \mathbf{E}(t)$$

$$\mathbf{A}(f) = -\sum_{k=0}^{p} \mathbf{A}(k) e^{-i2\pi fk}$$

Important Choices

- Model Order
  - Determines complexity of spectrum you can model
  - Larger orders need more data
- Window Length
  - Window must be long enough to contain sufficient data for your chosen model order
  - Must be long enough to encompass the time-scale of interactions
  - Yet not too long as to smear temporal dynamics or include non-stationary data

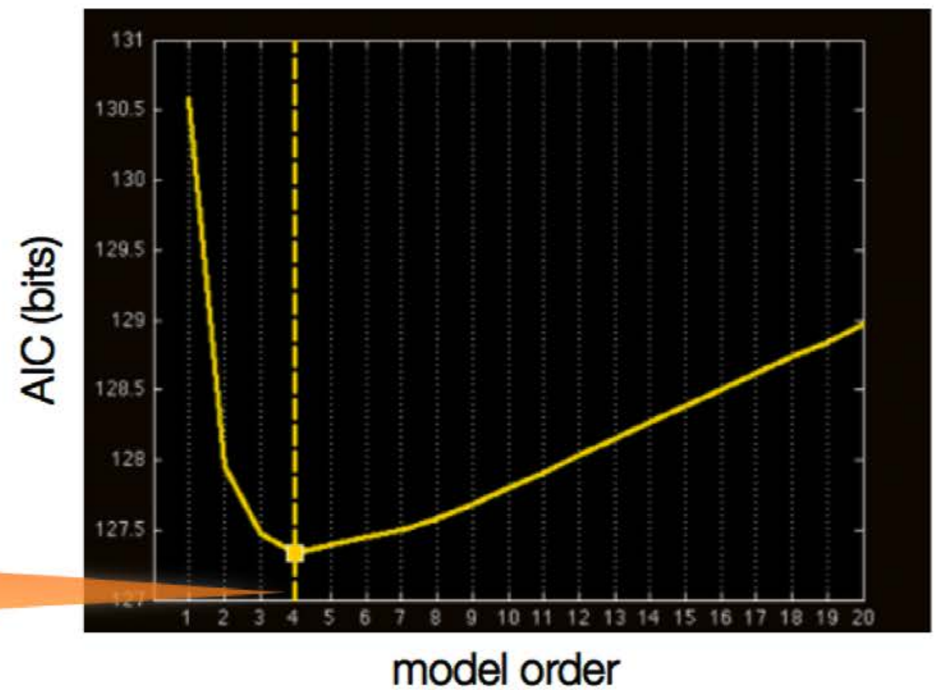
Selecting a VAR Model Order

- Model order is typically determined by minimizing information criteria such as Akaike Information Criterion (AIC) for varying model order (p):

$$\mathrm{AIC}(p) = 2\log(\det(\mathbf{V})) + M^2p/N$$

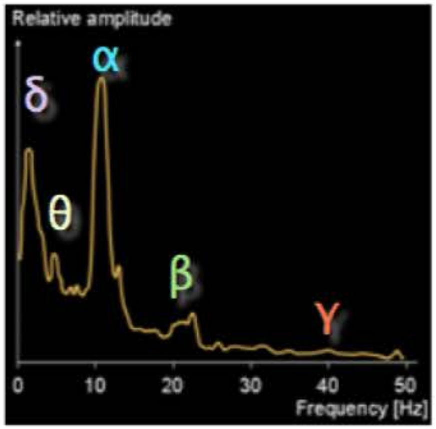
Penalizes high model orders (parsimony)

entropy rate (amount of prediction error)



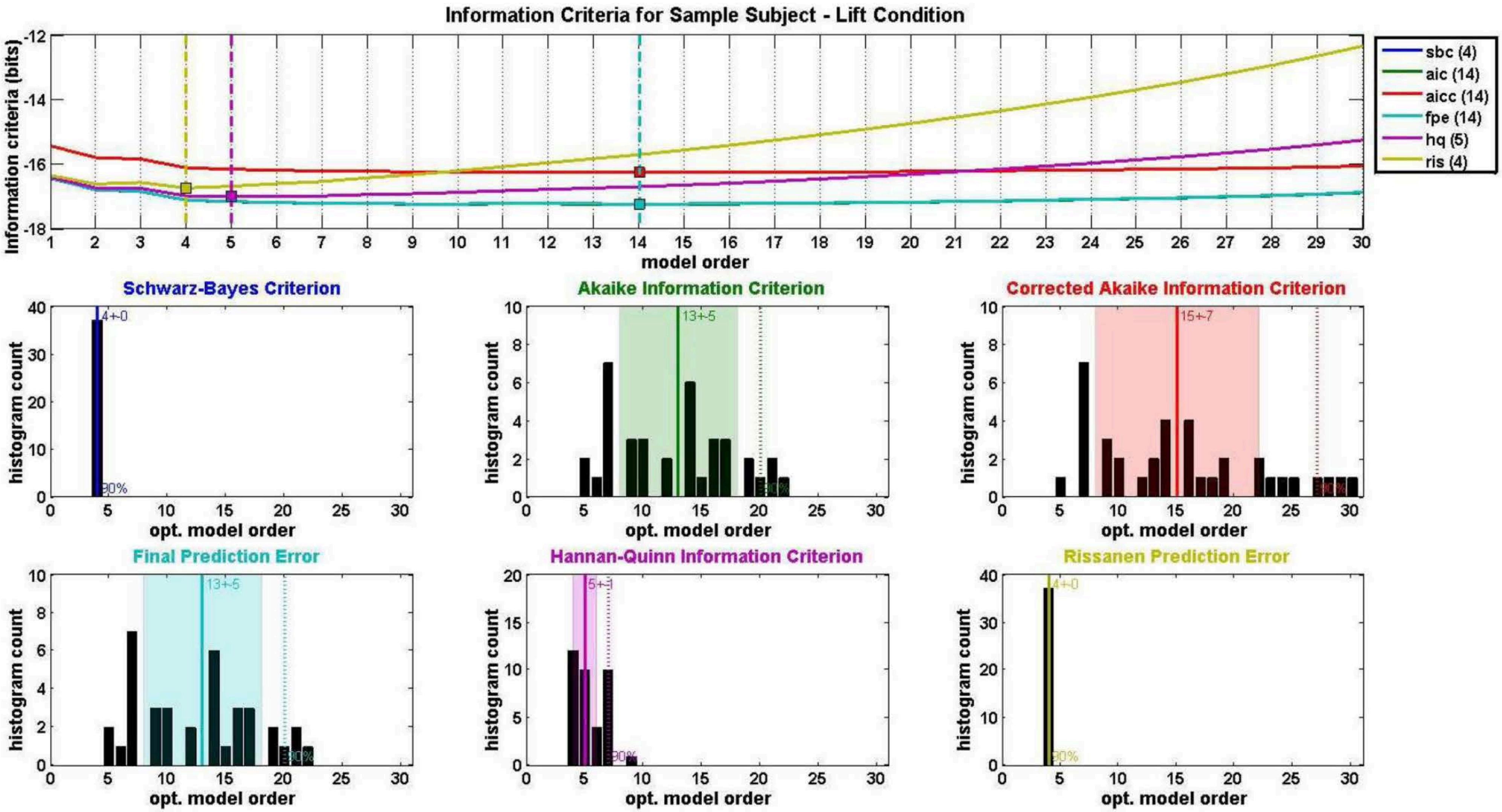
Selecting a VAR Model Order

- Other considerations:
  - A M-dimensional VAR model of order *p* has at most *Mp/2* spectral peaks distributed amongst the *M* variables. This means we can observe at most *p/2* peaks in each variables' spectrum (or in the causal spectrum between each pair of variables)



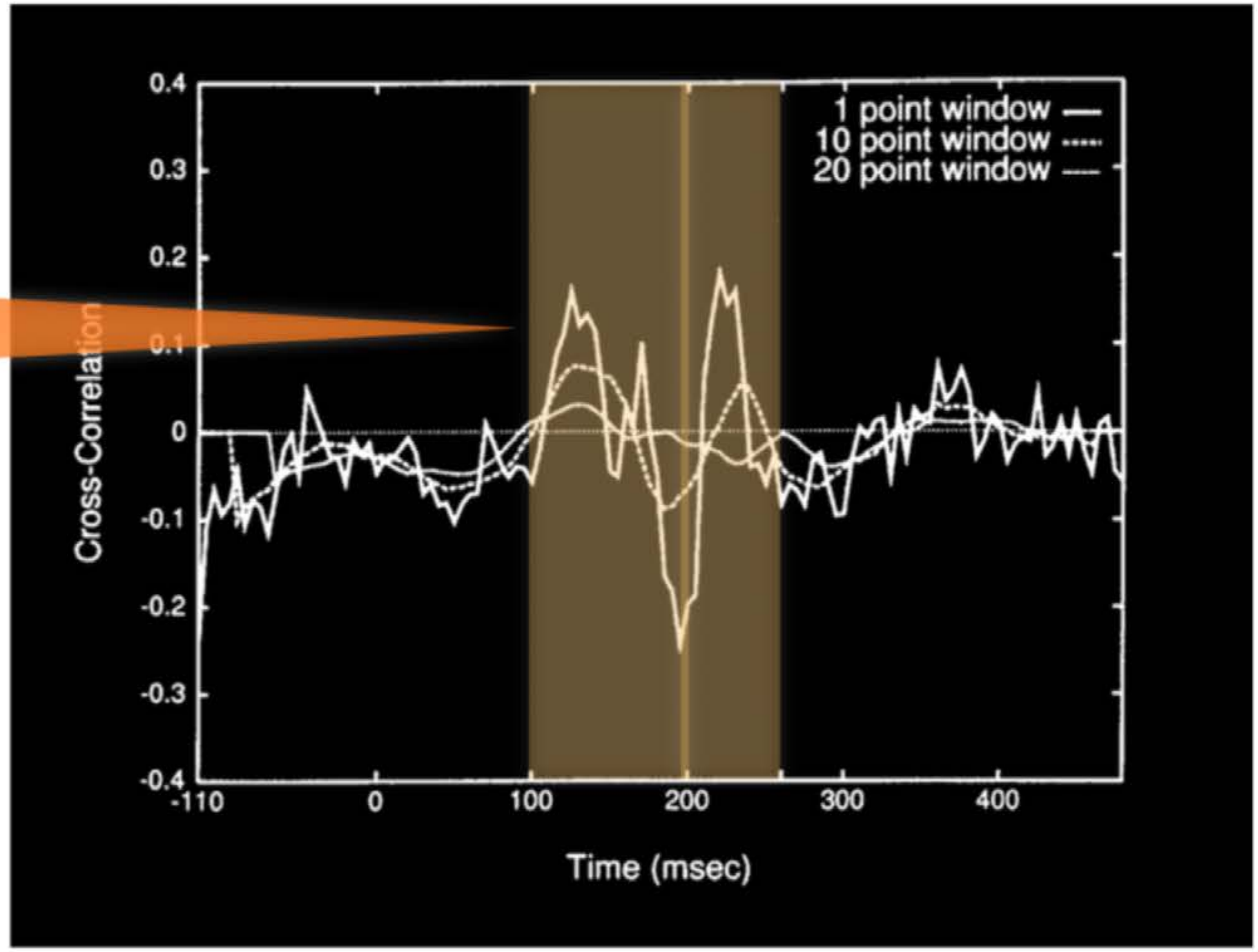
  - Optimal model order depends on sampling rate (higher sampling rate often requires higher model orders)

Order selection in reality



Consideration: Local Stationarity

Too-large windows may not be locally-stationary



Consideration: Sufficient data

M = number of variables
p = model order
N_{tr} = number of trials
W = length of each window (sample points)

We have M^2p model coefficients to estimate. This requires a minimum of M^2p independent samples.
So we have the constraint $M^2p <= N_{tr} W$.
In practice, however, a better heuristic is $M^2p <= (1/10)N_{tr} W$.

Or: $\mathbf{W >= 10(M^2p/N_{tr})}$

10x more data points than parameters to estimate

SIFT will let you know if your window length is not optimal

Example Application

EEG-Based Quantification of Cortical Current Density and Dynamic Causal Connectivity Generalized across Subjects Performing BCI-Monitored Cognitive Tasks

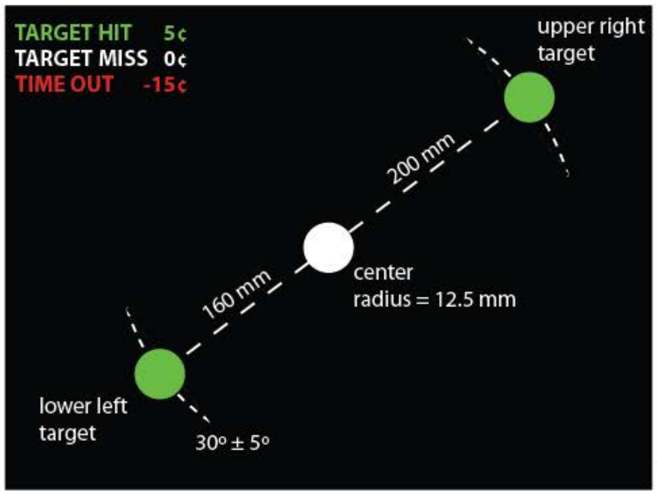
Hristos Courellis[1,2], Tim Mullen[1], Howard Poizner[3], Gert Cauwenberghs[2,3] and John R. Iversen[1]*

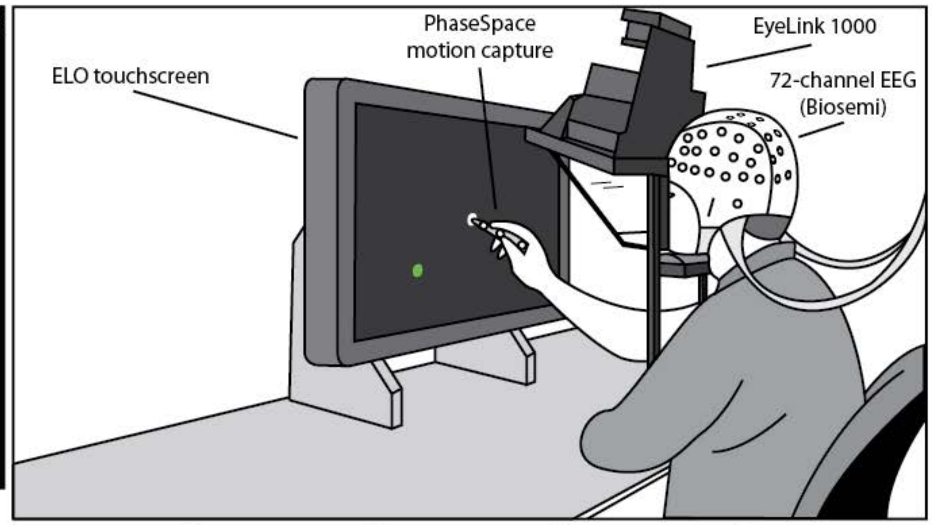
Frontiers in Neuroscience | www.frontiersin.org

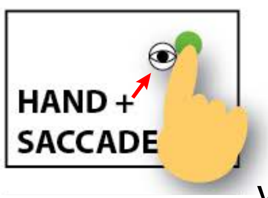
May 2017 | Volume 11 | Article 180

How does brain plan visually guided movements?

- Pointing Task (Park, et al. 2014, *IEEE Trans Neural Syst Rehabil Eng)*

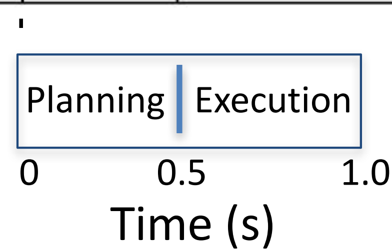






vs.

1	2	3	4	5
hold	target onset hold	center offset	eye/hand initiation	eye/hand arrival, feedback
500 - 700	500 - 700	< time window (e.g., 450 ms)		

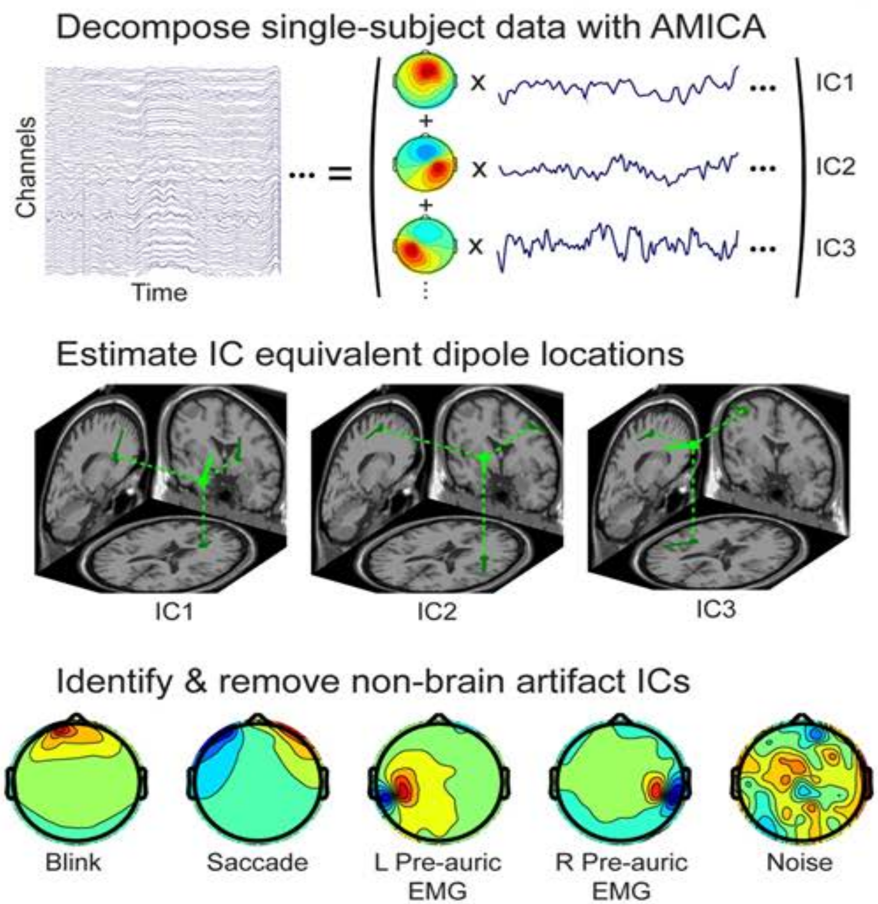


← Analysis Window

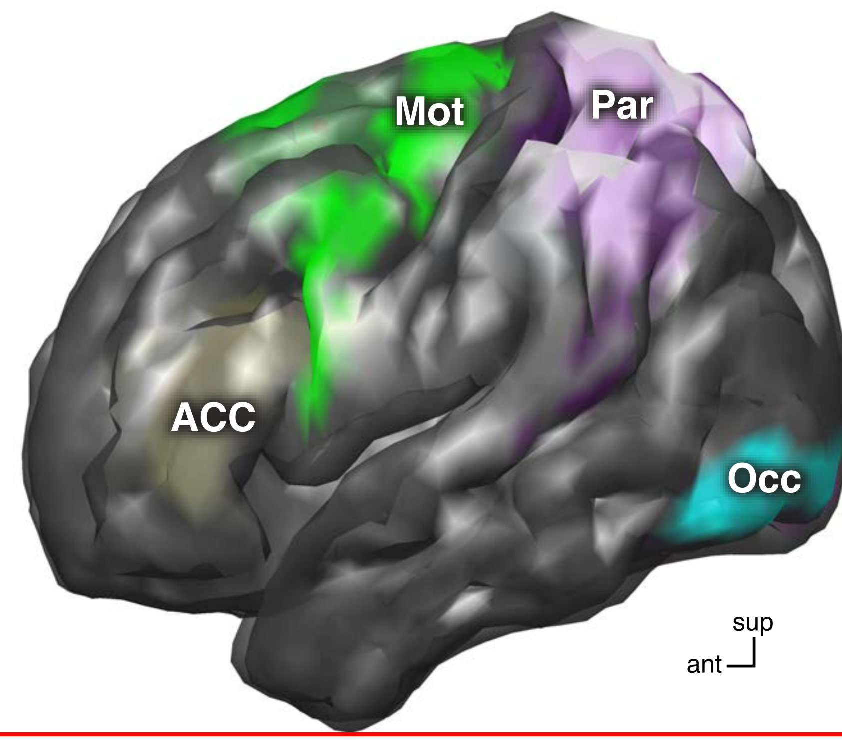
N=10 (right-handed, mean age=21)
70 channel EEG (Biosemi)
512 Hz; 128Hz for connectivity

ICA source space analysis

Independent Component Analysis



Cortical ROIs



Group SIFT: Project ICs onto cortical surface using LORETA; extract ROI time series. Advantage: Same ROIs for all subjects enables statistical comparison. (*Use BCILAB srcpot*)

Analysis Methods I

- Segmentation–based MVAR

$$\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}^{(k)}(t)\mathbf{X}(t-k) + \mathbf{E}(t)$$

$$\mathbf{A}(f) = -\sum_{k=0}^{p} \mathbf{A}^{(k)} e^{-i2\pi fk}; \mathbf{A}^{(0)} = I$$

$$\mathbf{A}(f)^{-1} = \mathbf{H}(f)$$

$$A(t) = \arg\min_{\hat{A}} \left(\overbrace{\left\| Y - Z\tilde{A} \right\|_2^2}^{\text{prediction error}} + \underbrace{\boxed{\lambda}}_{\text{regularization}} \underbrace{\sum_{ij} \left\| \overbrace{\tilde{A}_{ij}^{(1)}, \ldots, \tilde{A}_{ij}^{(p)}}^{\text{smoothness (L2) (preserves spectrum)}} \right\|_2}_{\text{group sparsity (L1)}} \right)$$

Analysis Methods II

- Time-varying SdDTF ("short-time direct directed transfer function")

- Directed measure of direct (unmediated) causal flow between ROIs

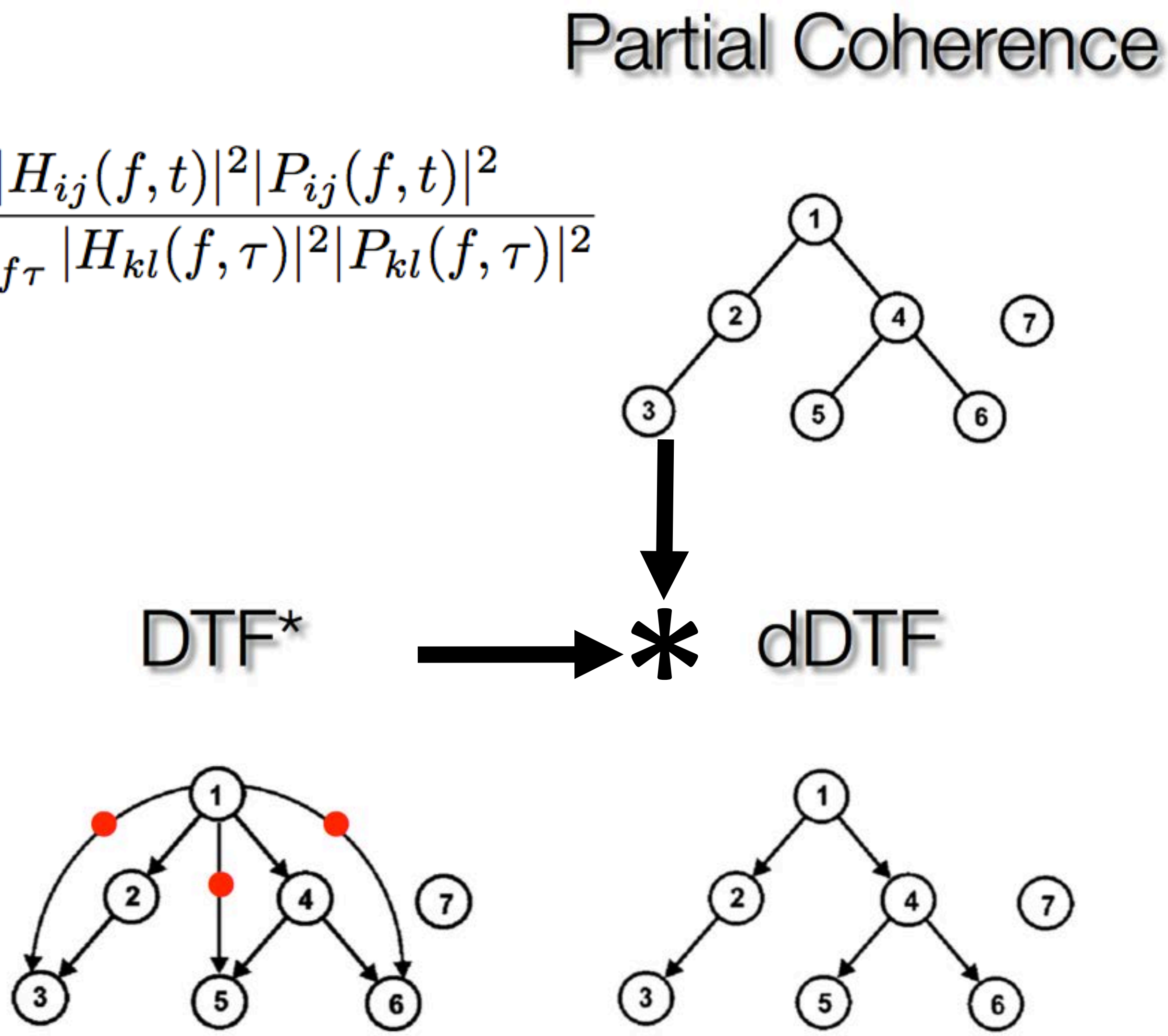
- Combines DTF and partial coherence; windowed (0.5s, 30ms).

$$\eta_{ij}^2(f,t) = \frac{|H_{ij}(f,t)|^2 |P_{ij}(f,t)|^2}{\sum_{klf\tau} |H_{kl}(f,\tau)|^2 |P_{kl}(f,\tau)|^2}$$

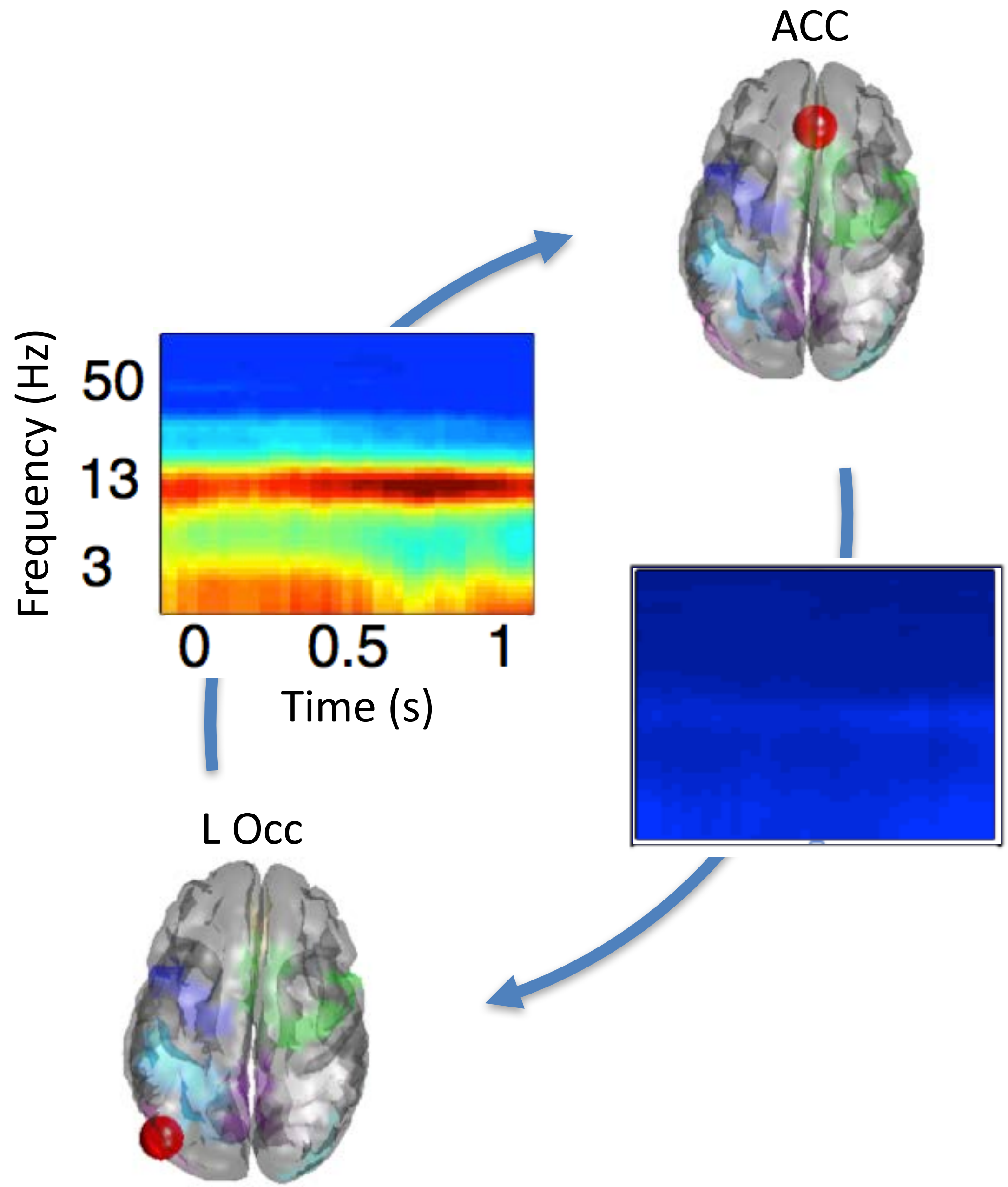
(Korzeniewska, et al. 2008)

dDTF

$$\eta_{ij}^2(f,t) = \frac{|H_{ij}(f,t)|^2 |P_{ij}(f,t)|^2}{\sum_{klf\tau} |H_{kl}(f,\tau)|^2 |P_{kl}(f,\tau)|^2}$$



SIFT Analysis

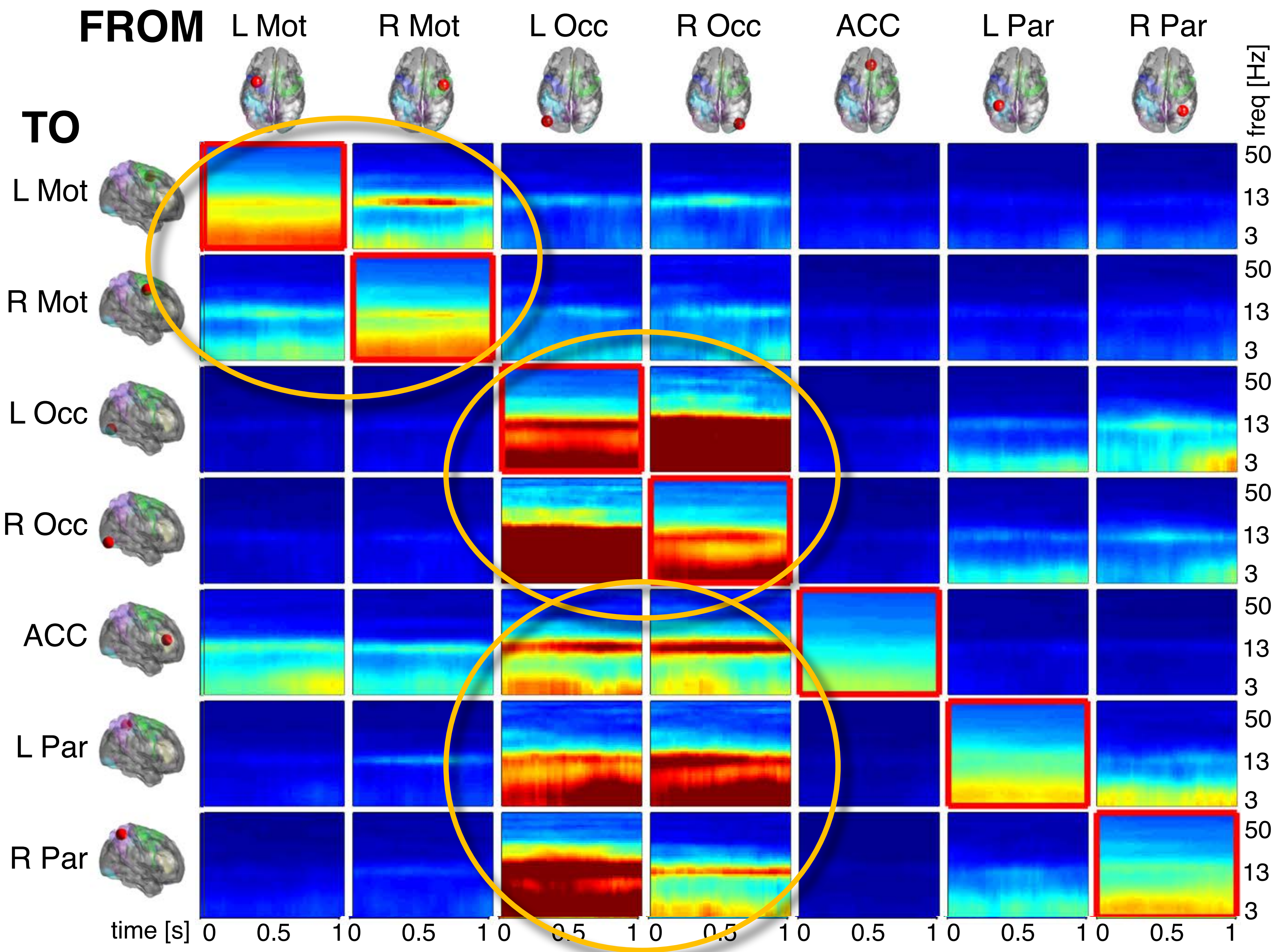


- Time-varying SdDTF

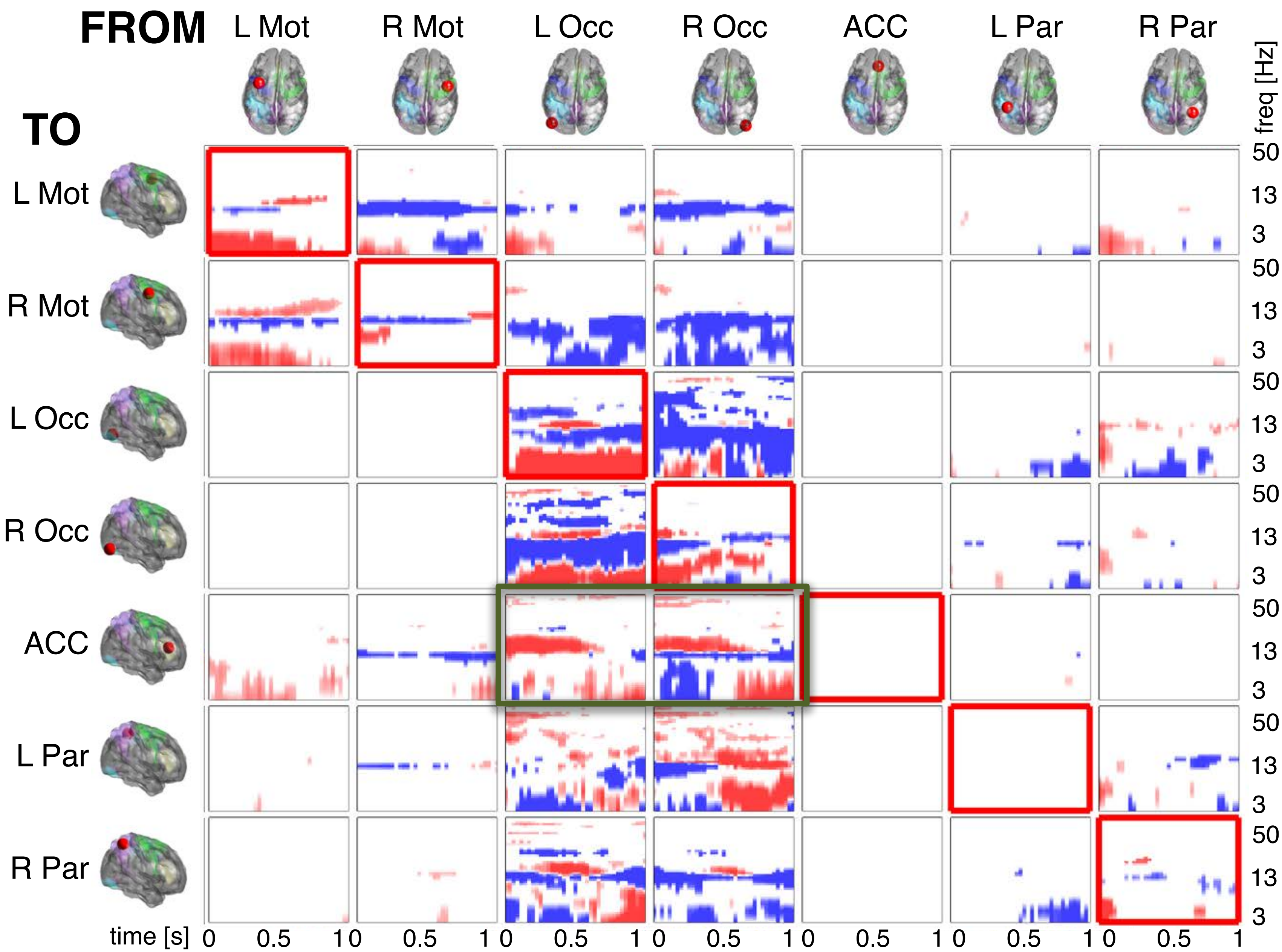
Directed measure of direct causal flow between ROIs

Averaged across subjects

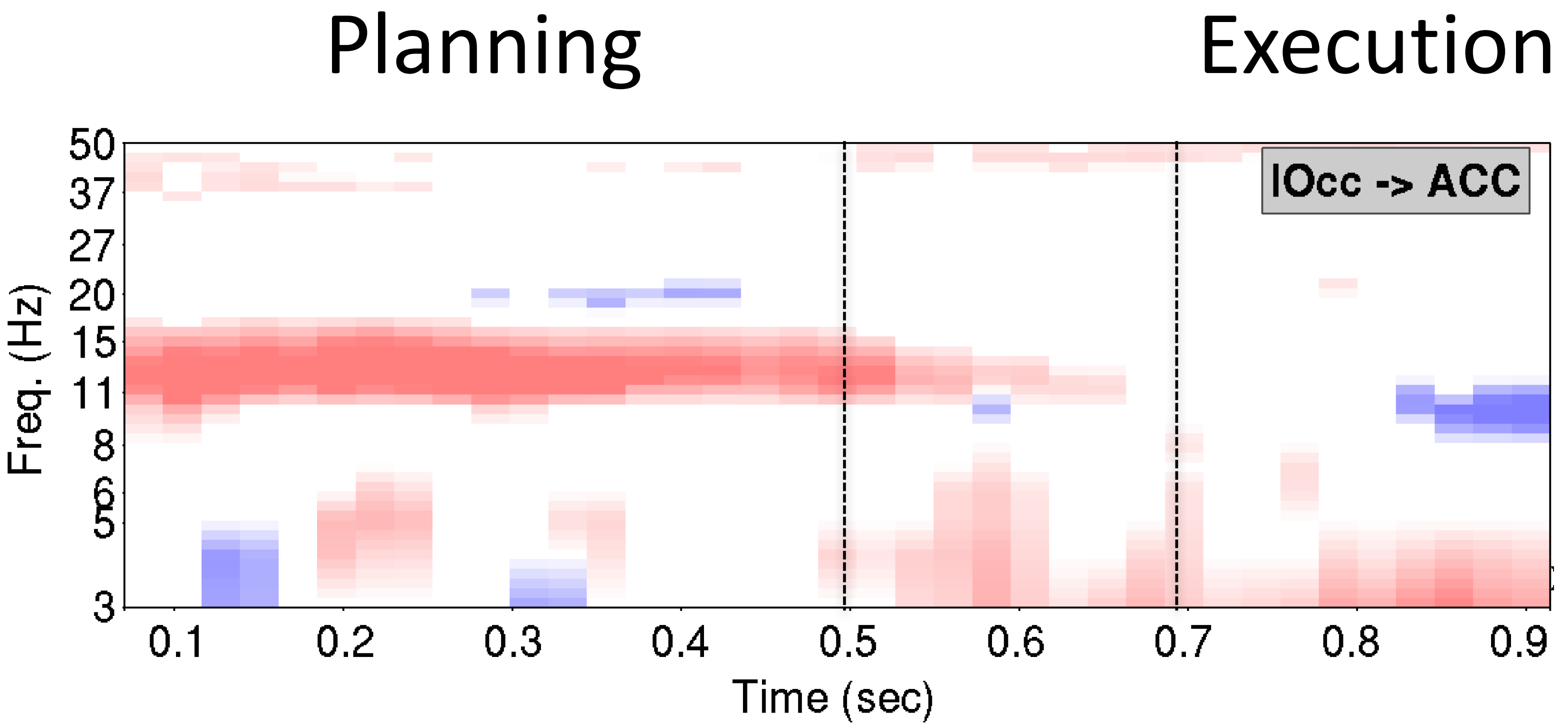
dDTF during reaching



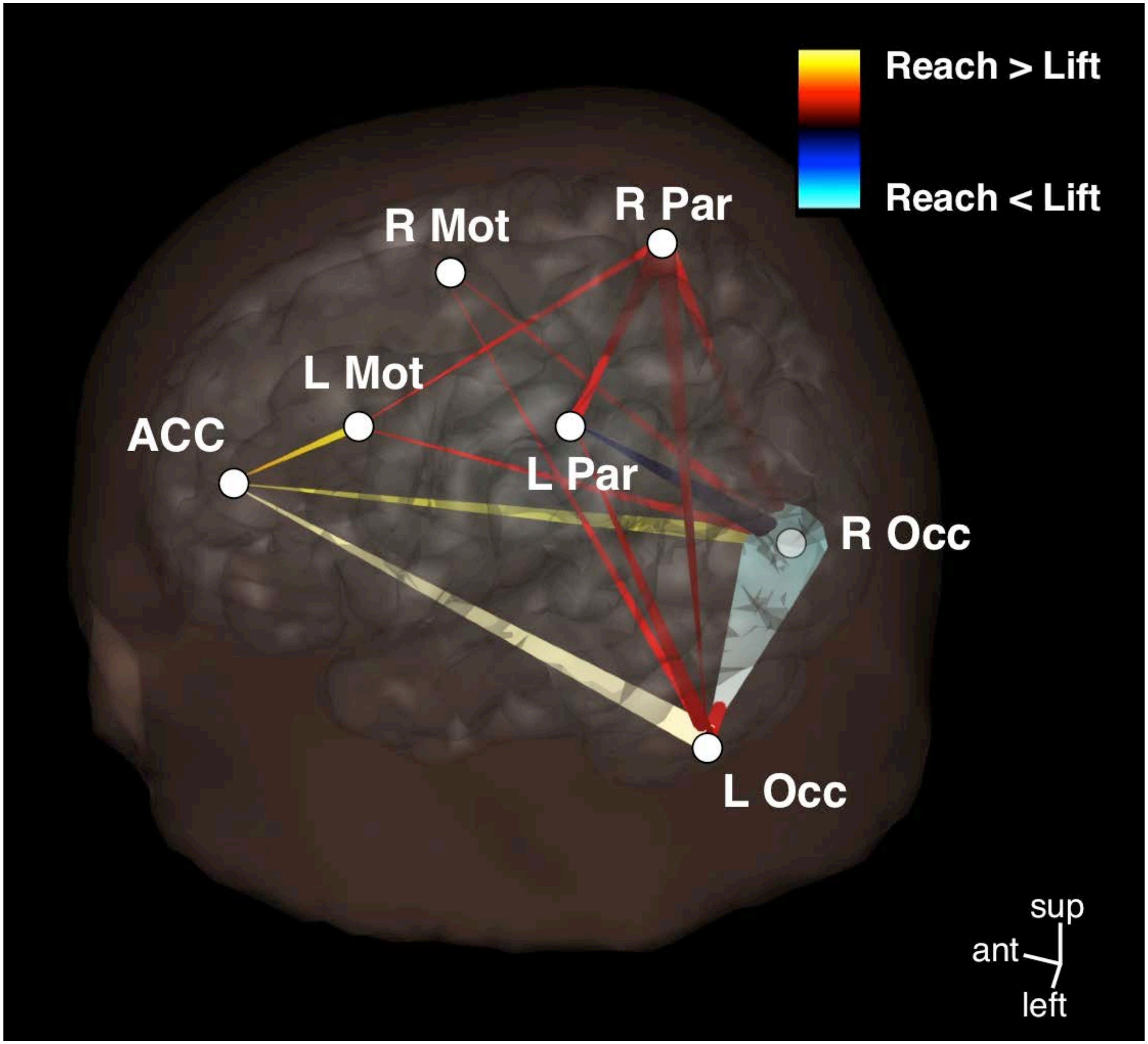
Changed causal flow during reaching



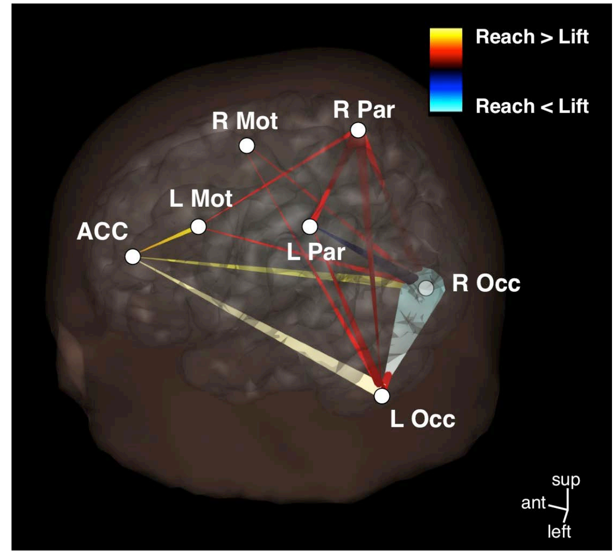
Occipital → ACC



Greater causal flow during movement planning



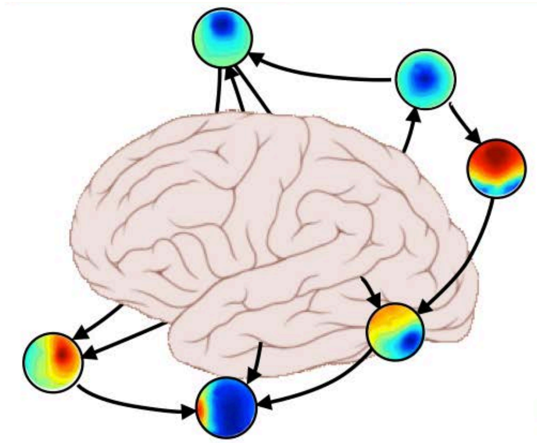
Discussion



- SIFT is a capable toolkit for causal dynamical analysis at source level
- **Parietal** network expected for visually guided action (e.g. Heider, et al., 2010)
- **ACC** more strongly driven by Occipital & Motor. Locus for translation of intention into action (Paus, 2001; Srinivasan, et al. 2013). ACC drives SMA (not shown).
- Causal network results depend on the number of nodes
  - E.g. Occipital → ACC could be mediated by region not included in model
  - There will always be a tradeoff between network size and amount of data needed to fit the model.
  - Regularization

History of group-level SIFT

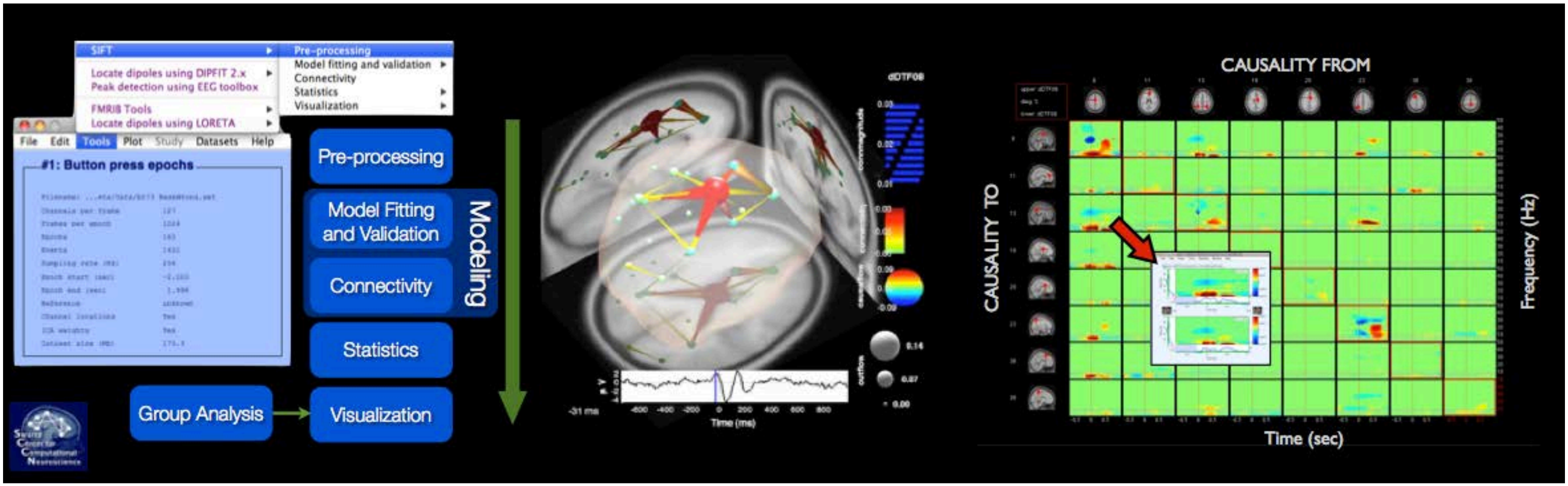
- Approaches
  - Tim Mullen & Wes Thompson (since 2010) '**Hierarchical Bayesian Modeling**' that interpolate missing values (i.e. inconsistency in dipole locations across subjects).
- ROI-based approaches
  - Iversen, et al, 2014; Courellis, et al, 2017: project IC activation onto cortical surface and define activity in anatomically defined cortical ROIs.
  - Nima Bigdely-Shamlo (in his PhD dissertation in 2014) **'Network Projection'** that uses dipole density and anatomical ROI. (Makoto Miyakoshi)



SIFT

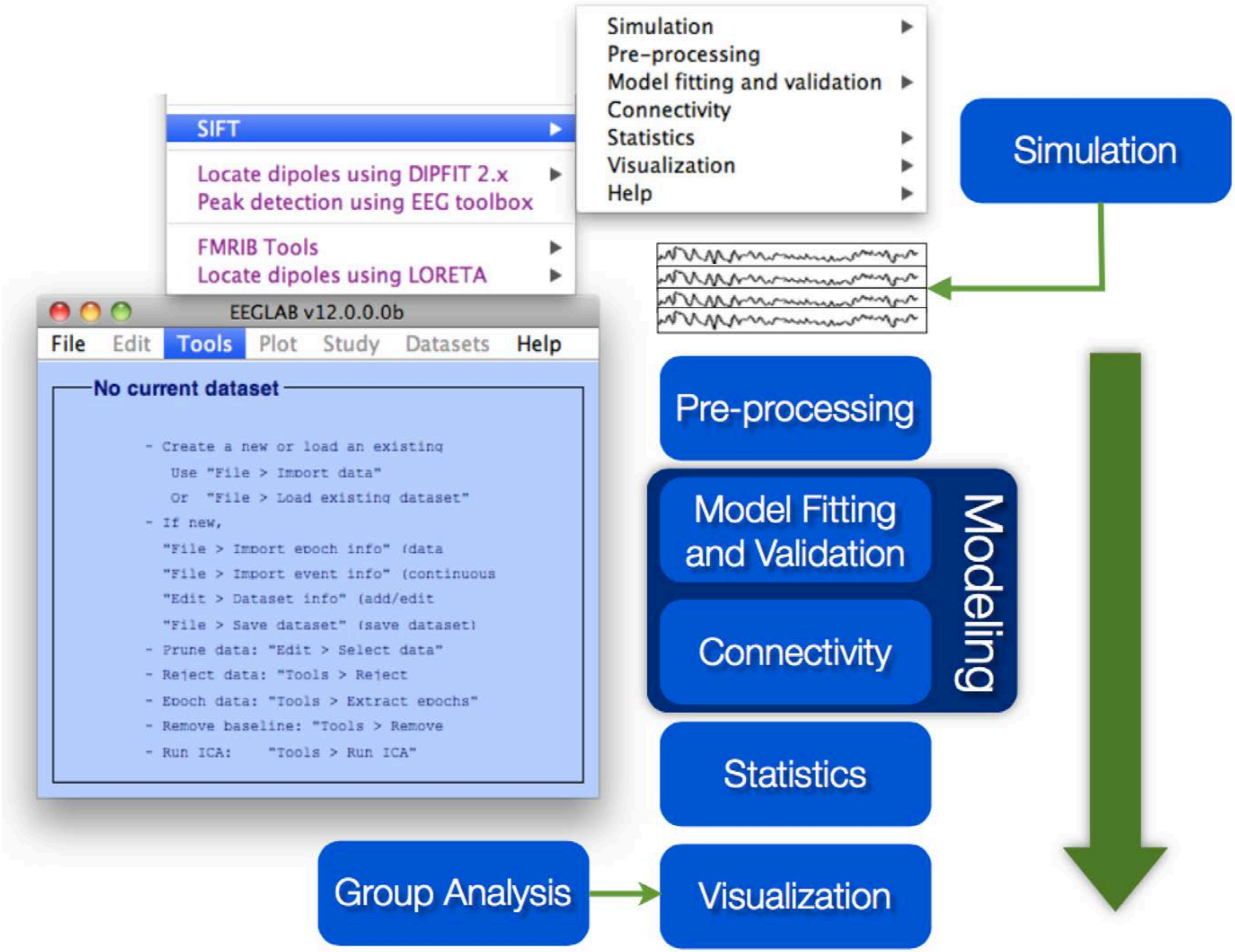
Source Information Flow Toolbox

http://sccn.ucsd.edu/wiki/SIFT
Mullen, et al, *Journal of Neuroscience Methods* (in prep, 2012)
Mullen, et al, *Society for Neuroscience*, 2010
Delorme, Mullen, Kothe et al, *Computational Intelligence and Neuroscience*, vol 12, 2011

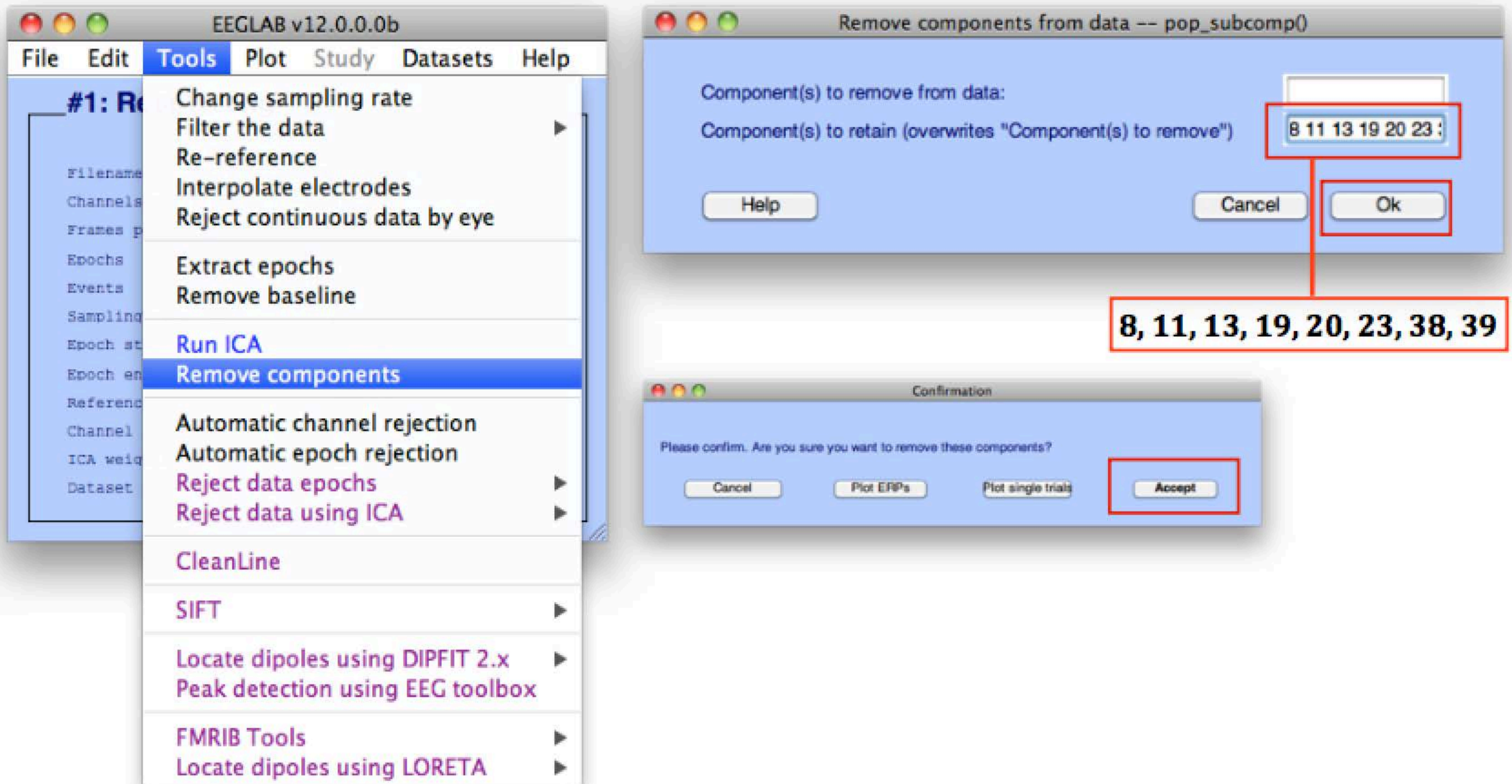


- A toolbox for (source-space) electrophysiological information flow and causality analysis (single- or multi-subject) integrated into the EEGLAB software environment.
- Emphasis on vector autoregression and time-frequency domain approaches
- Standard and novel interactive visualization methods for exploratory analysis of connectivity across time, frequency, and spatial location

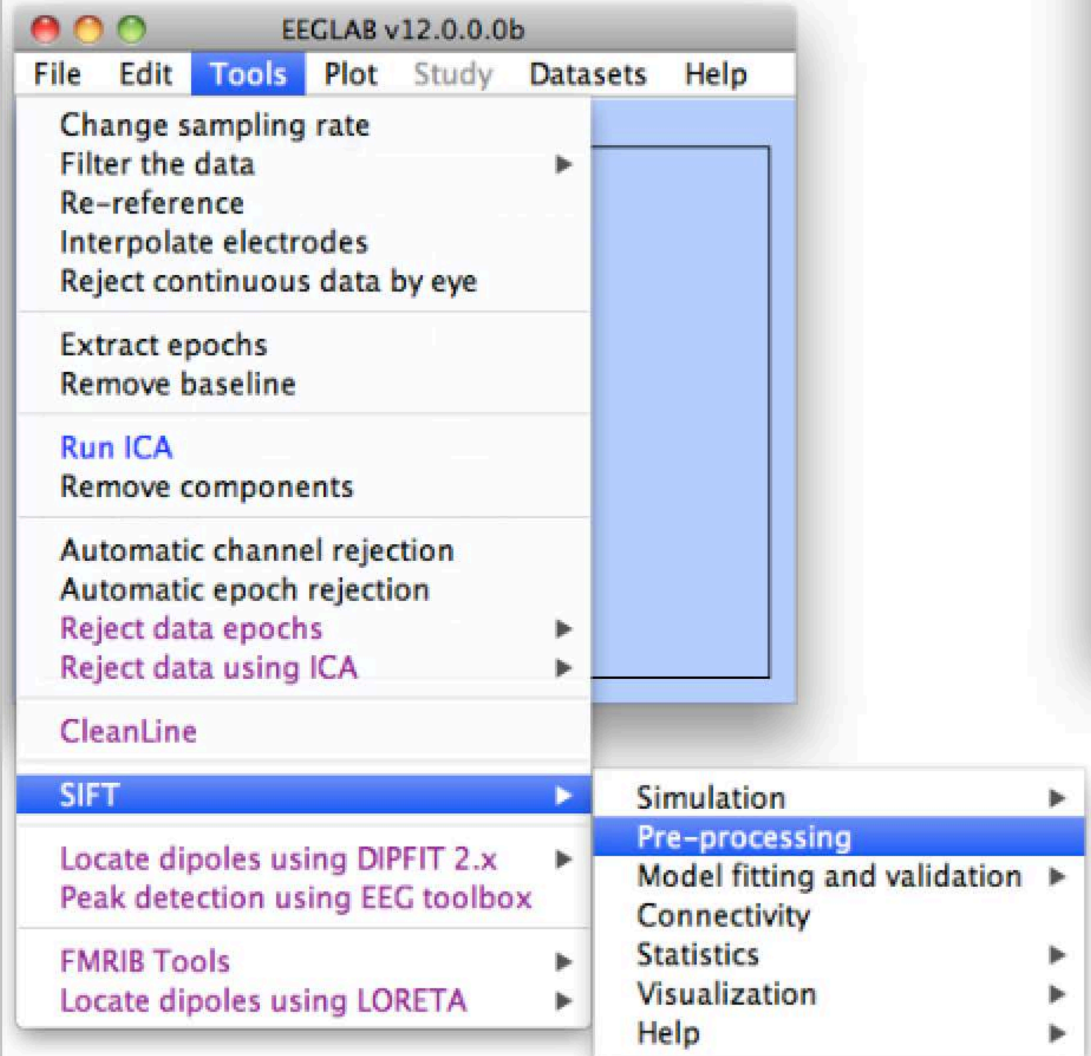
SIFT Workflow

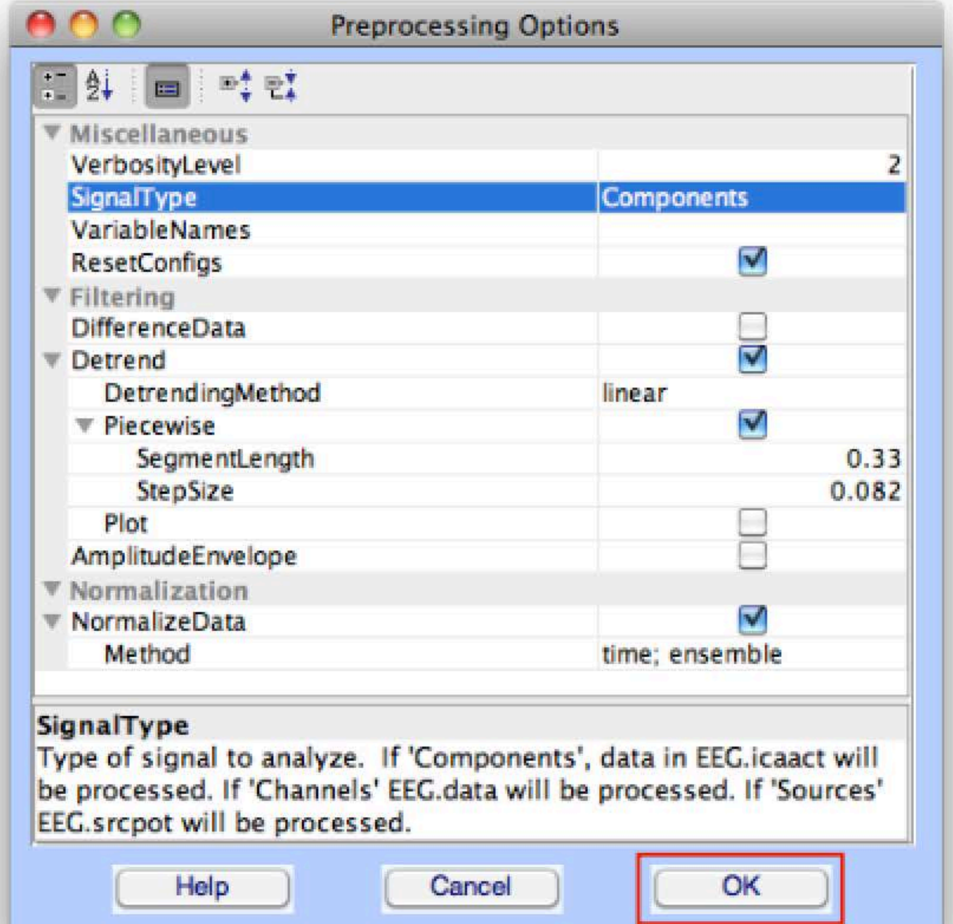


3 Preprocessing: Select Components

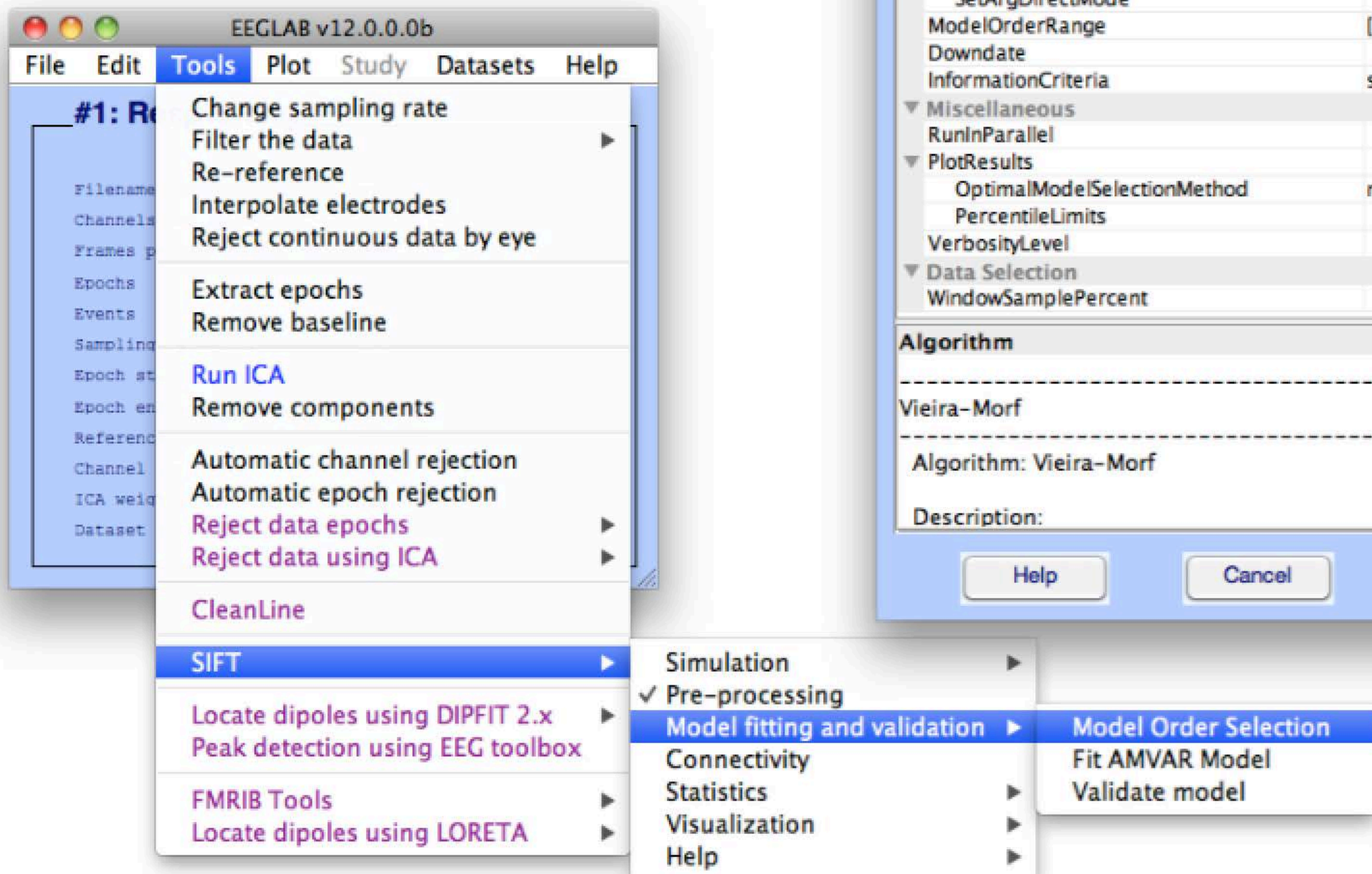


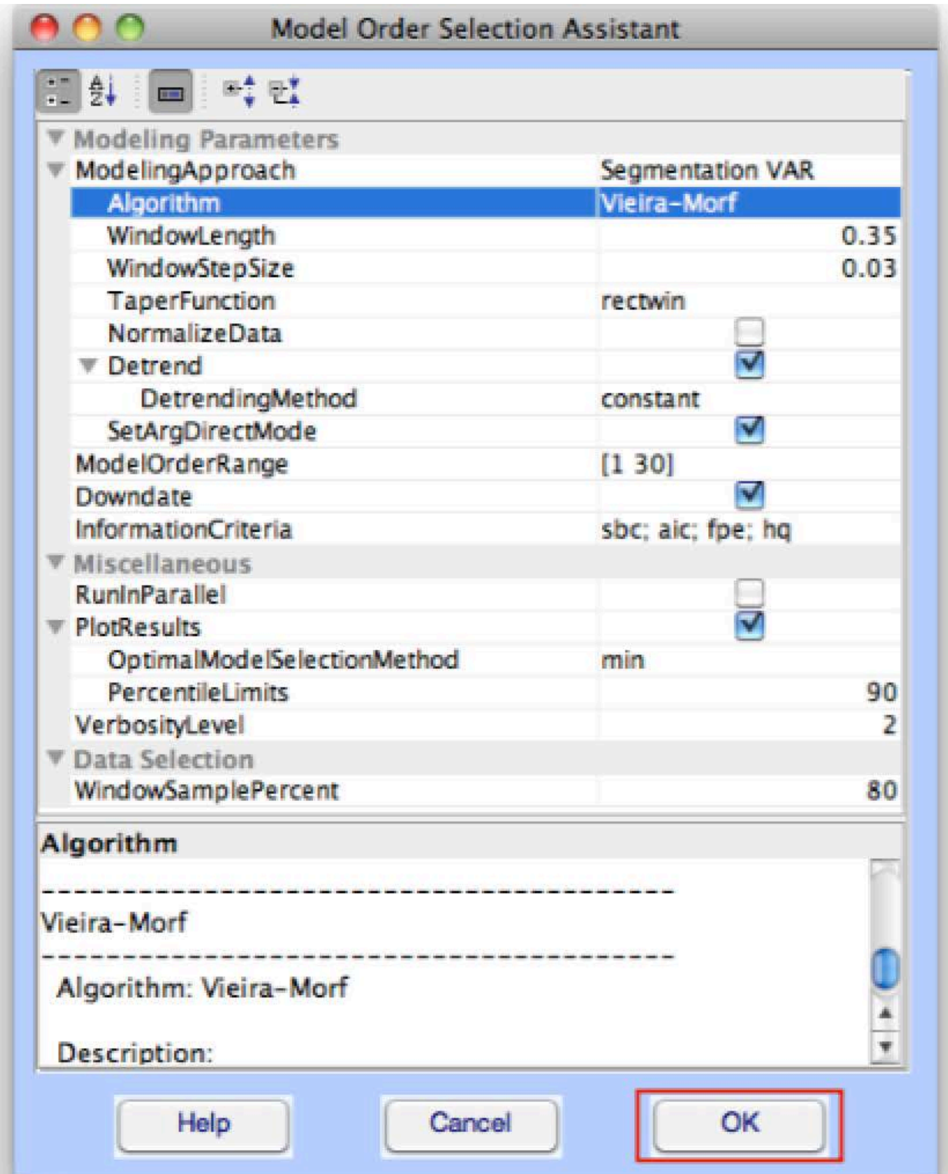
3 Preprocessing: SIFT





4 Model Order Selection





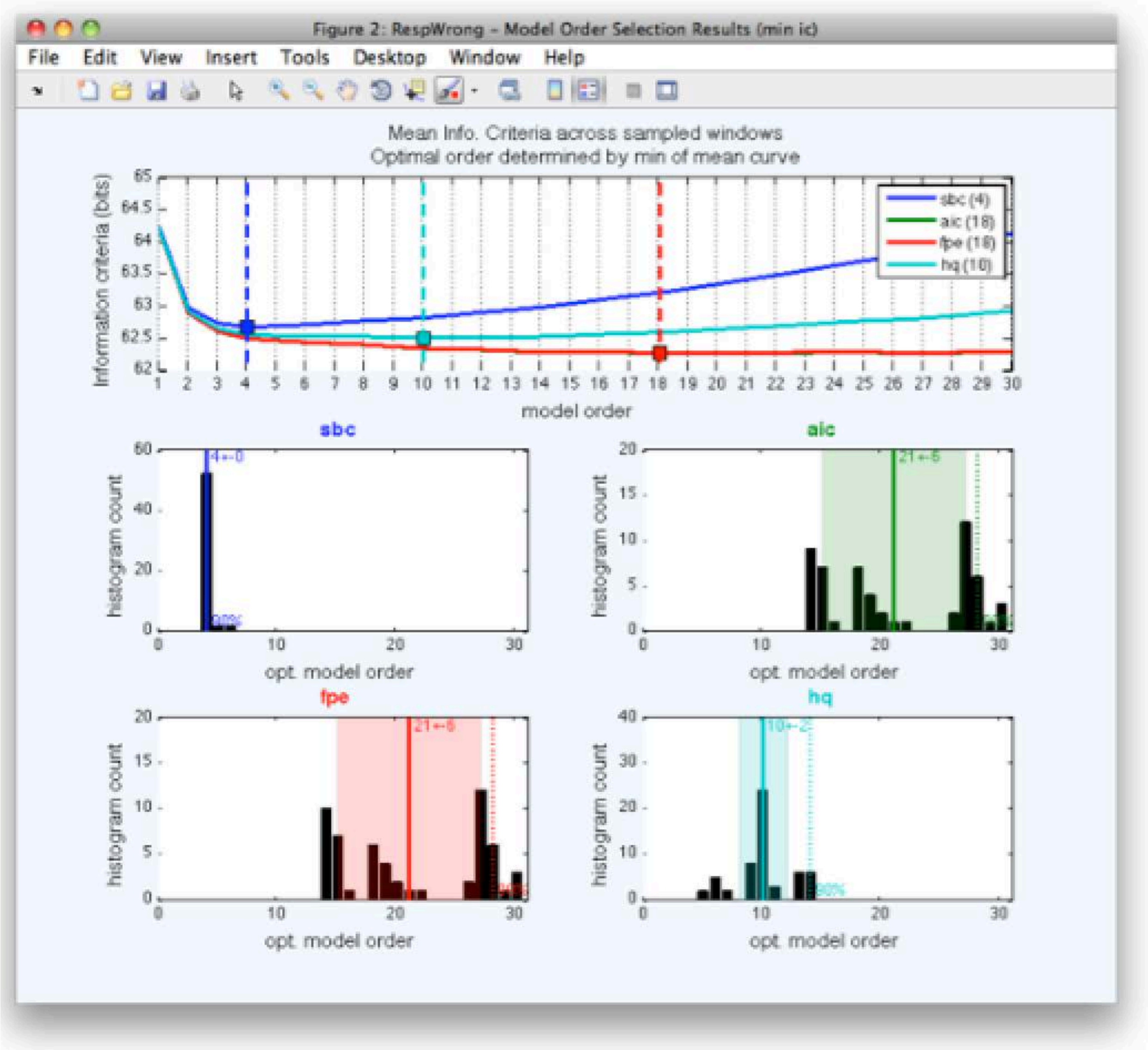
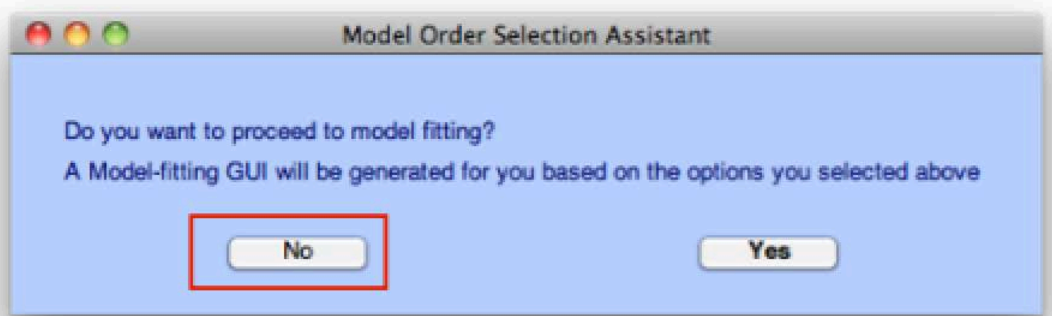
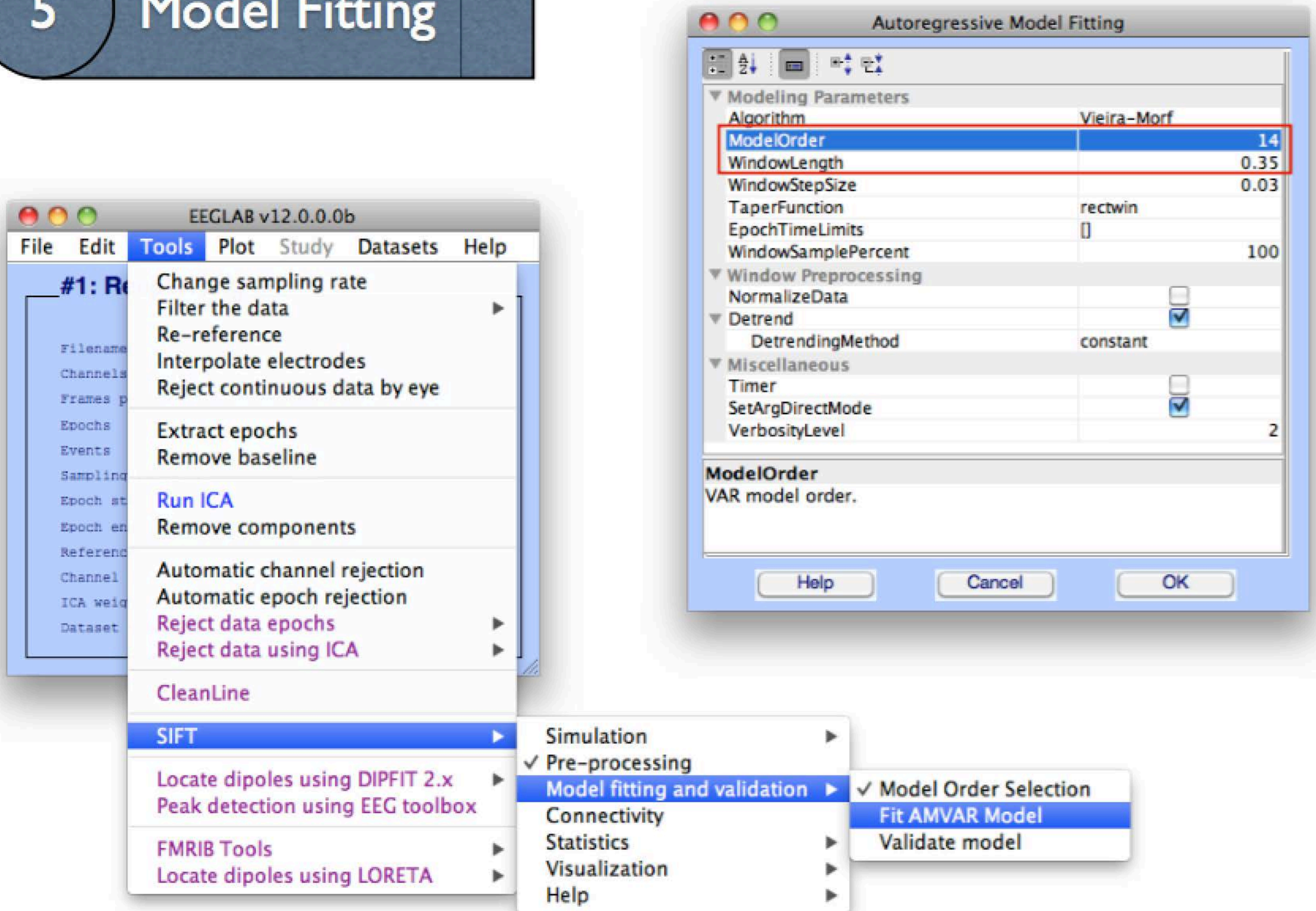


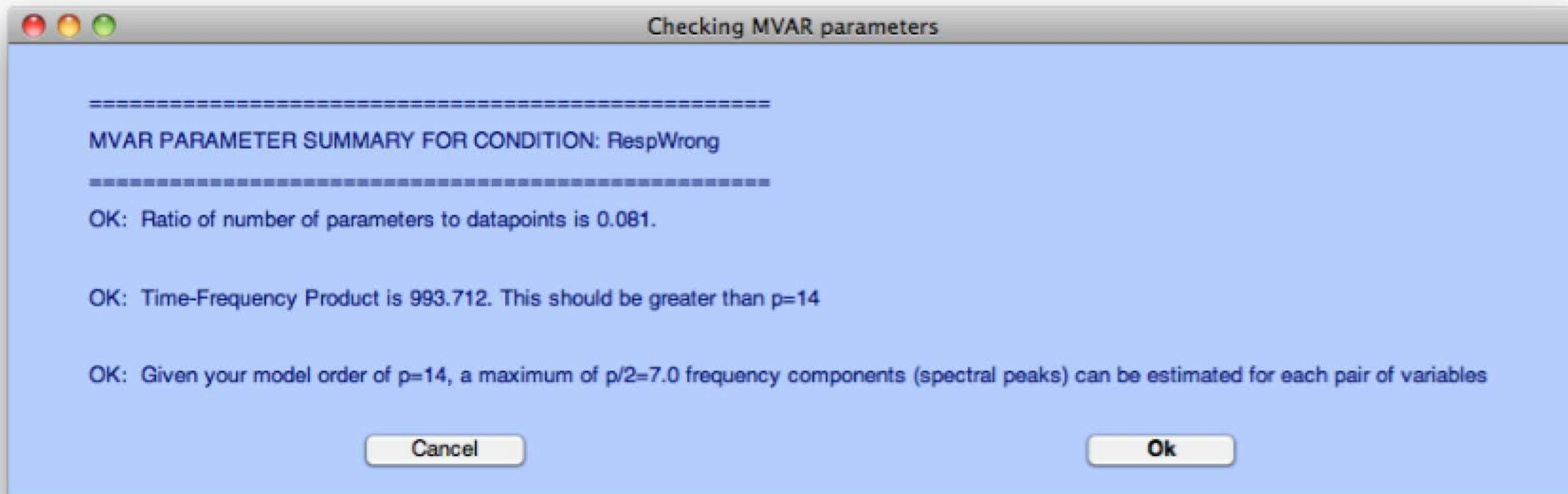
Figure 2: RespWrong - Model Order Selection Results (min ic)
File Edit View Insert Tools Desktop Window Help
Mean Info. Criteria across sampled windows
Optimal order determined by min of mean curve
Information criteria (bits)
model order
sbc (4)
aic (18)
fpe (18)
hq (10)
sbc
aic
fpe
hq
histogram count
opt. model order


Model Order Selection Assistant
Do you want to proceed to model fitting?
A Model-fitting GUI will be generated for you based on the options you selected above
No
Yes

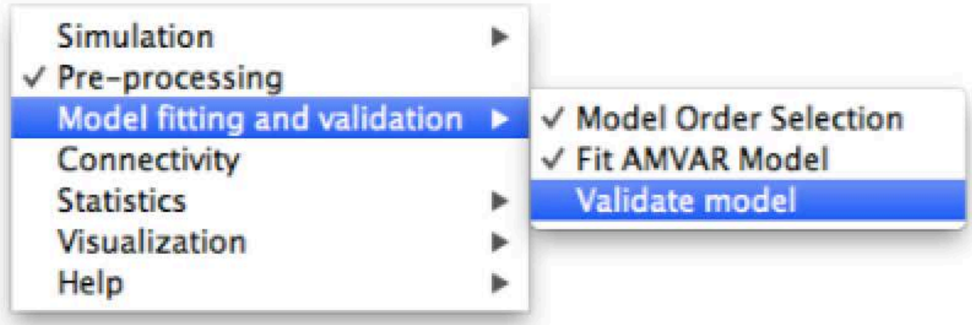
5 Model Fitting

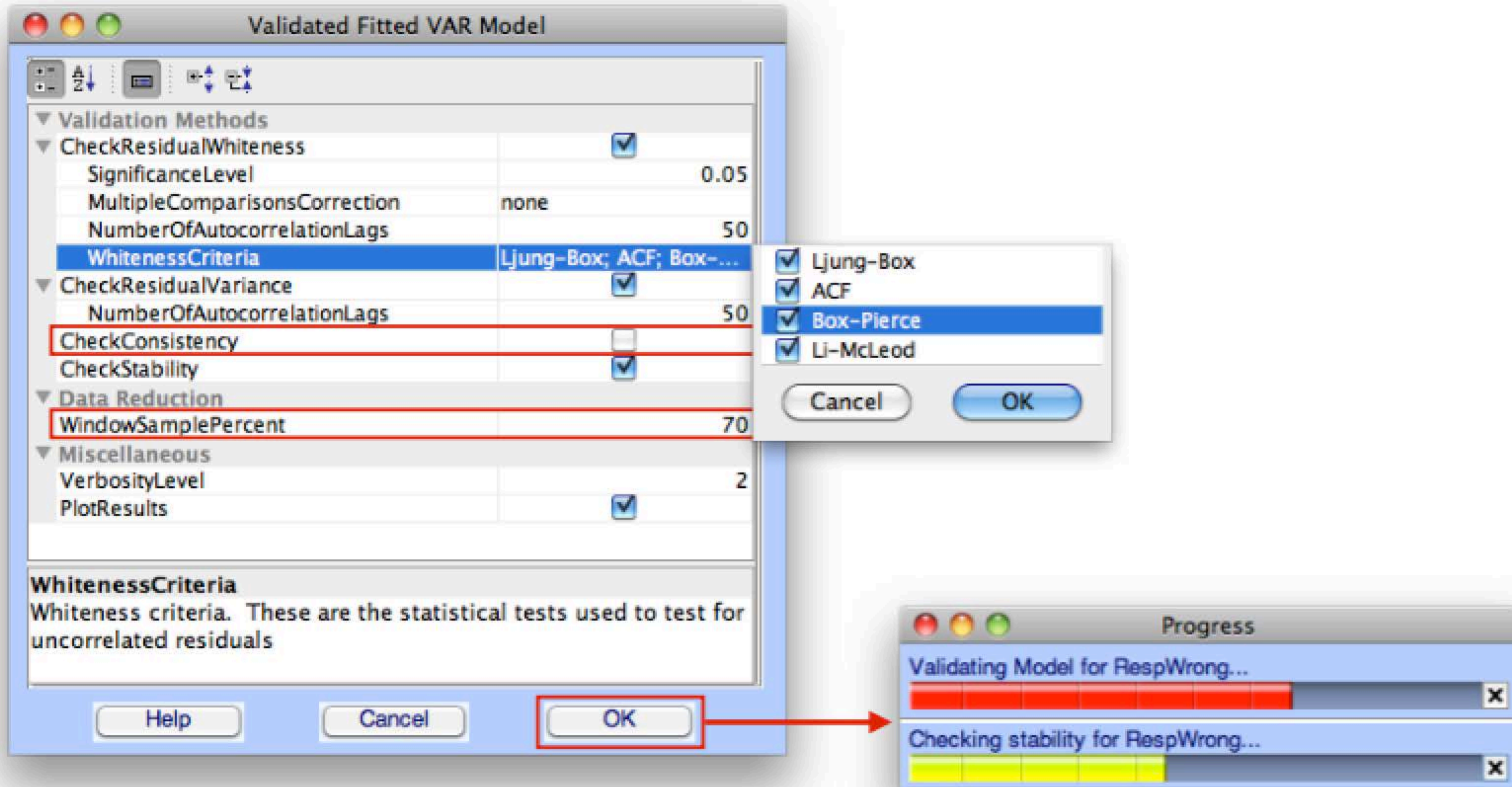


5 Model Fitting

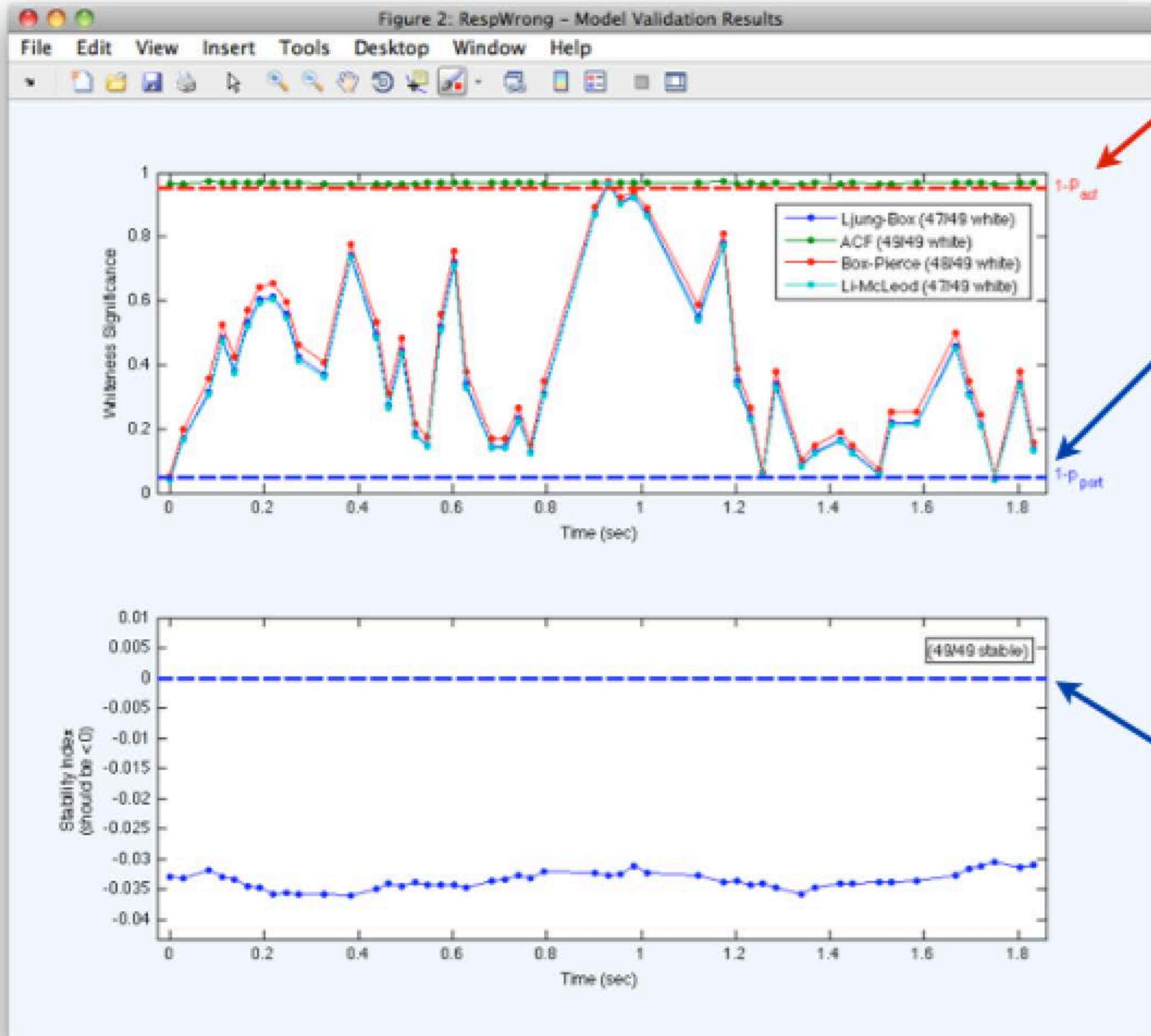


6 Model Validation





6 Model Validation

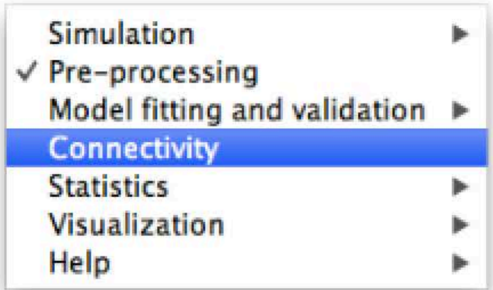


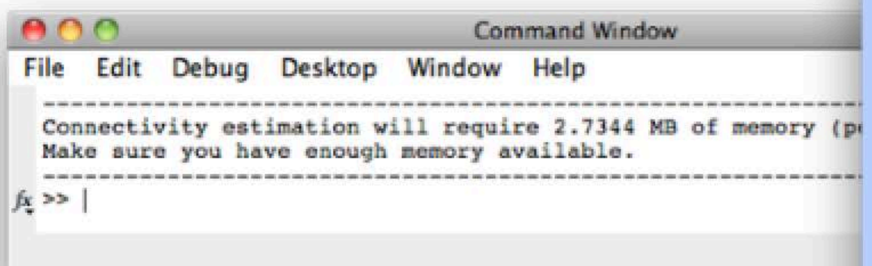
ACF statistic should be above this line

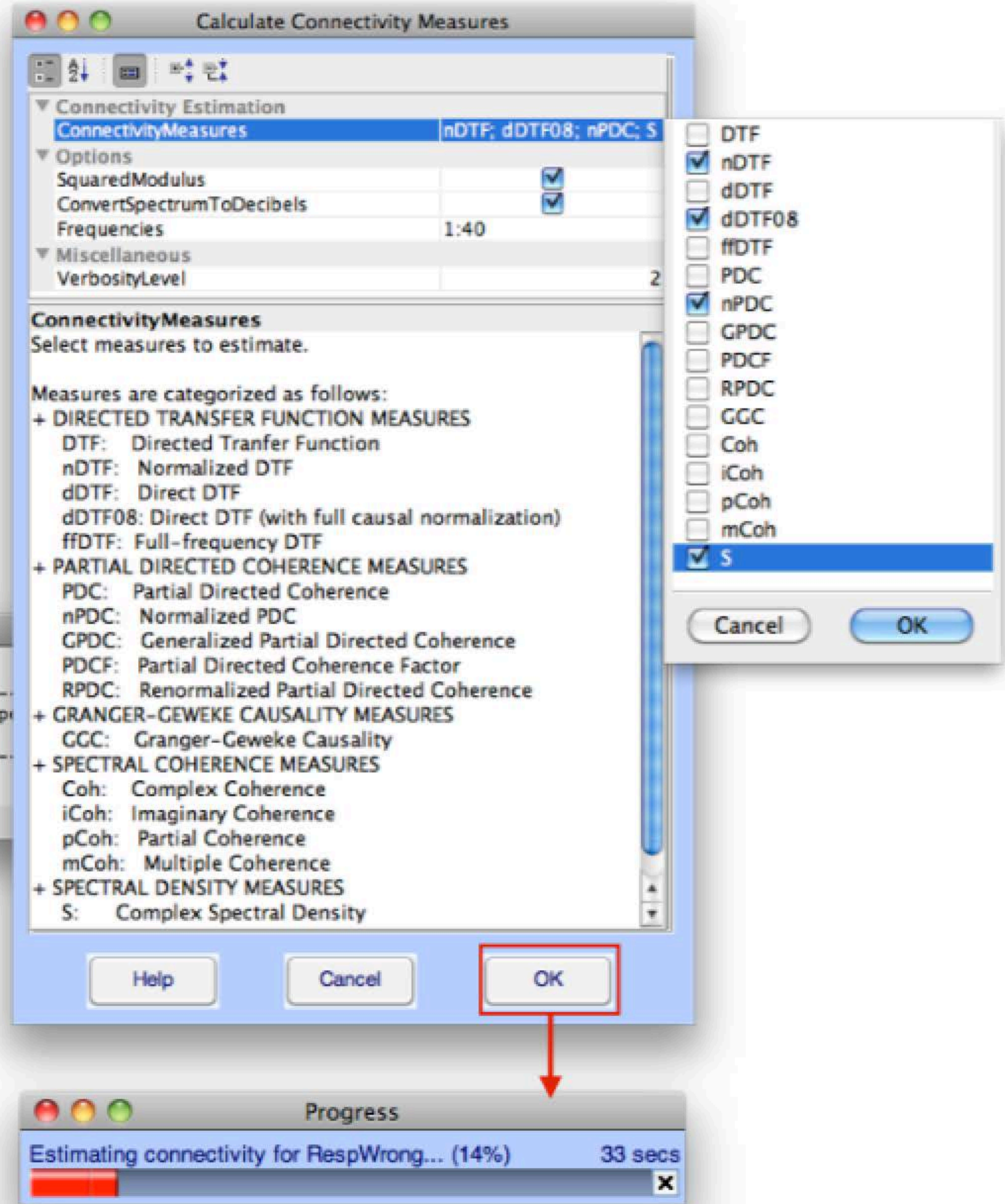
Portmanteau statistics should be above this line

Stability index should be < 0

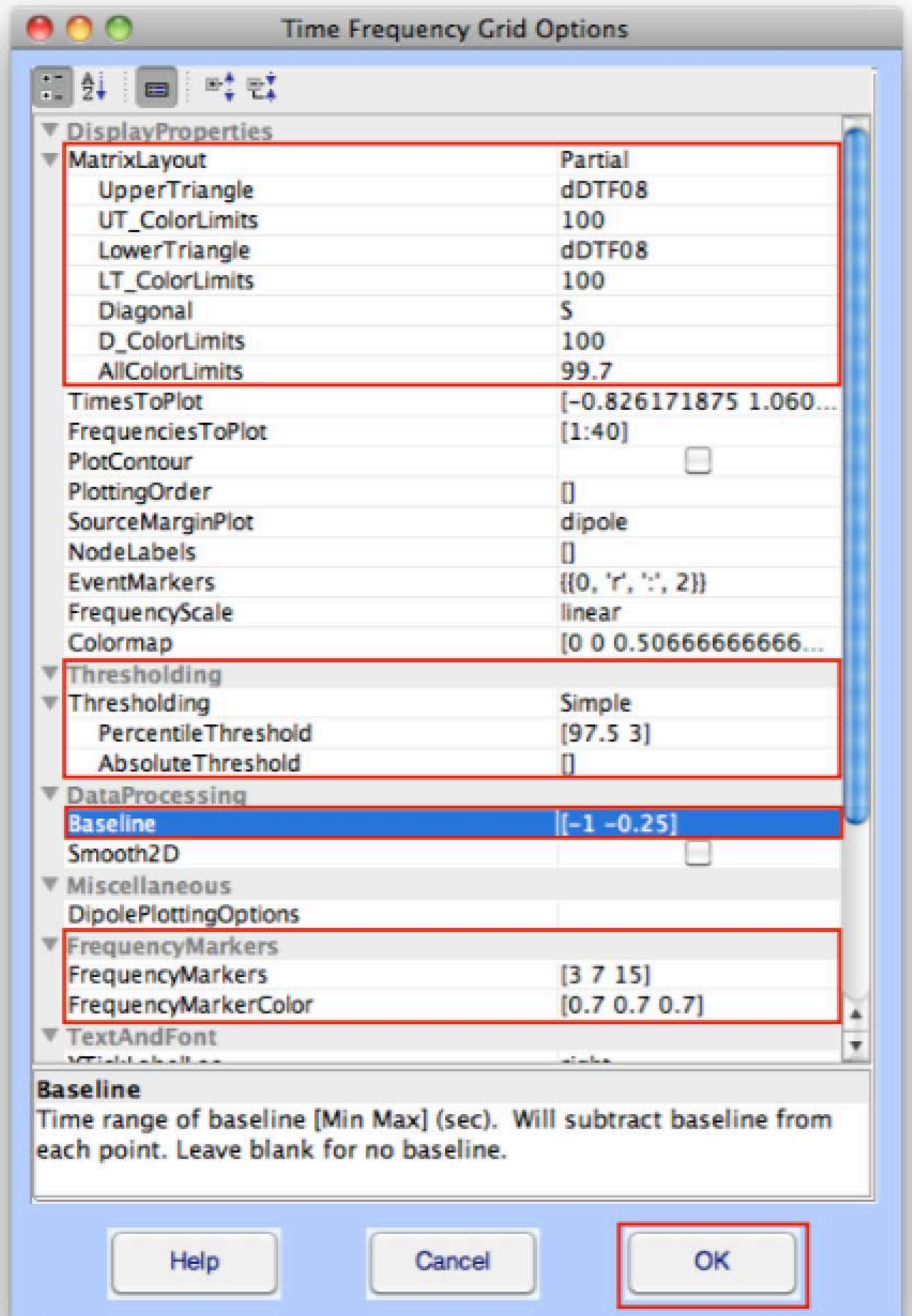
7 Connectivity



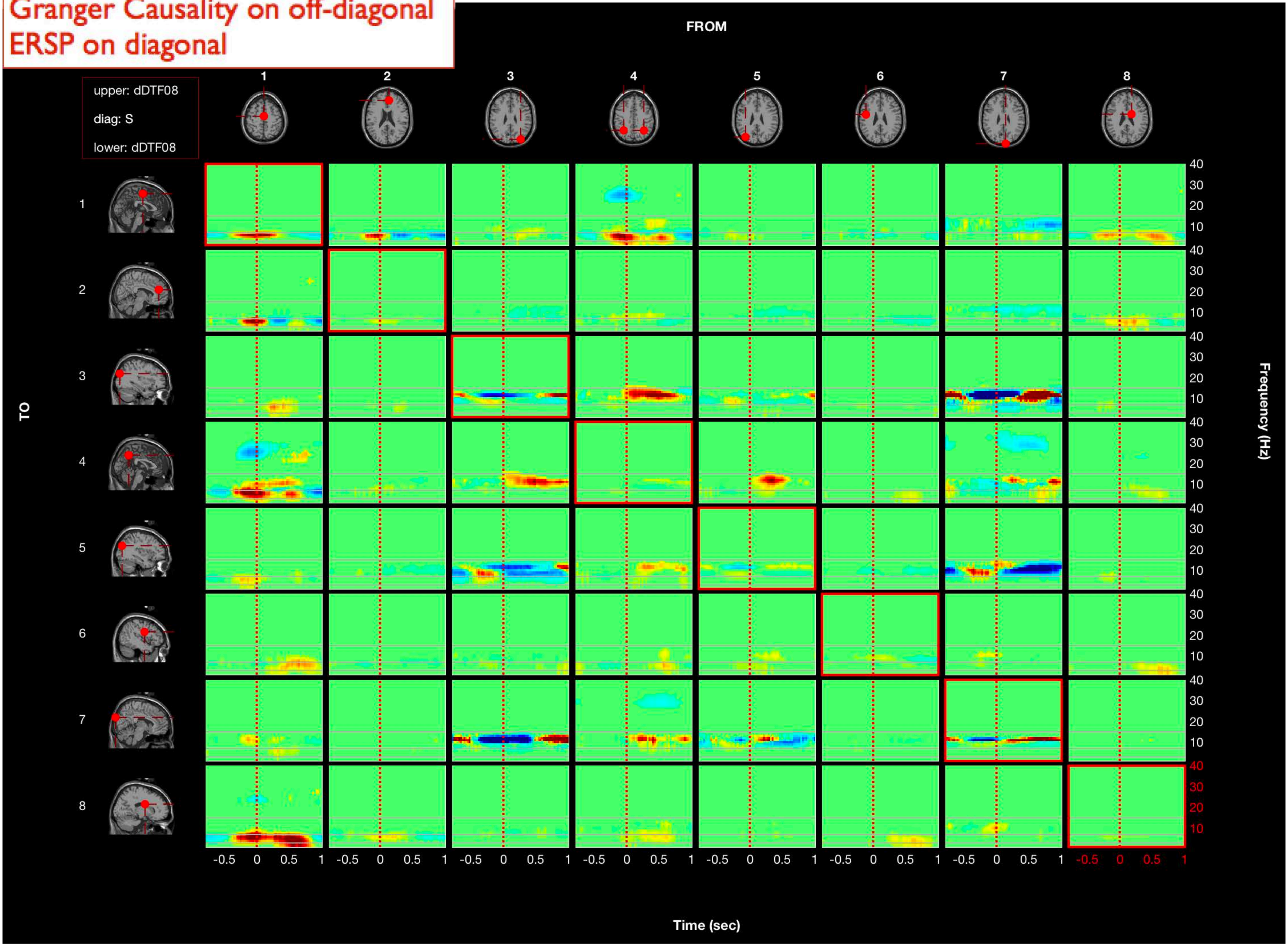


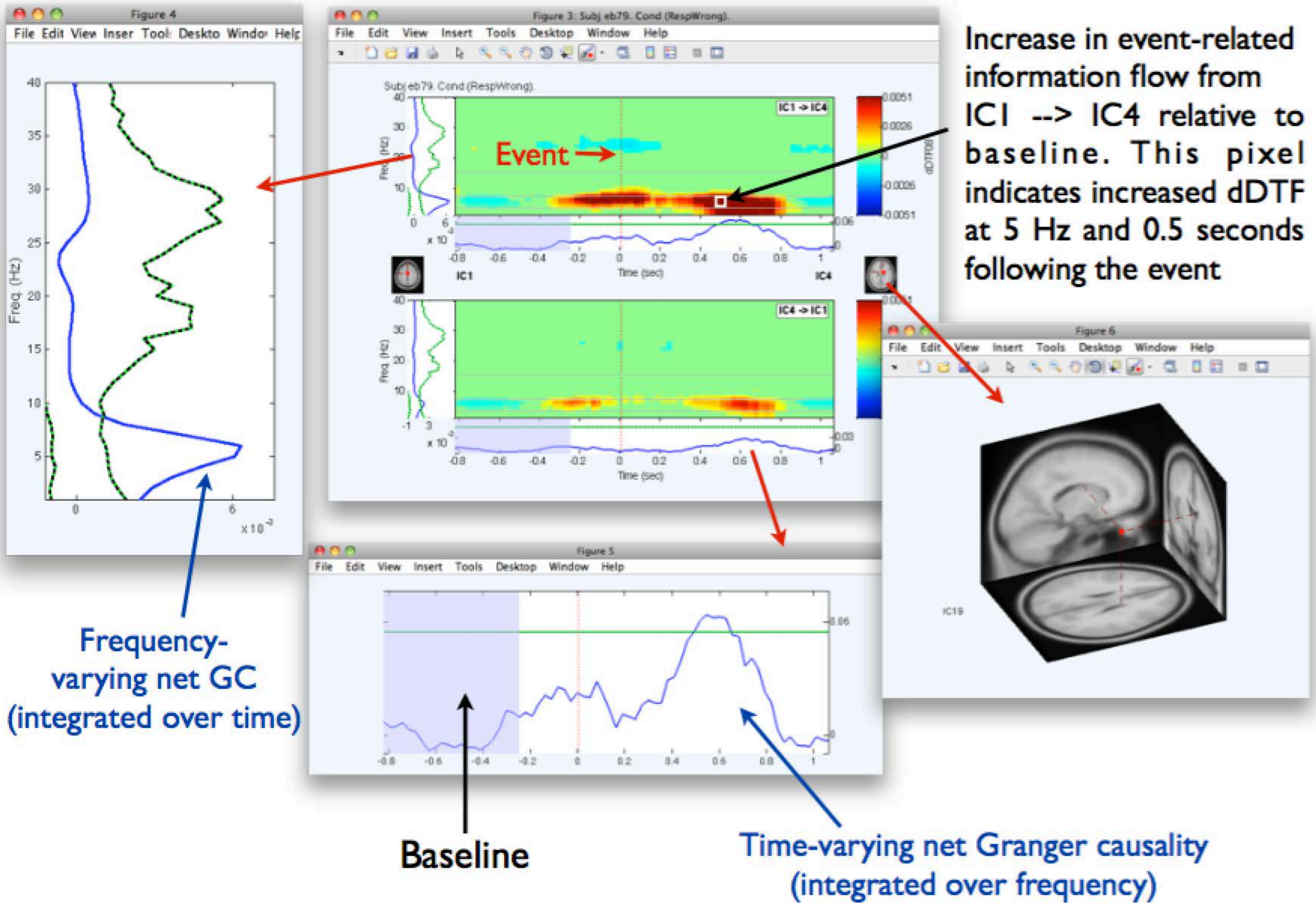


8 Visualization: Time-Frequency Grid



Granger Causality on off-diagonal
ERSP on diagonal




Increase in event-related information flow from IC1 --> IC4 relative to baseline. This pixel indicates increased dDTF at 5 Hz and 0.5 seconds following the event
Event
Frequency-varying net GC (integrated over time)
Baseline
Time-varying net Granger causality (integrated over frequency)
Figure 4
Figure 3: Subj eb79. Cond (RespWrong).
Figure 5
Figure 6
IC1 -> IC4
IC4 -> IC1
Time (sec)
Freq. (Hz)

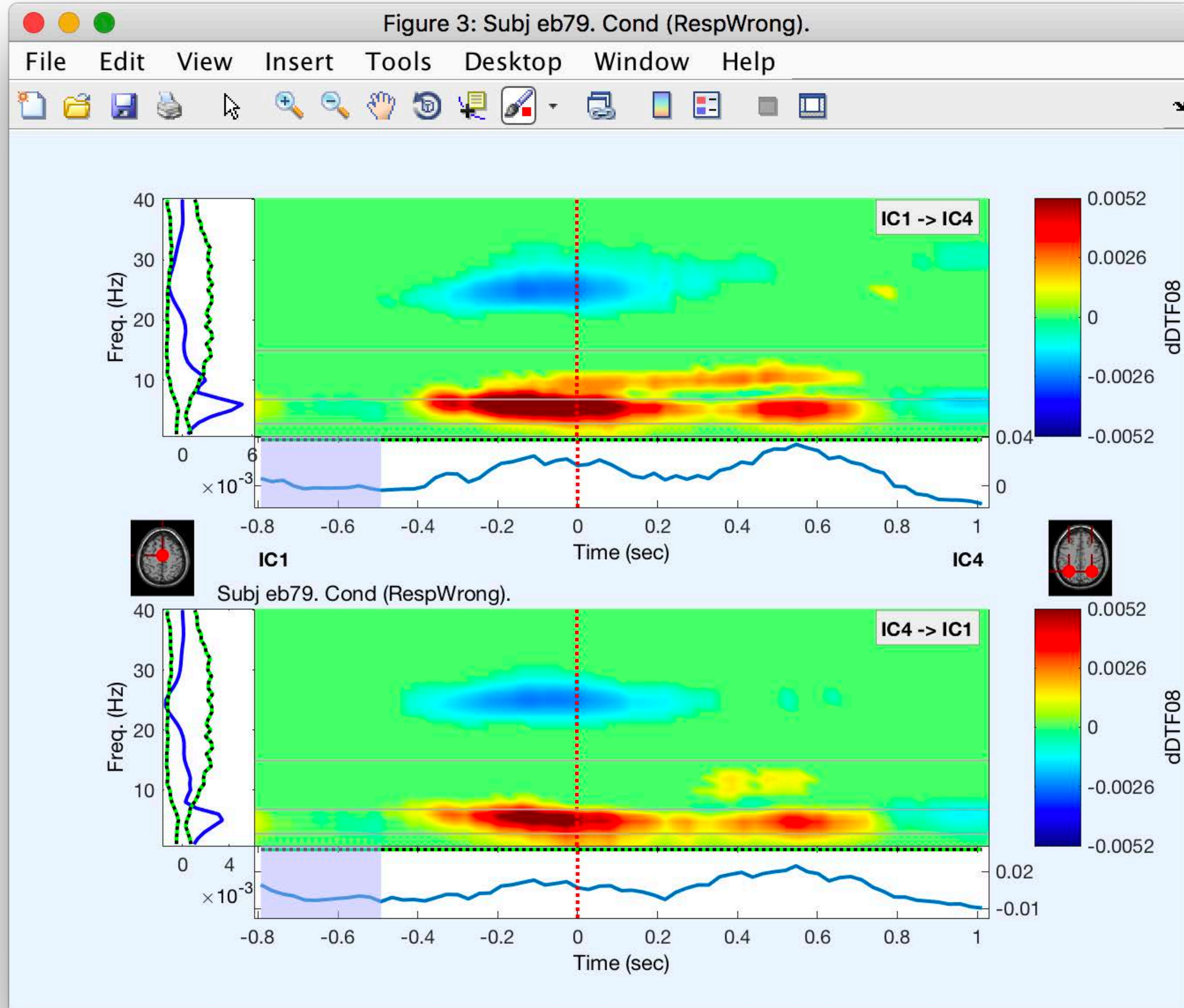
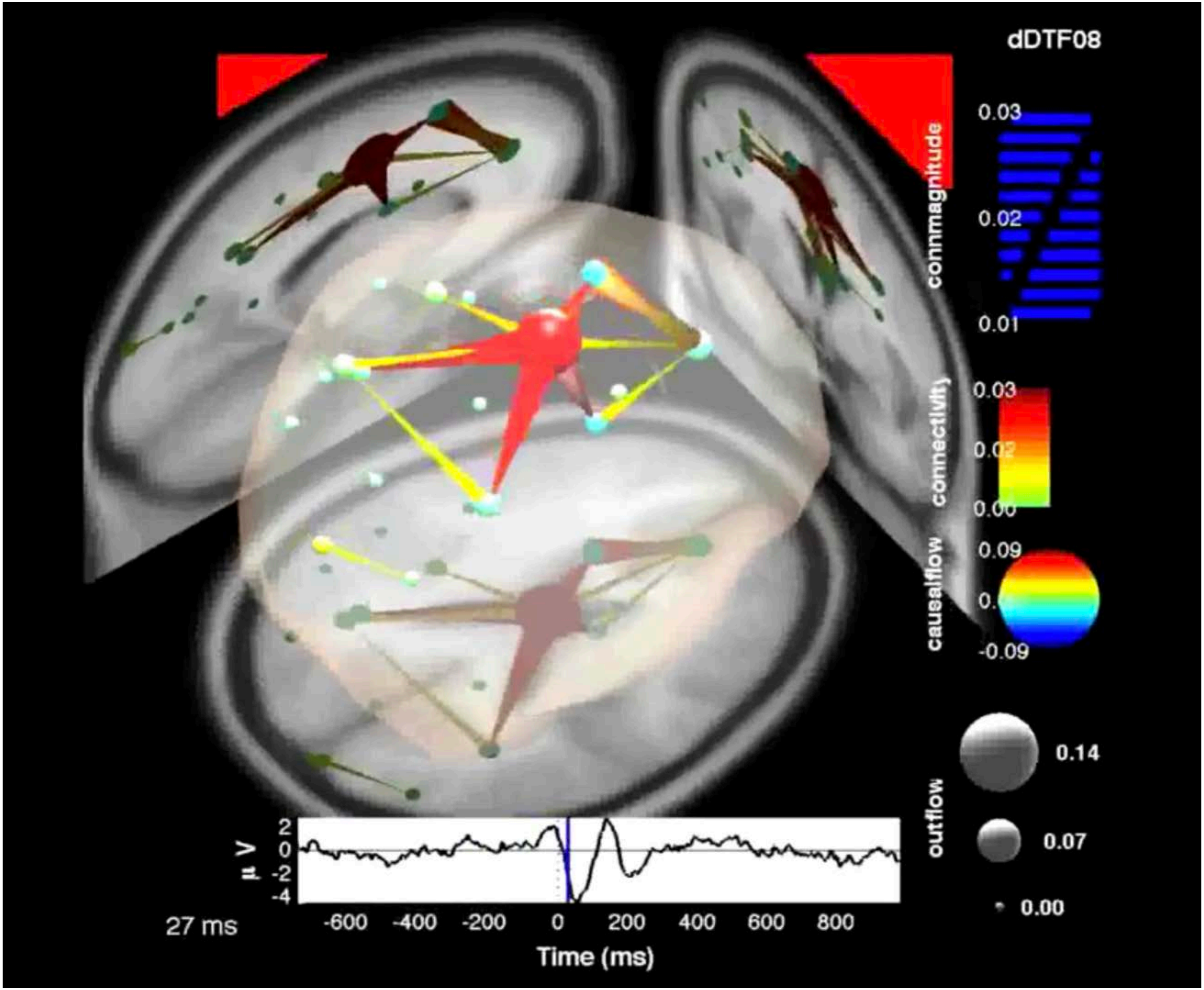
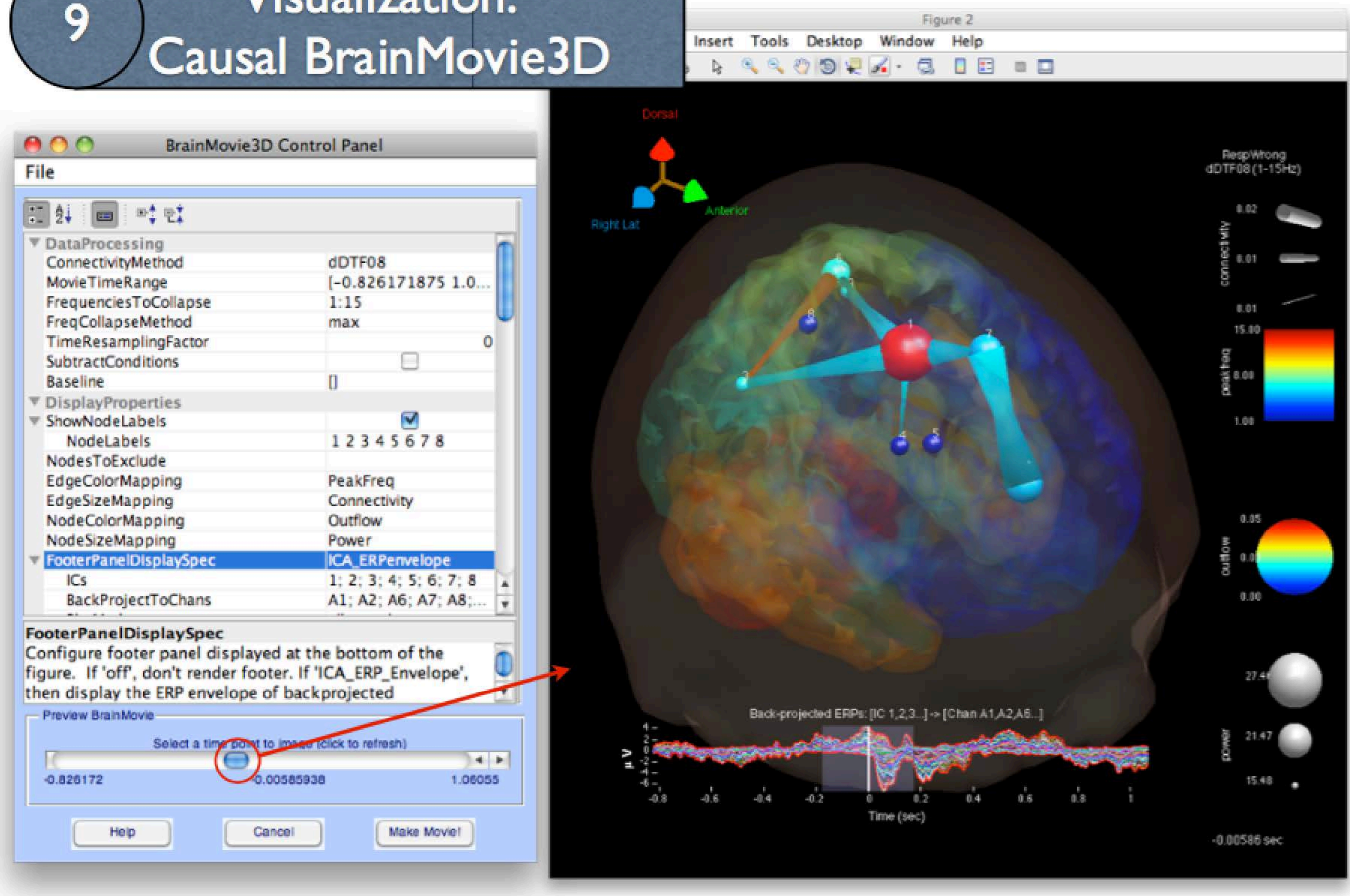
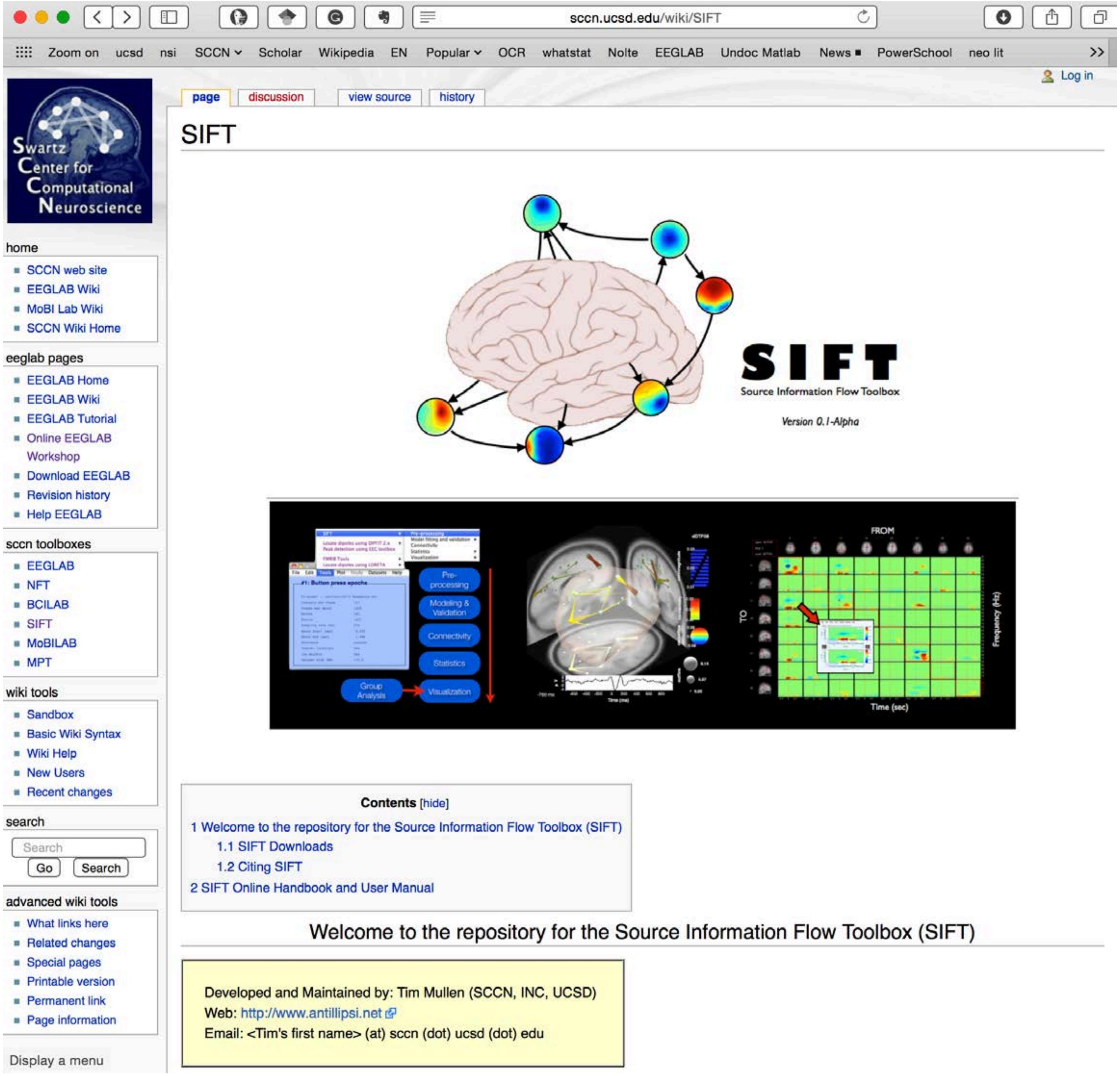


Figure 3: Subj eb79. Cond (RespWrong).
File Edit View Insert Tools Desktop Window Help
IC1 -> IC4
Freq. (Hz)
Time (sec)
dDTF08
IC1
IC4
Subj eb79. Cond (RespWrong).
IC4 -> IC1


dDTF08
0.03
0.02
0.01
connmagnitude
0.03
0.02
0.00
connectivity
0.09
-0.09
causalflow
0.14
0.07
0.00
outflow
μV
2
0
-2
-4
27 ms
-600
-400
-200
0
200
400
600
800
Time (ms)

9 Visualization: Causal BrainMovie3D





sccn.ucsd.edu/wiki/SIFT

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SIFT

SIFT
Source Information Flow Toolbox
Version 0.1-Alpha

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1.2 Citing SIFT
2 SIFT Online Handbook and User Manual

Welcome to the repository for the Source Information Flow Toolbox (SIFT)

Developed and Maintained by: Tim Mullen (SCCN, INC, UCSD)
Web: http://www.antillipsi.net
Email: <Tim's first name> (at) sccn (dot) ucsd (dot) edu

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