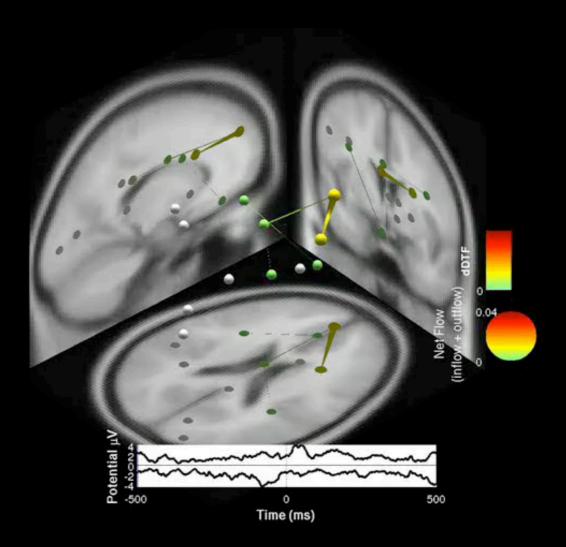
# Modeling Distributed Brain Network Dynamics

### **Tim Mullen**

12th EEGLAB Workshop UC San Diego La Jolla, CA November 20, 2010

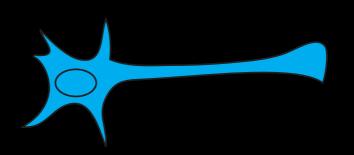






Structural Connectivity

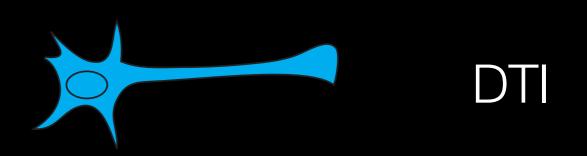
anatomical





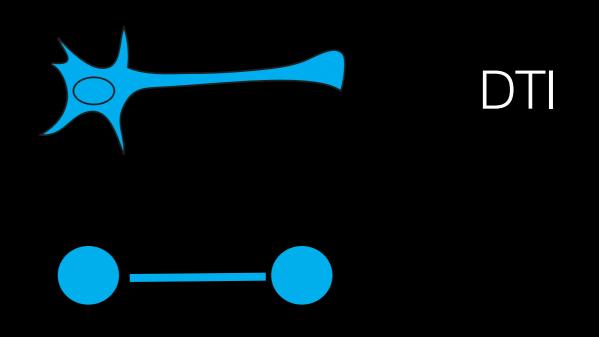
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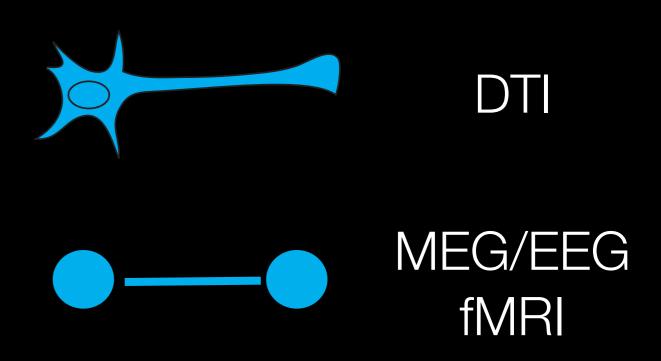


- Structural Connectivity
  - anatomical
- Functional Connectivity
  - symmetric, correlative



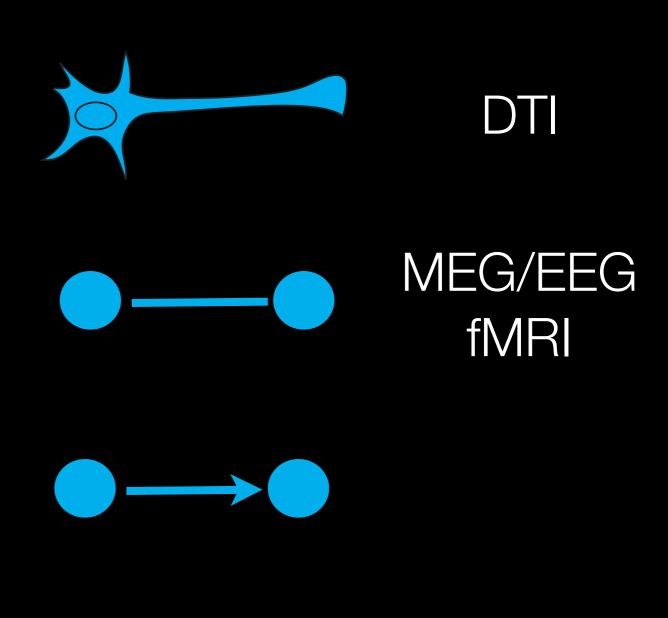


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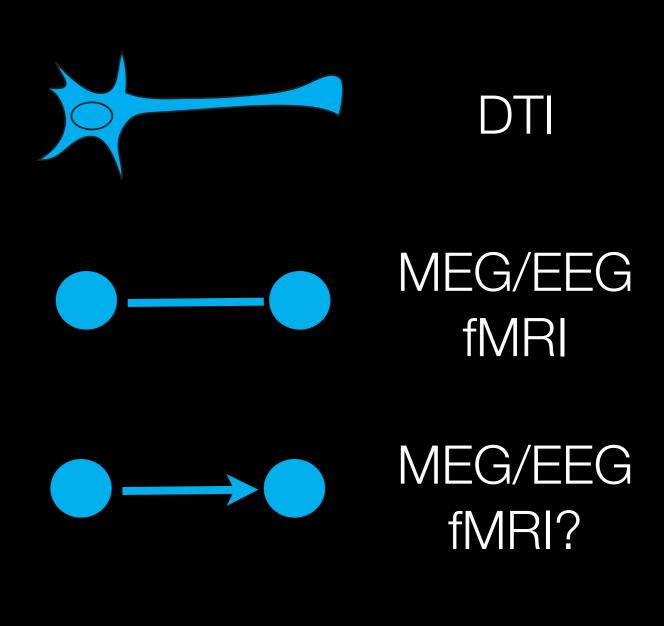


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- Effective Connectivity
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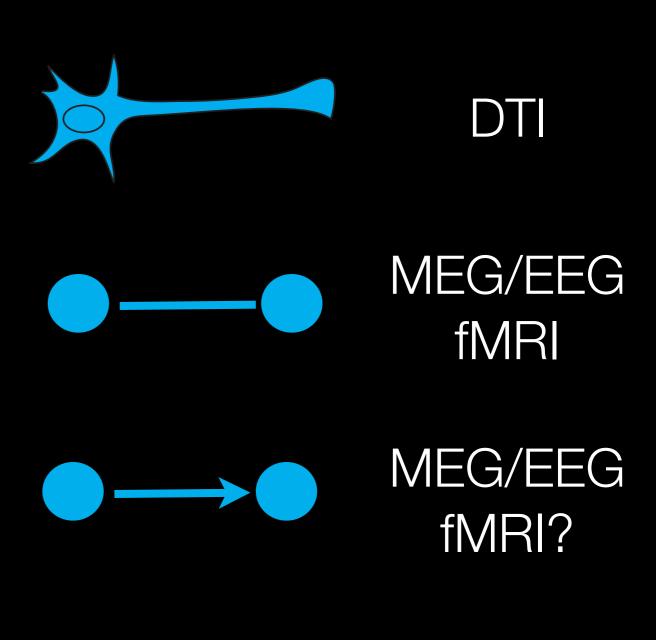


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# Many ways to model effective connectivity in EEG

- Coherence, Phase-locking value
- Cross-correlation
- Transfer Entropy
- Dynamic Causal Models
- Structural Equation Models
- Granger-Causal methods



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# Granger Causality

- First introduced by Wiener (1958). Later reformulated by Granger (1969) in the context of linear stochastic autoregressive models
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  - 1. causes should precede their effects in time
  - 2. information in a cause's past should improve the prediction of the effect, above and beyond the information contained in the effect's own past.

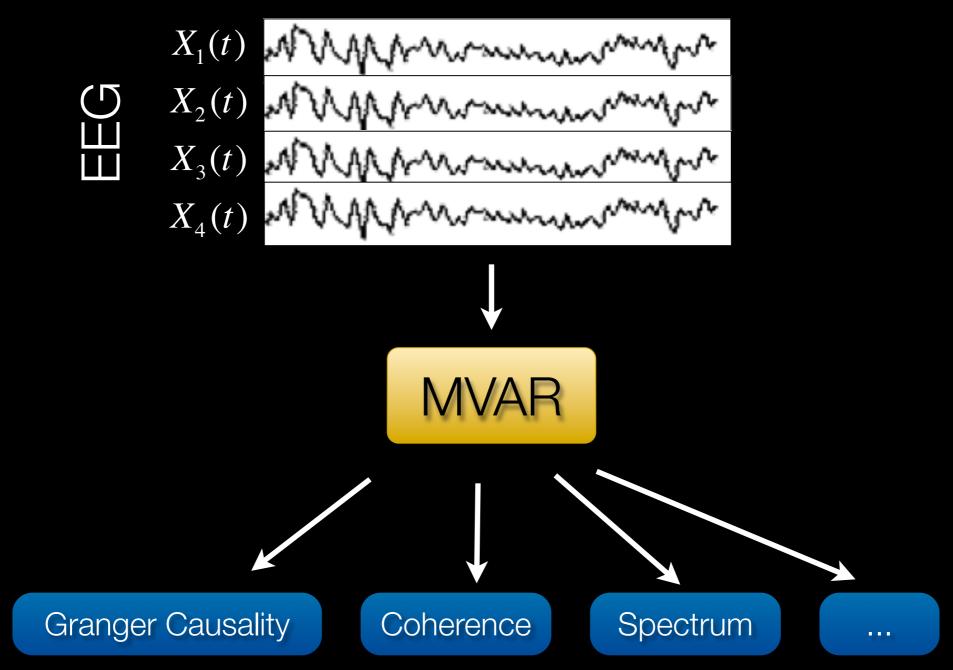


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This is **not** the same as (cross-)correlation!







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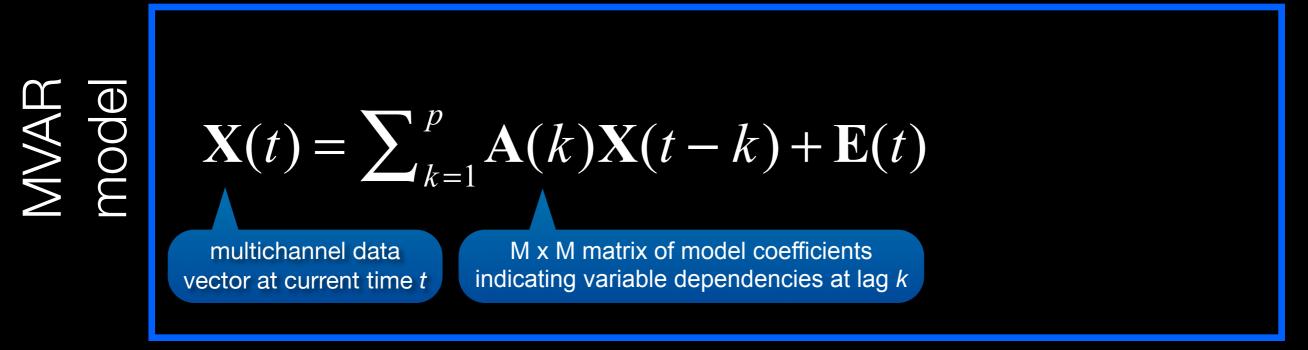
MVAR model

 $\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}(k) \mathbf{X}(t-k) + \mathbf{E}(t)$ 

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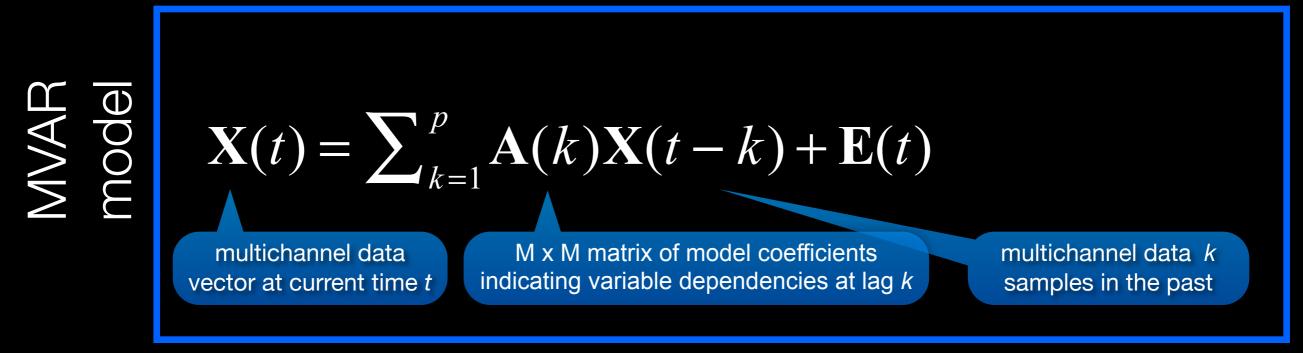
 $\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}(k)\mathbf{X}(t-k) + \mathbf{E}(t)$ multichannel data vector at current time t

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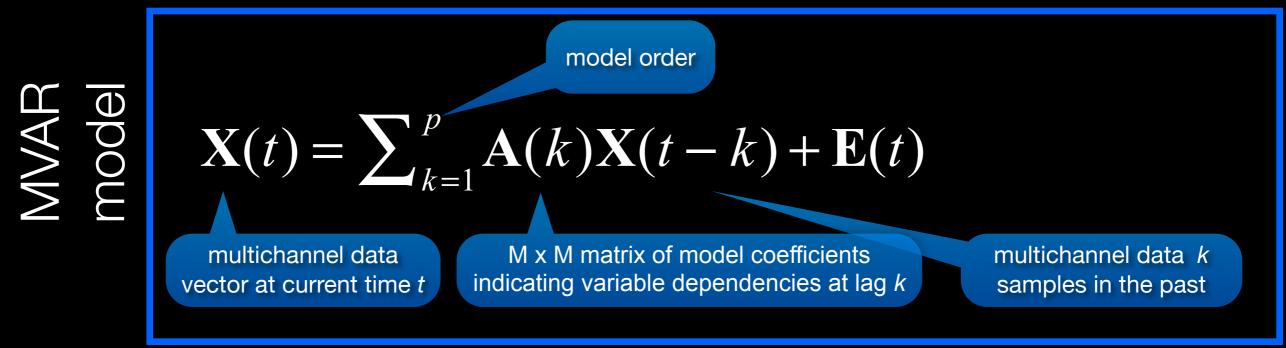
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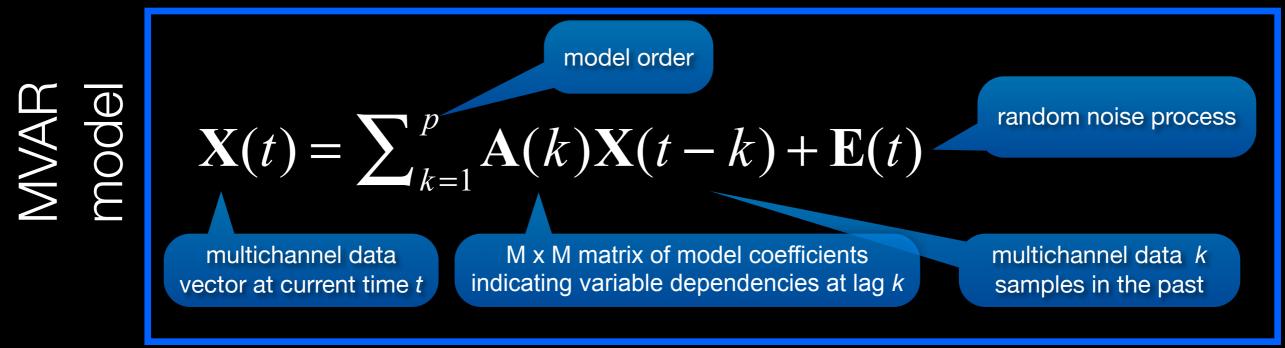
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 $\mathbf{E}(t) = N(0, \mathbf{V})$ 

 Model order is typically determined by minimizing information criteria such as Akaike Information Criterion (AIC) for varying model order (p):

 $AIC(p) = 2log(det(V)) + M^2p/N$ 

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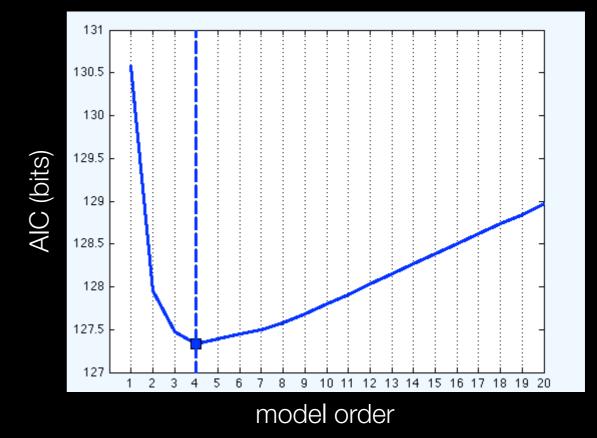
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130.5

130

129.5

129

128.5

128

127.5

1 2 3 4 5

6

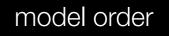
AIC (bits)

 $AIC(p) = 2log(det(V)) + M^2p/N < P$ 

Penalizes high model orders (parsimony)

entropy rate (amount of prediction error)

optimal order



10 11 12 13 14 15 16 17 18 19 20

9

8

"Weak" stationarity of the data

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#### Stability

- Technically, an MVAR process is stable if the reverse characteristic polynomial of the process has all roots outside the complex unit circle (all eigenvalues of A have modulus less than 1)
- Importantly, stability implies stationarity and SIFT provides you techniques for verifying the stability

## Granger Causality Test: Does X<sub>4</sub> granger-cause X<sub>1</sub>?

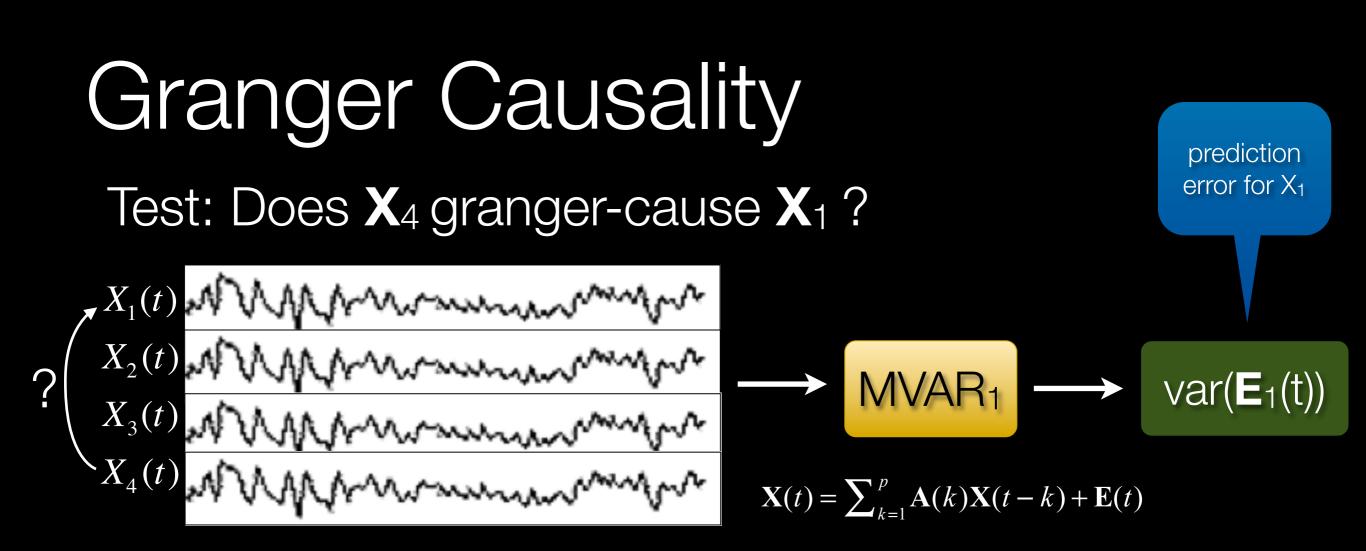
 $X_2(t)$  MMMM 2  $X_3(t)$ mmm 



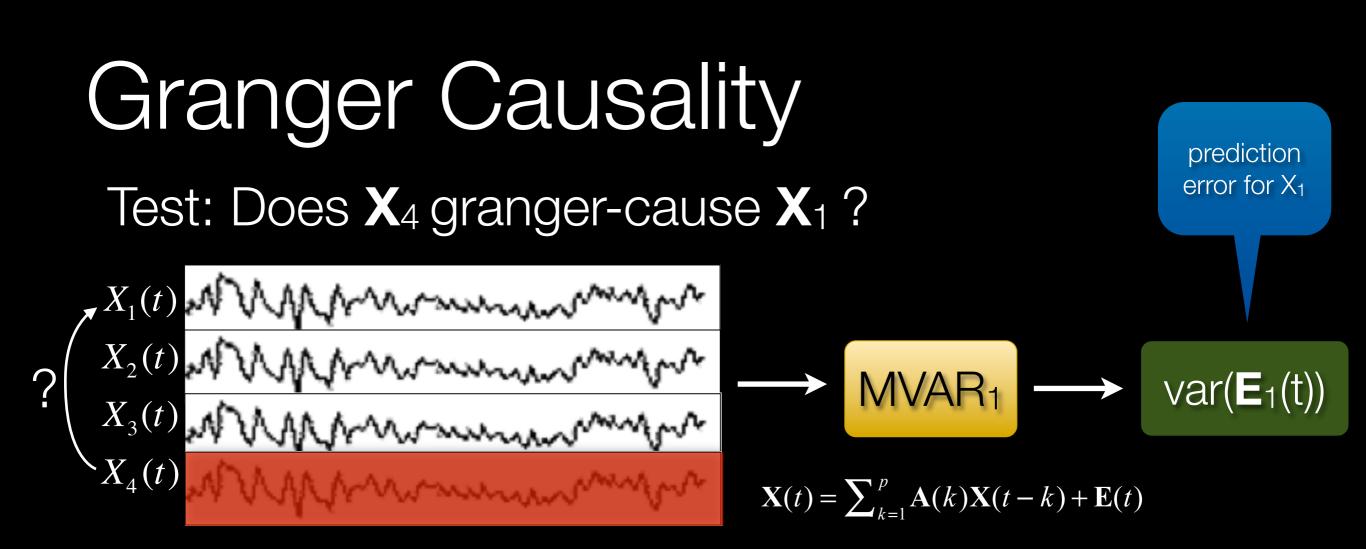
### Granger Causality Test: Does X<sub>4</sub> granger-cause X<sub>1</sub>?

$$\begin{array}{c}
X_{1}(t) & & & & \\
X_{2}(t) & & & & \\
X_{3}(t) & & & & \\
X_{4}(t) & & & & \\
\end{array} \xrightarrow{} MVAR_{1} \\
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X(t) = \sum_{k=1}^{p} A(k)X(t-k) + E(t)
\end{array}$$

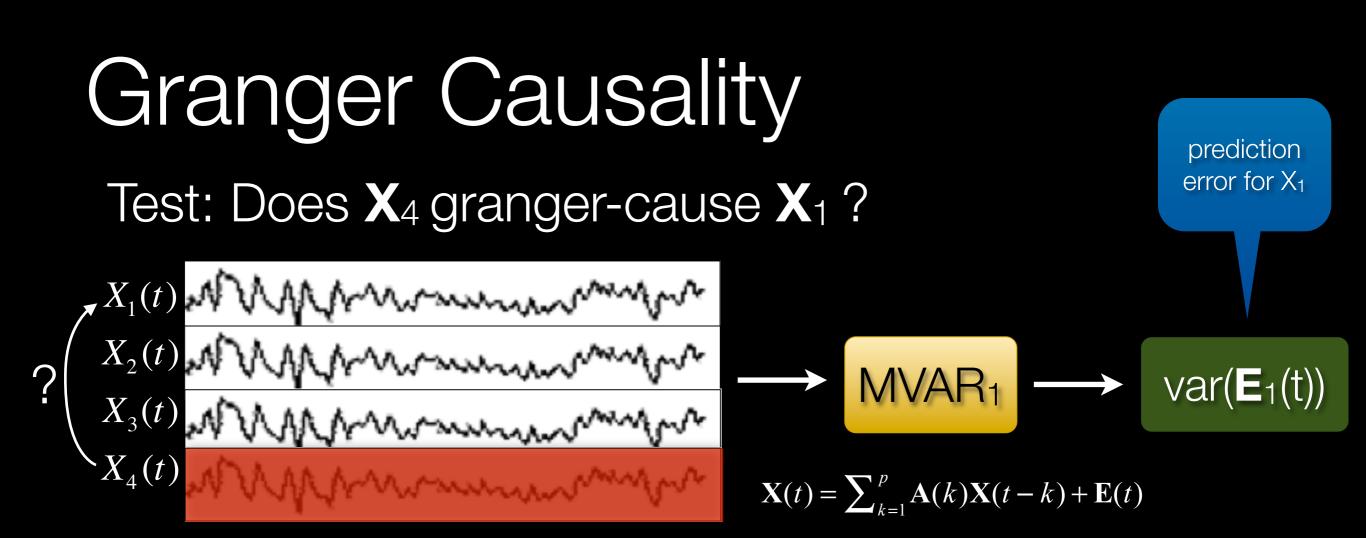






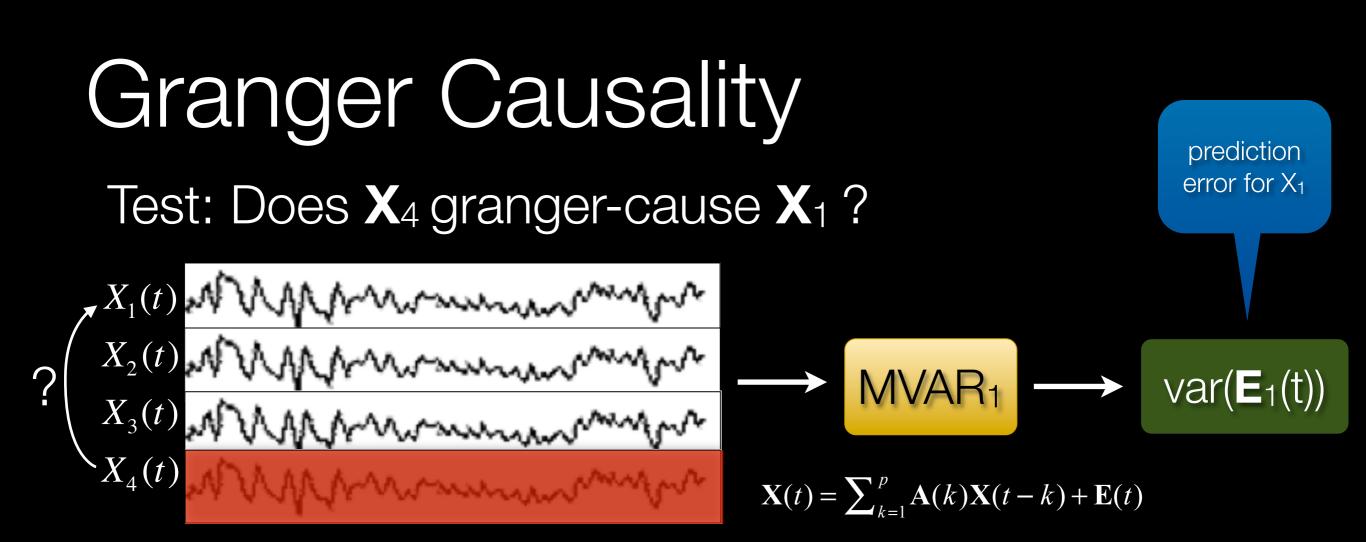


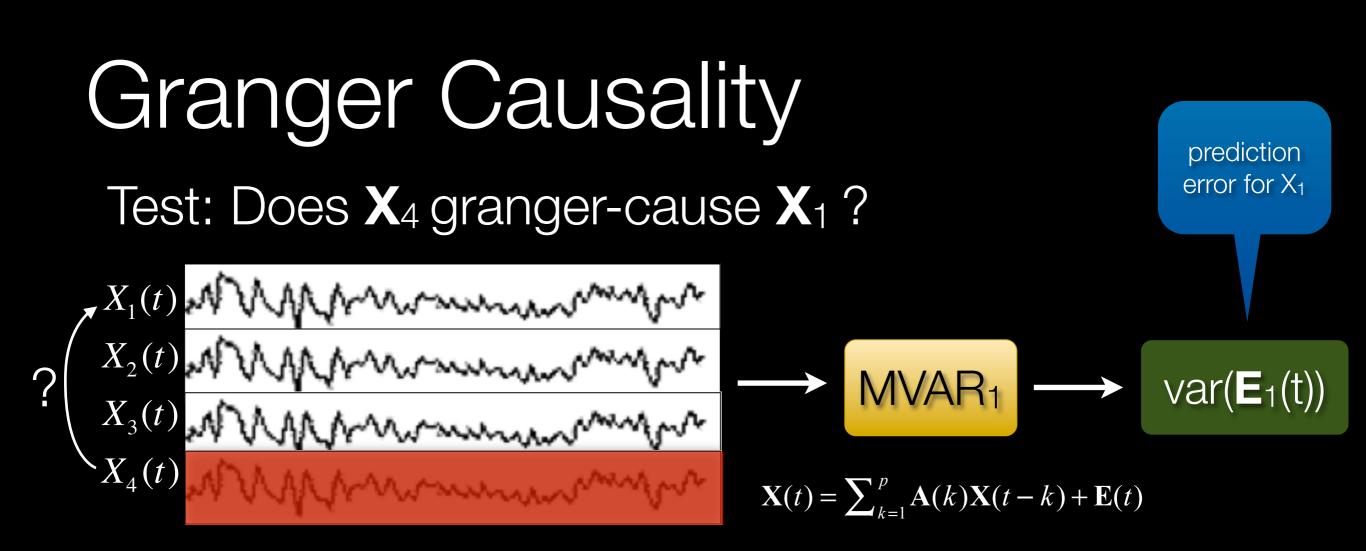




$$\begin{array}{c} X_1(t) & \mathcal{M}_{\mathcal{M}} & \mathcal{M}_{\mathcal{M}} \\ X_2(t) & \mathcal{M}_{\mathcal{M}} & \mathcal{M}_{\mathcal{M}} \\ X_3(t) & \mathcal{M}_{\mathcal{M}} & \mathcal{M}_{\mathcal{M}} \\ \end{array}$$





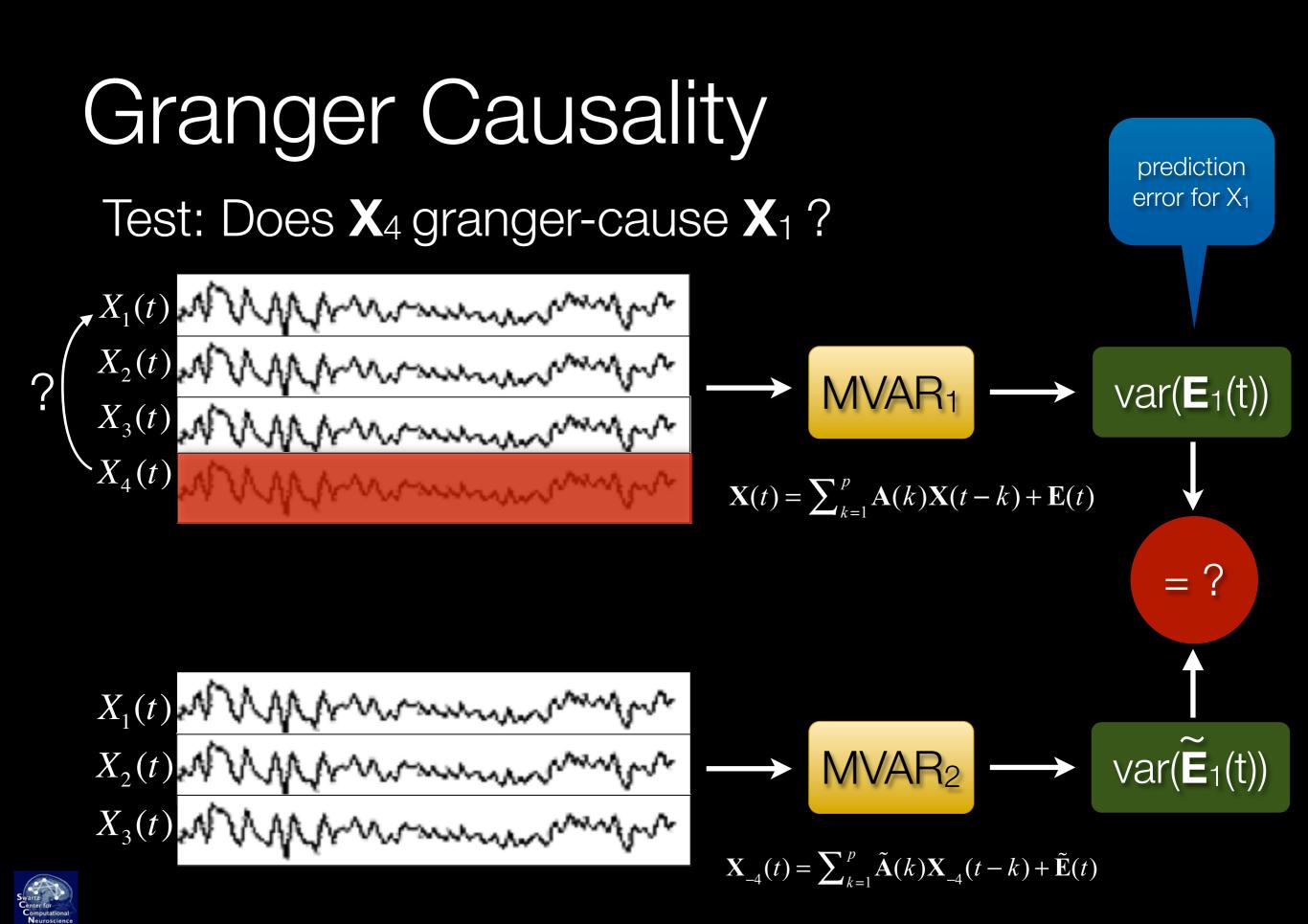


$$X_1(t)$$
 MMM man  $M$   
 $X_2(t)$  MMM man  $M$   
 $X_3(t)$  MMM man  $M$ 

$$\rightarrow$$
 MVAR<sub>2</sub>  $\rightarrow$  var( $\tilde{\mathbf{E}}_1(t)$ )

 $\mathbf{X}_{-4}(t) = \sum_{k=1}^{p} \tilde{\mathbf{A}}(k) \mathbf{X}_{-4}(t-k) + \tilde{\mathbf{E}}(t)$ 





# Granger Causality

## Granger Causality

Granger (1969) quantified this definition for bivariate processes in the form of an F-ratio:

$$F_{X_{1} \leftarrow X_{2}} = \ln\left(\frac{var(\tilde{E}_{1})}{var(E_{1})}\right) = \ln\left(\frac{var(X_{1}(t) \mid X_{1}(\cdot))}{var(X_{1}(t) \mid X_{1}(\cdot), X_{2}(\cdot))}\right)$$

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Alternately, for a multivariate interpretation we can fit a single MVAR model to all channels and apply the following definition:

 $X_j$  granger-causes  $X_i$  condition on all other variables in **X** if and only if  $A_{ii}(k) >> 0$  for some lag  $k \in \{1, ..., p\}$ 

Example: 2-channel MVAR process of order 1

$$\begin{pmatrix} X_1(t) \\ X_2(t) \end{pmatrix} = \begin{pmatrix} 0.5 & 0 \\ 0.7 & 0.2 \end{pmatrix} \begin{pmatrix} X_1(t-1) \\ X_2(t-1) \end{pmatrix} + \begin{pmatrix} E_1(t) \\ E_2(t) \end{pmatrix}$$

 $\overline{X_1(t)} = -0.5 \overline{X_1(t-1)} + 0 \overline{X_2(t-1)} + E_1(t)$  $\overline{X_2(t)} = 0.7 \overline{X_1(t-1)} + 0.2 \overline{X_2(t-1)} + E_2(t)$ 

Which causal structure does this model correspond to?

a)  $(1 \rightarrow 2)$  b)  $(1 \leftarrow 2)$  c)  $(1 \leftarrow 2)$ 

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(2)

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1)  $\leftarrow$  2) C) 1)  $\leftarrow$ 

 $\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}(k) \mathbf{X}(t-k) + \mathbf{E}(t)$ 

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Fourier-transforming A(k) we obtain

$$\mathbf{A}(f) = -\sum_{k=0}^{p} \mathbf{A}(k) e^{-i2\pi fk}$$

Likewise, X(f) and E(f) correspond to the fourier transforms of the data and residuals, respectively

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We can then define the spectral matrix  $\mathbf{X}(f)$  as follows:

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**Definition**: If  $|\mathbf{A}_{ij}(f)|$  is significantly non-zero, then  $X_j$  grangercauses  $X_i$  (at frequency f) conditioned on all other vars in **X** 

# Granger Causality – Frequency Domain Estimators

■(some) Coherence measures

 $C_{ij}(f) = \frac{S_{ij}(f)}{\sqrt{S_{ii}(f)S_{jj}(f)}}$ 

Coherence

$$P_{ij}(f) = \frac{\hat{S}_{ij}(f)}{\sqrt{\hat{S}_{ii}(f)\hat{S}_{jj}(f)}} \qquad \hat{\mathbf{S}} = \mathbf{S}^{-1}$$

Partial coherence

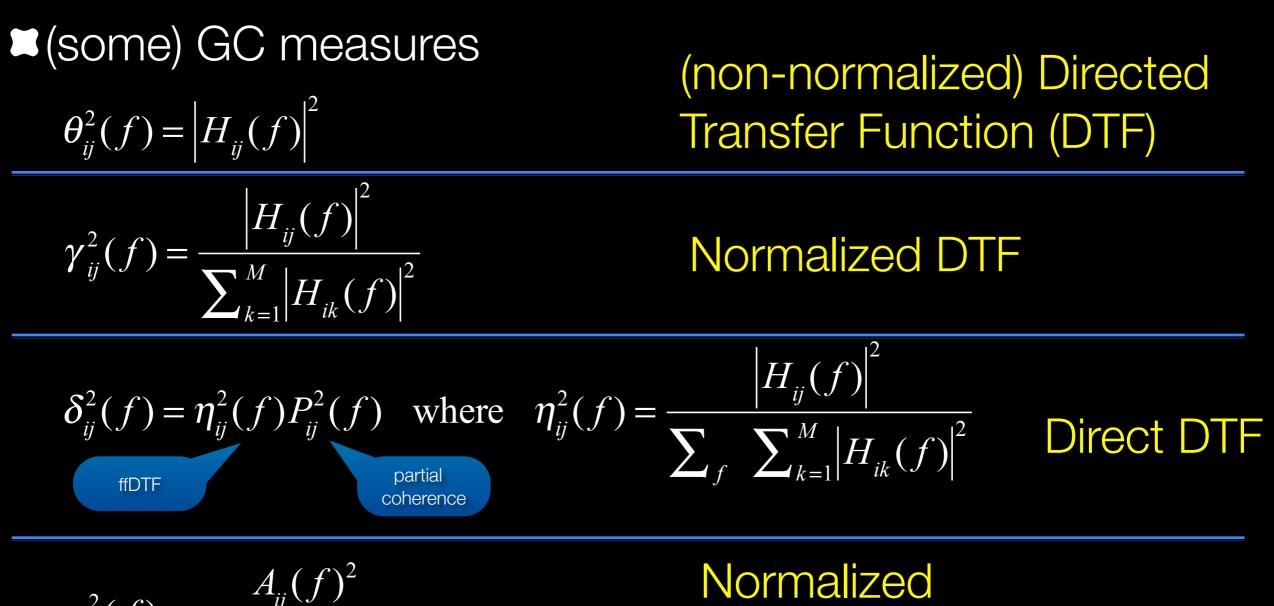
$$G_{i}(f) = \sqrt{1 - \frac{\det(\mathbf{S}(f))}{S_{ii}(f)\mathbf{M}_{ii}(f)}}$$

Multiple coherence





# Granger Causality – Frequency Domain Estimators



$$\pi_{ij}^{2}(f) = \frac{A_{ij}(f)^{2}}{\sum_{k=1}^{M} |A_{kj}(f)|^{2}}$$

Normalized Partial Directed Coherence (PDC)

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- event-related responses
- transient network changes during sequential information processing

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- event-related responses
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- Electrophysiological processes often exhibit oscillatory phenomena, making them well-suited for frequencydomain analysis
- How can we perform time-varying, frequency-domain analysis of network dynamics?

#### Many ways to do time-varying MVAR estimation

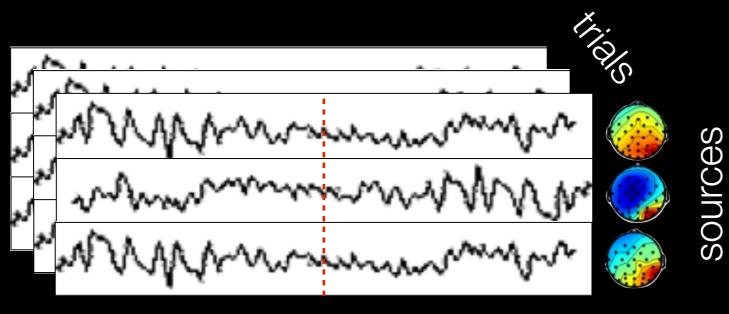
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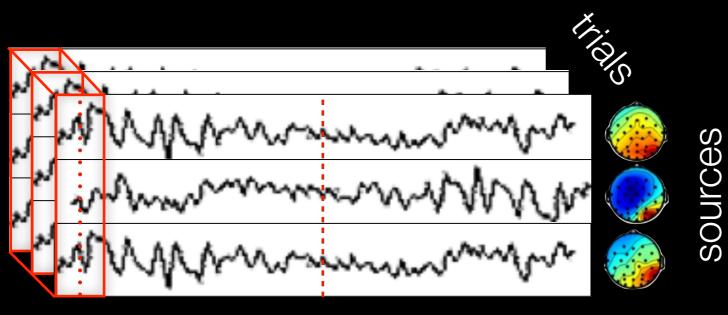
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Analogous to shorttime fourier transform

time

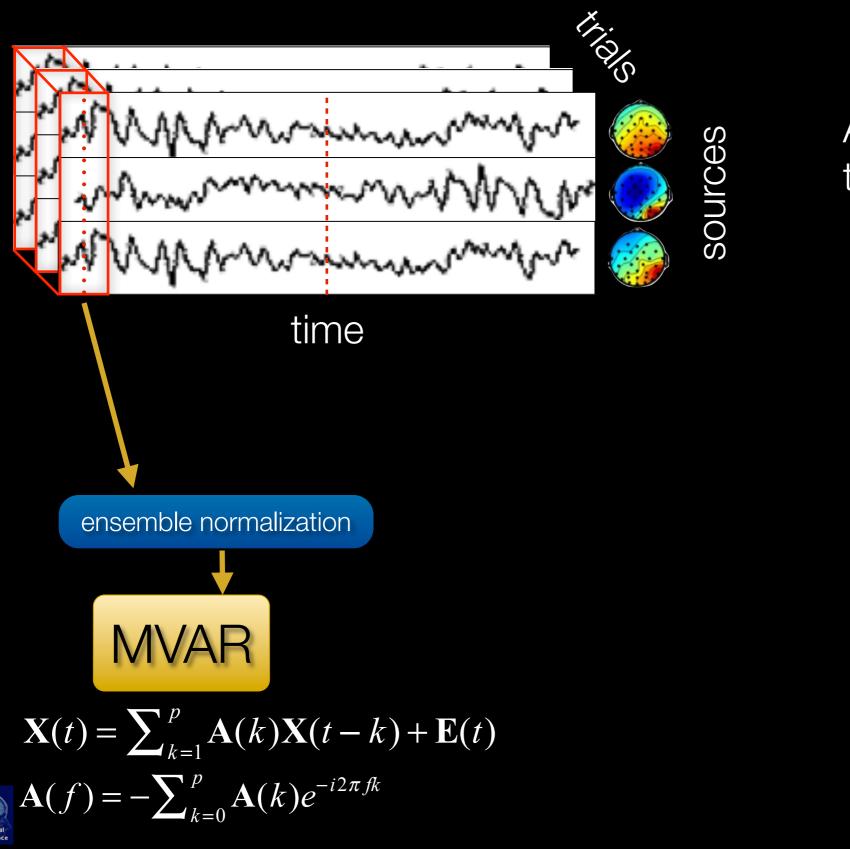




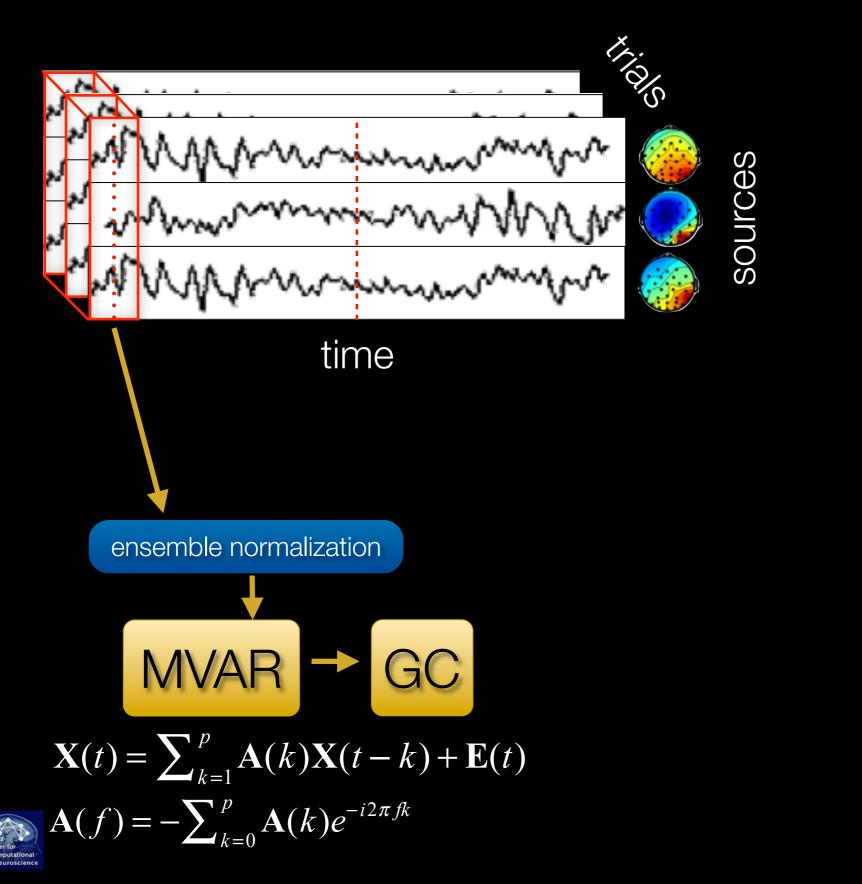
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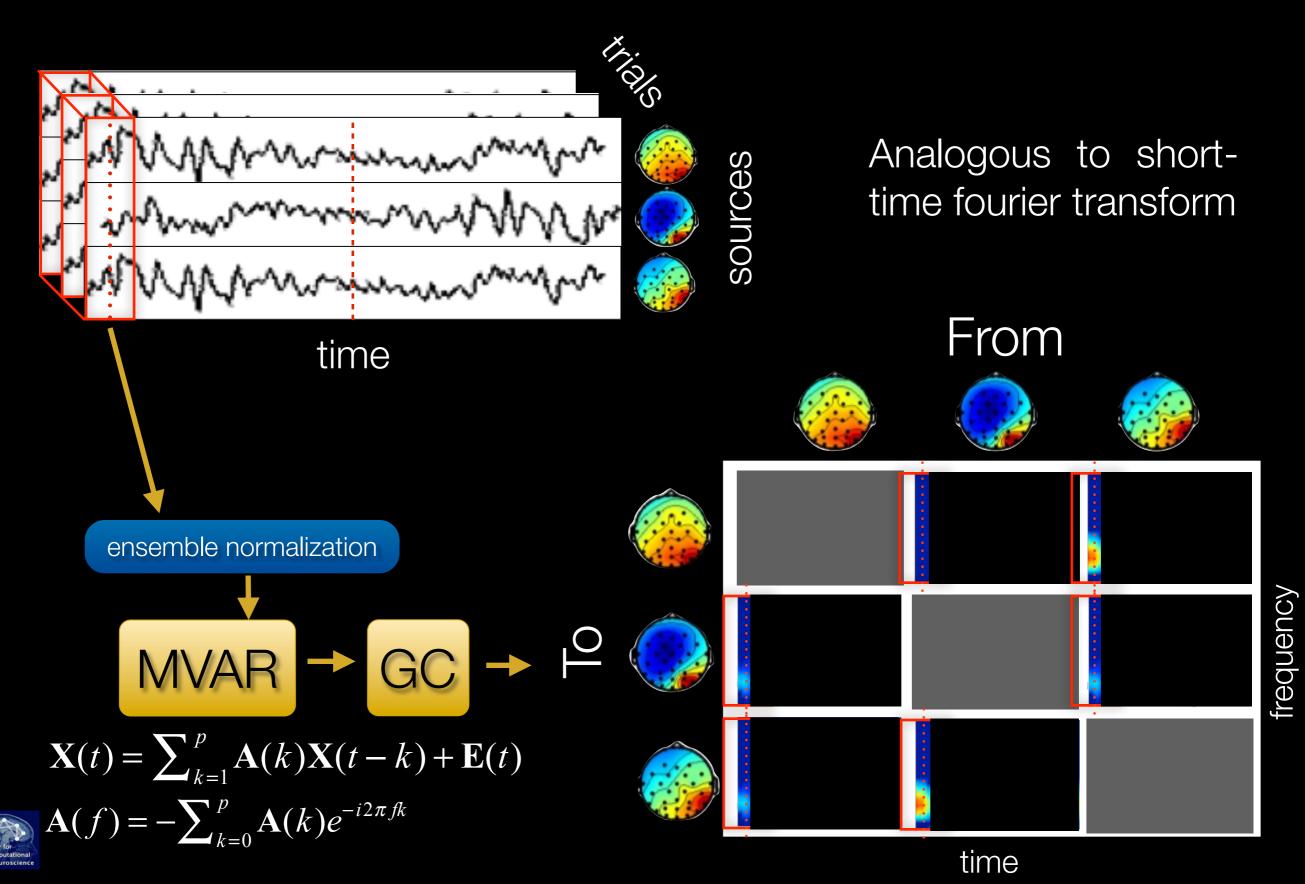


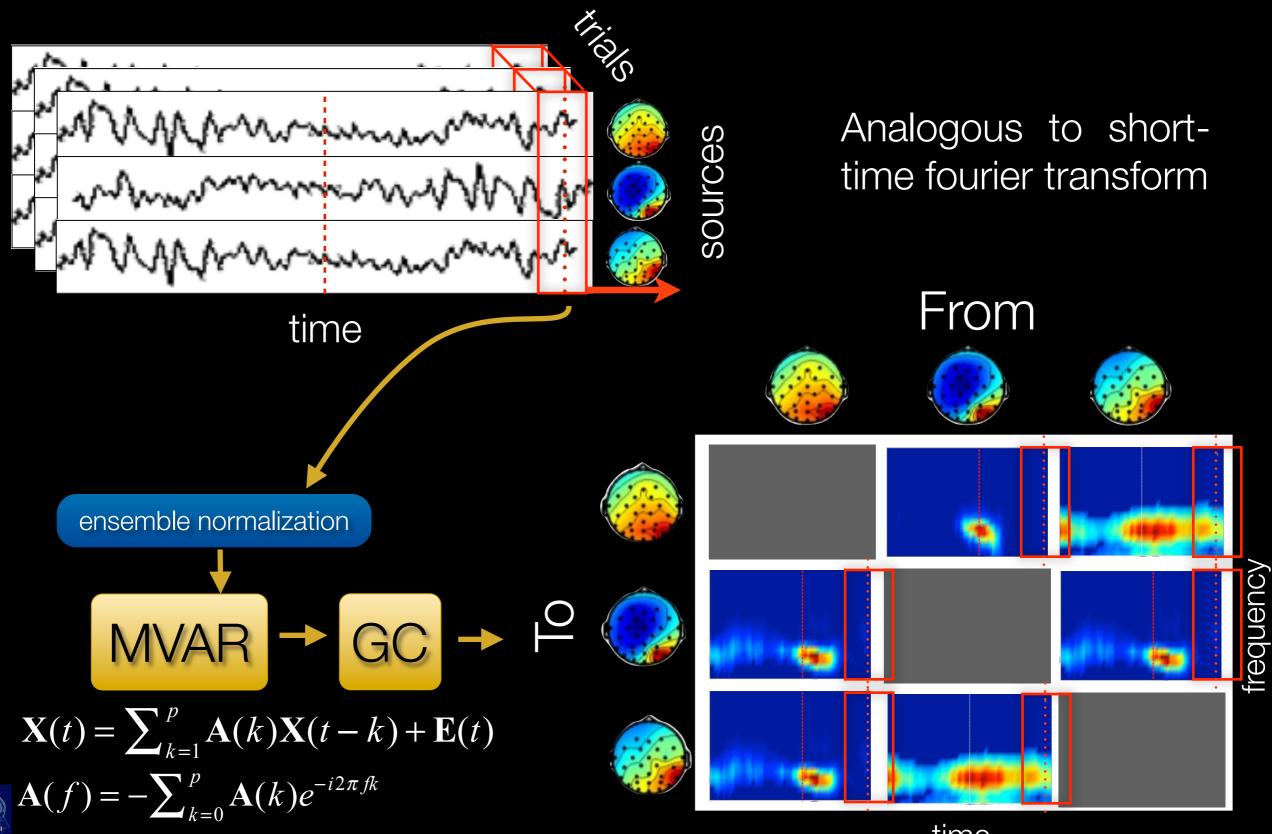


Analogous to shorttime fourier transform



#### Analogous to shorttime fourier transform





time

- What is a good window length?
- Considerations:

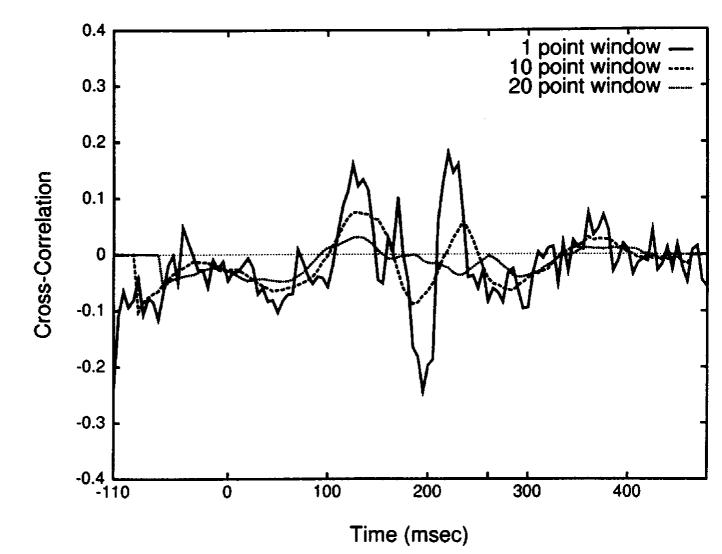
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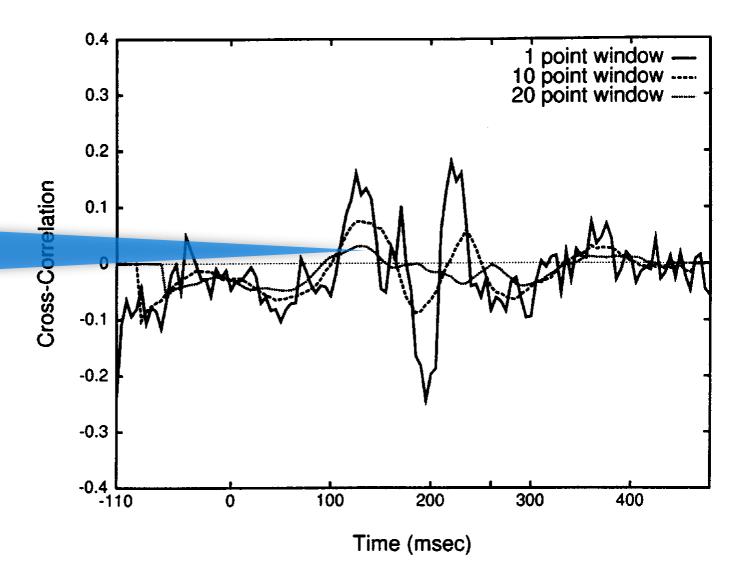
- Considerations:
  - Temporal smoothing
  - Local stationarity
  - Sufficient amount of data
  - Process dynamics

#### **Consideration: Temporal Smoothness**

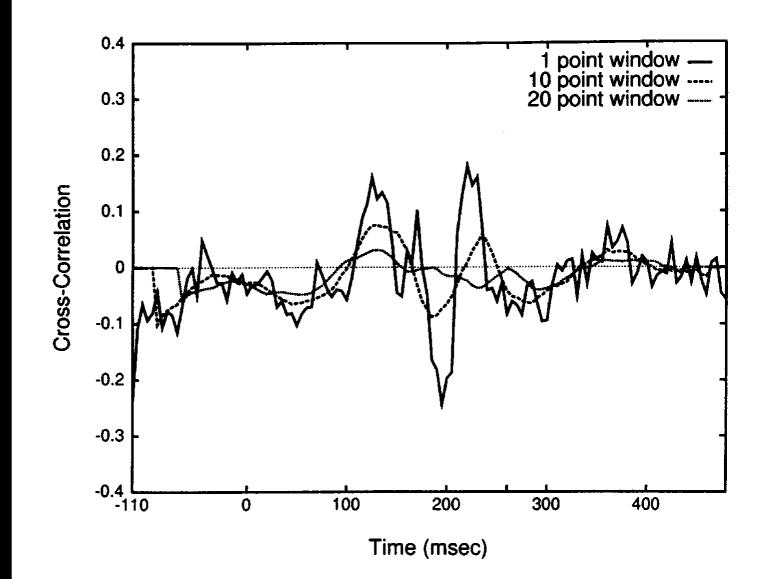


#### **Consideration: Temporal Smoothness**

Too-large windows may smooth out interesting transient dynamic features.

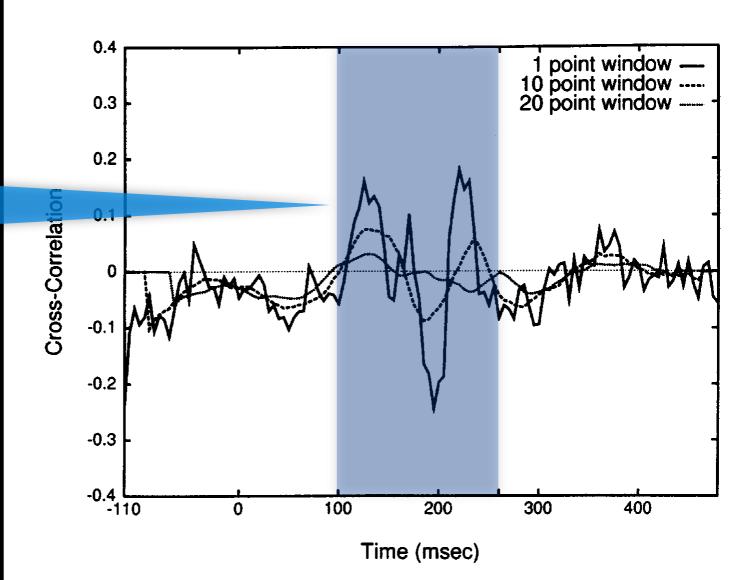


#### **Consideration: Local Stationarity**

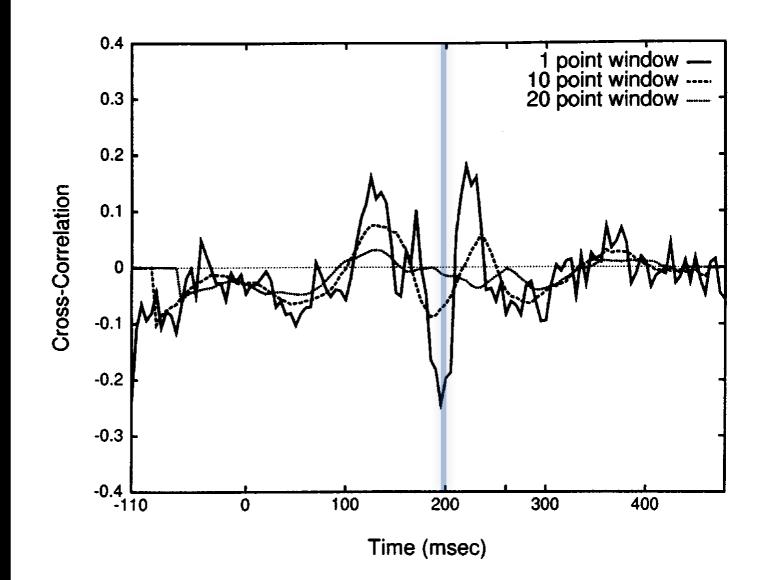


#### **Consideration: Local Stationarity**

Too-large windows may not be locally-stationary



#### **Consideration: Local Stationarity**



**Consideration: Sufficient data** 

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M = number of variables

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M = number of variables p = model order

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$$\label{eq:model} \begin{split} M &= number \mbox{ of variables} \\ p &= model \mbox{ order} \\ N_{tr} &= number \mbox{ of trials} \end{split}$$

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- M = number of variables
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- W = length of each window (sample points)

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We have  $M^2p$  model coefficients to estimate. This requires a minimum of  $M^2p$  independent samples. So we have the constraint  $M^2p <= N_{tr}W$ .

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- $N_{tr}$  = number of trials
- W = length of each window (sample points)

We have  $M^2p$  model coefficients to estimate. This requires a minimum of  $M^2p$  independent samples. So we have the constraint  $M^2p \le N_{tr}W$ . In practice, however, a better heuristic is  $M^2p \le (1/10)N_{tr}W$ .

#### **Consideration: Sufficient data**

- M = number of variables
- p = model order
- $N_{tr} =$  number of trials
- W = length of each window (sample points)

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Or: W >= 10(M<sup>2</sup>p/N<sub>tr</sub>)

10x more data points than parameters to estimate

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Or: W >= 10(M<sup>2</sup>p/N<sub>tr</sub>)

10x more data points than parameters to estimate

SIFT will let you know if your window length is not optimal

#### **Consideration: Process dynamics**

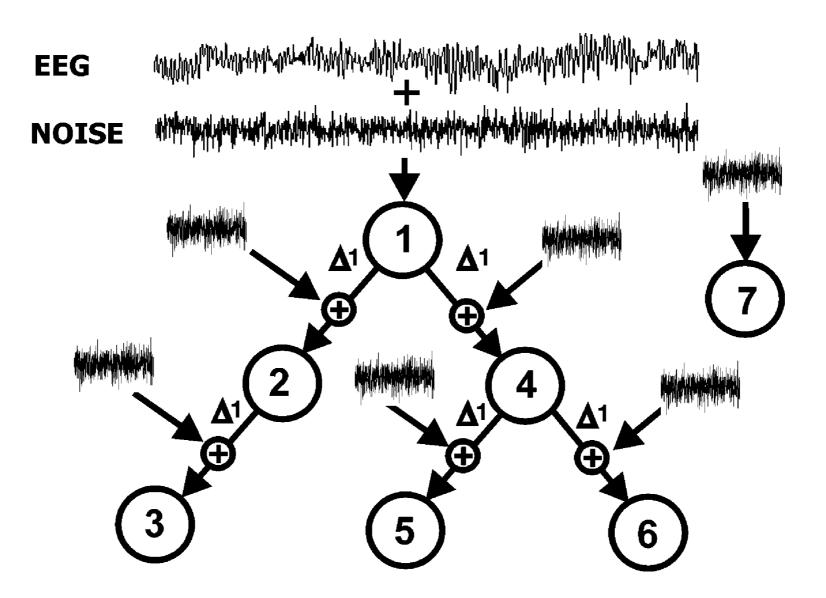
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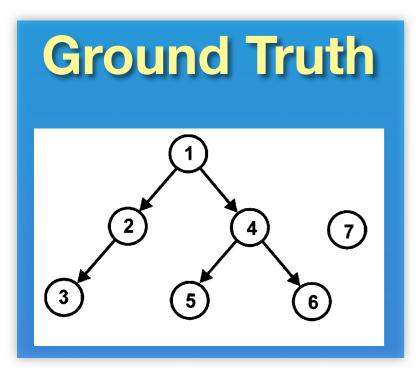
- Your window must be larger than the maximum expected interaction time lag between any two processes.
- Your window should be large enough to span ~1 cycle of the lowest frequency of interest

# Which Measure to Use?

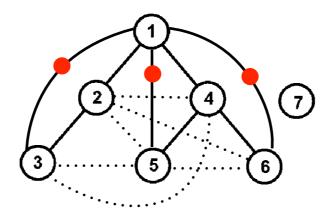


Kus et al, 2004

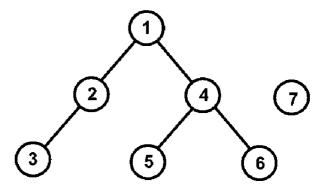




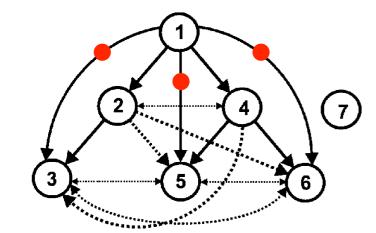
Coherence



Partial Coherence



**Bivariate GC** 





2

2

5

 $\overline{\mathbf{7}}$ 

 $\overline{7}$ 

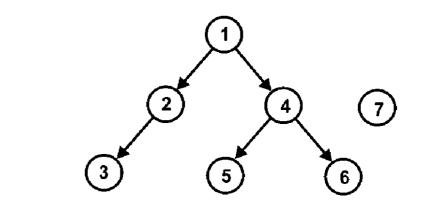
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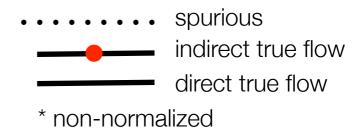
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4

4

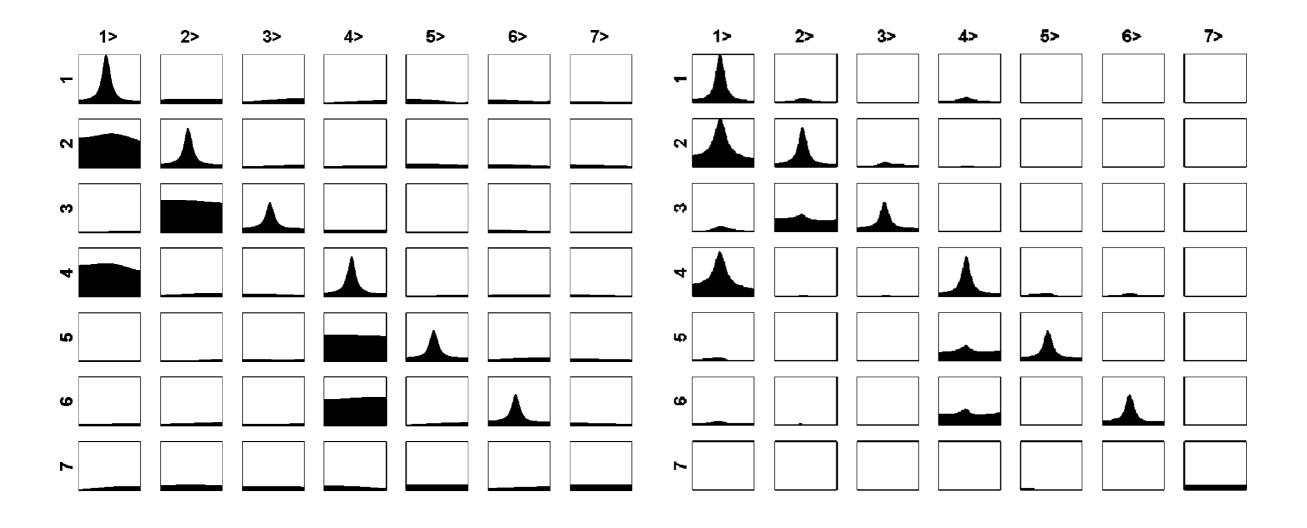








# PDC versus DTF methods (spectral considerations)

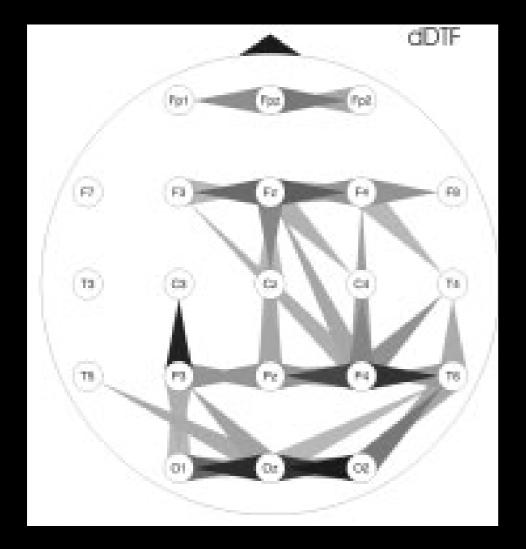


PDC

dDTF

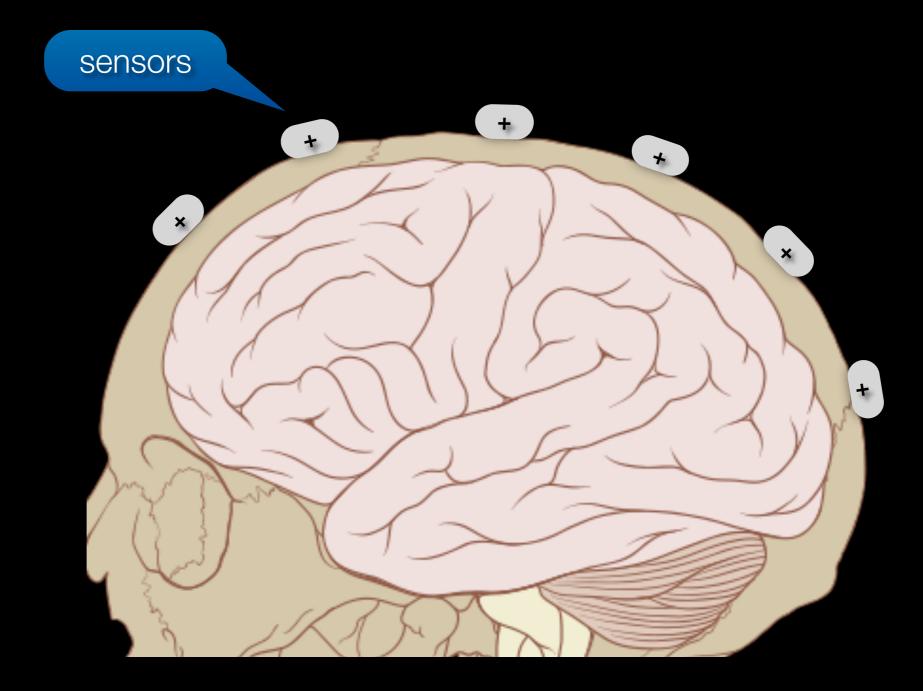


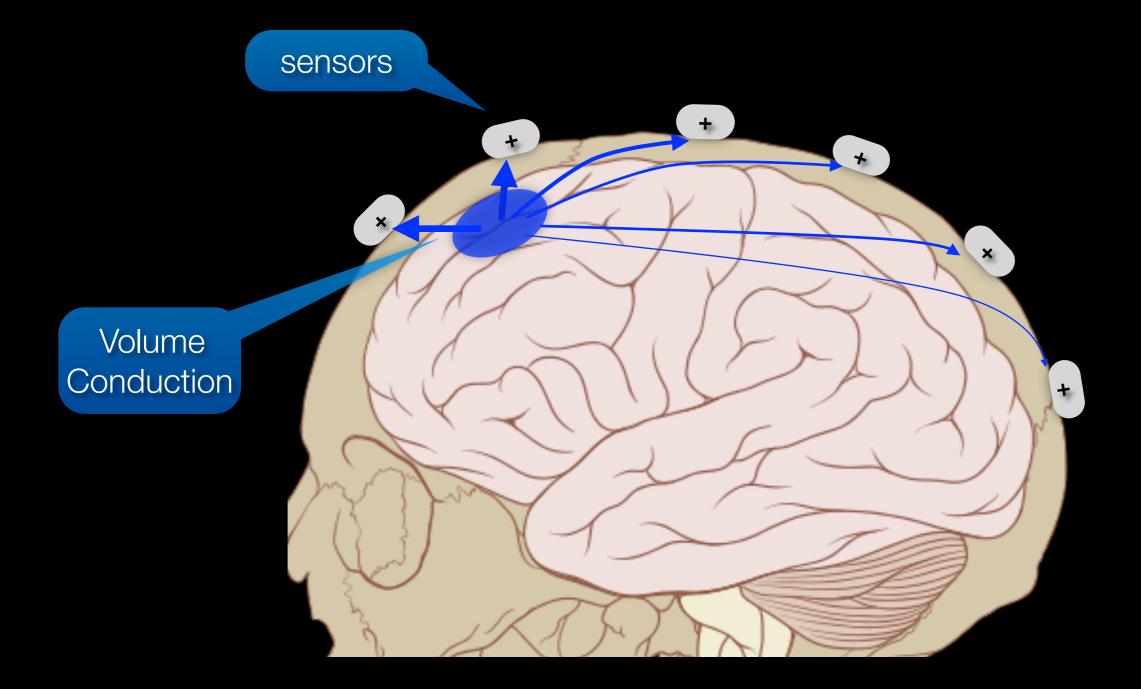
Or

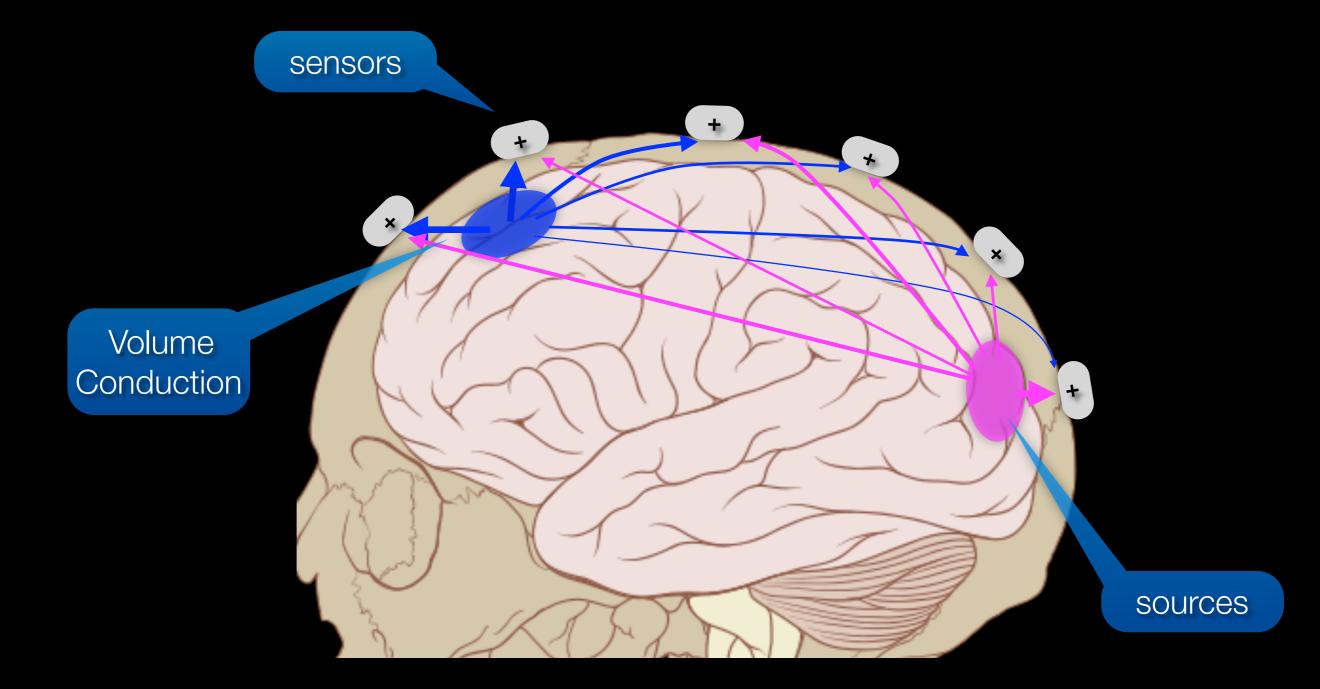


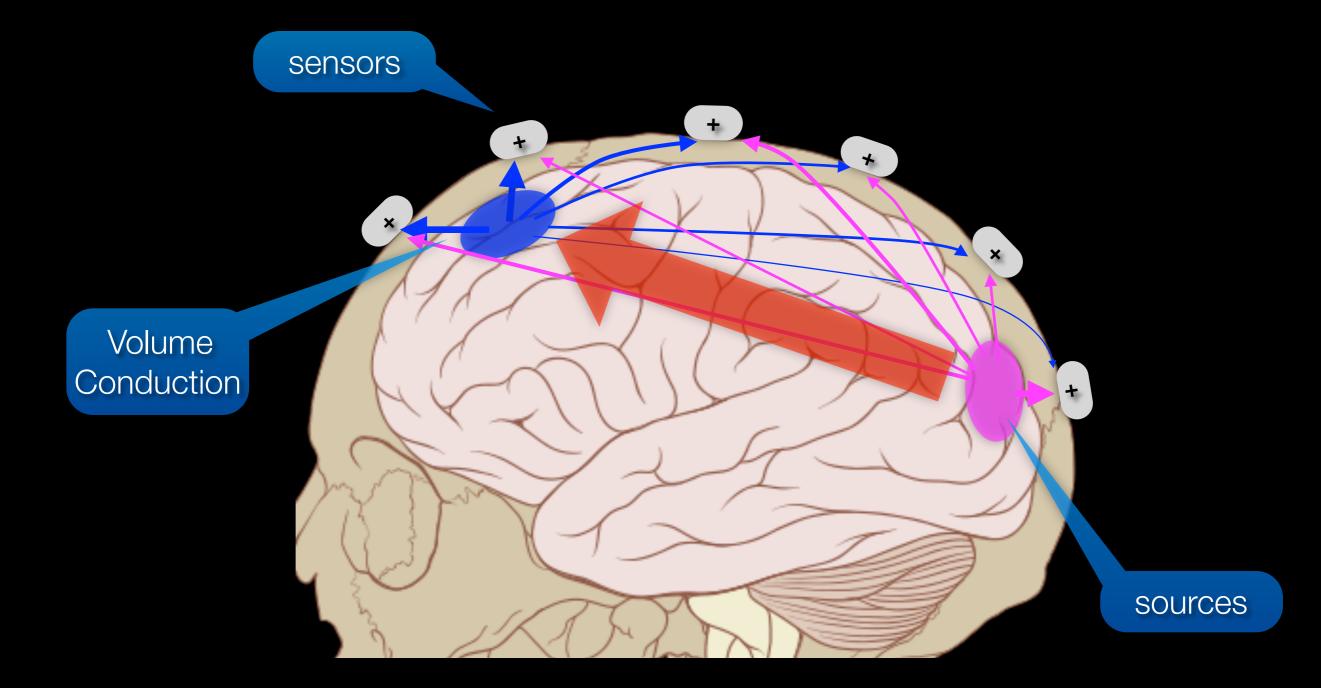
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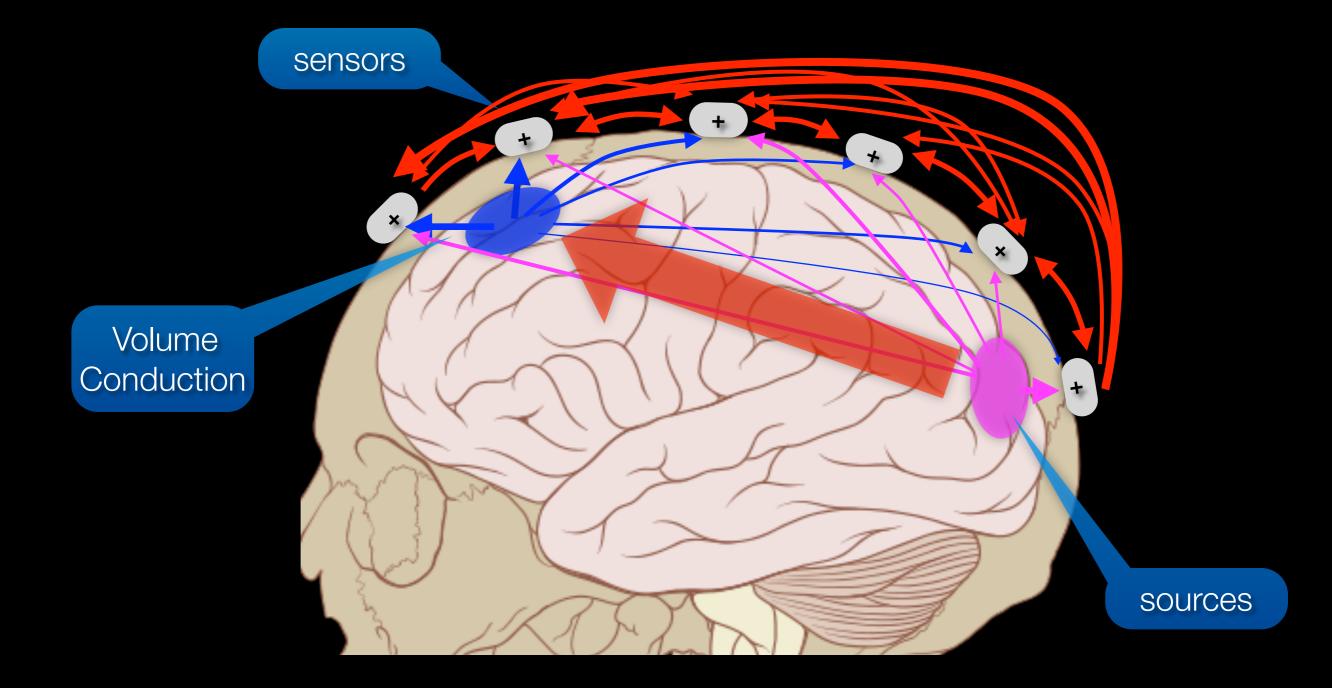


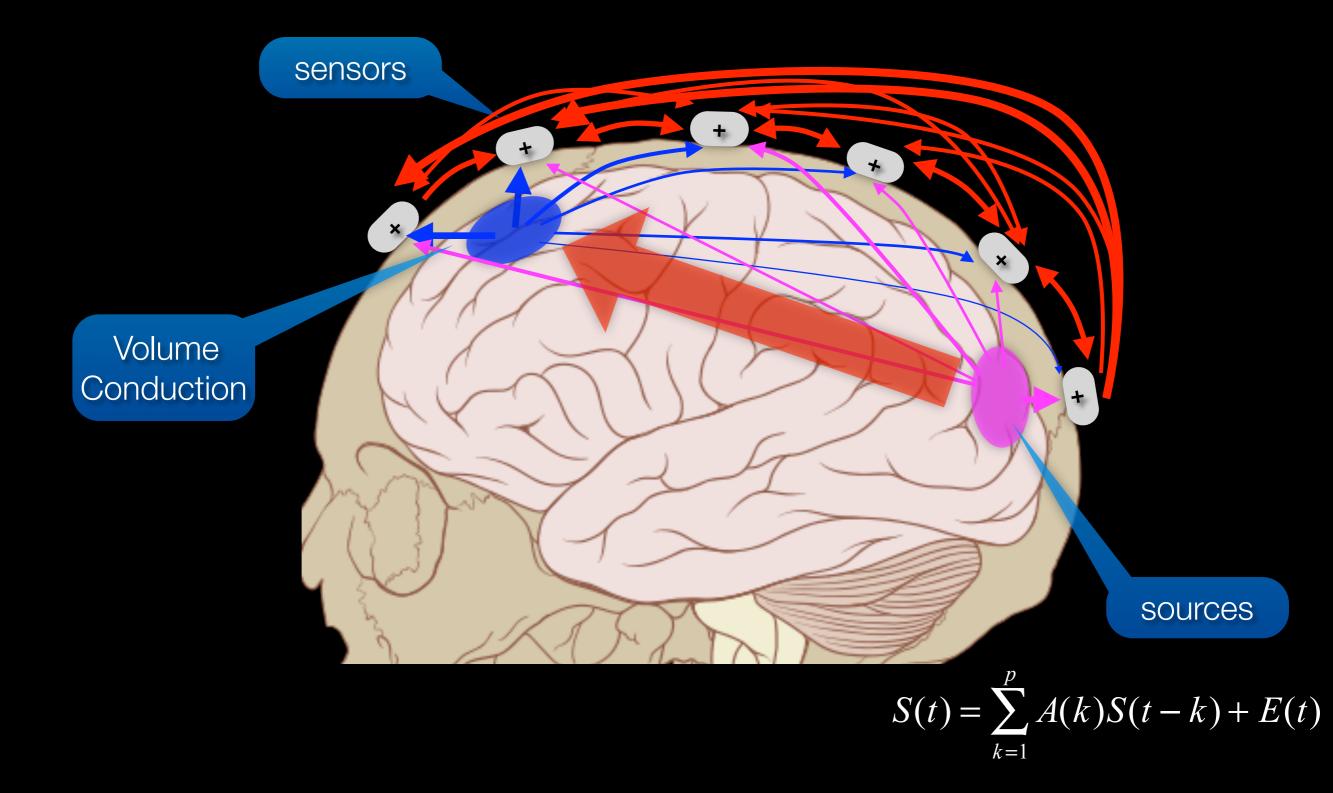


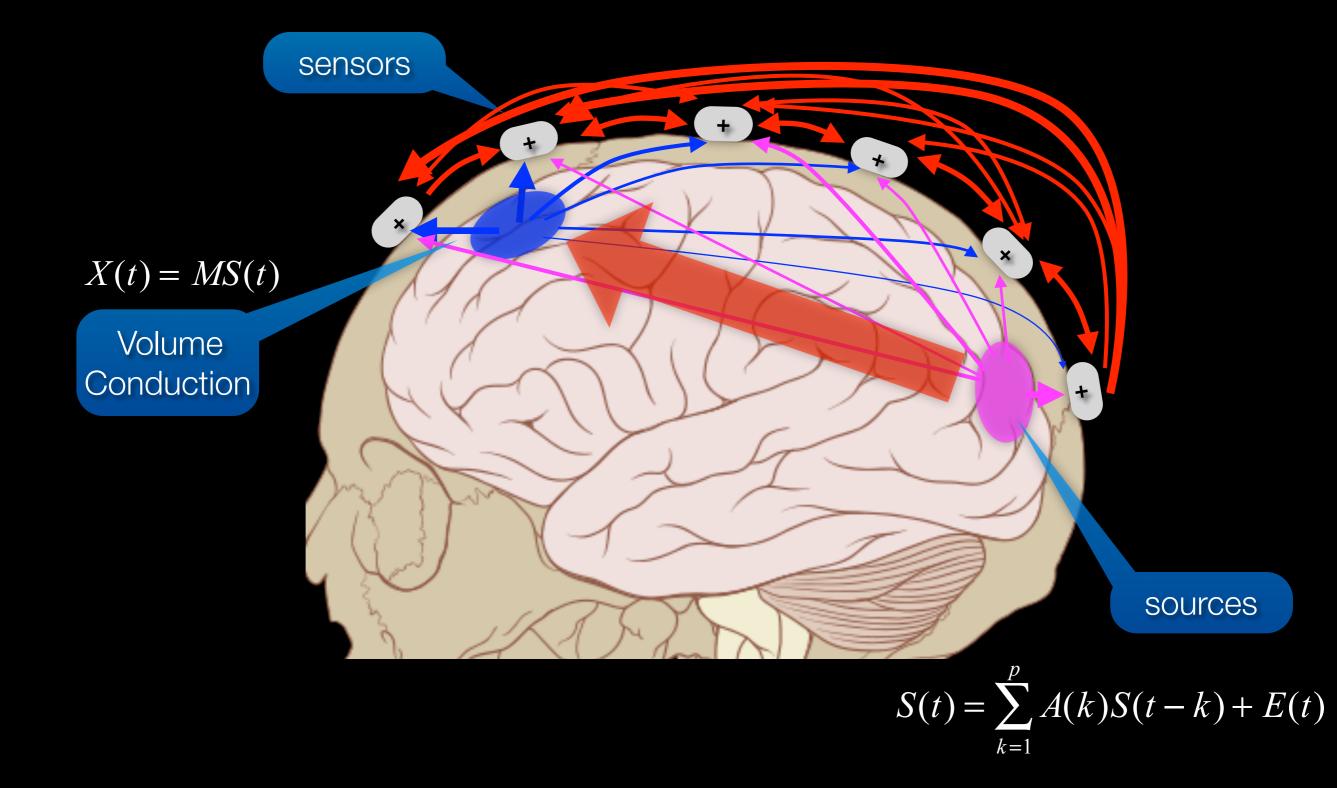


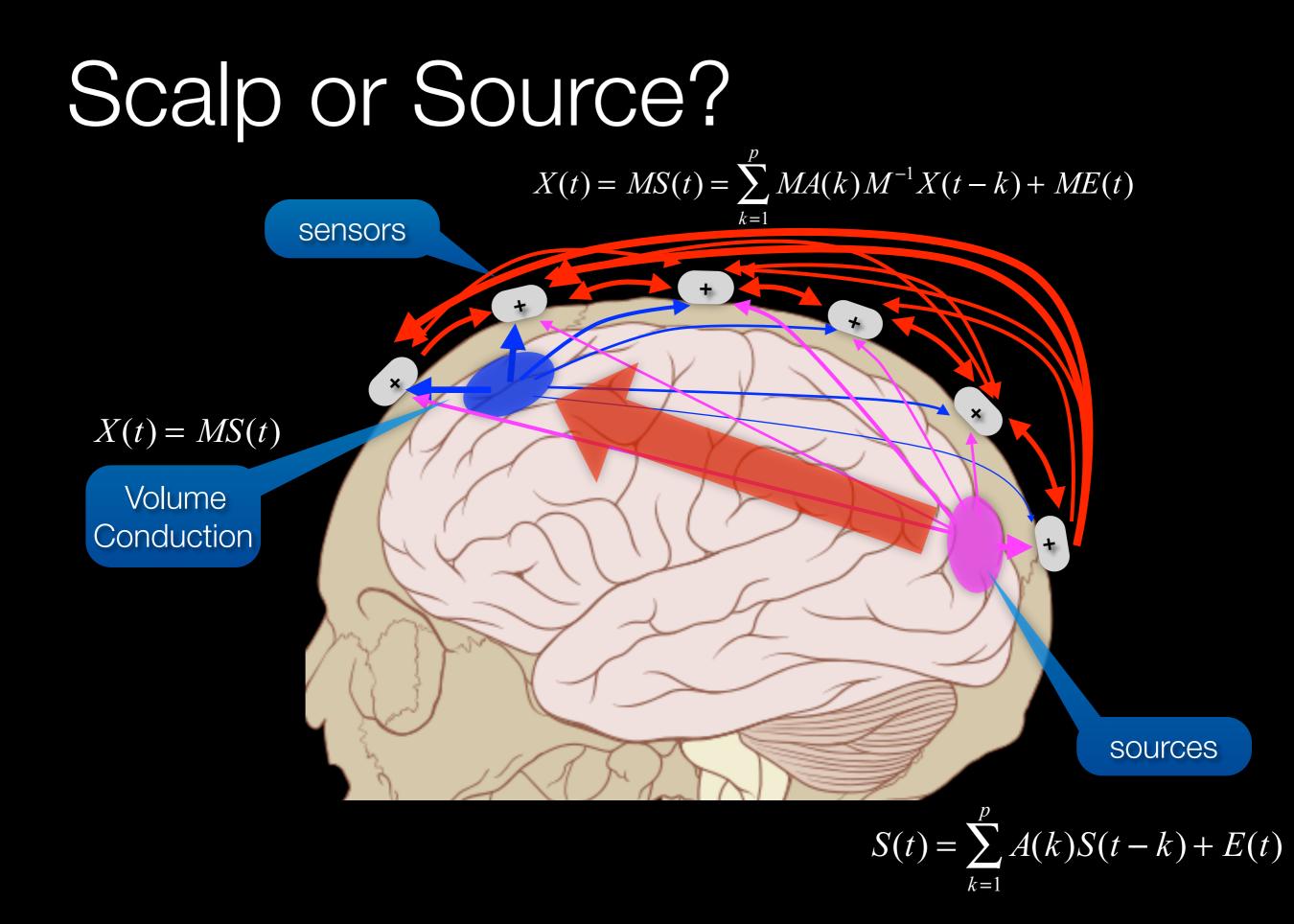


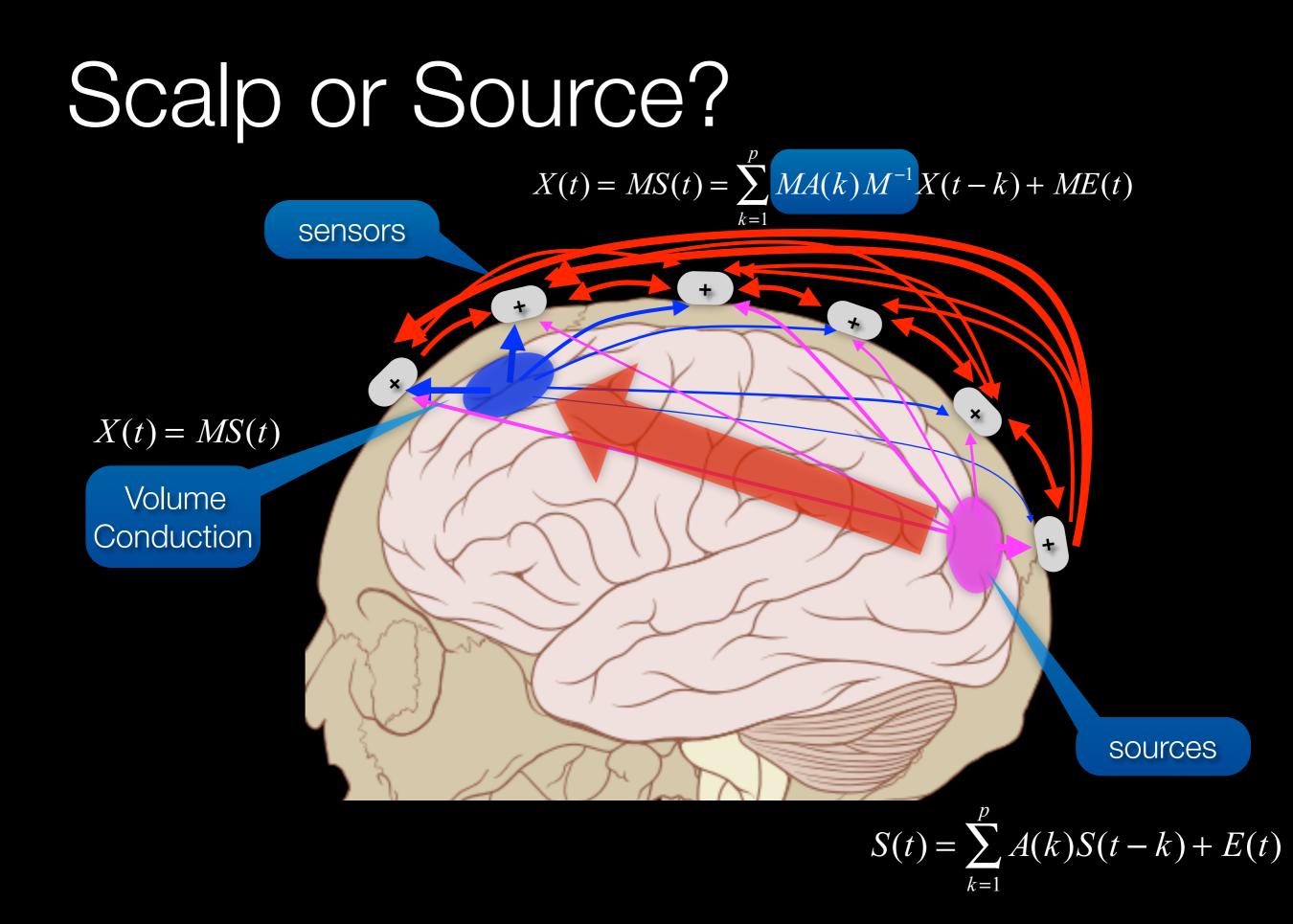


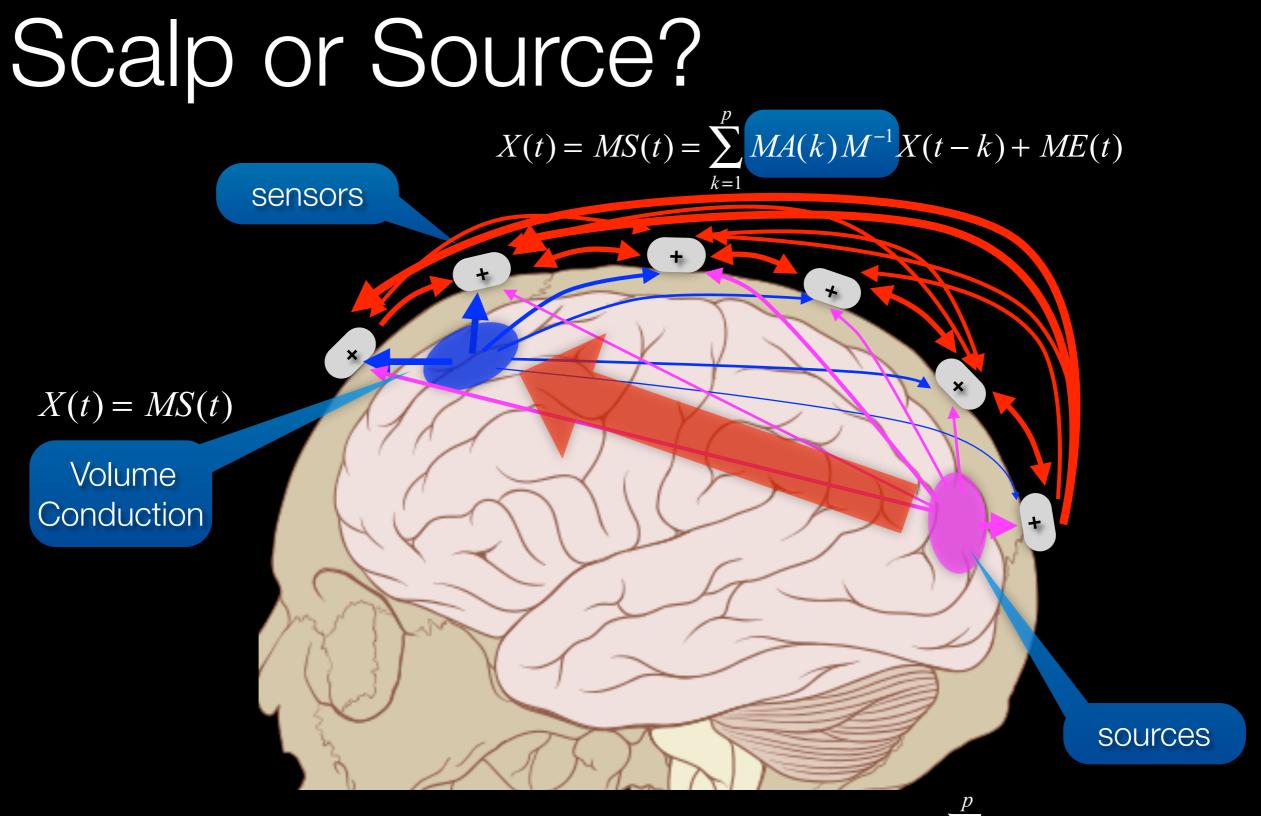












**Solution?** Source Separation

 $S(t) = \sum_{k=1}^{p} A(k)S(t-k) + E(t)$ 



Isn't it a contradiction to examine dependence between Independent Components?



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- Instantaneous (e.g., Infomax) ICA only explicitly enforces instantaneous independence. Time-delayed dependencies may be preserved



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- Instantaneous (e.g., Infomax) ICA only explicitly enforces instantaneous independence. Time-delayed dependencies may be preserved
- ICA seeks to maximize *global* independence (over entire recording session), transient dependencies are often preserved



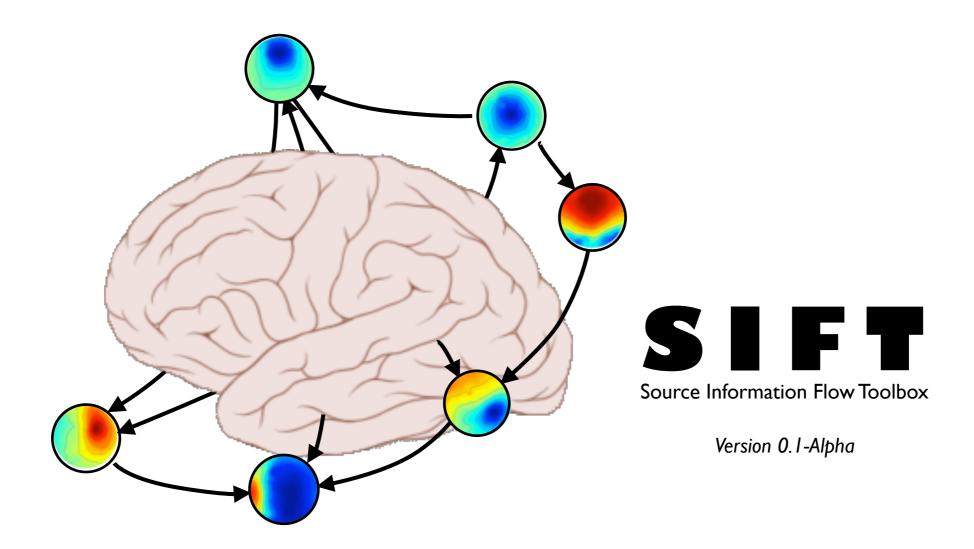
SCSA EM

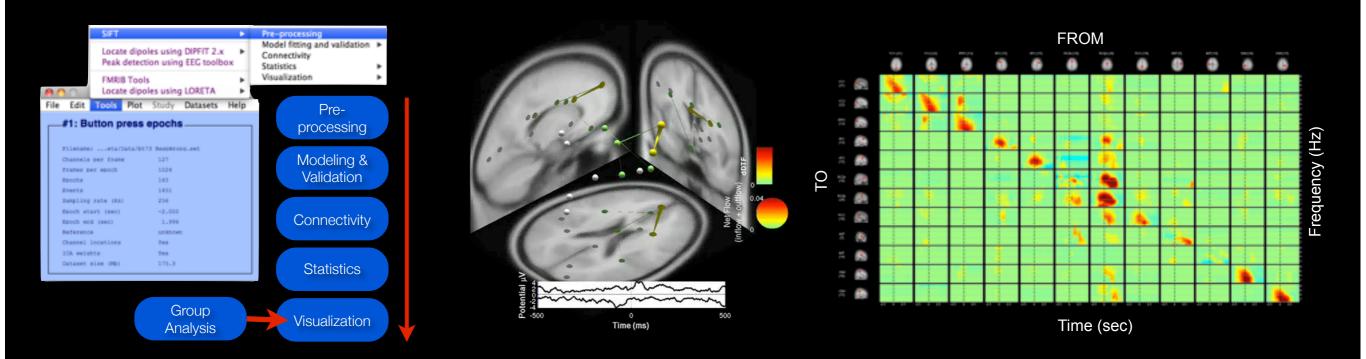
0.5

0.6

SCSA **2**<sup>CSA</sup> CICAAR **Connectivity Error** ICA 02 0.3 0.4 0.5 0.6 SCSA EM SCSA EM SCSA SCSA – CSA + CSA **Z** CICAAR **MVARICA MVARICA** ICA **ICA** 0.2 0.2 0.3 01 0.3 0.4 0.5 0.6 01 0.4 0.5 0.6 SCSA EM SCSA EM SCSA SCSA nation Error N CSA LO CSA ┉┉ <mark>┝╺╫</mark>╋┽╴╶┾┽╍┼╴ Z CICAAR ╓<sub>┿╫╴┿┼</sub>┽ MVARICA **MVARICA ICA ICA** 0.6 0.1 0.2 0.3 0.4 0.5 0.6 0.2 0.3 0.4 0.5 SCSA EM SCSA EM SCSA SCSA ლ CSA co CSA Ż <sub>CICAAR</sub> **MVARICA MVARICA** ICA **ICA** 0.2 0.3 0.4 0.5 0.6 0.2 0.3 0.4 0.5 0.6 01 0.1 1-AUC 1-AUC

Haufe et al, 2008







 A new (alpha) toolbox for source-space electrophysiological information flow and causality analysis (single-subject or group analysis) integrated into the EEGLAB software environment



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- Novel interactive visualization methods for exploratory analysis of connectivity across time, frequency, and spatial location



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- Modular architecture intended to support multiple modeling approaches
- Emphasis on time-frequency domain approaches
- Novel interactive visualization methods for exploratory analysis of connectivity across time, frequency, and spatial location
- Requirements: EEGLAB, MATLAB<sup>TM</sup> 2008b, Signal Processing Toolbox, Statistics Toolbox (the latter two dependencies may be removed in the future)



### SIFT: Acknowledgements

- Arnaud Delorme
- Scott Makeig
- Christian Kothe
- Nima Bigdely-Shamlo
- Wes Thompson
- SCCN

		SIFT				-	Pre-processing		
		Locate dipoles using DIPFIT 2.x Peak detection using EEG toolbox					Model fitting and validation Connectivity Statistics	•	
		FMRI	B Tools	5		•	Visualization	•	
0	0	Locat	e dipo	les using	LORETA	•			
File	Edit	Tools	Plot	Study	Datasets	Help			
#	#1: Button press epochs								

Filename: ...eta/Data/bt73 RespWrong.set

Channels per frame	127
Frames per epoch	1024
Epochs	165
Events	1451
Sampling rate (Hz)	256
Epoch start (sec)	-2.000
Epoch end (sec)	1.996
Reference	unknown
Channel locations	Yes
ICA weights	Yes
Dataset size (Mb)	175.3



	SIFT					-	Pre	e-processing	
Locate dipoles using DIPFIT 2.x Peak detection using EEG toolbox					Model fitting and validation Connectivity Statistics				
		FMRI	B Tools	5		•	Vis	sualization	
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Reference

ICA weights



		SIFT				•	Pre-processing	
		Locate dipoles using DIPFIT 2.x Peak detection using EEG toolbox					Model fitting and validation Connectivity Statistics	•
		FMRI	B Tools	5		•	Visualization	►
0	0	Locat	e dipo	les using	LORETA	►		
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#	#1: Bi	utton p	ress	Marine Marine				

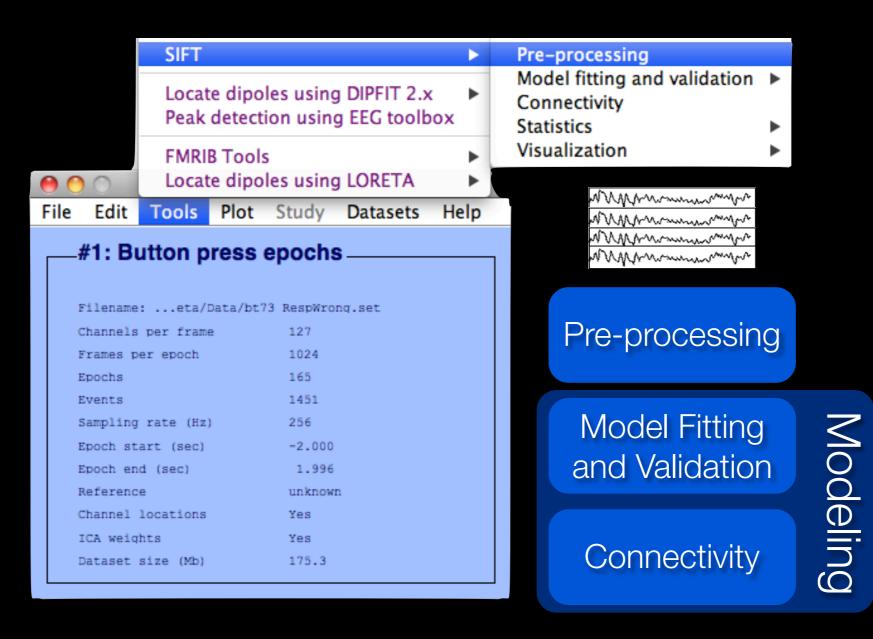
#### \_#1: Button press epochs -

Filename: ...eta/Data/bt73 RespWrong.set

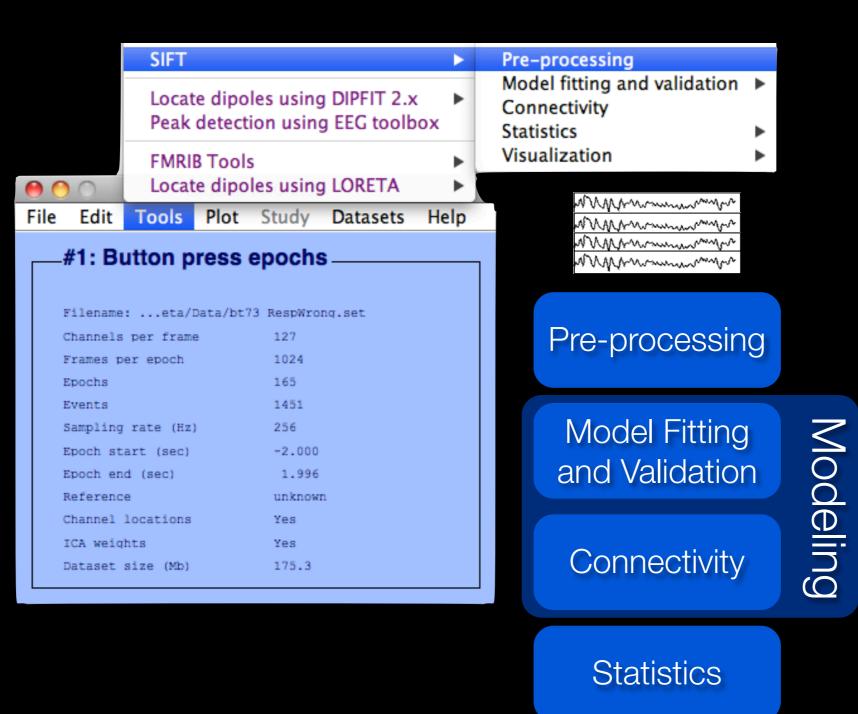
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#### Pre-processing

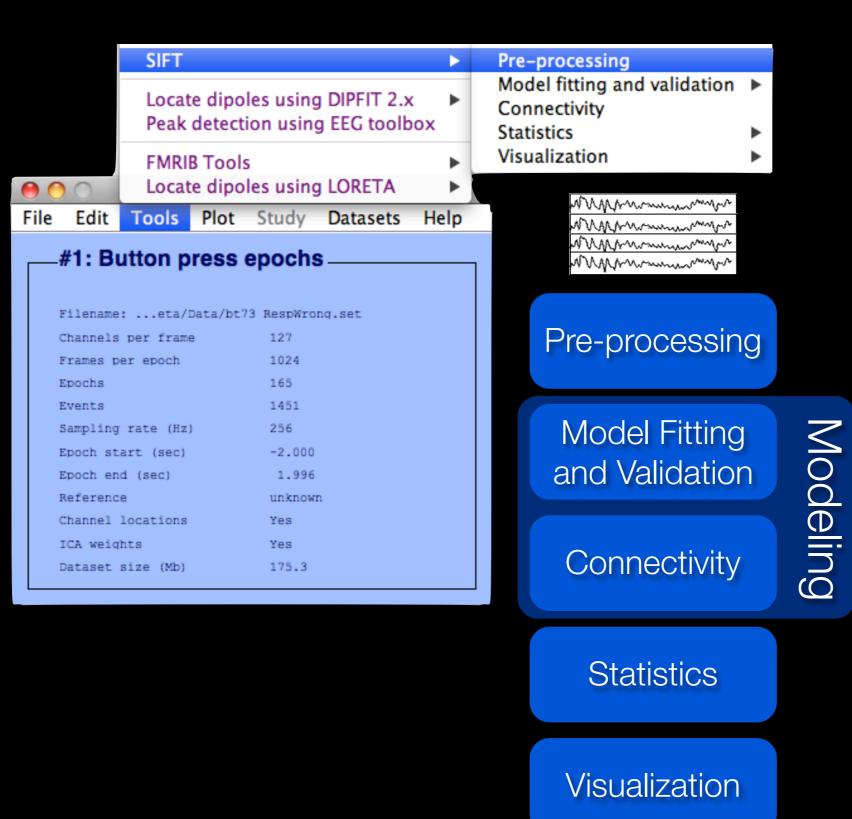




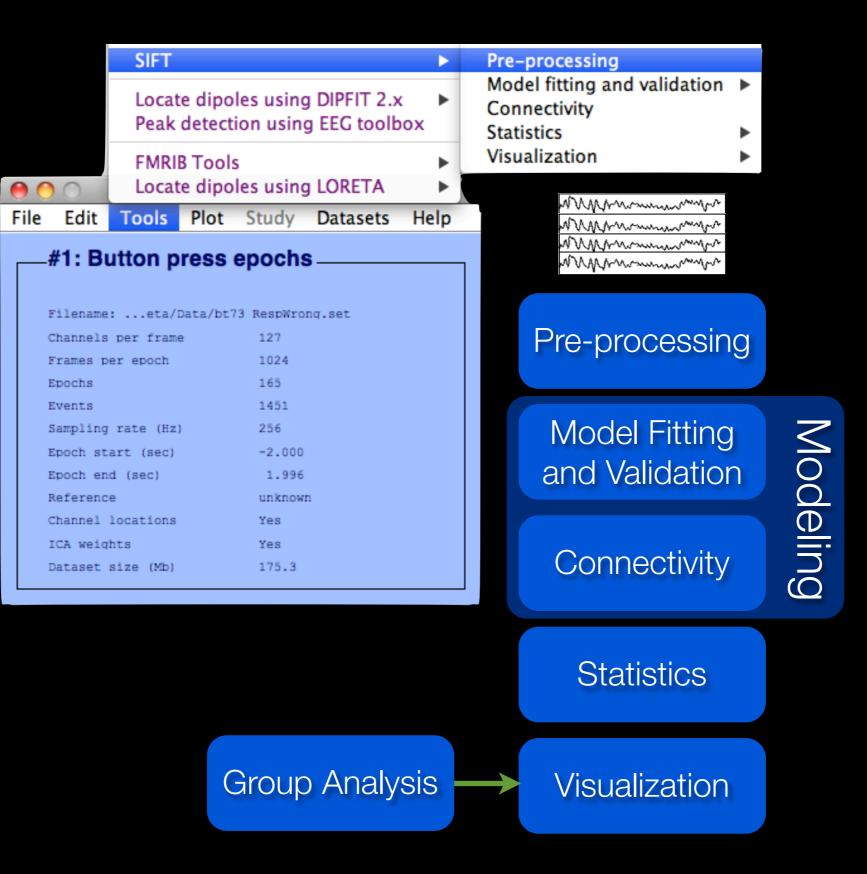




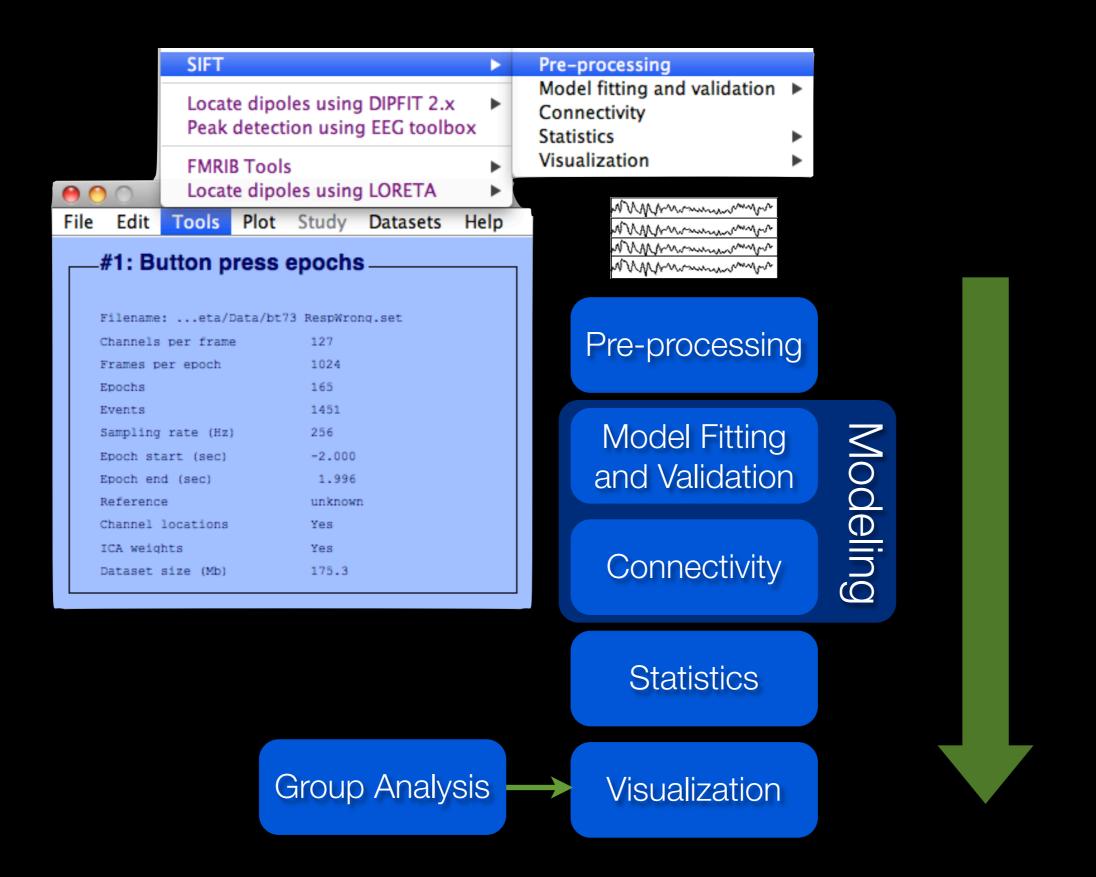














#### Preprocessing

#### Modeling

#### Statistics

#### Source-separation and localization (performed externally using EEGLAB or other toolboxes)

- Filtering/Detrending
- Downsampling
- Differencing
- Normalization (temporal or ensemble)
- Trial balancing
- Tests for stationarity of the data (linear methods)



#### Preprocessing

#### Modeling

#### Statistics

#### Visualization

#### Pre-processing

Model fitting and validation Connectivity Statistics Visualization

\varTheta 🕙 🕙 Preprocessing O	ptions					
∄ 2↓ 📼 🗠 ₽‡						
▼ Miscellaneous						
VerbosityLevel	2					
▼ Data Selection						
<ul> <li>SelectComponents</li> </ul>						
ComponentsToKeep	1; 2; 3; 4; 5; 6;					
EpochTimeRange	[-0.5 0]					
TrialSubsetToUse	0					
▼ Filtering						
NewSamplingRate	0					
FilterData	[0.01 0]					
<ul> <li>DifferenceData</li> </ul>	$\checkmark$					
DifferencingOrder	1					
Detrend	$\checkmark$					
DetrendingMethod	linear					
Normalization						
▼ NormalizeData						
Method	ensemble					
NormalizeData Data normalization. Normalize trials across time, ensemble, or both						
Help Cancel OK						





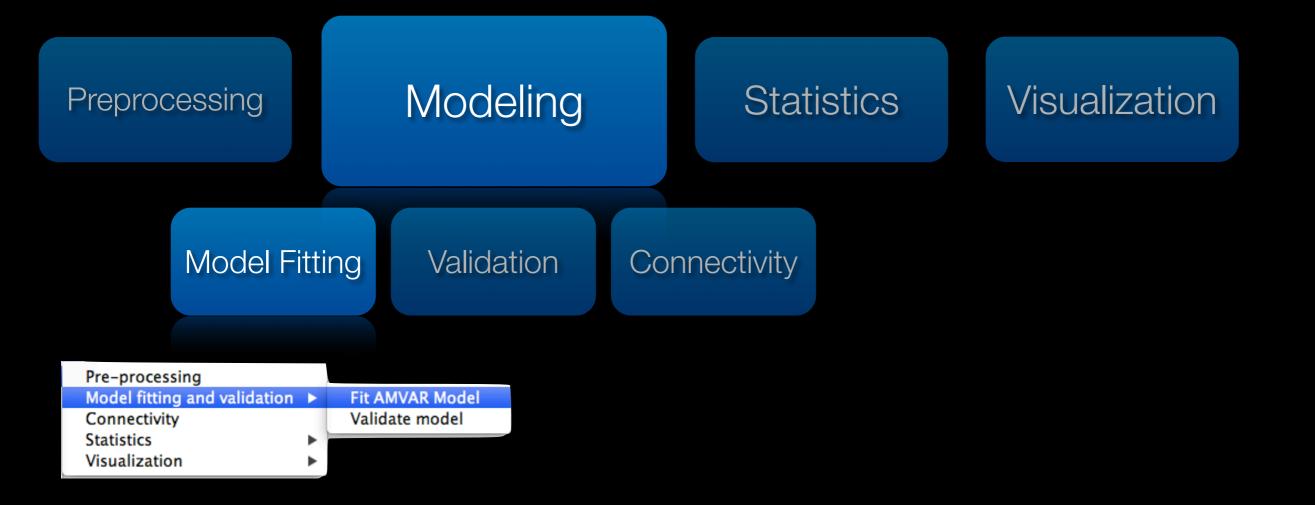




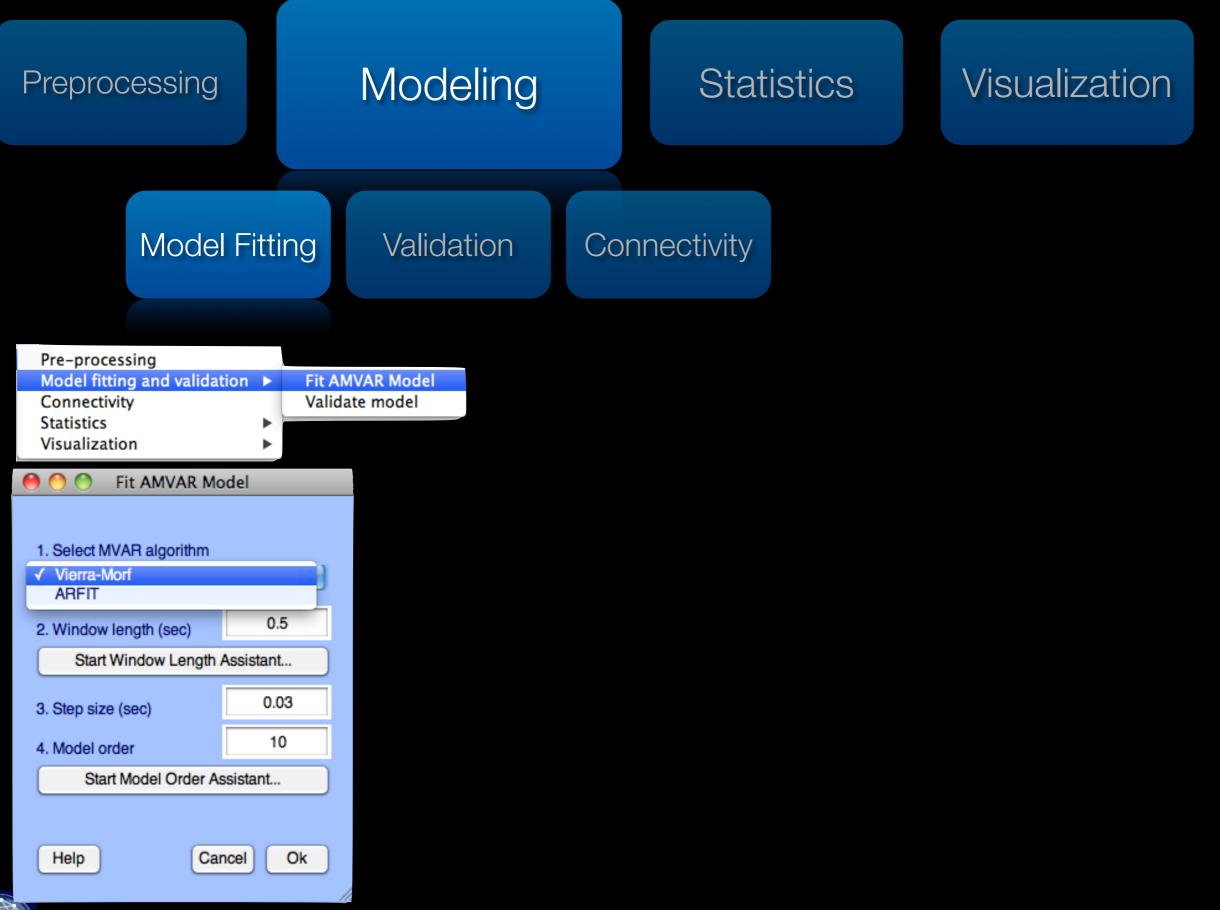


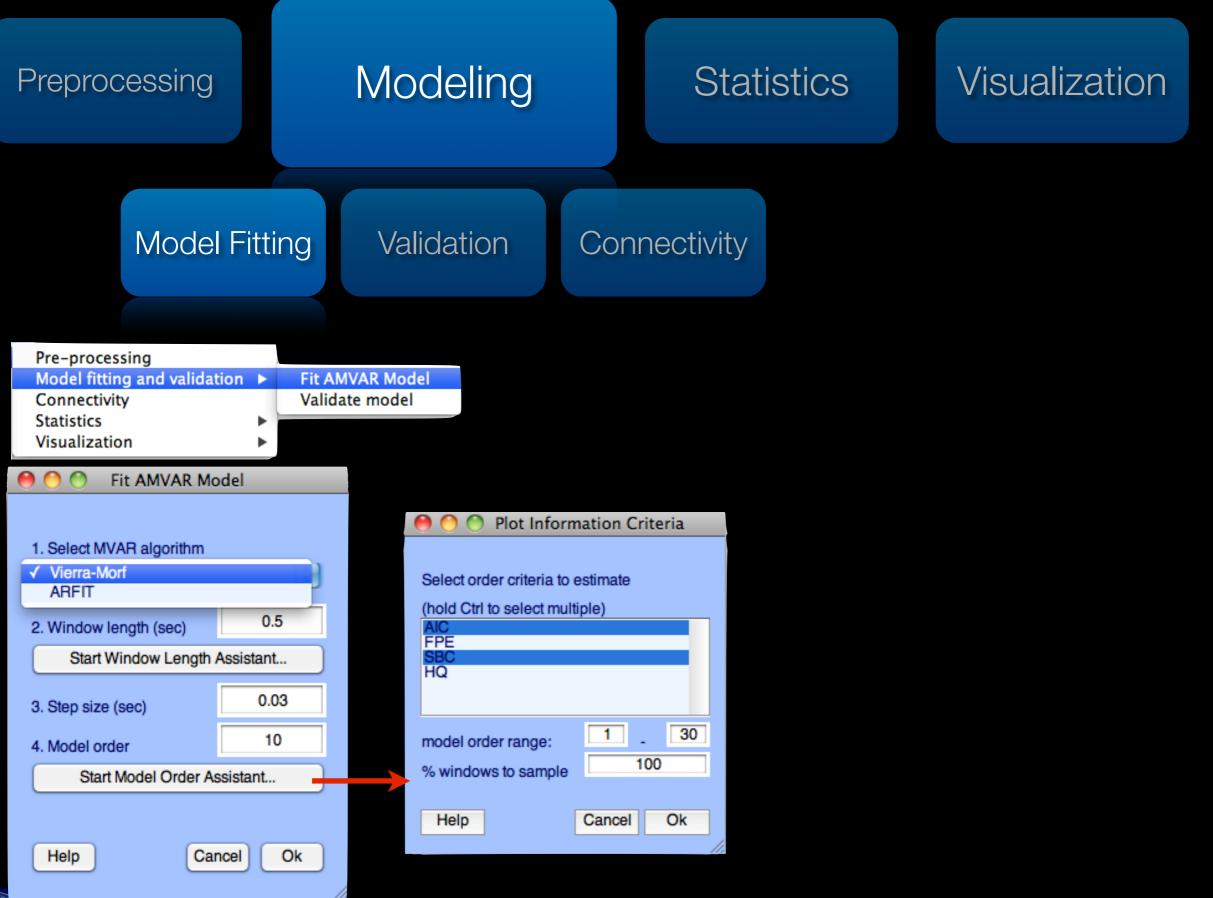
Ρ	Preprocessing		Modeling		Statistics	Visualization			
		Model Fitt	ing Validation	Con	nectivity				
			Linear		Nonlinear/Nonstationary				
	met	MVAR Mo Sparse M Bayesian Kalman Fi	VAR MVAR		Dual Extended Kalman Filtering				
	ametri	phase spe	netric MVAR (minimur ectral factorization) e phase distribution	Transfer Entropy					

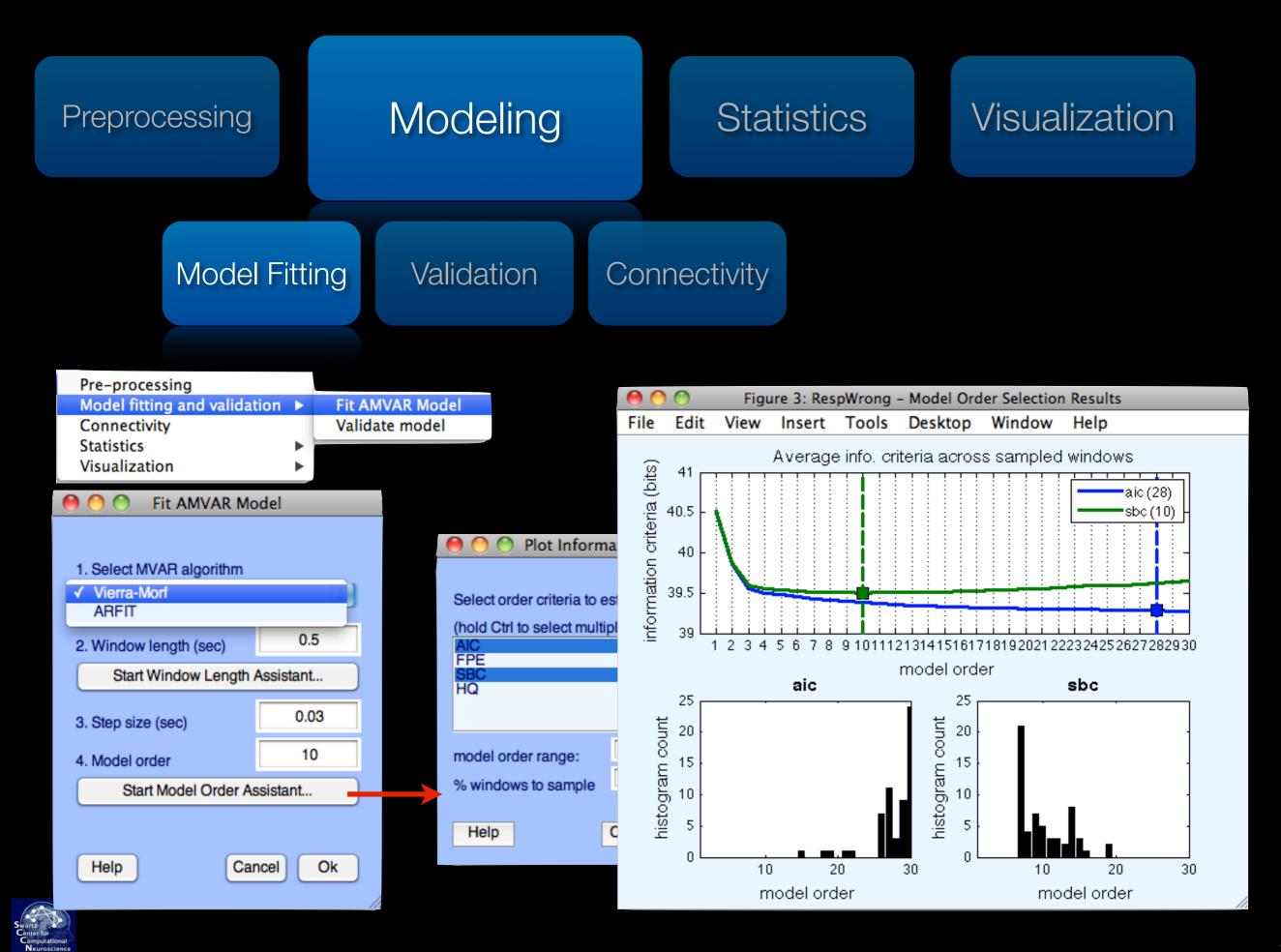














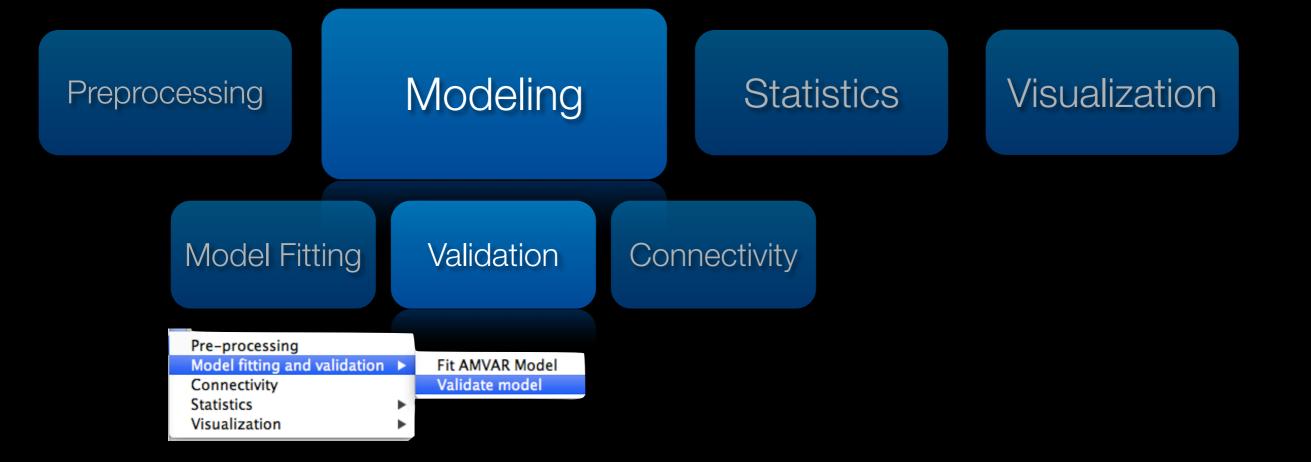
- Whiteness of Residuals
  - Portmanteau tests
  - Autocorrelation function
- Model Consistency
- Model Stability



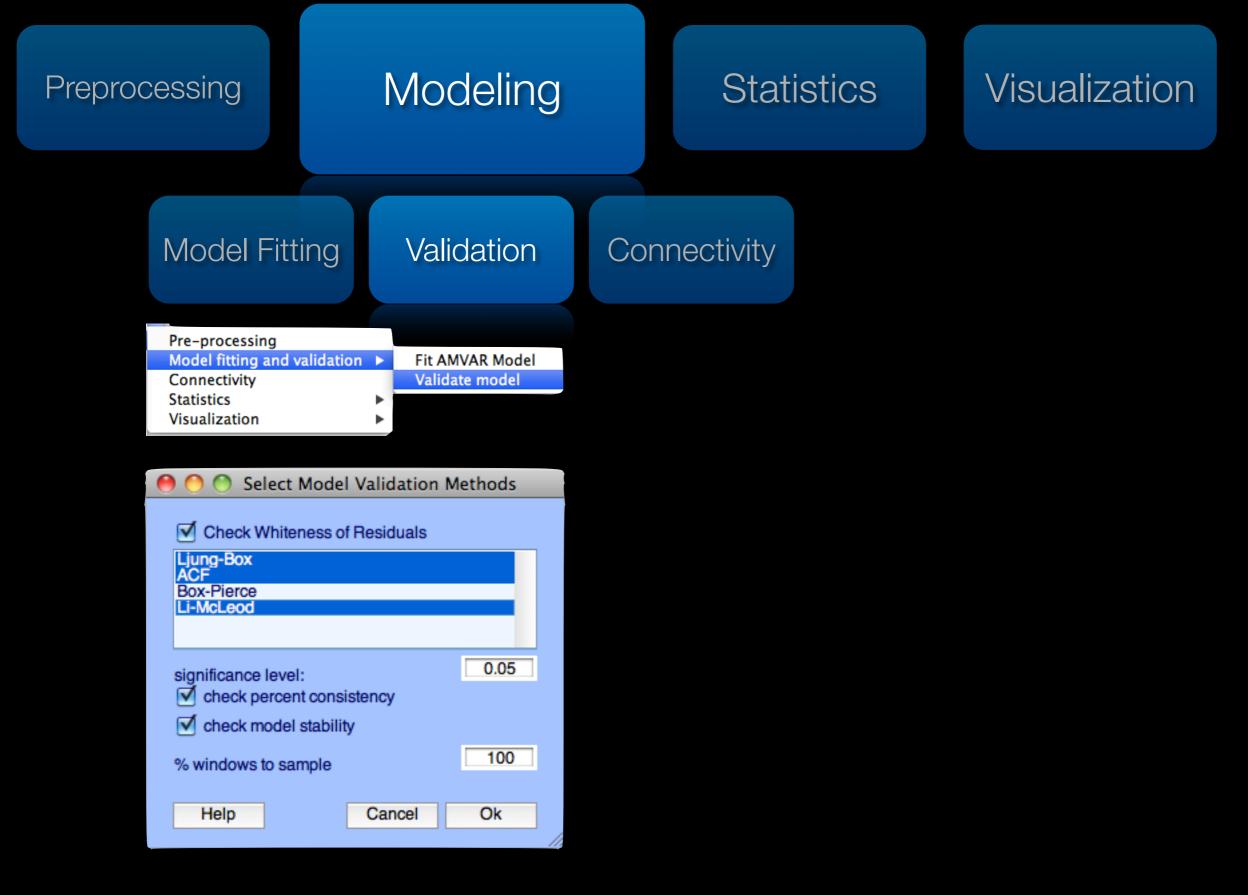




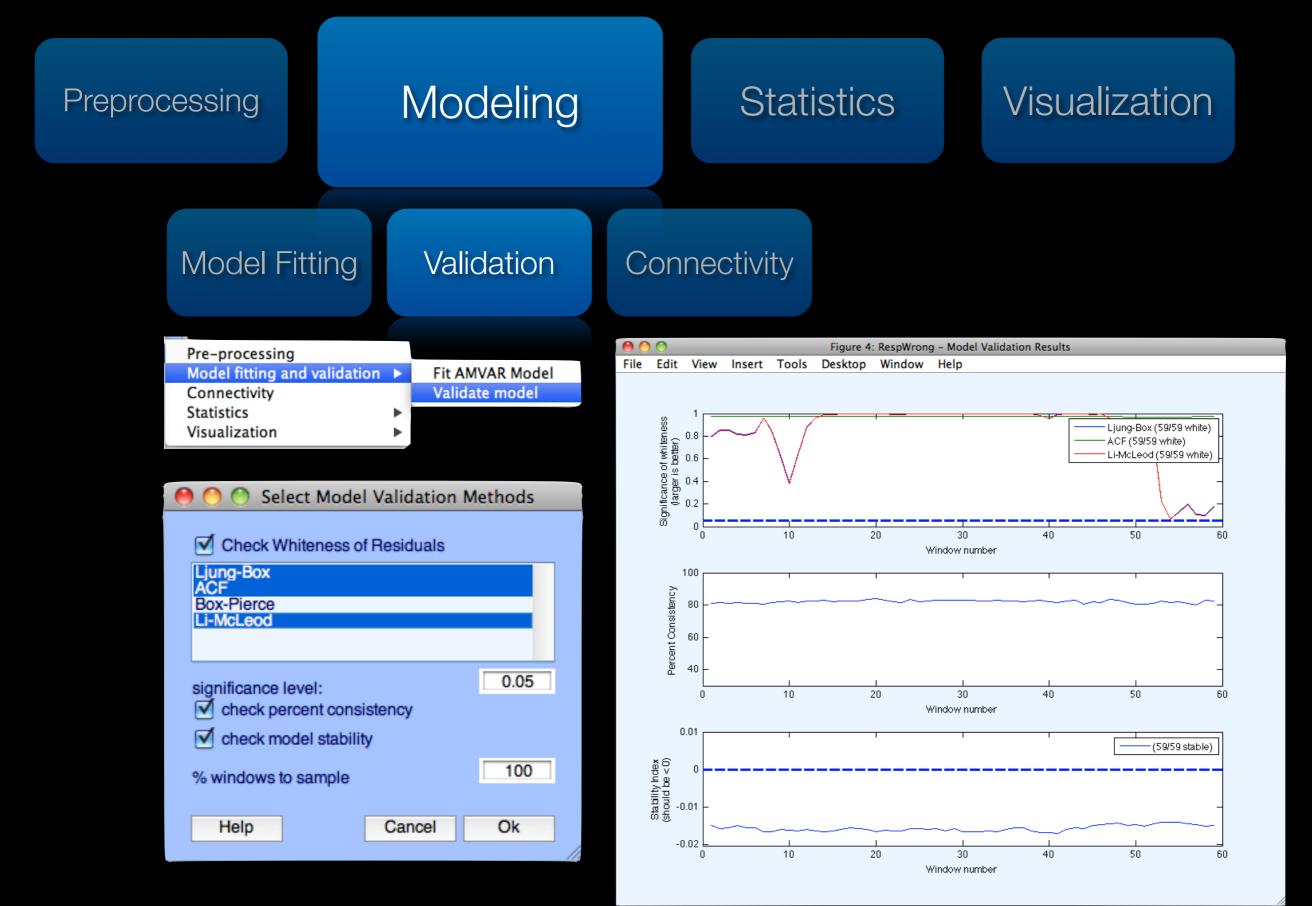








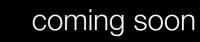






Preprocessing	Modeling	Sta	atistics	Visualization
Model Fitt	ting Validation Co	nnectivity	y	
	MVAR		Other	
<ul> <li>Power spectrum (ERSP)</li> <li>Coherence (Coh), Partial Coherence (pCoh), Multiple Coherence (mCoh)</li> <li>Partial Directed Coherence (PDC)</li> <li>Generalized PDC (GPDC)</li> <li>Partial Directed Coherence Factor (PDCF)</li> <li>Renormalized PDC (rPDC) *</li> <li>Directed Transfer Function (DTF)</li> <li>Direct Directed Transfer Function (dDTF)</li> <li>Granger-Geweke Causality (GGC)</li> <li>Conditional GGC</li> <li>Blockwise GGC *</li> </ul>		-Transfer Entra -Multivariate p (mPLV) *	opy * ohase-locking value	





Preprocessing	Modeling	Statistics	Visualization
Model Fitt		nnectivity	
Pre-processing Model fitting and val Connectivity Statistics Visualization	idation  Select connectivity mease (hold Ctrl to select multiple  Directed Tranfer Function Direct DTF (dDTF) Direct DTF (dDTF) Direct DTF (with full) Full-frequency DTF ( PARTIAL DIRECTED Partial Directed Cohe Normalized PDC (nP Generalized Partial Di Partial Directed Cohe Renormalized Partial FGRANGER-GEWEKG Granger-Geweke Ca SPECT RAL COHERE Complex Coherence () SPECT RAL DENSIT Complex Spectral De	ble) ER FUNCTION MEASURES Action (DTF) (TF) Causal normalization) (fDTF) COHERENCE MEASURES Prence (PDC) (D) Directed Coherence (GPDC) Erence Factor (PDCF) Directed Coherence (RPDC) ECAUSALITY MEASURES ausality (GGC) ENCE MEASURES (Coh) (Coh) (MEASURES ensity Hitude of complex measures	
Itional	Help	Cancel Ok	

#### Preprocessing

## Modeling

# Statistics

### Visualization



# Statistics

### Visualization

## Parametric

Asymptotic analytic estimates of confidence intervals Applies to: PDC, nPDC, DTF, nDTF, rPDC Tests: H<sub>null</sub>, H<sub>base</sub>, H<sub>AB</sub>

Confidence intervals using thinplate smoothing splines Applies to: dDTF Tests: H<sub>base</sub>, H<sub>AB</sub>



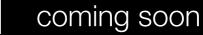


 $H_{AB}$ :  $\mathbf{C}^{A_{ij}} = \mathbf{C}^{B_{ij}}$ 









# **Statistics**

### Visualization

## Parametric

# Non-parametric

#### Asymptotic analytic estimates of confidence intervals Applies to: PDC, nPDC, DTF,

nDTF, rPDC Tests: H<sub>null</sub>, H<sub>base</sub>, H<sub>AB</sub>

#### Confidence intervals using thinplate smoothing splines Applies to: dDTF Tests: H<sub>base</sub>, H<sub>AB</sub>

#### Phase-randomization

Applies to: all Tests: H<sub>null</sub>

#### Permutation Tests

Applies to: all Tests: H<sub>AB</sub>, H<sub>base</sub>

# Bootstrap and Jacknife

Applies to: all Tests: H<sub>AB</sub>, H<sub>base</sub>



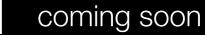


 $H_{AB}$ :  $\mathbf{C}^{A_{ij}} = \mathbf{C}^{B_{ij}}$ 









#### Preprocessing

### Modeling

### Statistics

## Visualization











Statistics

### Visualization

# Interactive Time-Frequency Grid











### Visualization

# Interactive Time-Frequency Grid

# Interactive 3D Causal Brainmovie









Statistics

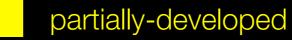
### Visualization

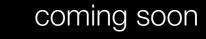
Interactive Time-Frequency Grid

Interactive 3D Causal Brainmovie

Causal Density Movie









Statistics

## Visualization

Interactive Time-Frequency Grid

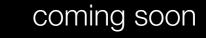
Interactive 3D Causal Brainmovie

Causal Density Movie

Directed Graphs on anatomicals (ECoG)









Statistics

## Visualization

Interactive Time-Frequency Grid

Interactive 3D Causal Brainmovie

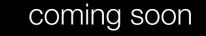
Causal Density Movie

Directed Graphs on anatomicals (ECoG)

and more...









Statistics

Visualization

Interactive Time-Frequency Grid

Interactive 3D Causal Brainmovie

Causal Density Movie

Directed Graphs on anatomicals (ECoG)

### and more...

All of these currently support single-subject or (in beta version) group analysis ROI connectivity analysis can currently be performed using dipole clustering



# Interactive Time-Frequency Grid

Pre-processing Model fitting and validation Connectivity	•	
Statistics	Þ.	
Visualization	•	Time-Frequency Grid
		BrainMovie3D
		Causal Projection

\varTheta 🔿 🔿 Time Frequency Grid Options			
	]		
DisplayProperties			
ConnectivityMethods	DTF		
ColorLimits	100		
TimesToPlot	[-0.75 0.98828125]		
FrequenciesToPlot	[1:50]		
PlotContour			
MatrixLayout	all		
PlottingOrder	0		
SourceMarginPlot	dipole		
NodeLabels	{ <b>'8', '11', '13', '19', '20'</b>		
EventMarkers	{{0, 'r', ':', 2}}		
FrequencyScale	linear		
Colormap	jet(300)		
▼ Thresholding			
<ul> <li>Thresholding</li> </ul>	Simple		
PercentileThreshold	100		
AbsoluteThreshold	0		
▼ DataProcessing			
Baseline	0		
Smooth2D			
SubplotExpansion			
SubplotExpansionProperties			
▼ FrequencyMarkers			
FrequencyMarkers	0		
FrequencyMarkerColor	0		
▼ TextAndFont			
TitleString			
TitleFontSize	12		
AxesFontSize	10		
TextColor	[1 1 1]		
BackgroundColor	[0 0 0]		
PercentileThreshold Percentile threshold. If of form [perc is applied elementwise across the sp			
Liele Corre			
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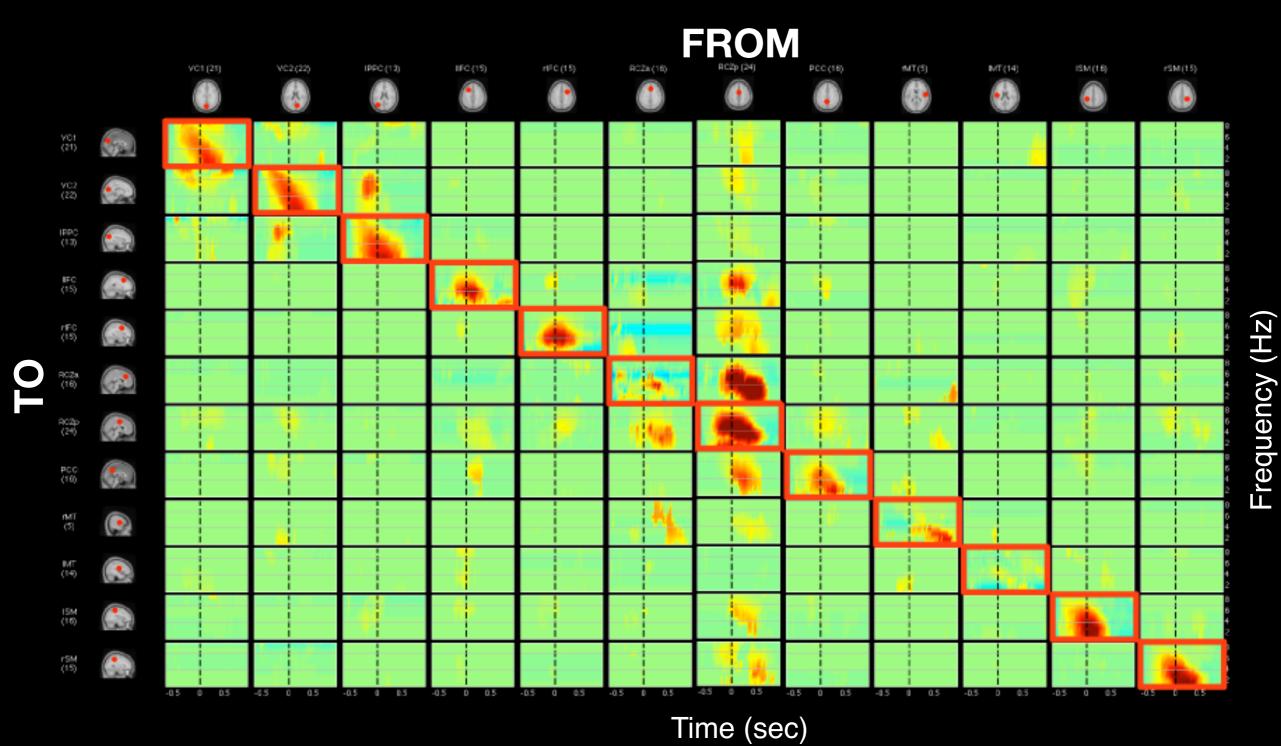


# Interactive Time-Frequency Grid

Pre-processing Model fitting and validation Connectivity	•	
Statistics	Þ.	
Visualization	•	Time-Frequency Grid
		BrainMovie3D
		Causal Projection

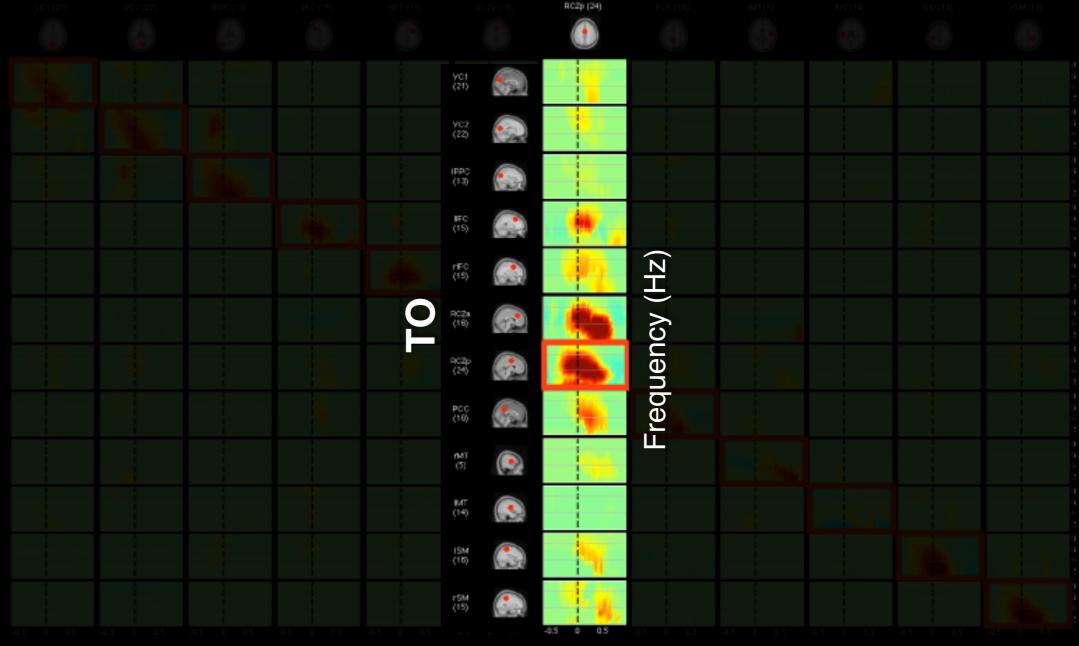
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	]		
DisplayProperties			
ConnectivityMethods	DTF		
ColorLimits	100		
TimesToPlot	[-0.75 0.98828125]		
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FrequencyScale	linear		
Colormap	jet(300)		
▼ Thresholding			
<ul> <li>Thresholding</li> </ul>	Simple		
PercentileThreshold	100		
AbsoluteThreshold	0		
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Baseline	0		
Smooth2D			
SubplotExpansion			
SubplotExpansionProperties			
▼ FrequencyMarkers			
FrequencyMarkers	0		
FrequencyMarkerColor	0		
▼ TextAndFont			
TitleString			
TitleFontSize	12		
AxesFontSize	10		
TextColor	[1 1 1]		
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PercentileThreshold Percentile threshold. If of form [perc is applied elementwise across the sp			
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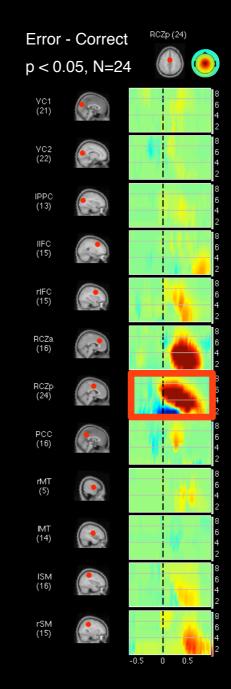
Swartz Center for Computational Neuroscience

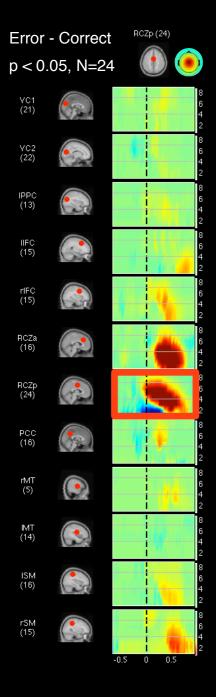
FROM

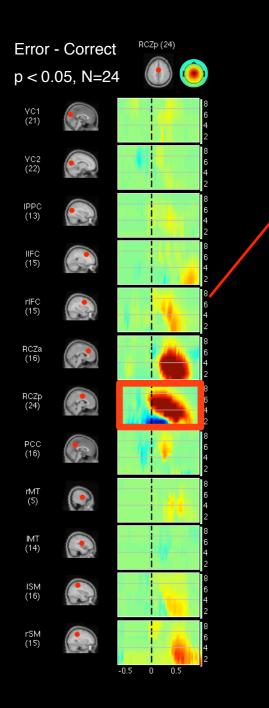


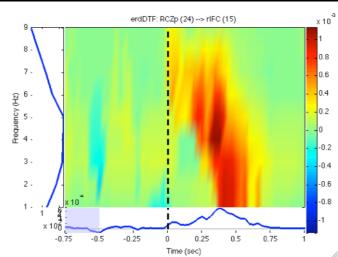
Time (sec)

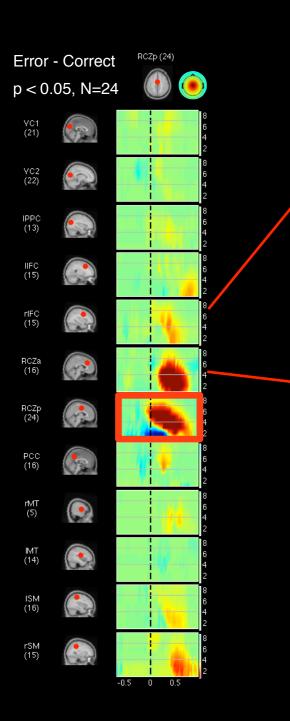


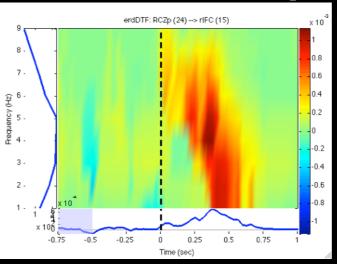


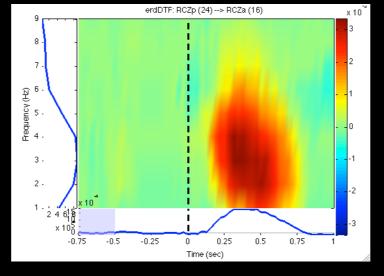


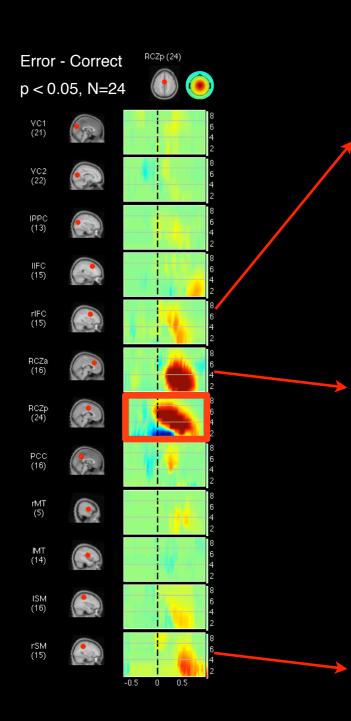


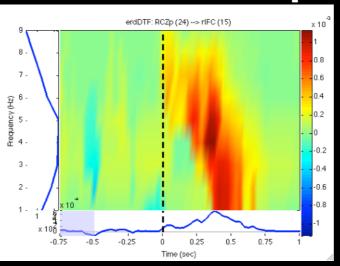


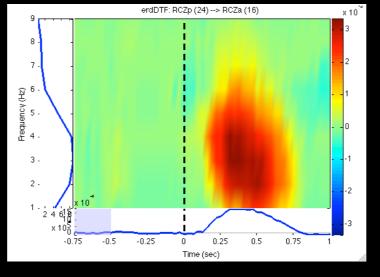


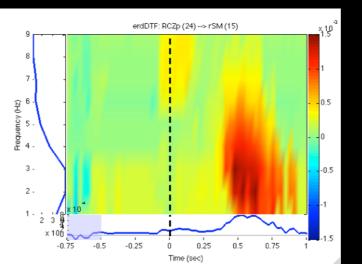


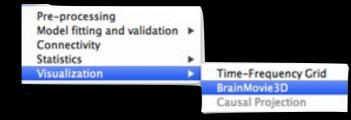














		Pre-processing Model fitting and validation Connectivity	•	
		Statistics	•	Time Freewood Cold
		Visualization	-	Time-Frequency Grid
				BrainMovie3D
				Causal Projection
(	•	O BrainMovie3D Cor	ntro	l Panel
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	▼	DataProcessing		0
		ConnectivityMethod		nDTF
		MovieTimeRange		[-0.75 0.98828125]
		FrequenciesToCollapse		[3:7]
		FreqCollapseMethod		mean
		TimeResamplingFactor		0
		SubtractConditions		
		Baseline		0
	W	DisplayProperties		
		NodeLabels		{'8', '11', '13', '19', '20', '2
		NodesToExclude		
		EdgeColorMapping		Connectivity
		EdgeSizeMapping		ConnMagnitude
		NodeColorMapping		AsymmetryRatio 🔹
		NodeSizeMapping		None
	¥	FooterPanelDisplaySpec		Outflow
		icaenvelopevars		Inflow
		backprojectedchans		CausalFlow
	W	BrainMovieOptions		Outdegree
		Visibility		Indegree
		RotationPath3D		CausalDegree
		InitialView		AsymmetryRatio
		ProjectGraphOnMRI		VII
		RenderCorticalSurface		
		Transparency		0.7
		UseOpenGL		on
		EventFlashTimes		0
		DisplayLegendPanel		on
		ShowLatency		
		DisplayRTProbability		10.0.01
		BackgroundColor		[0 0 0]

#### NodeColorMapping

Specify mapping for node color. This determines how we index into the colormap. Options are as follows. None: node color is not modulated. Outflow: sum connectivity strengths over outgoing edges. Inflow: sum connectivity strengths over incoming edges. CausalFlow: Outflow-Inflow. Asymmetry Ratio: node colors are defined by the equation C = 0.5\*(1 + 1)outflow-inflow/(outflow+inflow)). This is 0 for exclusive inflow, 1 for exclusive outflow, and 0.5 for balanced inflow/outflow

#### Preview BrainMovie





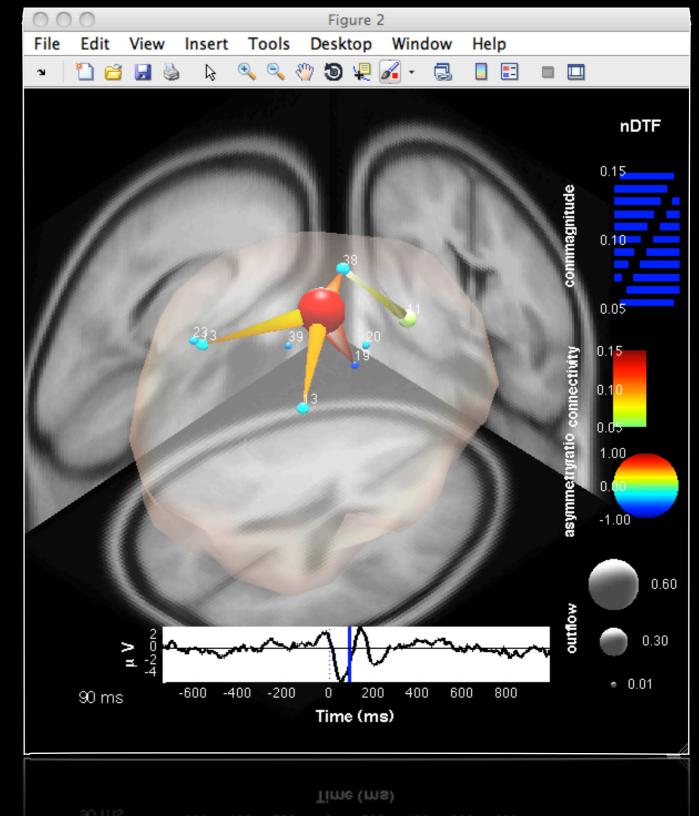
	Pre-processing Model fitting and validation Connectivity Statistics	*	
	Visualization	>	Time-Frequency Grid
		-	BrainMovie3D
			Causal Projection
•	O BrainMovie3D Cor	ntrol	Panel
	■_ ■‡ ₽ <u>↓</u>		
	DataProcessing		*DTE
	ConnectivityMethod		nDTF
	MovieTimeRange		[-0.75 0.98828125]
	FrequenciesToCollapse FreqCollapseMethod		[3:7] mean
	TimeResamplingFactor		mean
	SubtractConditions		
	Baseline		0
_			U I
	DisplayProperties NodeLabels		(19) 1111 1121 1101 1201 12
	NodeLabels		{'8', '11', '13', '19', '20', '2
			Connectivity
	EdgeColorMapping		Connectivity ConnMagnitude
	EdgeSizeMapping		AsymmetryRatio
	NodeColorMapping		
_	NodeSizeMapping		None
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_	backprojectedchans		CausalFlow
Y	BrainMovieOptions		Outdegree
	Visibility RotationPath3D		Indegree
	InitialView		CausalDegree
			AsymmetryRatio
	ProjectGraphOnMRI RenderCorticalSurface		
			0.7
	Transparency		••••
	UseOpenGL EventFlashTimes		on
			0
	DisplayLegendPanel		on
	ShowLatency		
	DisplayRTProbability BaskgroundColor		[0 0 0]
	BackgroundColor		[0 0 0]

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#### - Preview BrainMovie

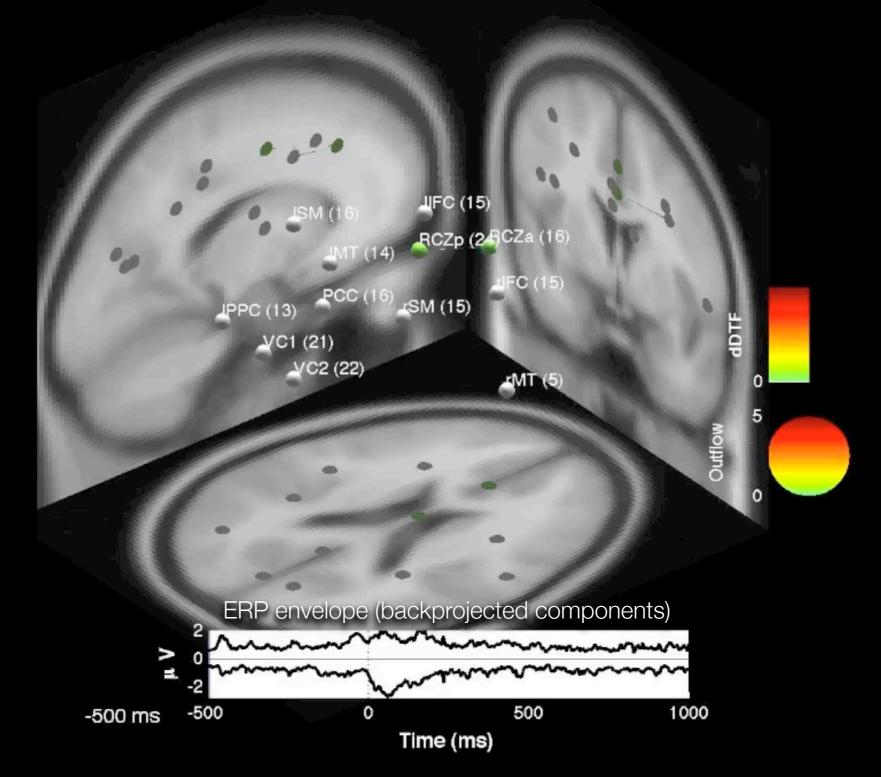




Error > Correct (p < 0.05, N=24)

dDTF

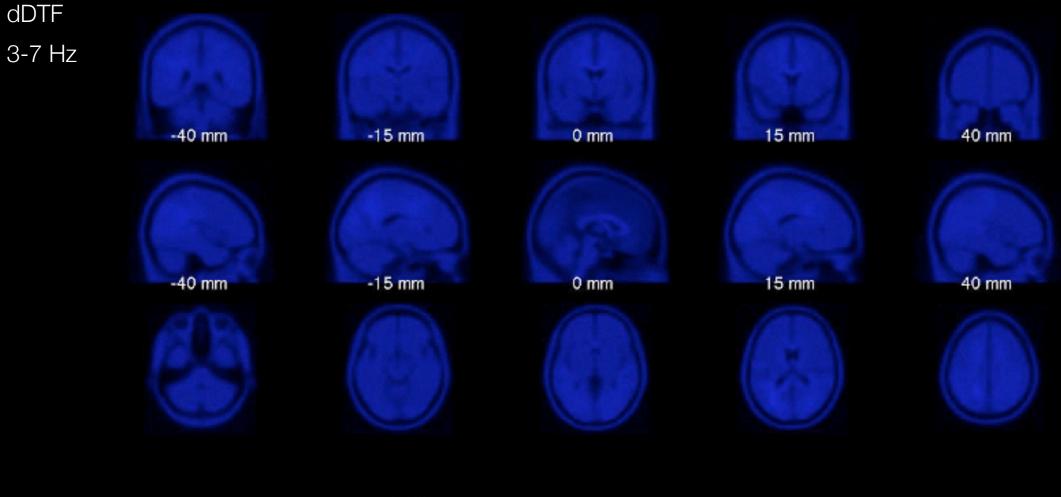
3-7 Hz



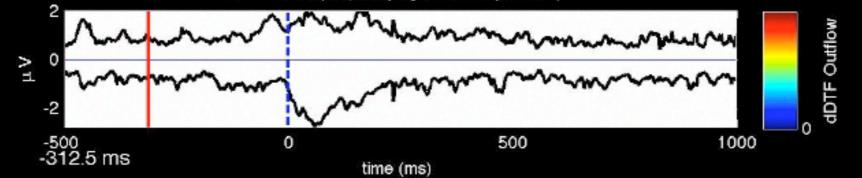


# Causal Density Movie

Error > Correct (p < 0.05, N=24)



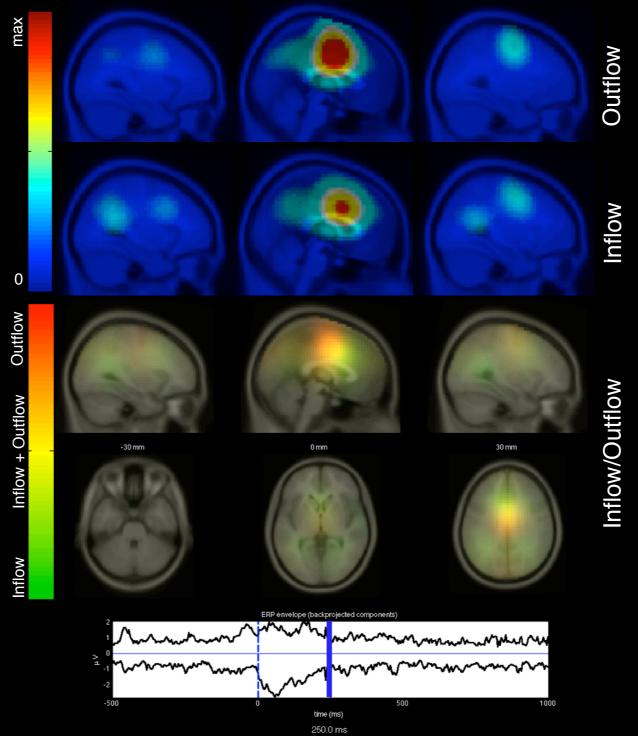
ERP envelope (backprojected components)





# Causal Density Movie

Error > Correct (p < 0.05) 3-7 Hz





# Group Analysis



### Group Analysis

# **Disjoint Clustering**

This approach adopts a 3-stage process: **1.** Identify K ROI's (clusters) by affinity clustering of sources across subject population using EEGLAB's Measure-Product clustering.

 Average all incoming and outgoing statistically significant connections between each pair of ROIs to create a [ K X K [x freq x time ] ] group connectivity matrix.
 Visualize the results using any of SIFTs visualization routines. This method suffers from low statistical power when subjects do not have high agreement in terms of source locations (missing variable problem).



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# **Bayesian Mixture Model**

A more robust approach (in development with Wes Thompson and to be released in SIFT 1.0b) uses smoothing splines and Monte-Carlo methods for joint estimation of posterior probability (with confidence intervals) of cluster centroid location and between-cluster connectivity. This method takes into account the "missing variable" problem inherent to the disjoint clustering approach and provides robust group connectivity statistics.



# Future Work

- Improvement of architecture, GUI, and EEGLAB integration
- Ongoing implementation/incorporation of state-of-the-art methods for effective connectivity analysis and visualization
- Improved group statistics
- Evaluation of relative suitability of various source-separation algorithms when combined with MVAR modeling

