

# Independent Component Analysis of Electrophysiological Data



**Scott Makeig**  
Institute for Neural Computation  
University of California San Diego

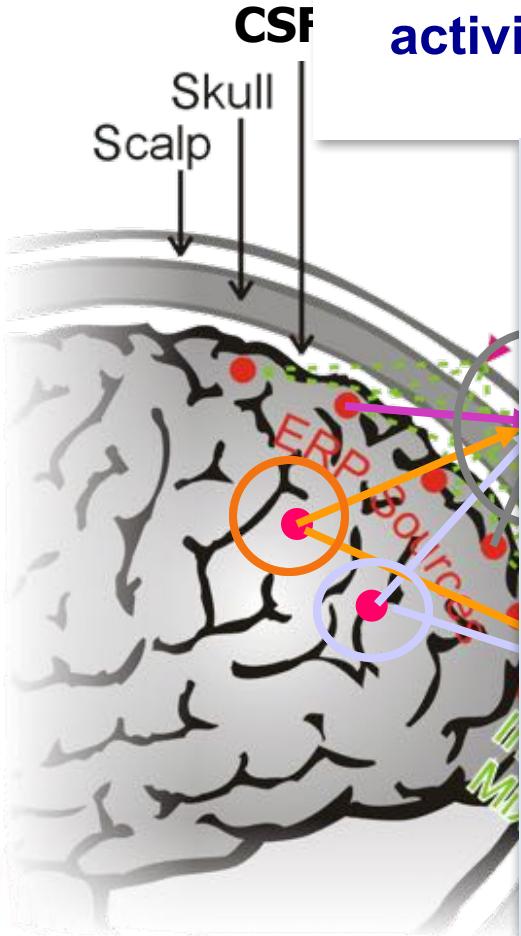
**26th EEGLAB Workshop**  
Be'er Sheva, Israel

October, 2017

# Blind EEG Source Separation by Independent Component Analysis



Tony Bell,  
developer  
of Infomax  
ICA



ICA can find distinct EEG source activities -- and their 'simple' scalp maps!

**Independent Component Analysis of Electroencephalographic Data**

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**Steve Makeig**  
Neuroethics Research Group  
P.O. Box 5122  
San Diego, CA 92106-5122  
[www.eegeeg.com/~makeig/sleep.html](http://www.eegeeg.com/~makeig/sleep.html)

**Woo-Ying Jung**  
Neuroethics Research Group and  
Computer-Based Neuroimaging Lab  
The Salk Institute, P.O. Box 8580  
San Diego, CA 92186-8580  
[jung.eegeeg.org](http://jung.eegeeg.org)

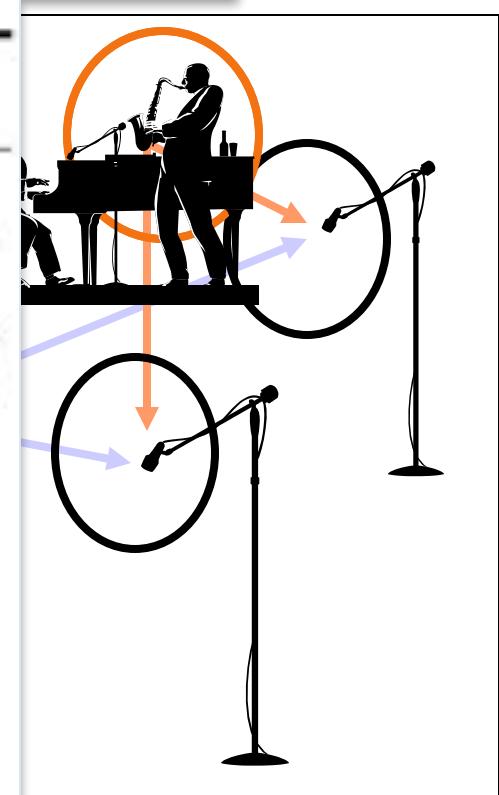
**Anthony J. Bell**  
Computational Neurobiology Lab  
The Salk Institute, P.O. Box 8580  
San Diego, CA 92186-8580  
[bell.eegeeg.org](http://bell.eegeeg.org)

**Sorenson J. Enghoff**  
Neuroethics Medical Institute and  
Computational Neurobiology Lab  
The Salk Institute, P.O. Box 8580  
San Diego, CA 92186-8580  
[enghoff.eegeeg.org](http://enghoff.eegeeg.org)

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**Abstract**

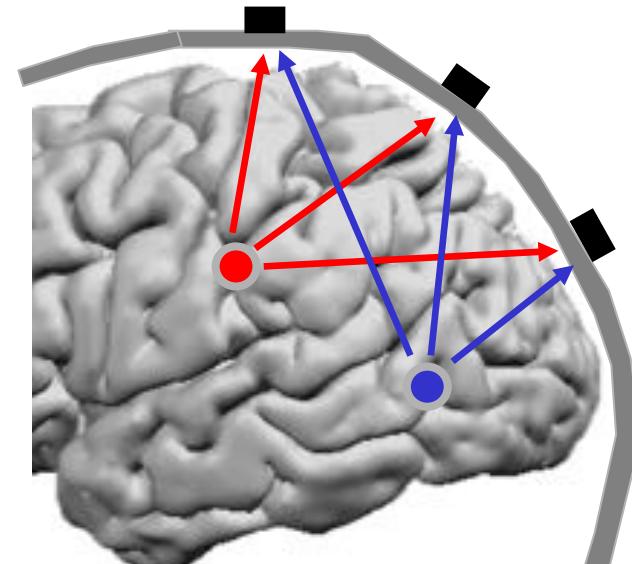
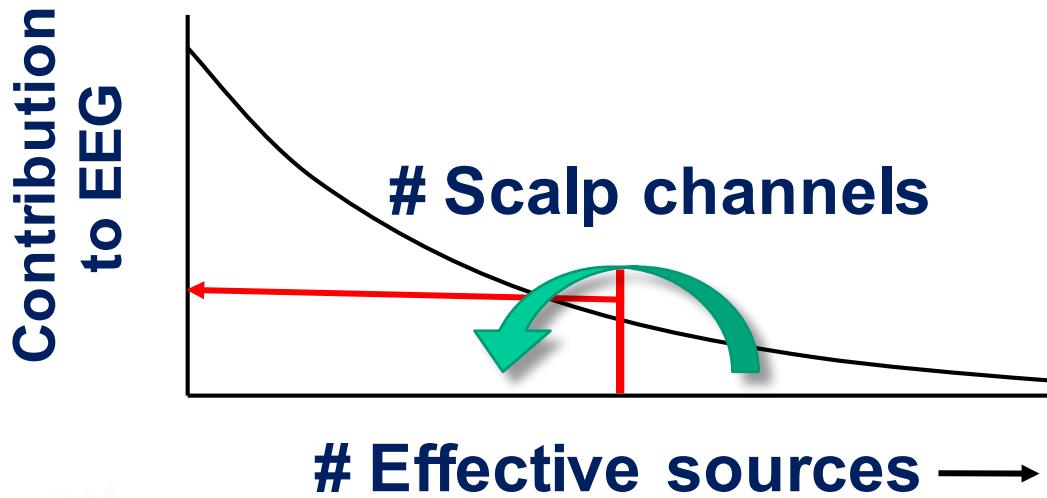
The issue of the distances between the skull and brain and their effects on waveforms, electroencephalographic (EEG) data collected from any point on the human scalp include activity generated within a large brain area. This spatial averaging of EEG data by volume-conduction does not hinder significant time delays, however, suggesting that the Independent Component Analysis (ICA) algorithm of Bell and Sejnowski<sup>1</sup> is favorable for performing blind source separation on EEG data. The ICA algorithm separates the problem of source identification from that of neural localization. This article describes of applying the ICA algorithm to EEG and evoked potential (EP) data collected during a sustained auditory detection task along with ICA matching it to waveform to different stimulus tasks. (2) ICA may be used to segregate various cortical EEG components (auditory and muscle/eye movements) from other averages. (3) ICA is capable of isolating overlapping EP phenomena, including alpha and theta bands and spatially separate EP components, to separate ICA channels. (4) Nonstationarities in EEG and behavioral data can be tracked using ICA via changes in the amount of statistical correlation between ICA-derived component channels.



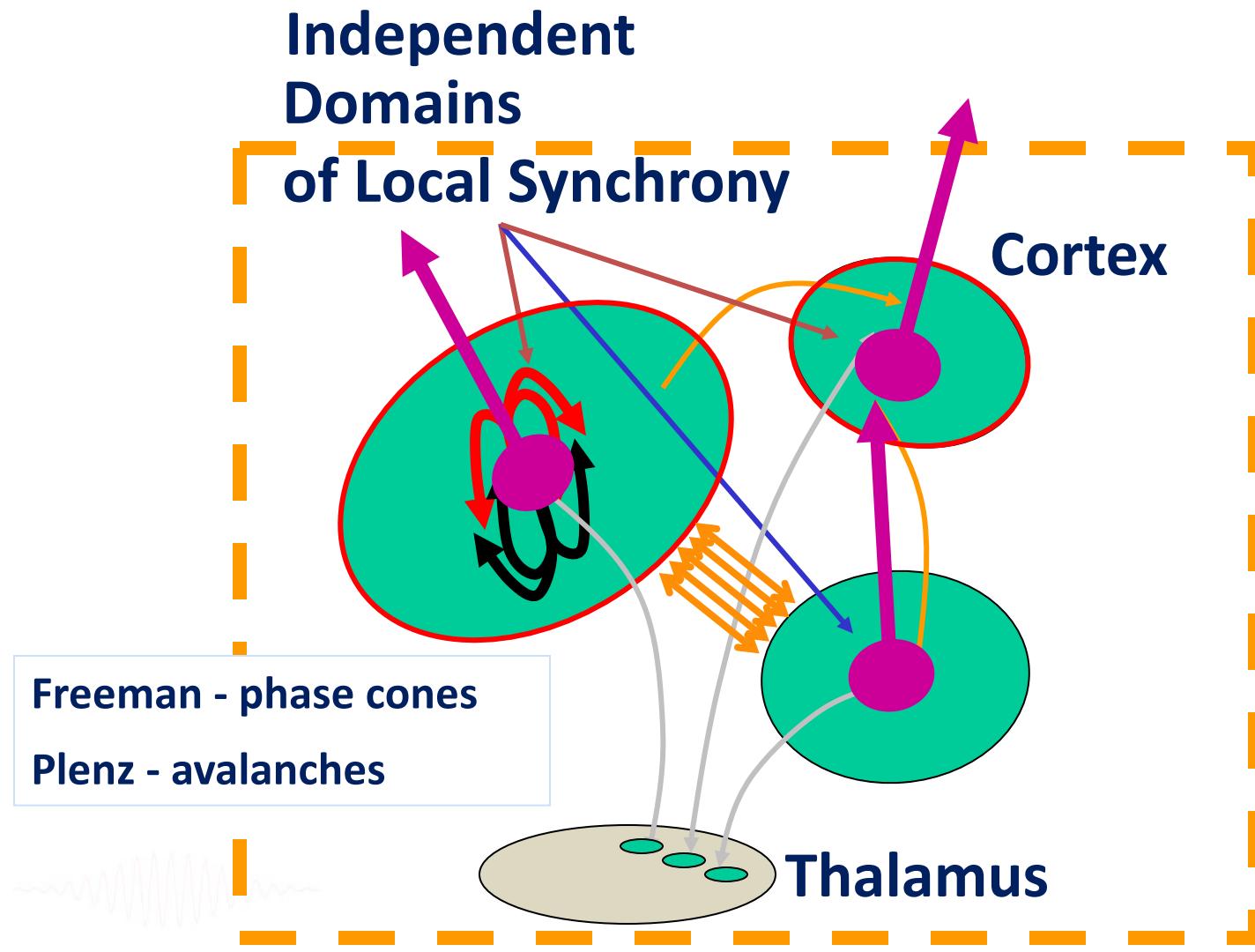
# ICA Assumptions

- Mixing is linear at electrodes
- Propagation delays are negligible
- Component locations are fixed
- Component time courses are independent
- # components  $\leq$  # scalp channels

✓ ✓ ? ? ?



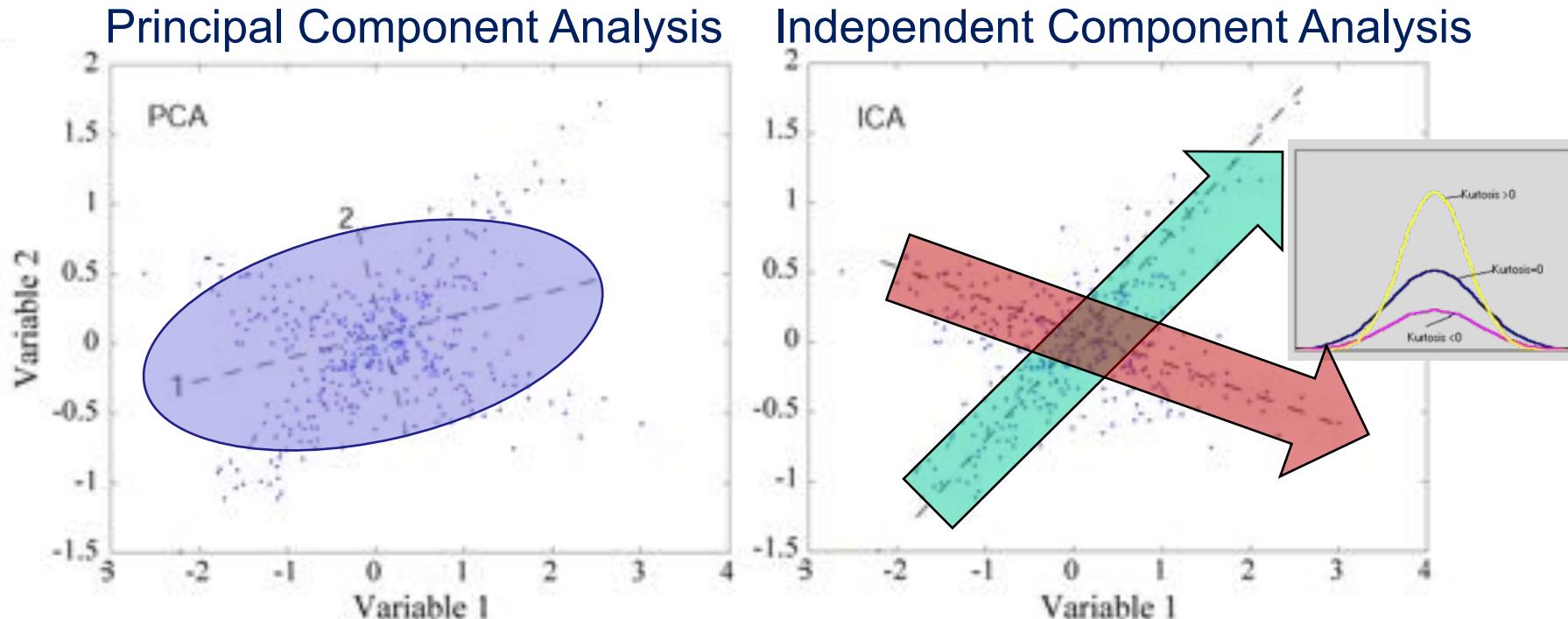
# Are EEG effective source signals independent?



# Properties of EEG Independent Components



# ICA vs. PCA



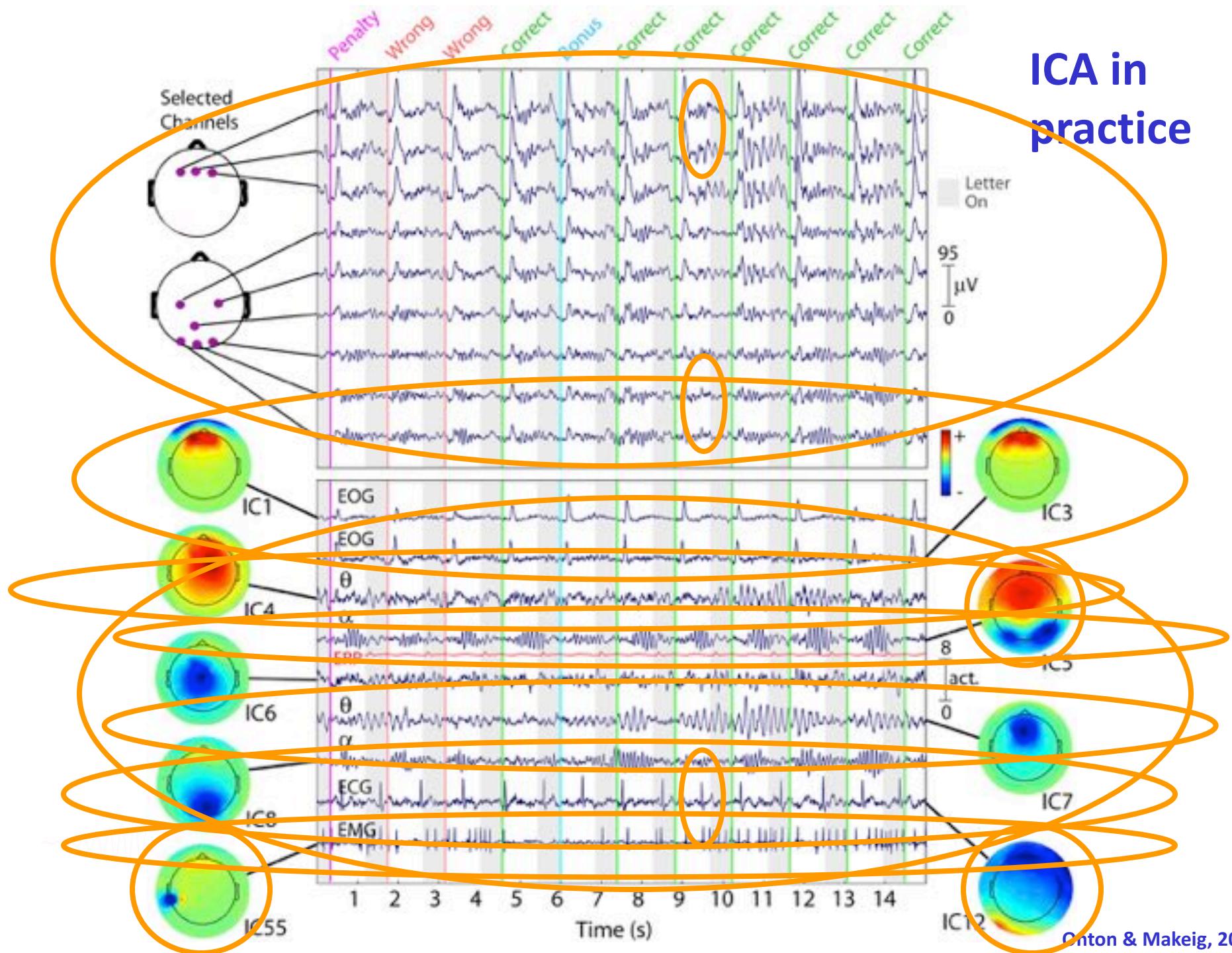
PCA simply decorrelates the outputs using an **orthogonal mixing matrix**.

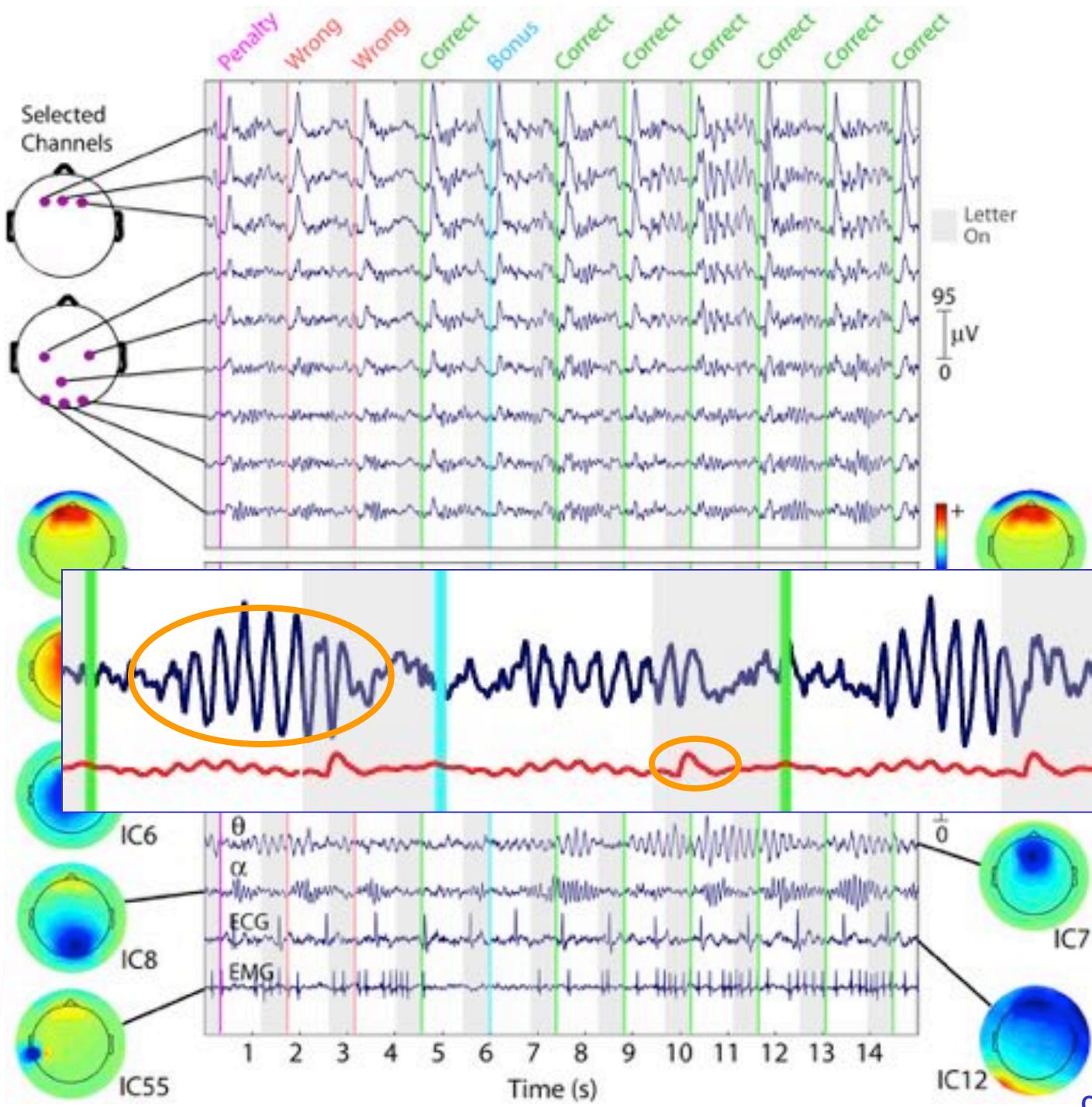
PCA makes each successive component account for as much **variance** in the data as possible.

ICA makes each component account for as much **temporally independent information** in the data as possible, with no constraints on the mixing matrix.

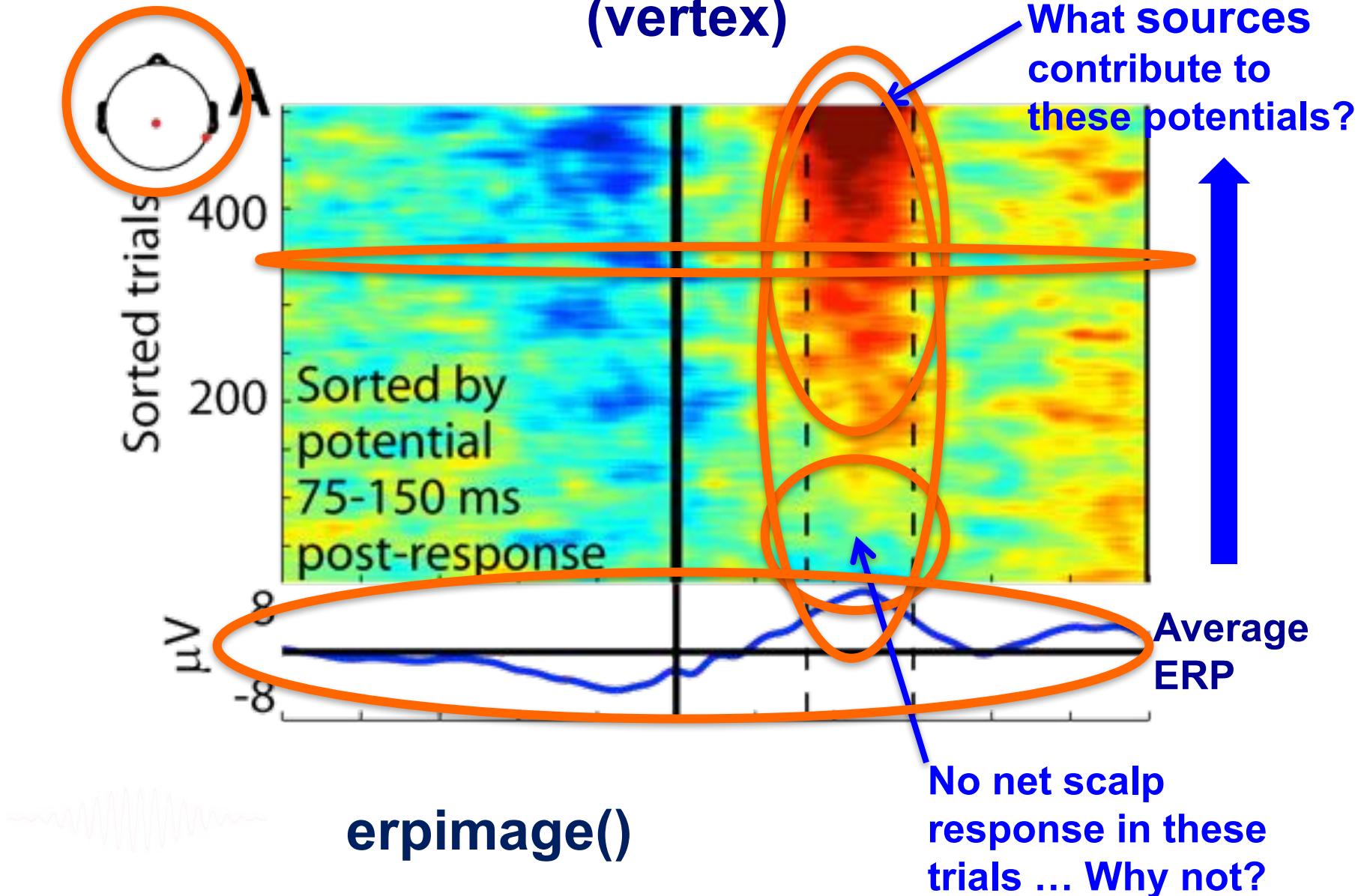
***PCA lumps – ICA splits!***

# ICA in practice

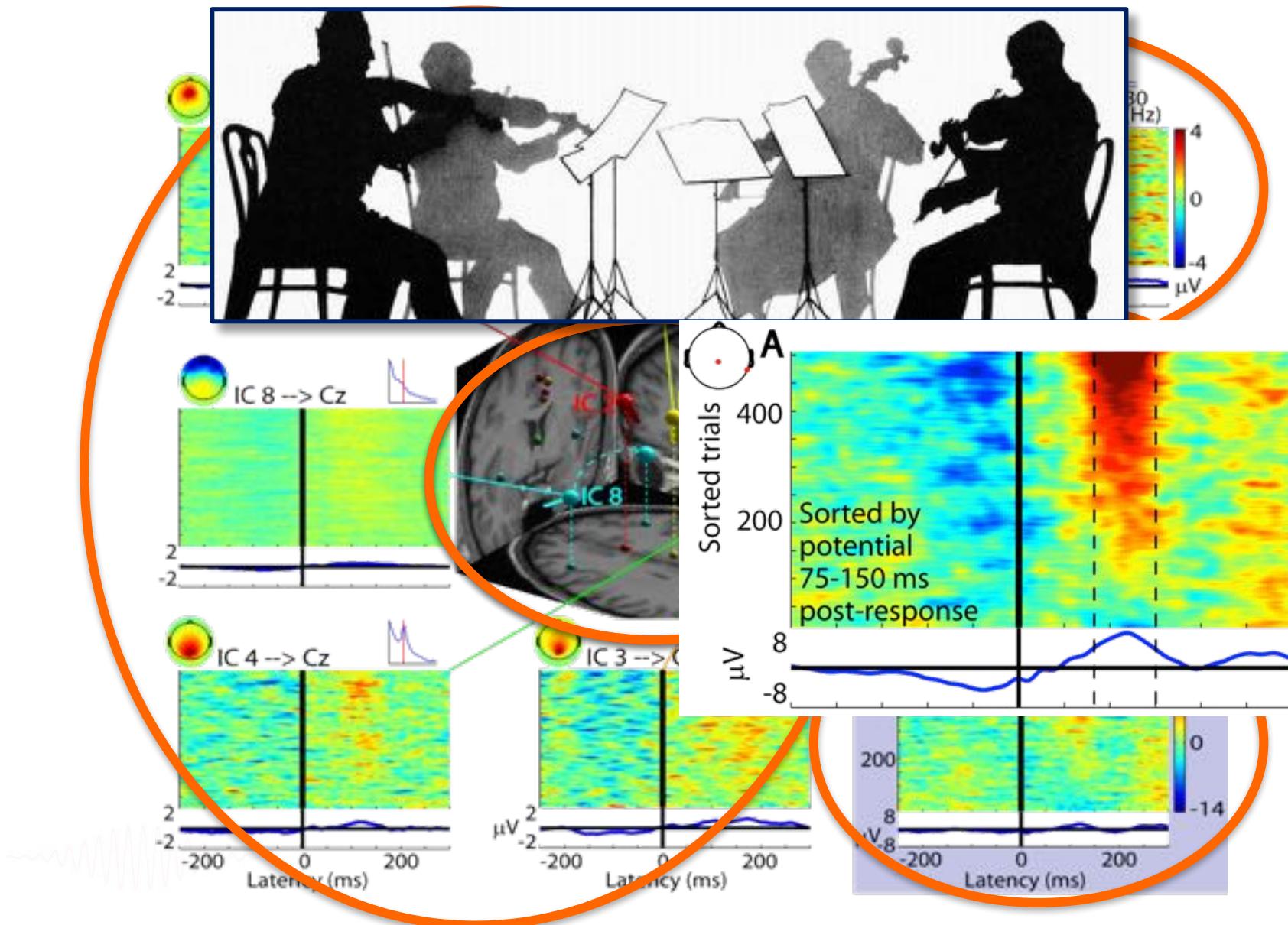


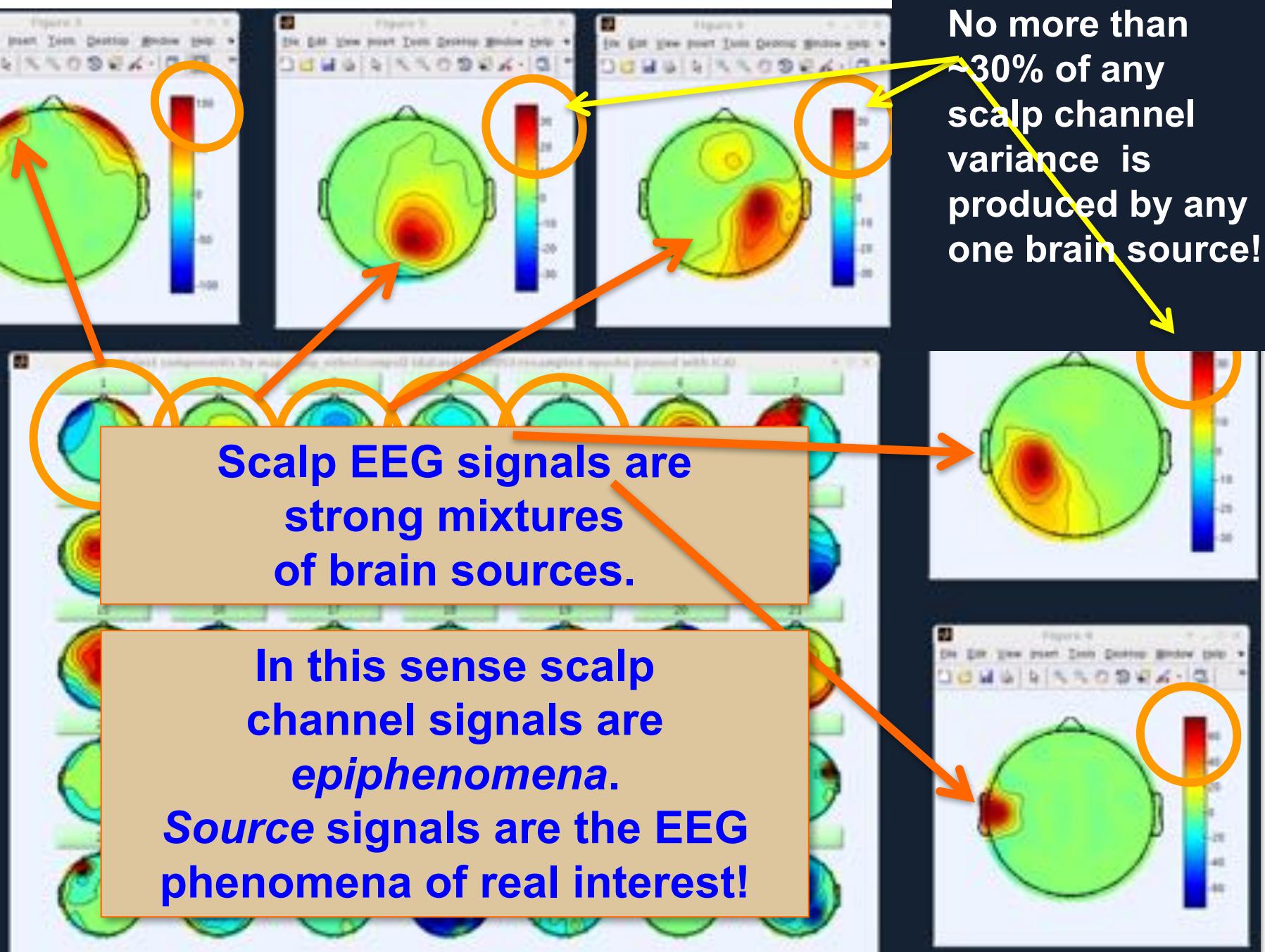


# A P300' visual target response at electrode Cz (vertex)

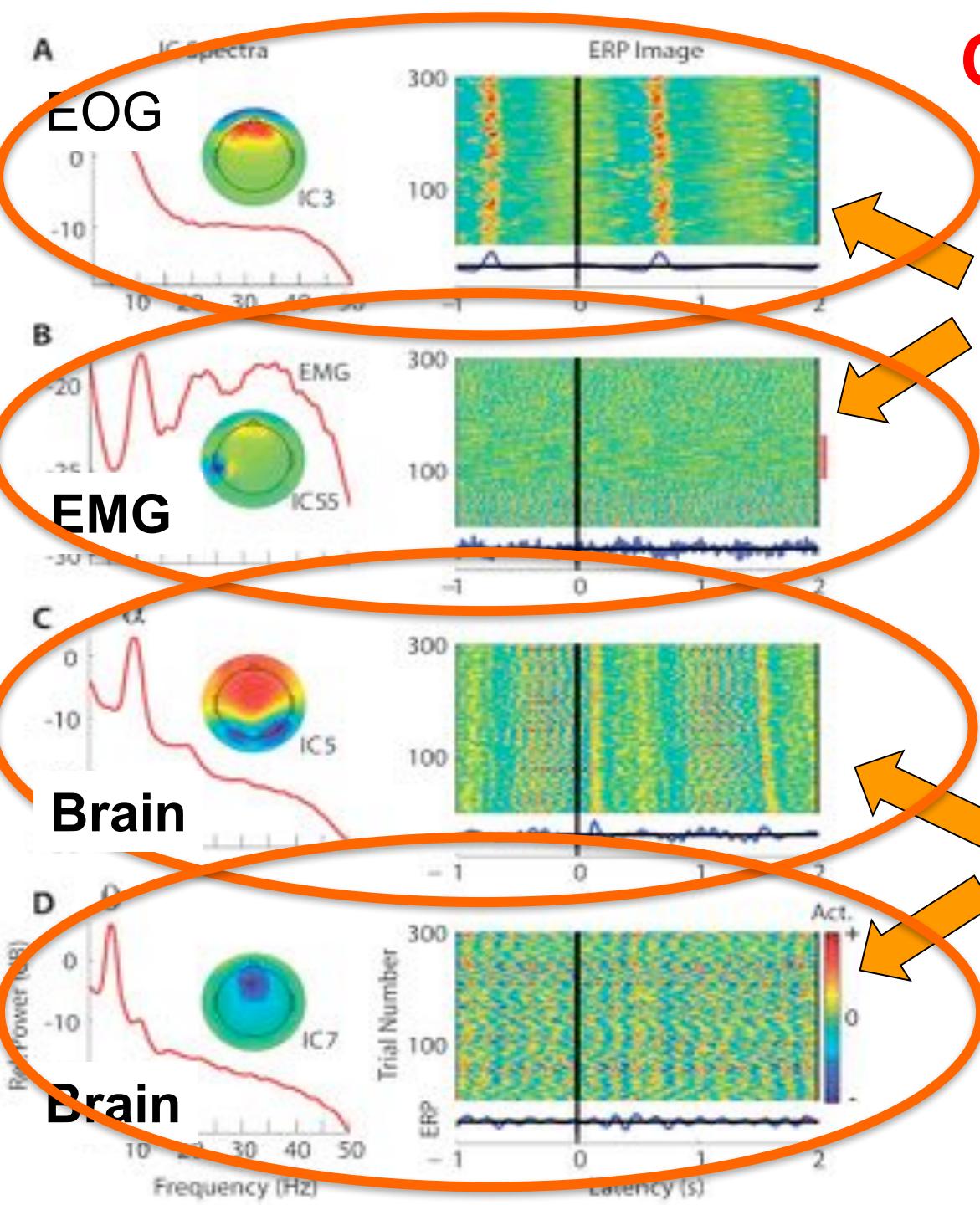


# The response (at Cz) sums 238 independent sources

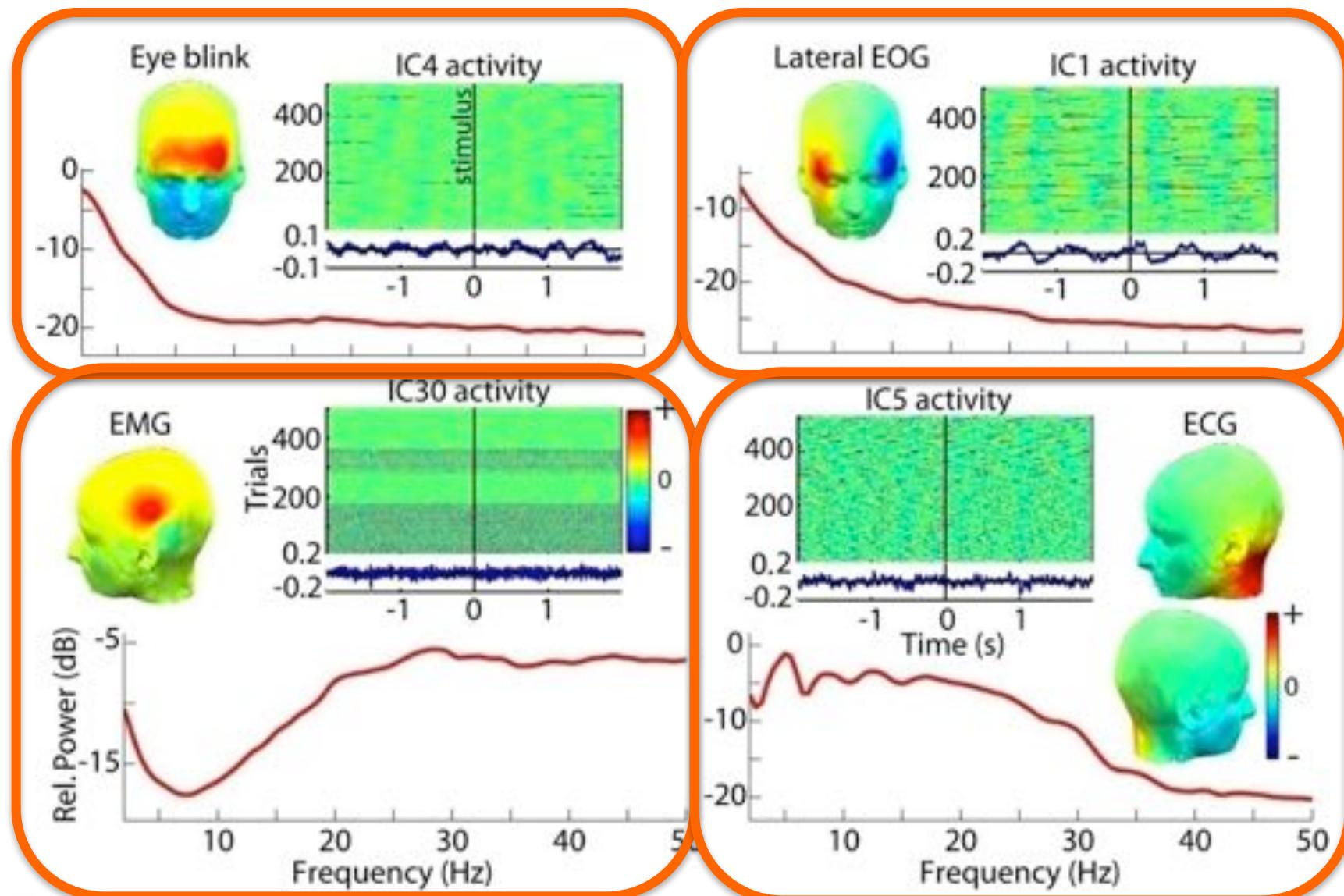




# Classifying ICs

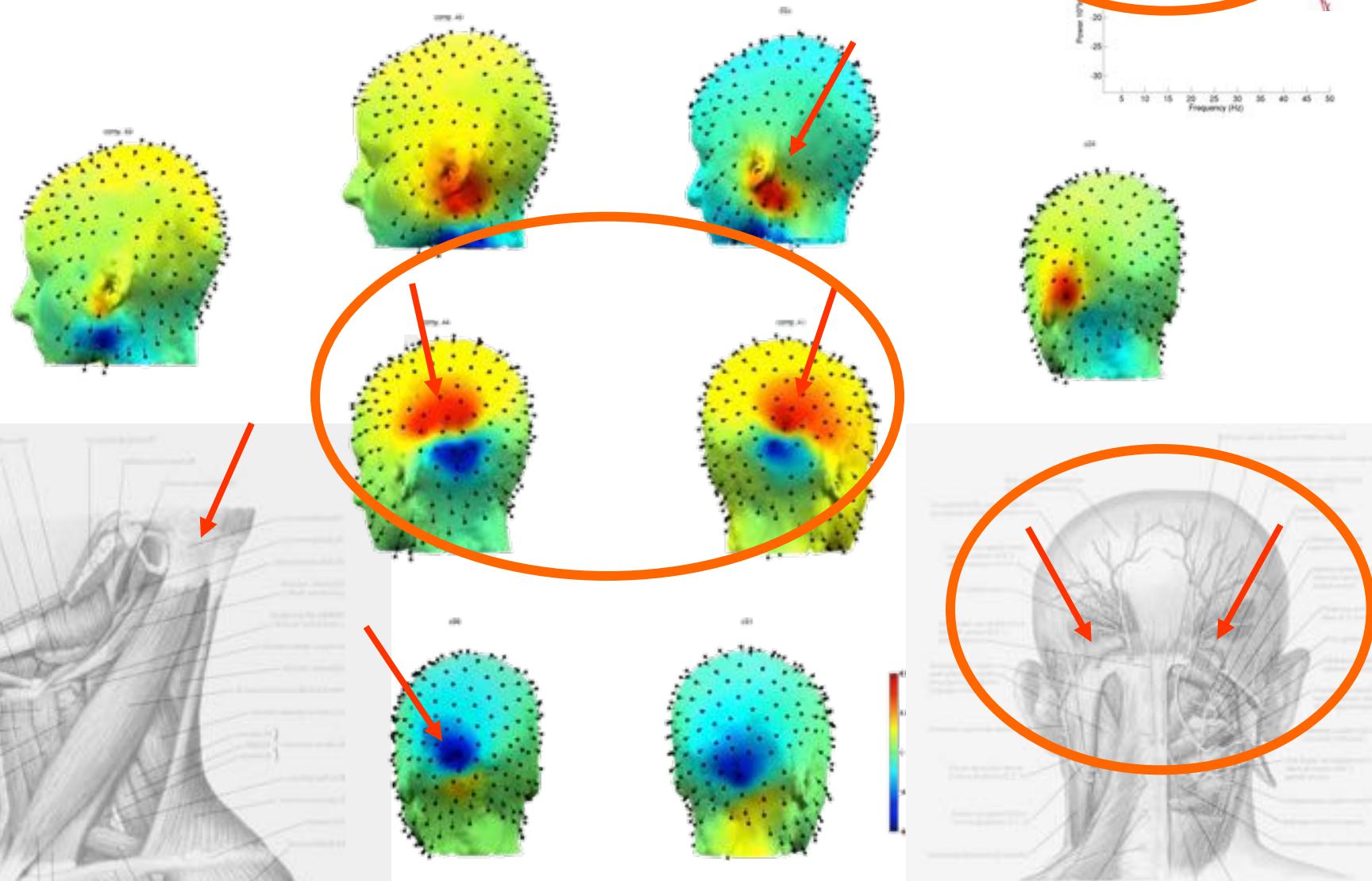


# ICA finds Non-Brain Independent Component (IC) Processes ...

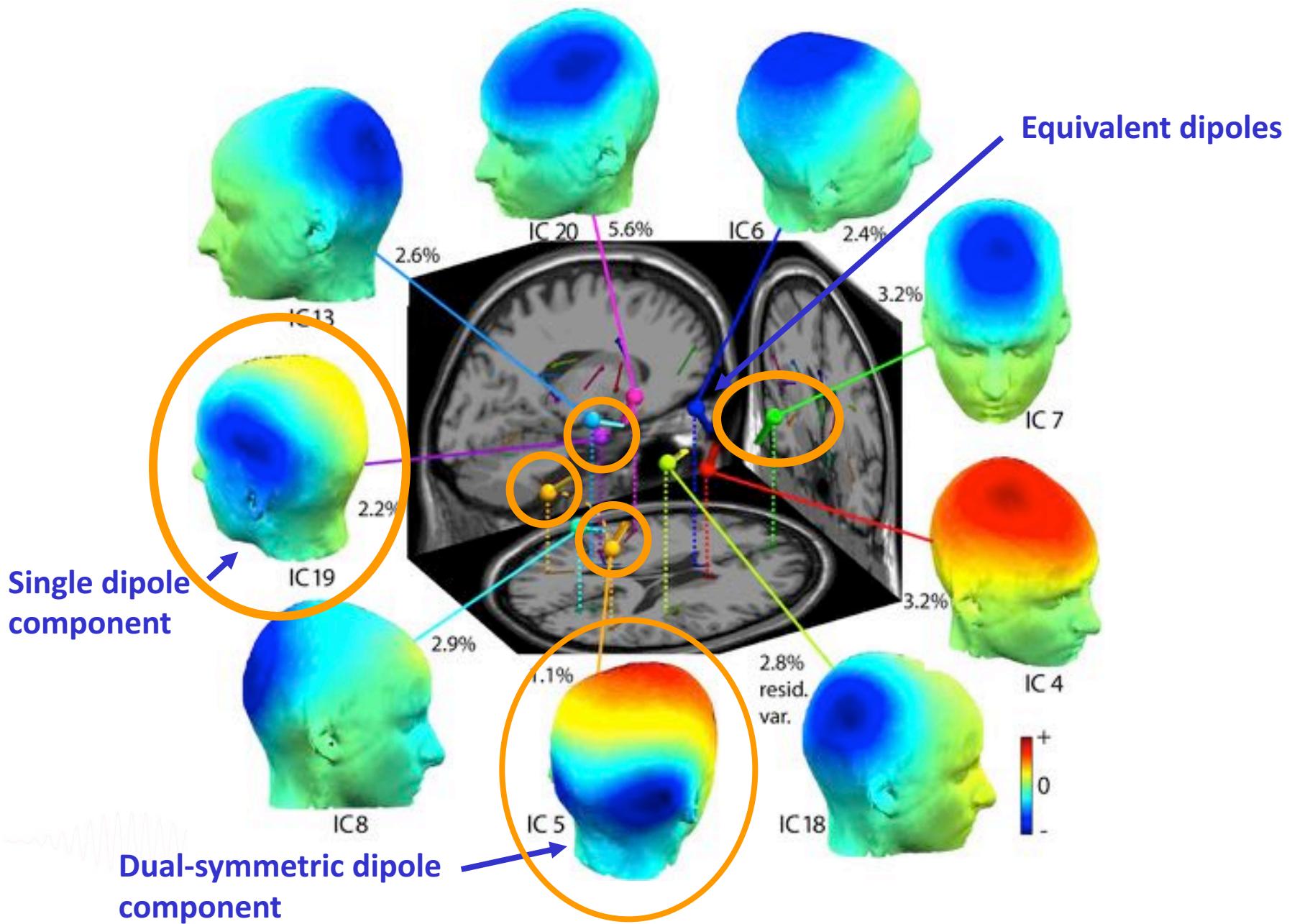


... separates them from the remainder of the data ...

# Independent muscle signals



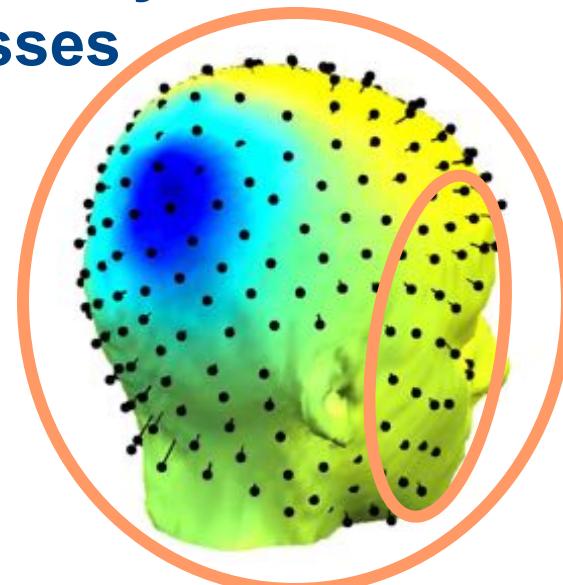
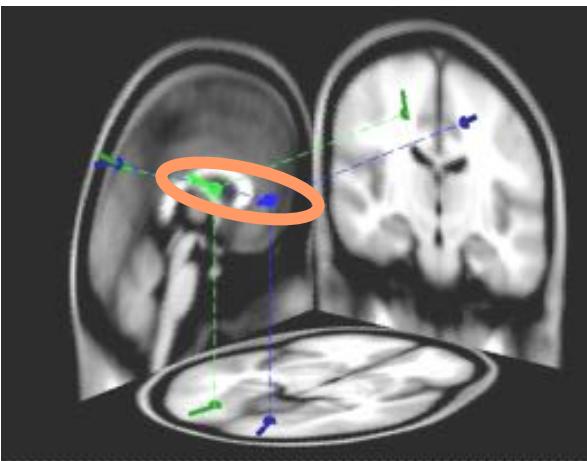
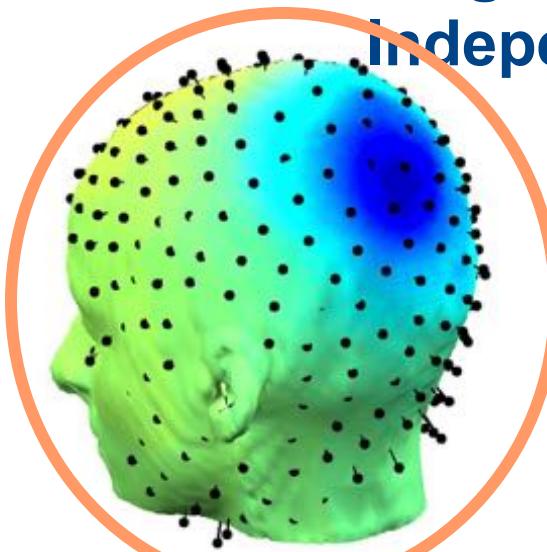
... and also separates cortical brain IC processes



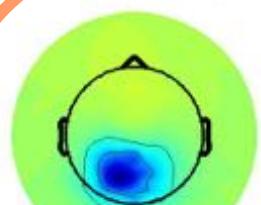
IC9

IC11

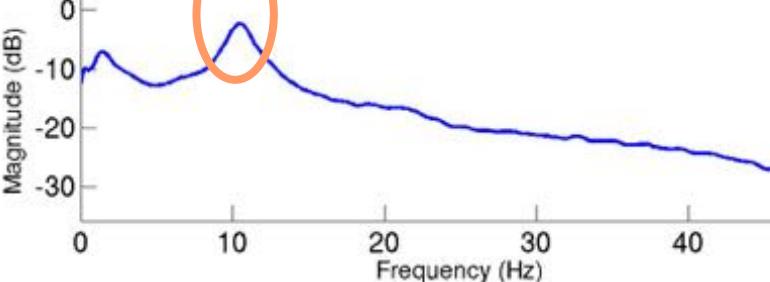
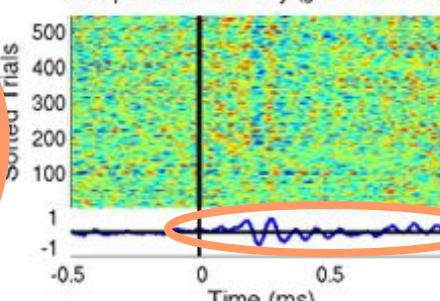
# Single Session - Two Maximally Independent Alpha Processes



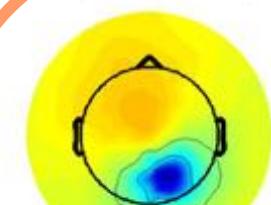
Component 9 map



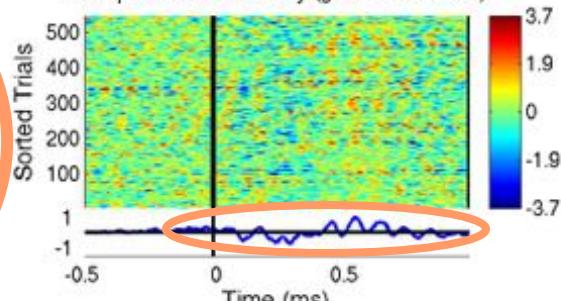
Component 9 activity (global offset 0.02)



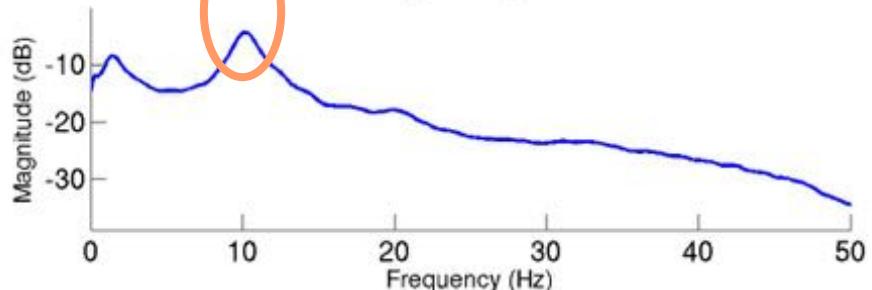
Component 11 map



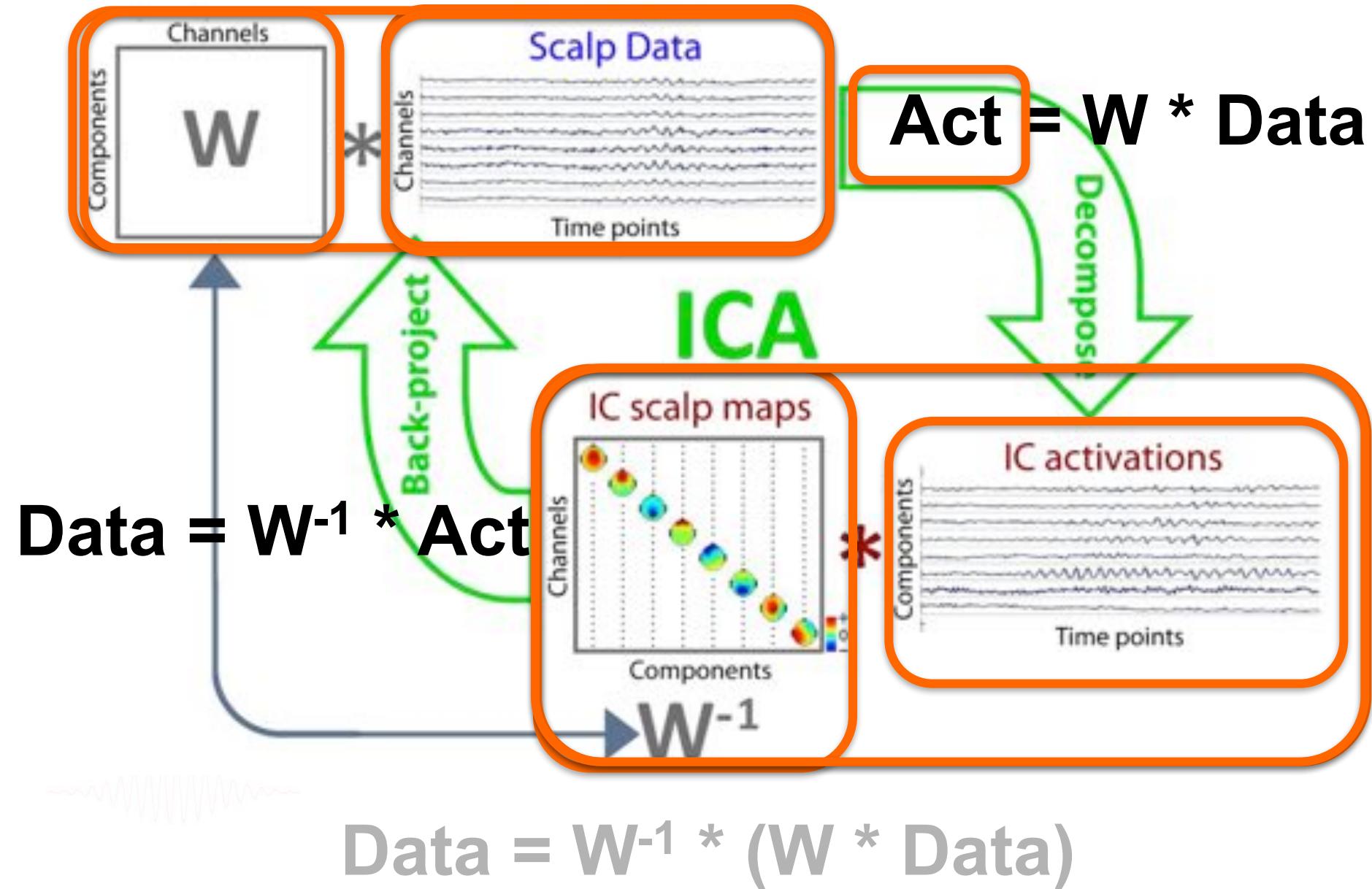
Component 11 activity (global offset -0.038)



Activity power spectrum



# ICA is a linear data decomposition method



# Infomax ICA learning approach

How to make the outputs statistical independent?

Minimize their redundancy or mutual information.

Consider the joint entropy of two components,

$$H(y_1, y_2) = H(y_1) + H(y_2) - I(y_1, y_2).$$

**Maximizing**  $H(y_1, y_2)$   $\Rightarrow$  **minimizing**  $I(y_1, y_2).$

The learning rule:

$$\Delta \mathbf{w} \leftarrow \frac{\partial H(\mathbf{y})}{\partial \mathbf{w}} \underbrace{\mathbf{w}^T \mathbf{w}}$$

Natural gradient  
normalization  
(Amari)

Is 0 if the two variables  
are independent

# Historical Remarks

- Herault & Jutten ("Space or time adaptive signal processing by neural network models", *Neural Nets for Computing Meeting*, Snowbird, Utah, 1986): **Seminal paper**
- Bell & Sejnowski (1995): Information maximization (**Infomax**)
- Makeig, Bell, Jung, Sejnowski (1996); ICA decomposition of EEG
- Amari et al. (1996): Natural gradient learning
- Cardoso (1996): Joint approximate diagonalization (JADE)
- Hyvarinen (1999): (fastICA)
- Lee/Girolami (1999): Mixture model ICA (**Extended Infomax**)
- Palmer (2006): Adaptive mixture ICA (**AMICA**)

## Applications of ICA to biomedical signals

- EEG/ERP analysis (Makeig, Bell, Jung & Sejnowski, **NIPS 1996**)
- fMRI analysis (McKeown et al., 1998)
- Fetal/mother ECG separation (Cardoso, 1998)
- Electrocorticography (ECoG) (Whitmer, 2010)

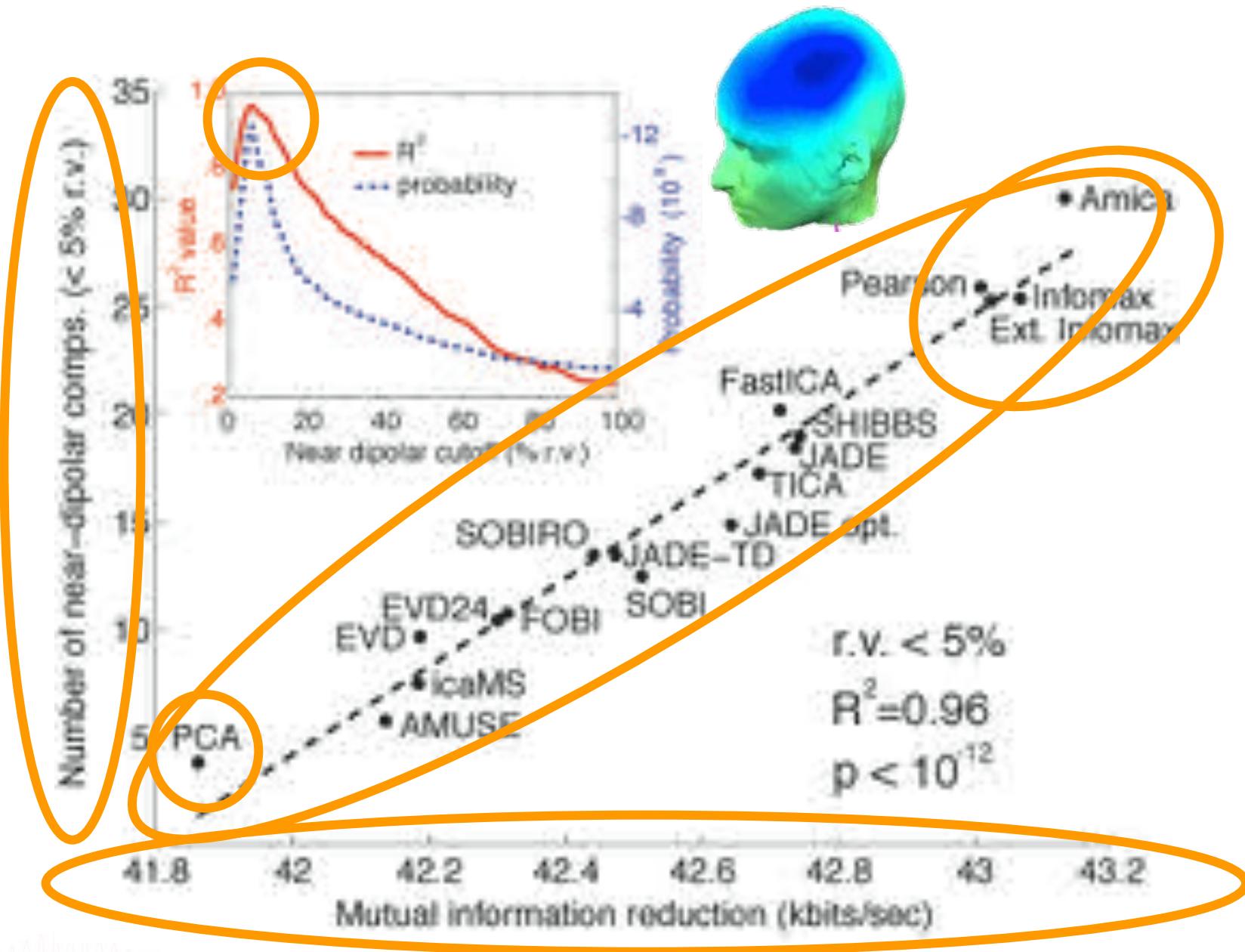
# Important Recent Result (2012)

Those linear decompositions of multi-channel EEG data that find ICs whose time courses are more temporally independent ...

Also find more ICs whose scalp maps are highly ‘dipolar’ – i.e., ICs compatible with the spatial projection of a single local cortical (or non-brain, artifactual) source process – whose location can be accurately estimated.

More independent time courses  $\leftrightarrow$  Larger number of dipolar ICs

Hypothesis: Dipolar ICs = Localized cortical source processes



**Delorme et al., PLOS One,**  
**2012**

S. Makeig, 2011

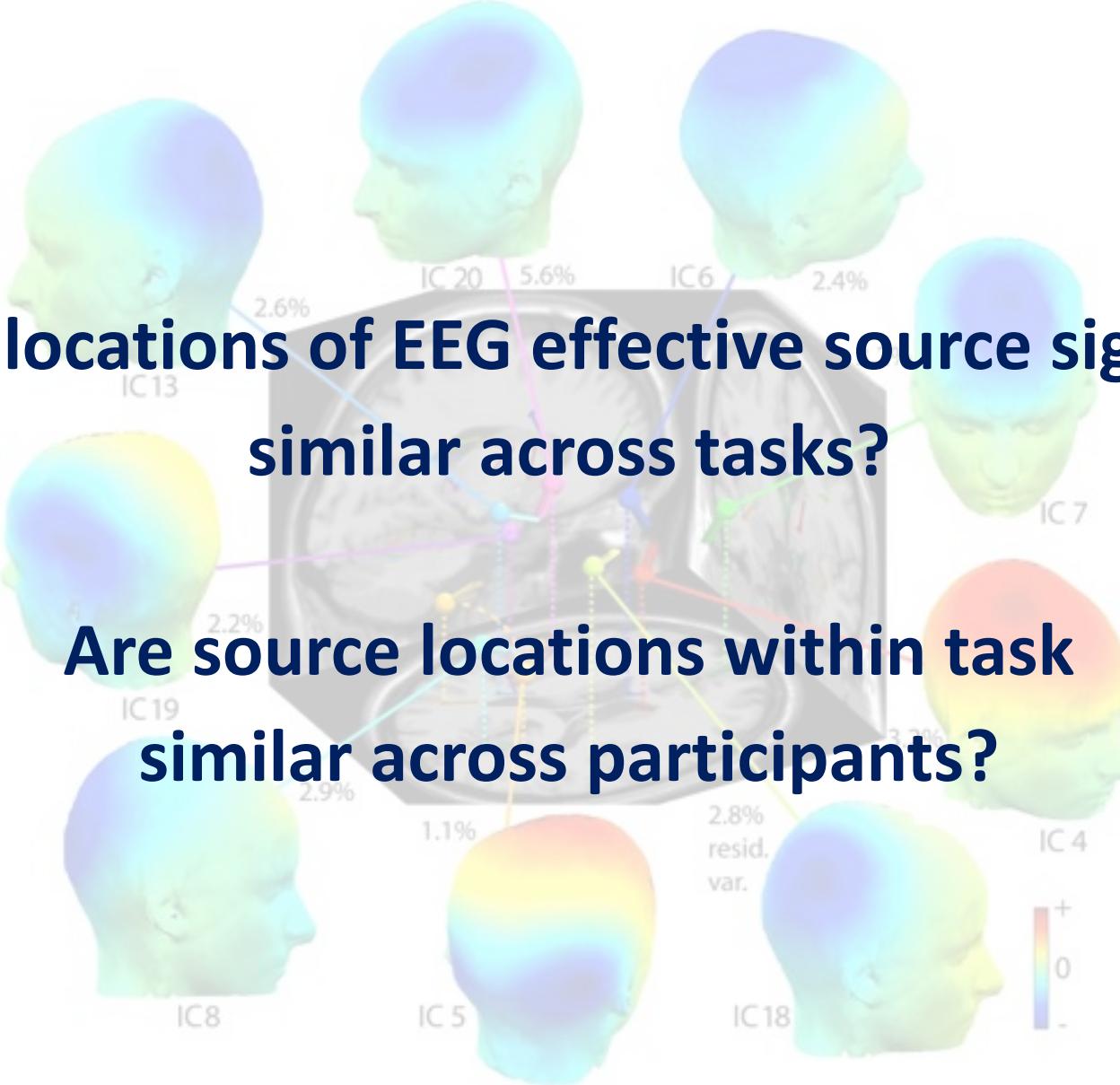
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More independent time courses  $\leftrightarrow$  Larger number of dipolar ICs

Dipolar ICs = Localized cortical source processes

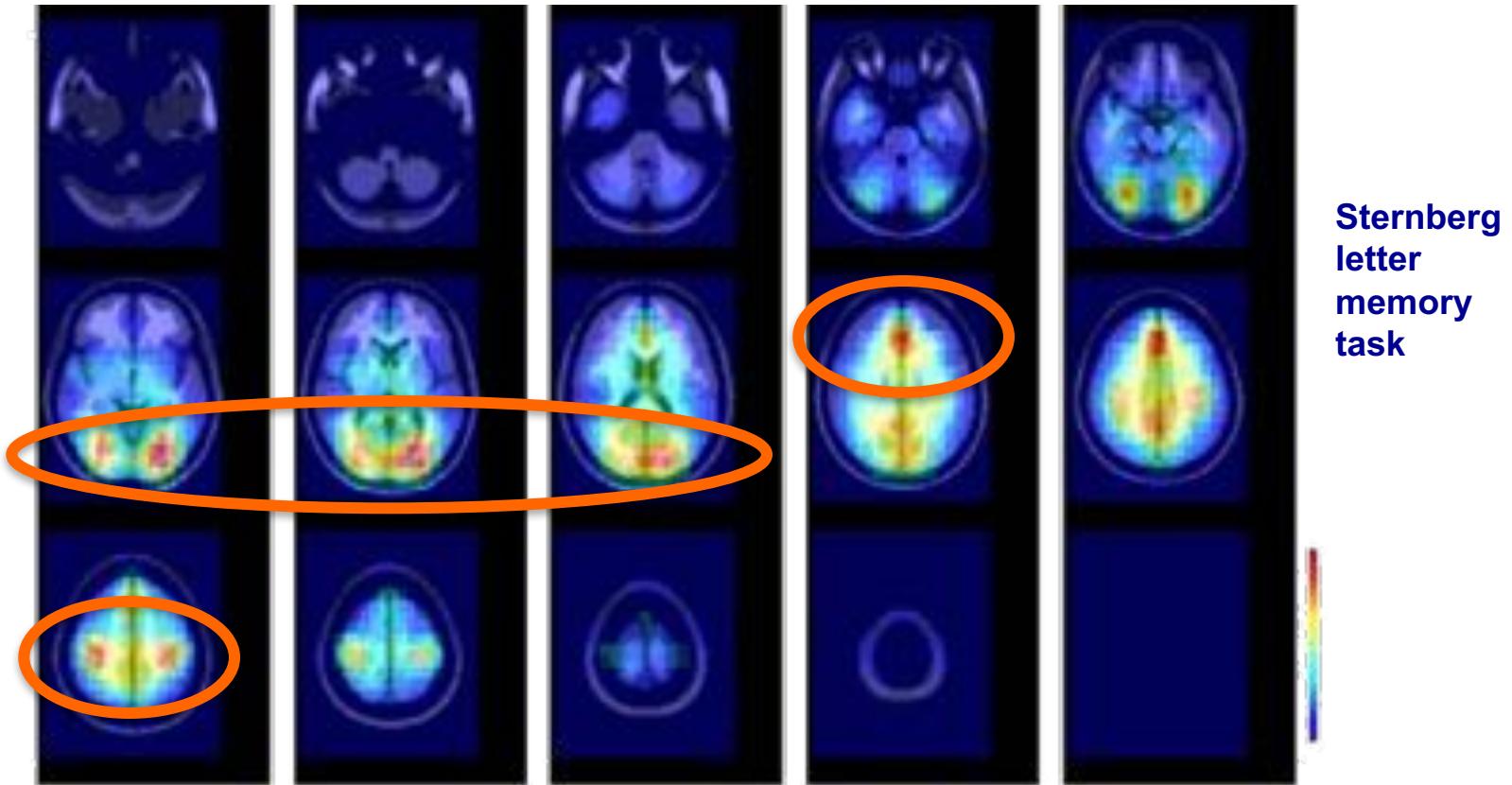


**Are locations of EEG effective source signals  
similar across tasks?**

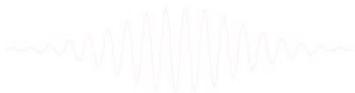
**Are source locations within task  
similar across participants?**

# Effective Source Density

## Visual Working Memory

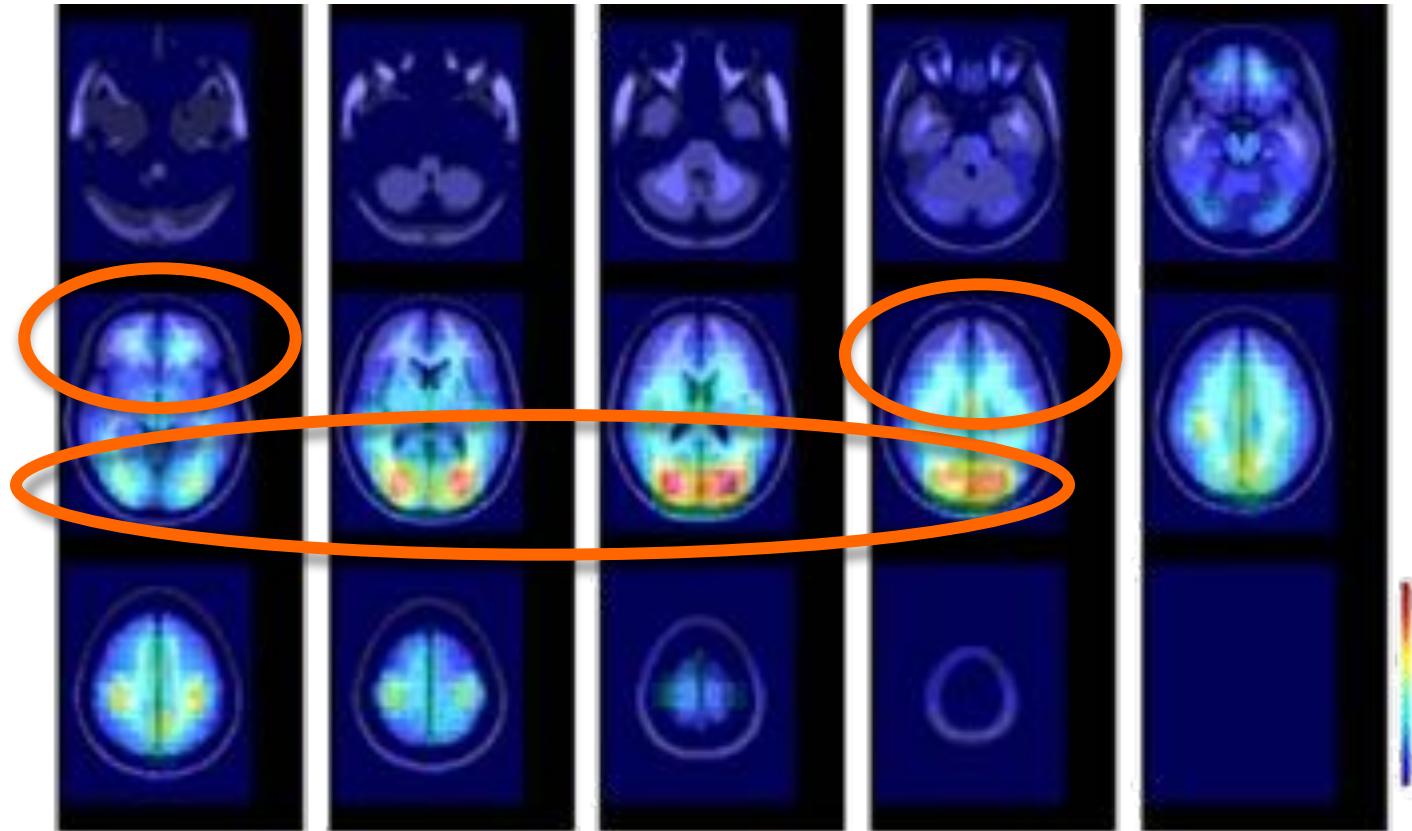


dipoledensity()

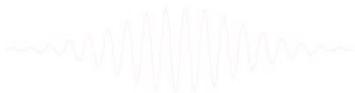


# Effective Source Density

## Eyes-closed emotion imagination

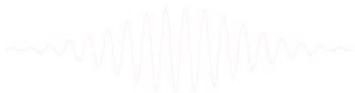
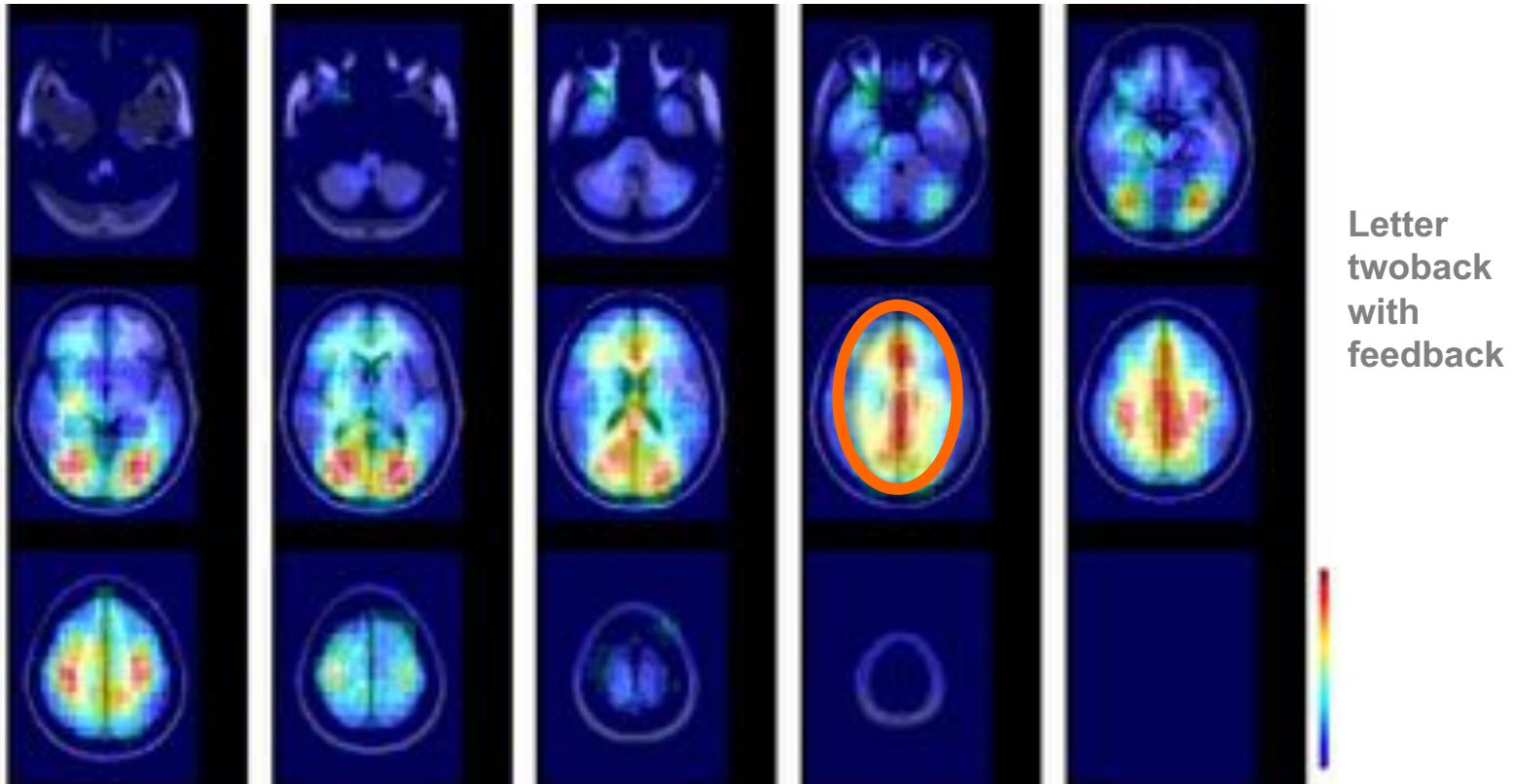


>> dipoledensity()



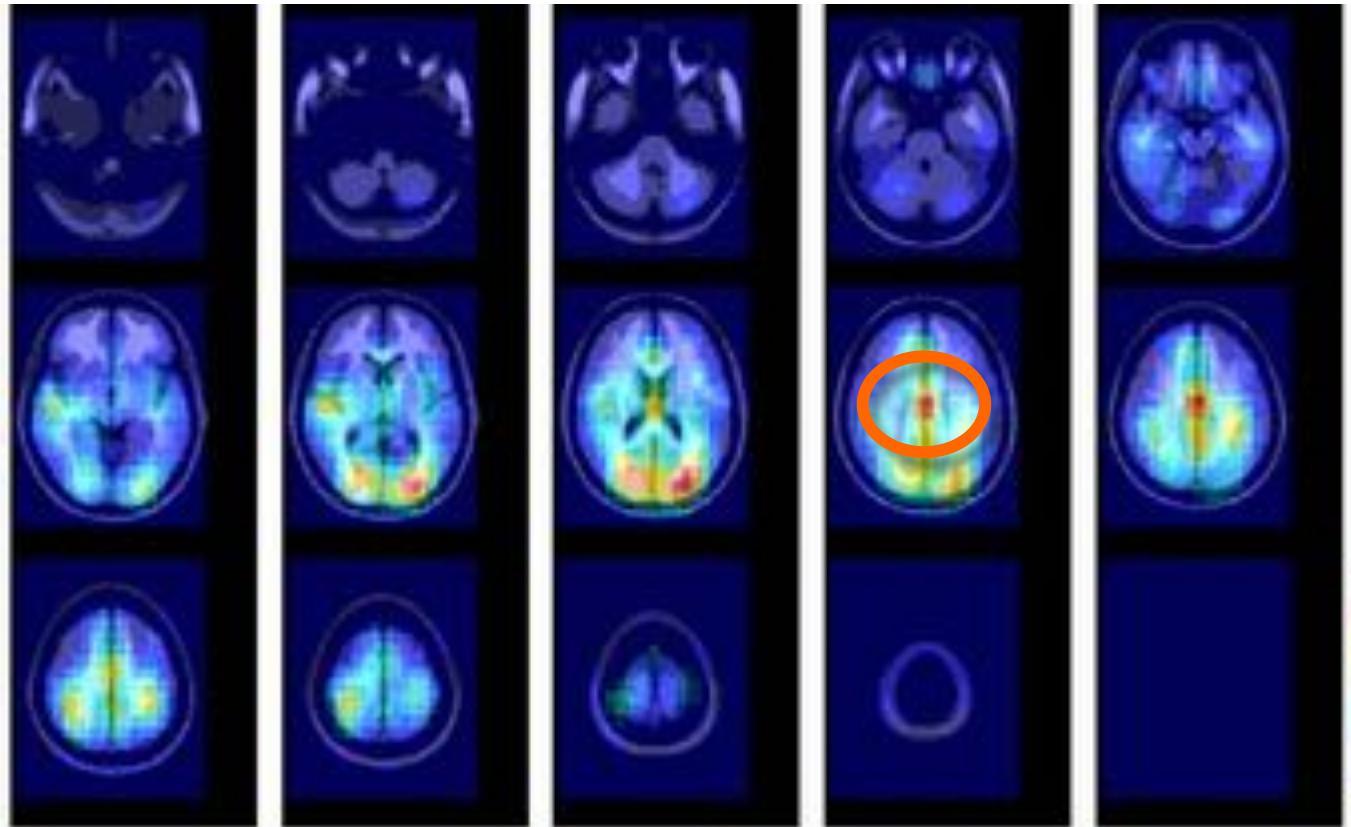
# Effective Source Density

## Letter twoback with feedback



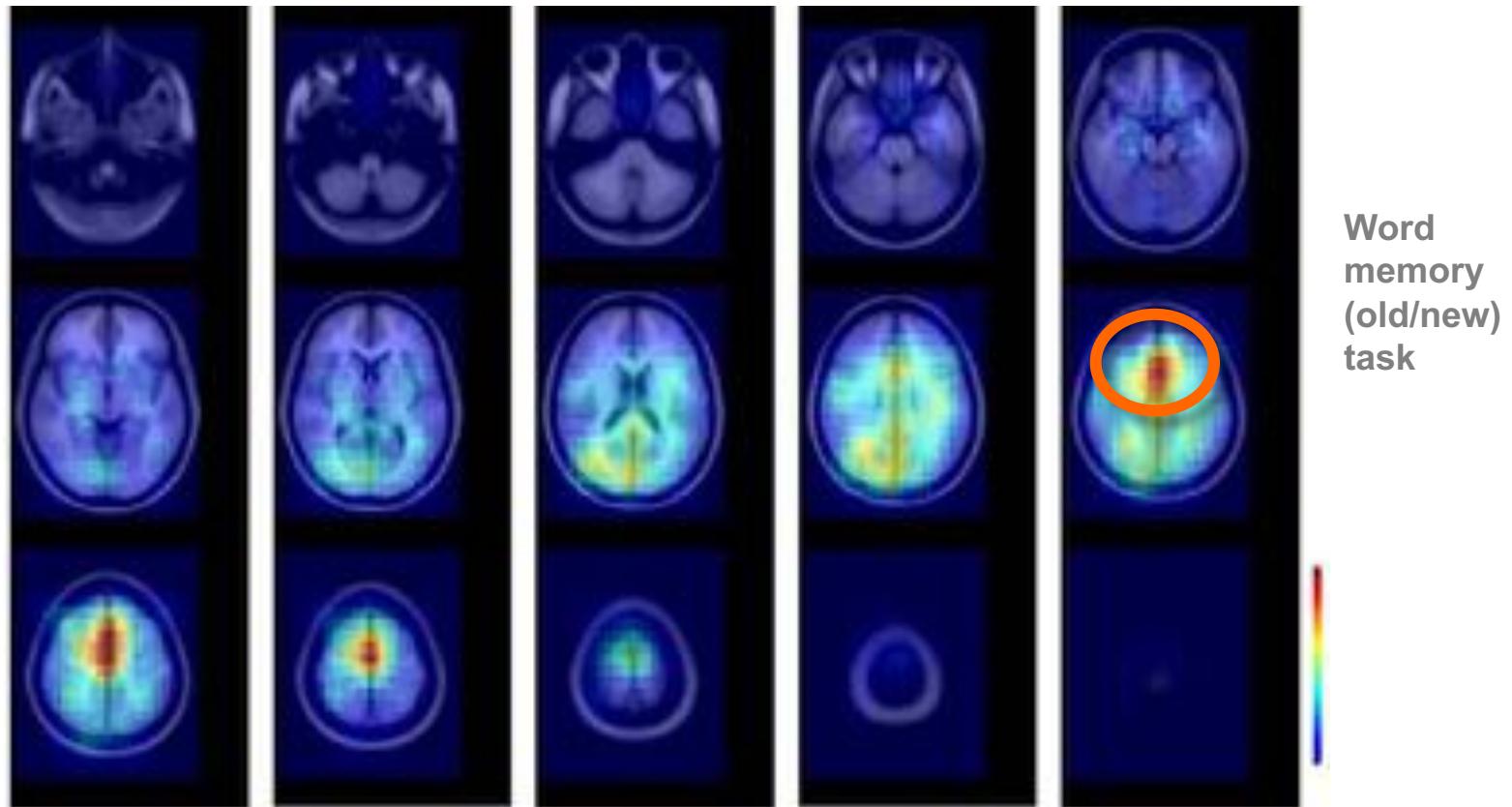
# Effective Source Density

## Auditory novelty oddball



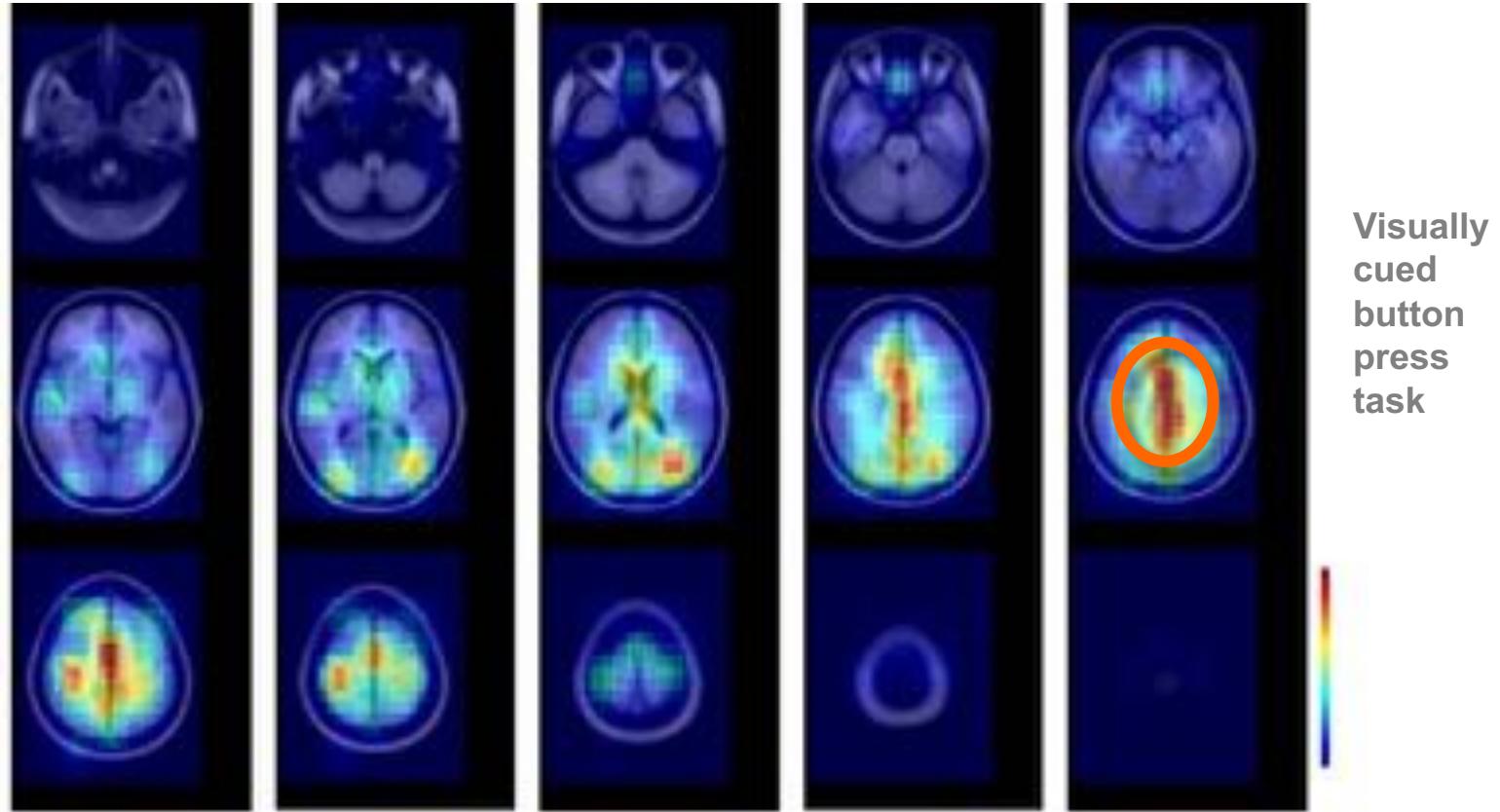
# Effective Source Density

## A. Old/new word memory



# Effective Source Density

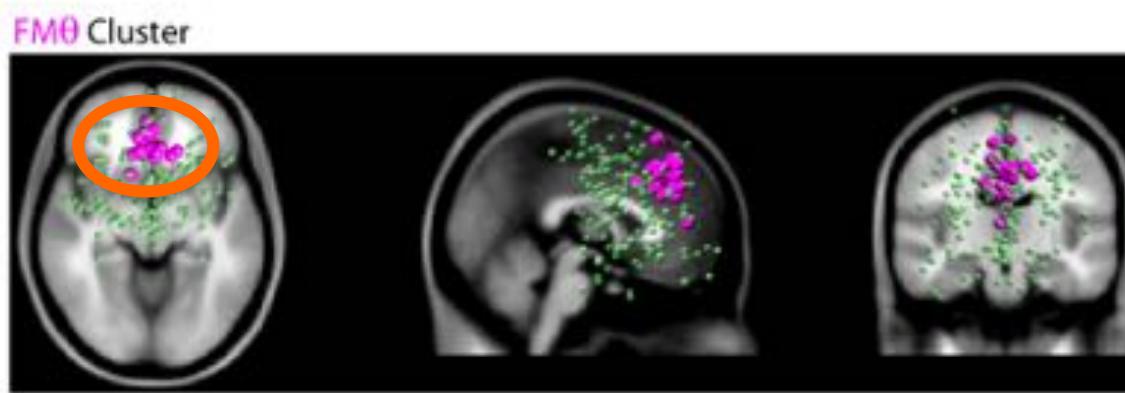
## B. Visually cued selective response



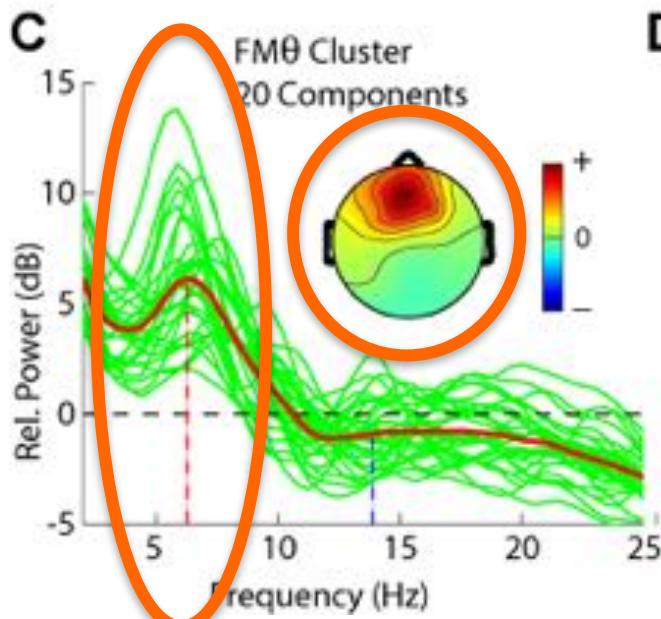
**Are source dynamics  
similar across participants?**

# Example: frontal midline theta cluster

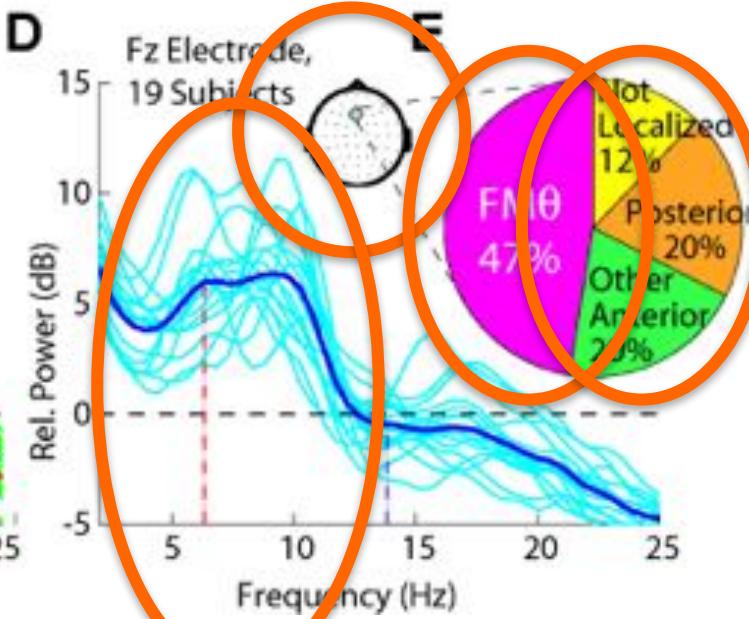
B



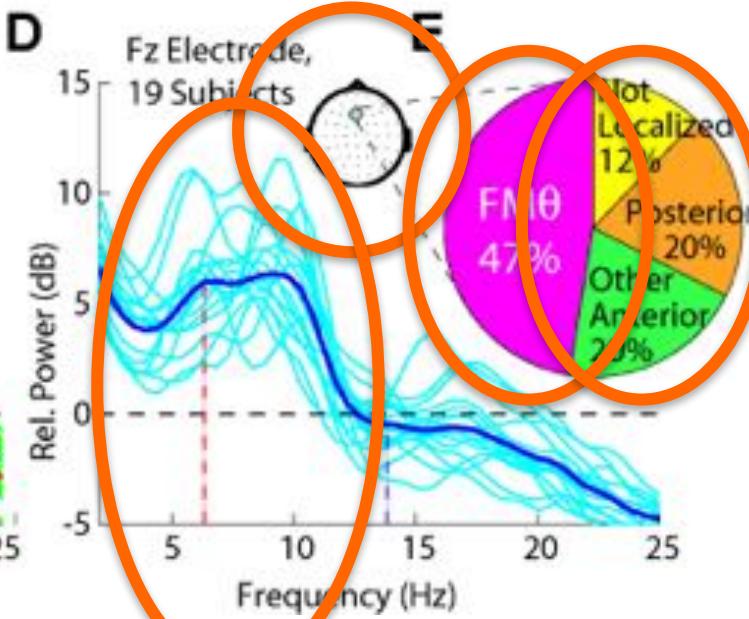
C



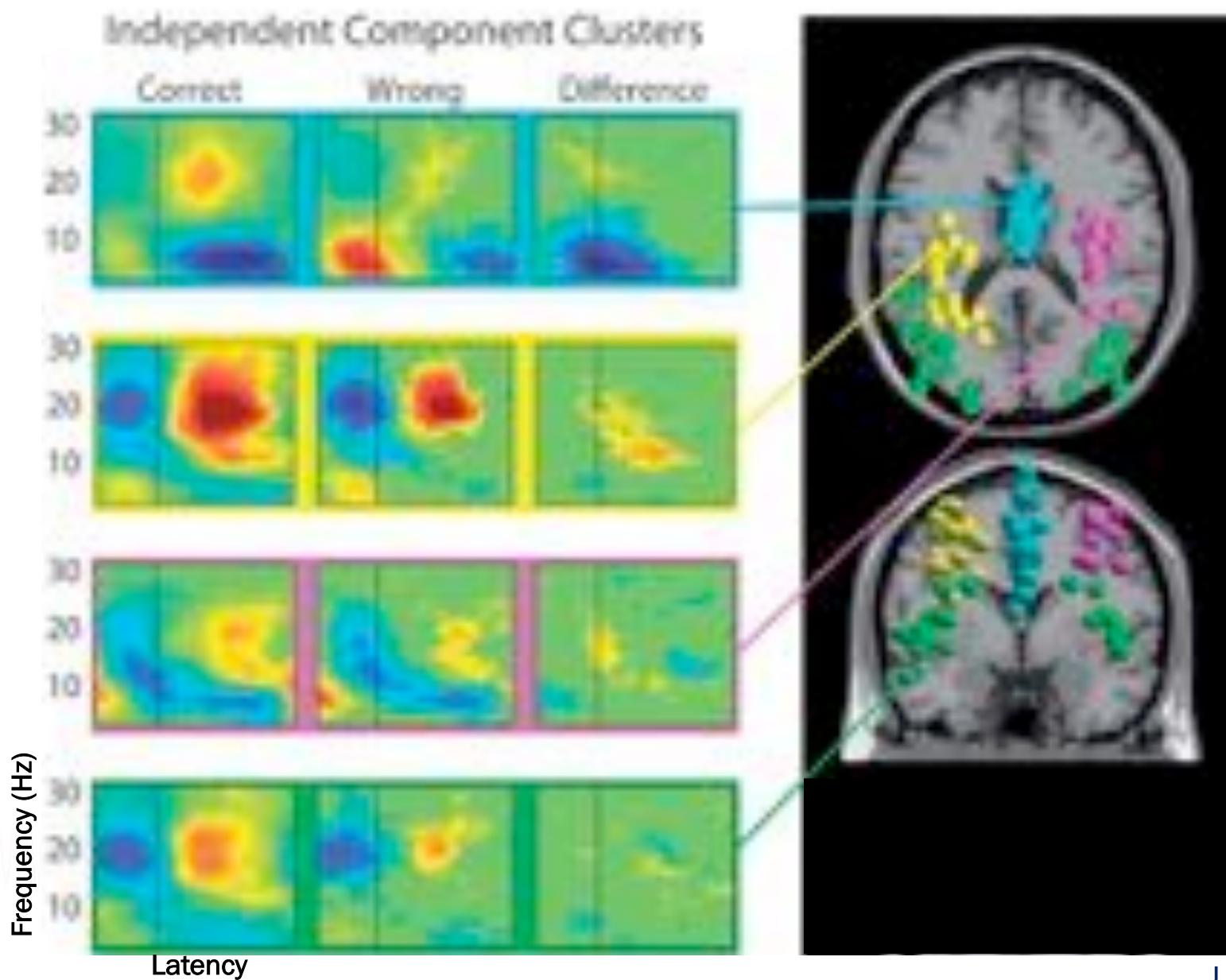
D



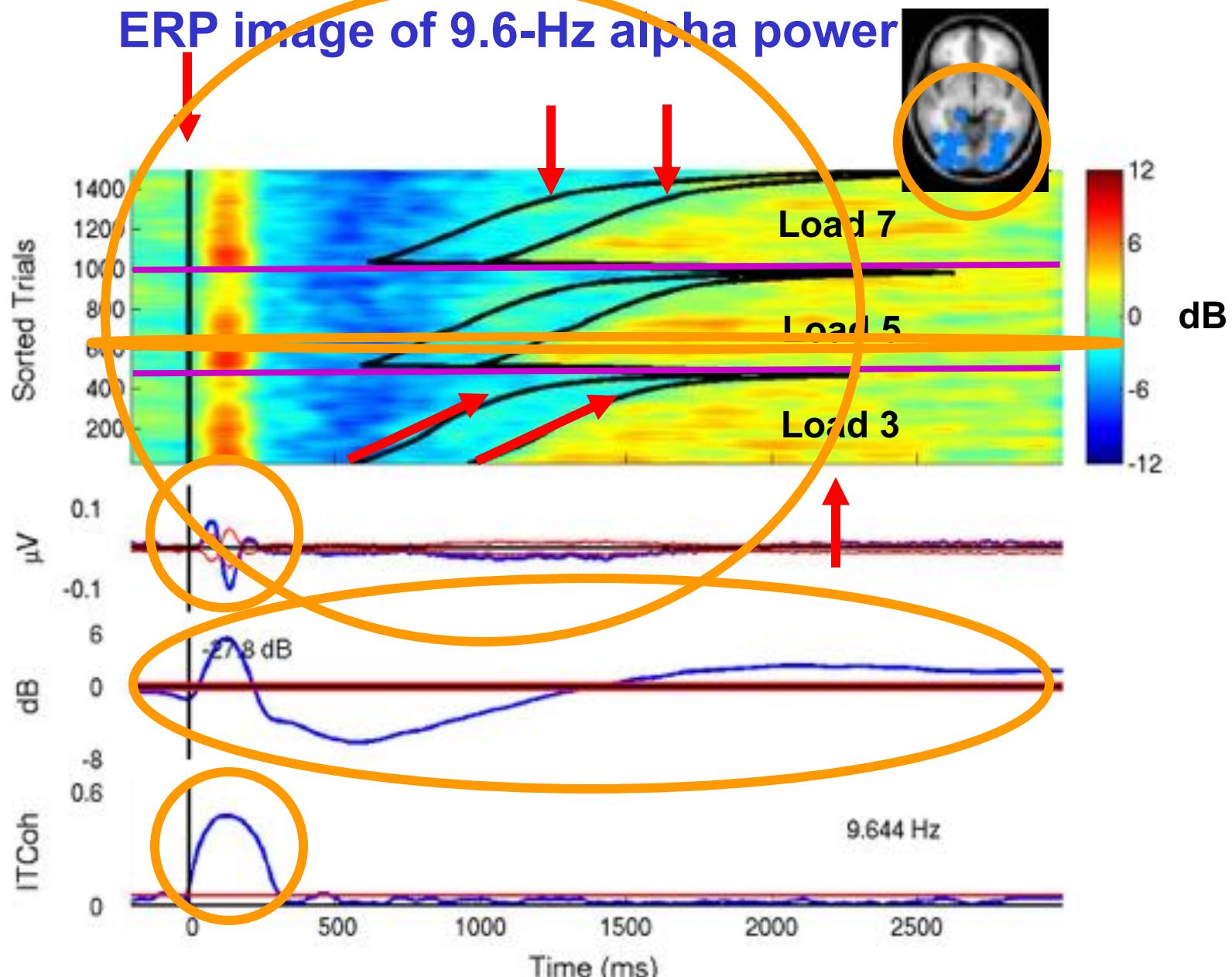
E



# Goal: To cluster equivalent ICs across subjects



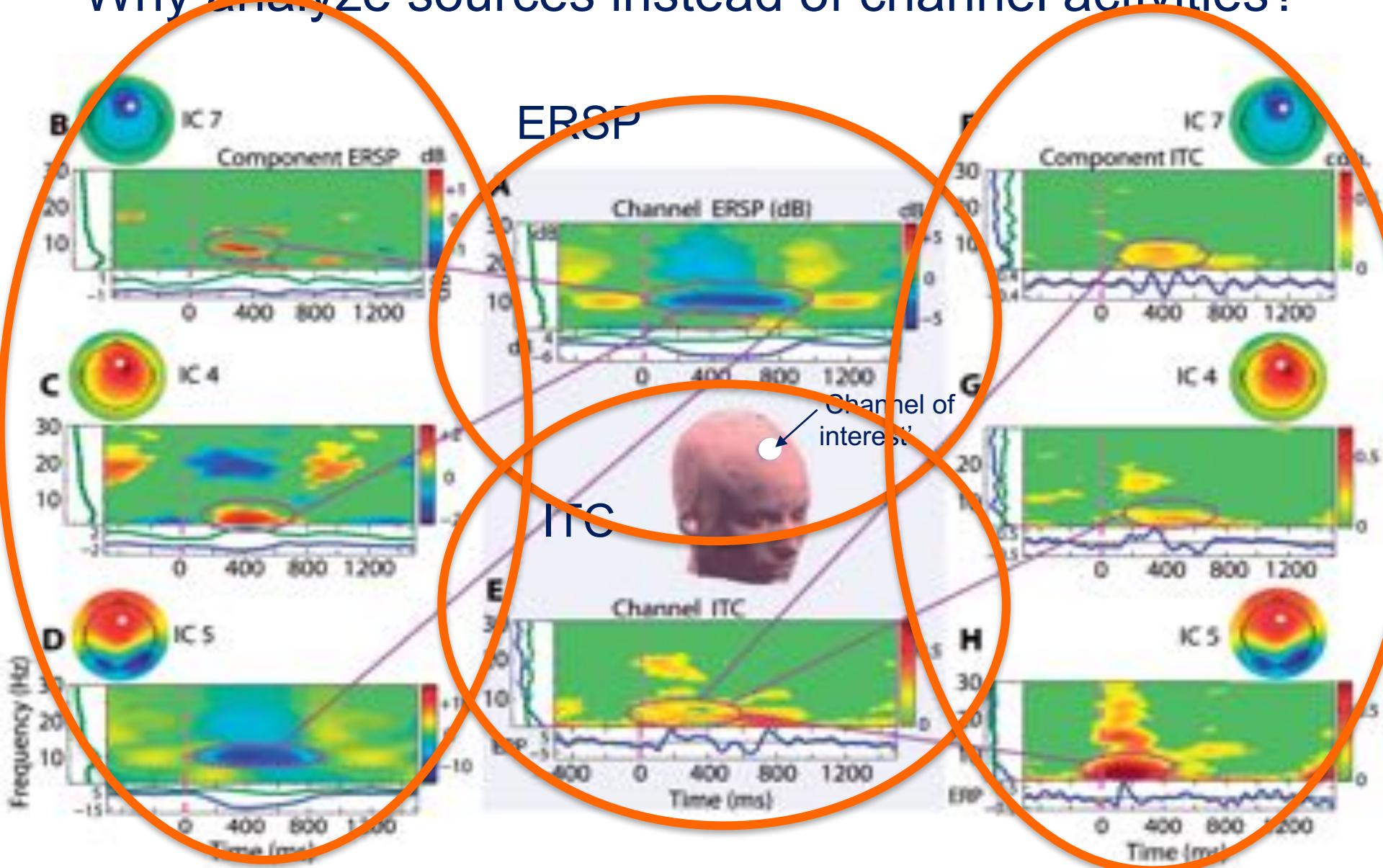
# ERP image of 9.6-Hz alpha power



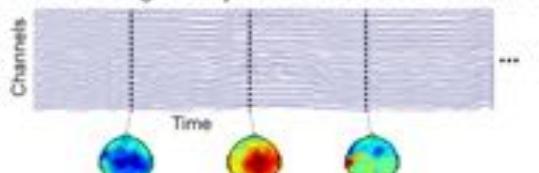
erpimage()

Onton, Delorme & Makeig, 2005.

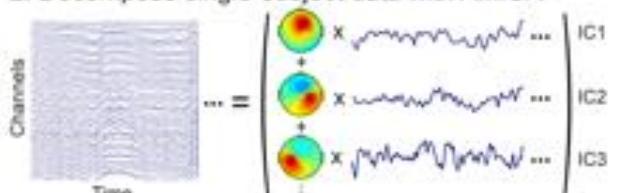
# Why analyze sources instead of channel activities?



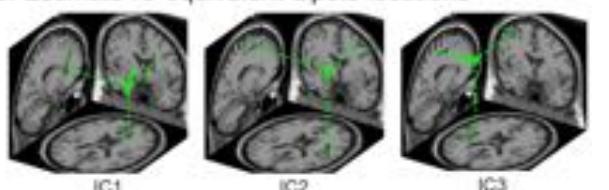
1. Record single-subject 68-channel EEG data



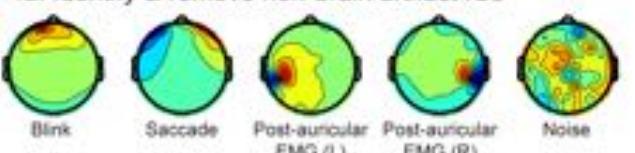
2. Decompose single-subject data with AMICA



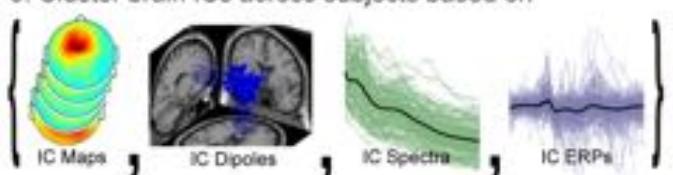
3. Estimate IC equivalent dipole locations



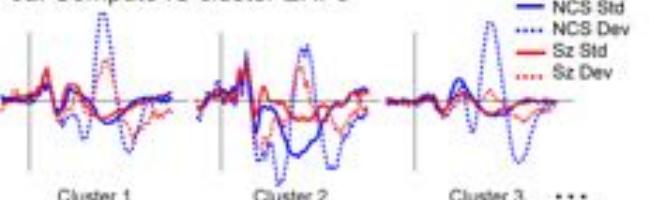
4a. Identify & remove non-brain artifact ICs



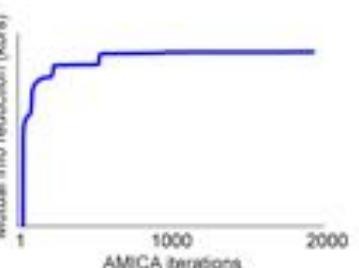
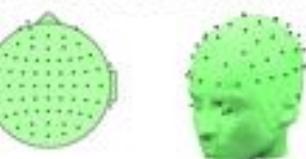
5. Cluster brain ICs across subjects based on



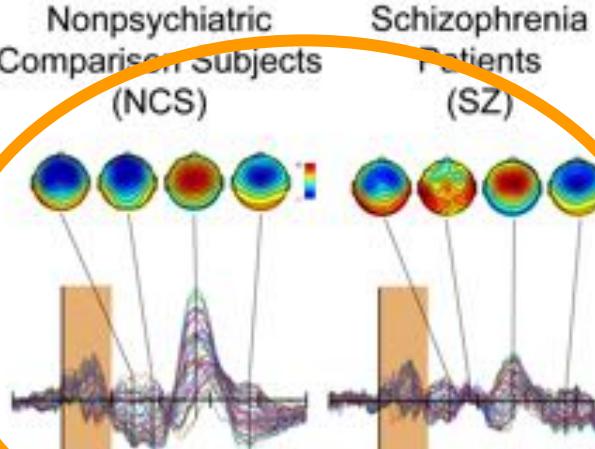
6a. Compute IC cluster ERPs



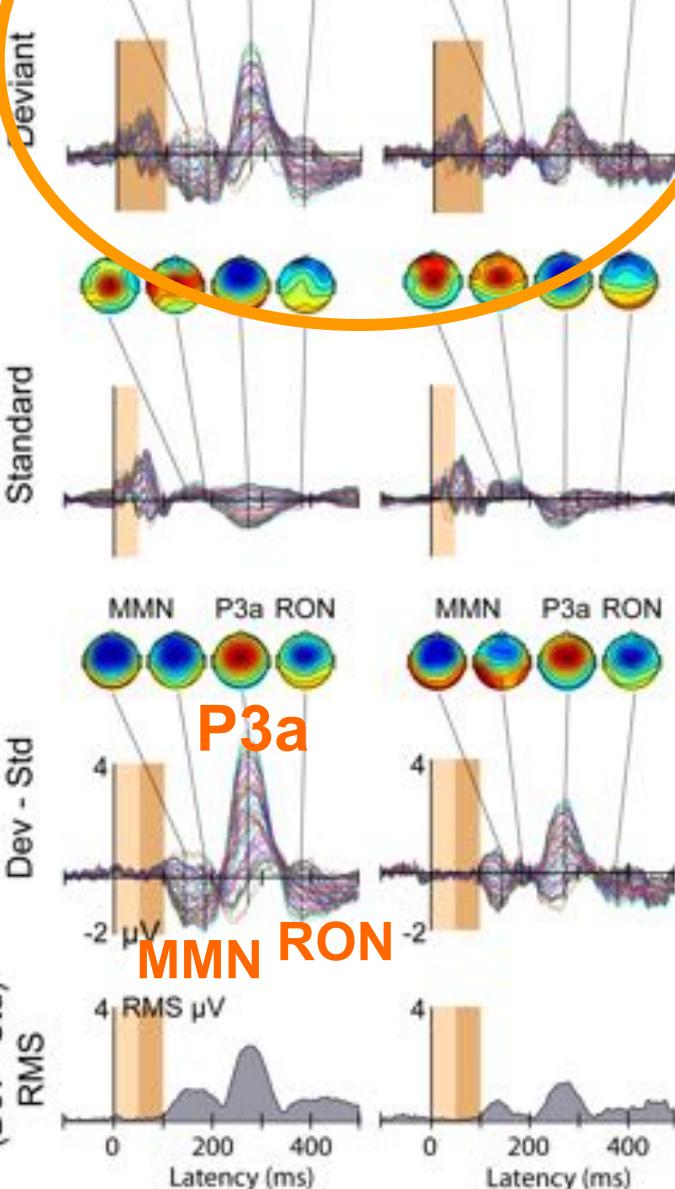
Record electrode locations



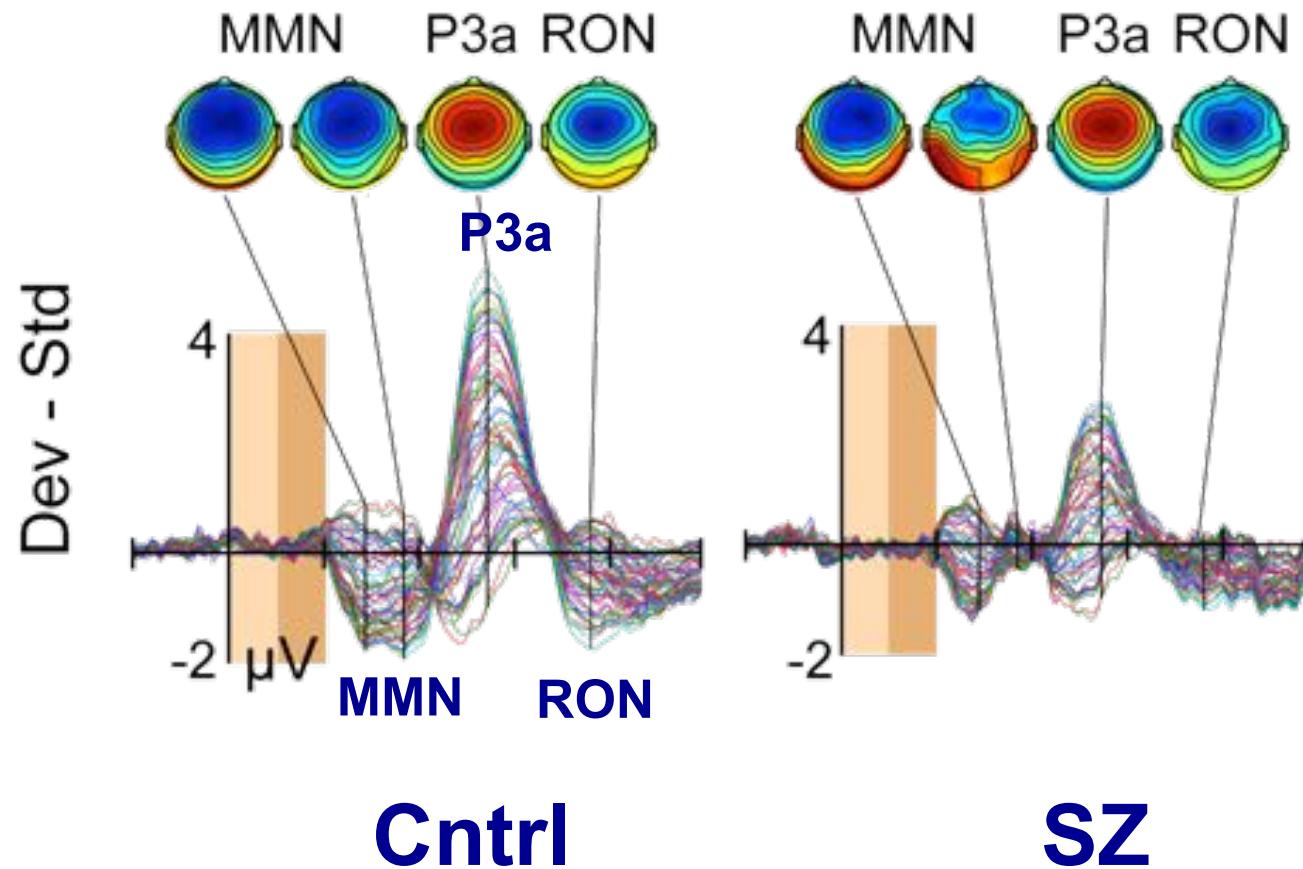
Nonpsychiatric  
Compariso. Subjects  
(NCS)



Schizophrenia  
Patients  
(SZ)

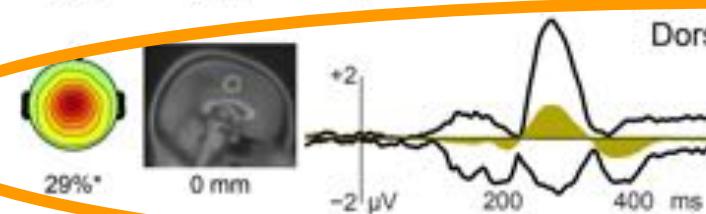
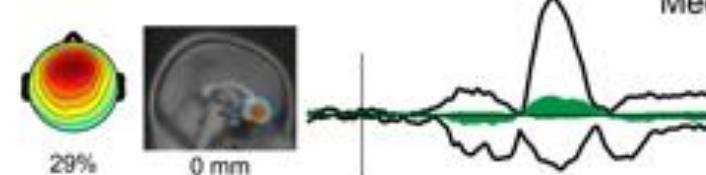
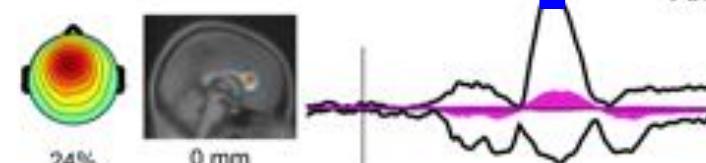
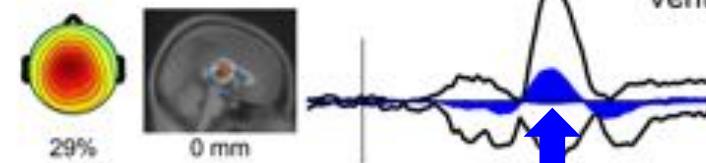
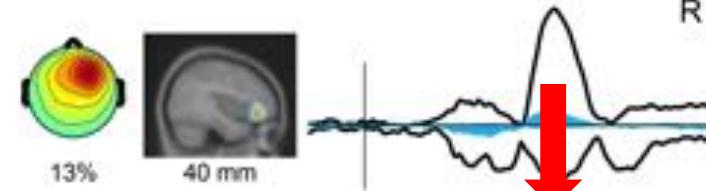
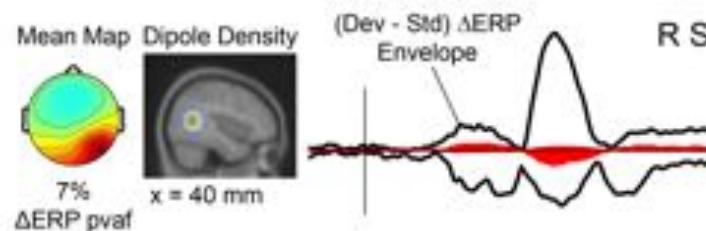


# Auditory Deviance Response



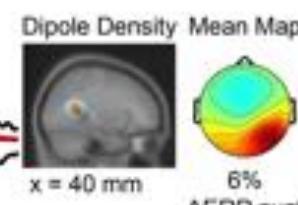
The deepest mental trap in electrophysiology  
lurks in the word “THE” !!!

### Nonpsychiatric Comparison Subjects (NCS)

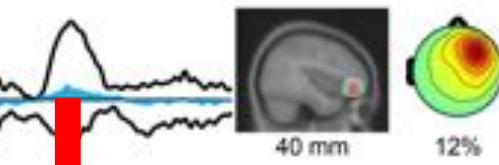


### Schizophrenia Patients (SZ)

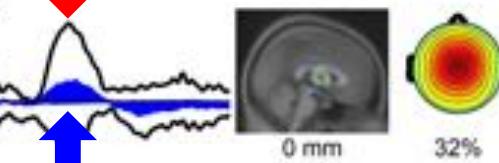
R Superior Temporal



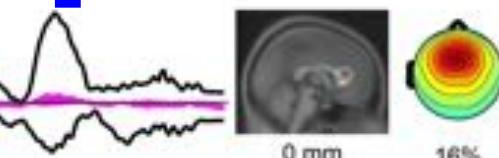
R Inferior Frontal



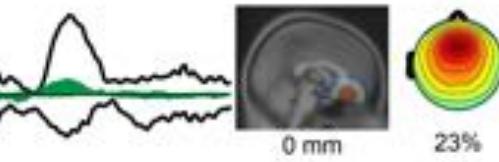
Ventral Mid Cingulate



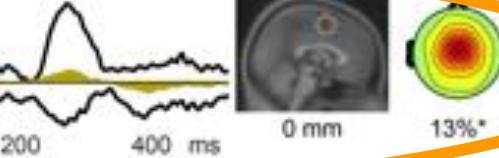
Anterior Cingulate



Medial Orbitofrontal



Dorsal Mid Cingulate



## PEAK AMPLITUDES

ERP

$r^2$

### Scalp Electrode (Fz)

Verbal IQ (WRAT)

Functional Capacity (UPSA)

R Superior Temporal

Working Memory (LNS Reorder)

Verbal IQ (WRAT)

### Immediate Verbal Memory (CVLT)

Delayed Verbal Memory (CVLT)

### Functional Capacity (UPSA)

Functional Capacity (UPSA)

R Inferior Frontal

### Negative Symptoms (SANS)

Psychosocial Functioning (SOF)

### Auditory Attention (LNS Forward)

Working Memory (LNS Reorder)

Verbal IQ (WRAT)

Ventral Mid Cingulate

### Positive Symptoms (SAPS)

### Negative Symptoms (SANS)

### Immediate Verbal Memory (CVLT)

Delayed Verbal Memory (CVLT)

Verbal IQ (WRAT)

Executive Functioning (WCST)

Anterior Cingulate

Functional Status (GAF)

Functional Status (GAF)

### Immediate Verbal Memory (CVLT)

Delayed Verbal Memory (CVLT)

Medial Orbitofrontal

### Positive Symptoms (SAPS)

### Negative Symptoms (SANS)

### Psychosocial Functioning (SOF)

### Functional Capacity (UPSA)

Dorsal Mid Cingulate

Verbal IQ (WRAT)

Executive Functioning (WCST)

P3a  
RON

0.11  
0.12

RON

0.15

RON

0.15

RON

0.28

RON

0.26

MMN

0.48

RON

0.26

RON

0.36

RON

0.24

MMN

0.38

MMN

0.30

MMN

0.46

RON

0.29

P3a

0.36

RON

0.41

RON

0.24

RON

0.29

RON

0.24

MMN

0.18

RON

0.17

RON

0.25

RON

0.17

P3a

0.40

P3a

0.54

P3a

0.37

P3a

0.32

P3a

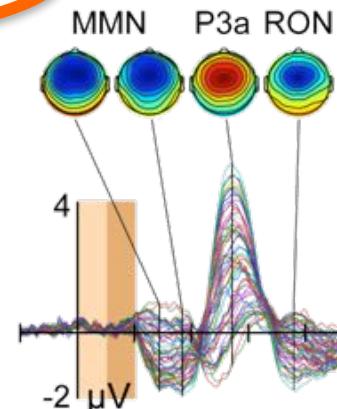
0.15

MMN

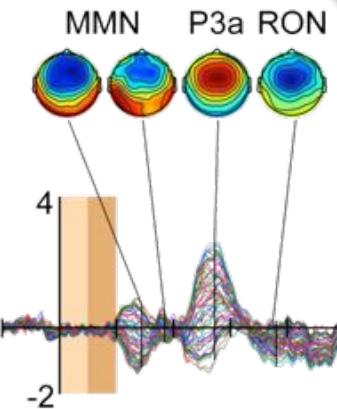
0.18

ADR

Dev - Std



Cntrl



SZ

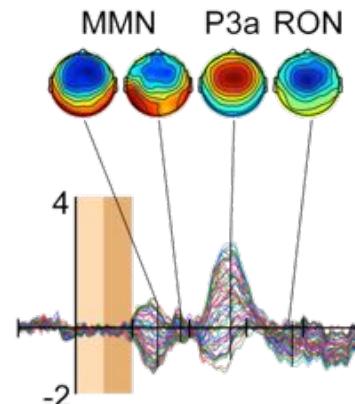
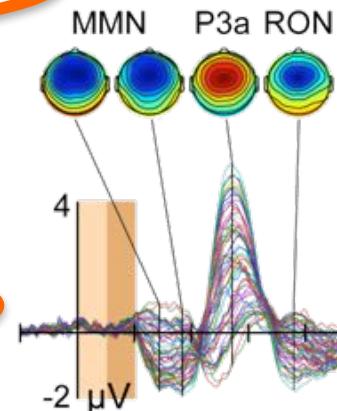
# PEAK LATENCIES

ERP

$r^2$

Scalp Electrode (Fz)		
---n/a---	---	---
R Superior Temporal		
Functional capacity (UPSA)	MMN	0.25
Delayed Verbal Memory (CVLT)	MMN	0.17
R Inferior Frontal		
<b>Negative Symptoms (SANS)</b>	<b>RON</b>	<b>0.51</b>
Psychosocial Functioning (SOF)	RON	0.25
<b>Executive Functioning (WCST)</b>	<b>MMN</b>	<b>0.30</b>
<b>Executive Functioning (WCST)</b>	<b>P3a</b>	<b>0.28</b>
Ventral Mid Cingulate		
<b>Negative Symptoms (SANS)</b>	<b>P3a</b>	<b>0.33</b>
<b>Negative Symptoms (SANS)</b>	<b>RON</b>	<b>0.33</b>
Psychosocial Functioning (SOF)	P3a	0.31
Verbal IQ (WRAT)	MMN	0.25
<b>Executive Functioning (WCST)</b>	<b>P3a</b>	<b>0.30</b>
Anterior Cingulate		
Functional Capacity (UPSA)	RON	0.17
Verbal IQ (WRAT)	MMN	0.24
Auditory Attention (LNS-Forward)	MMN	0.17
Medial Orbitofrontal		
<b>Negative Symptoms (SANS)</b>	<b>RON</b>	<b>0.41</b>
<b>Positive Symptoms (CAPS)</b>	<b>RON</b>	<b>0.40</b>
<b>Auditory Attention (LNS-Forward)</b>	<b>MMN</b>	<b>0.29</b>
<b>Executive Functioning (WCST)</b>	<b>P3a</b>	<b>0.32</b>
Dorsal Mid Cingulate		
Negative Symptoms (SANS)	MMN	0.20
Negative Symptoms (SANS)	P3a	0.17
Global Functioning (GAF)	RON	0.24
Functional Capacity (UPSA)	P3a	0.13

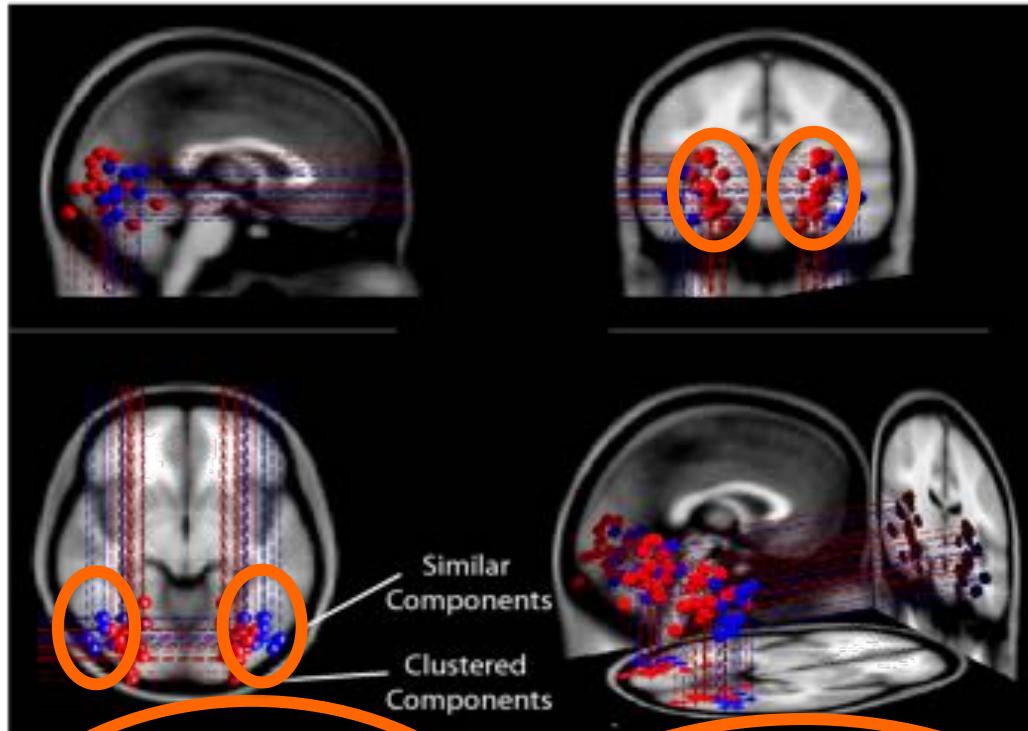
# ADR



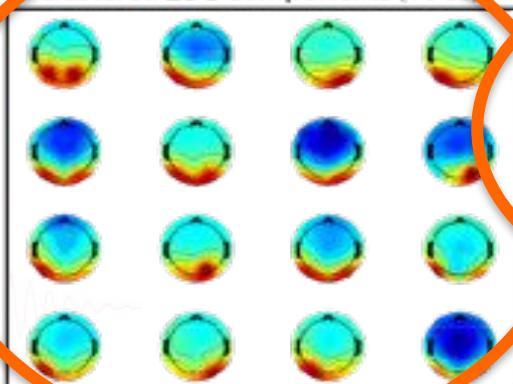
Cntrl

SZ

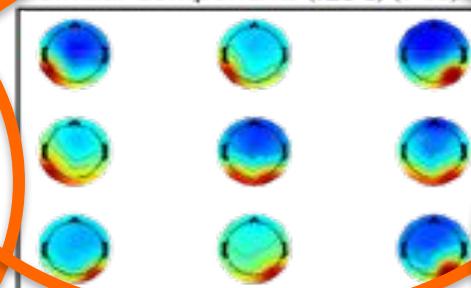
# Why don't all subjects contribute to every IC cluster?



Clustered LOC Components (16 ss)



Similar Components (fLOC) (9 ss)

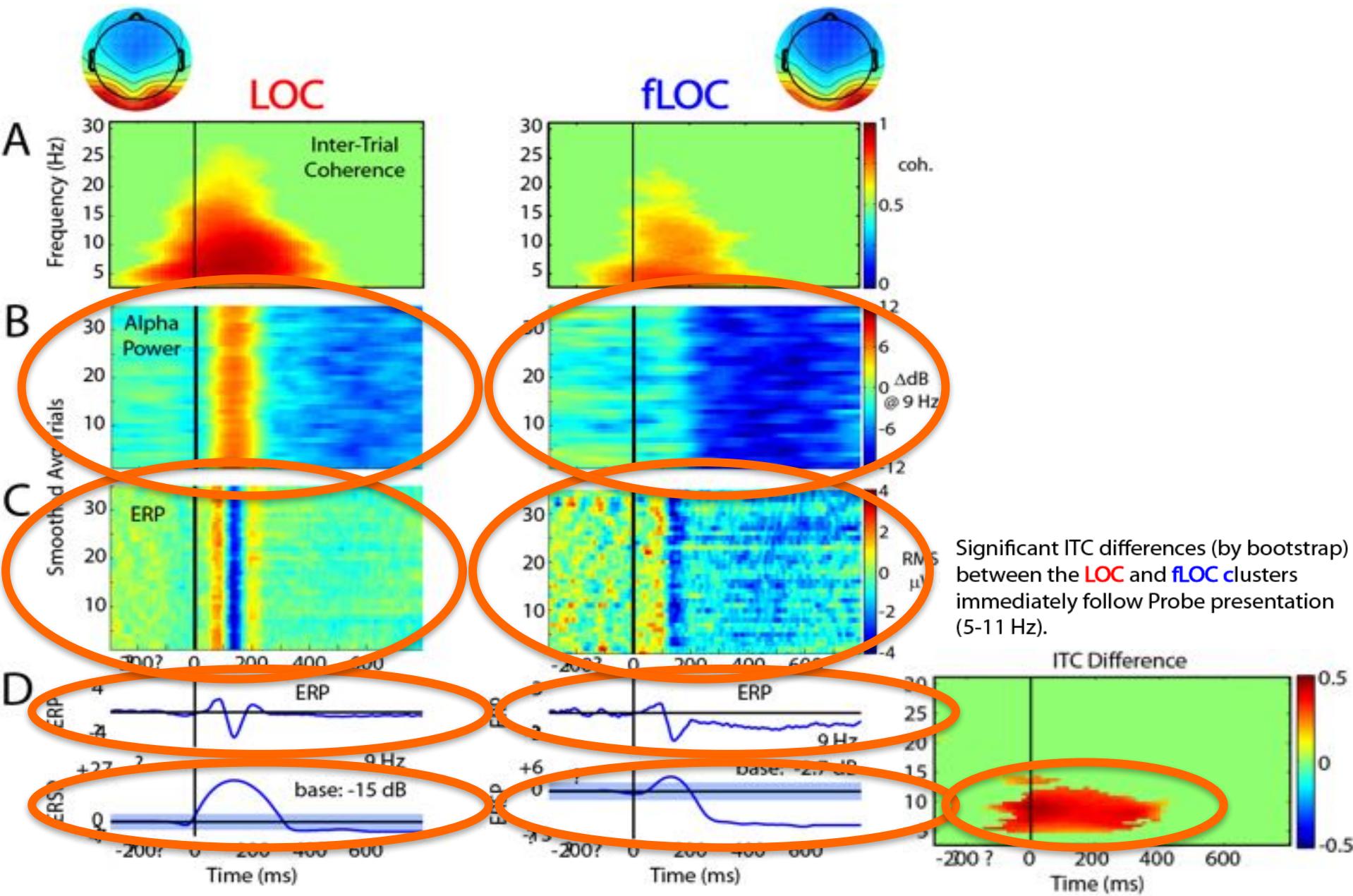


Mean of 9 fLOC Components

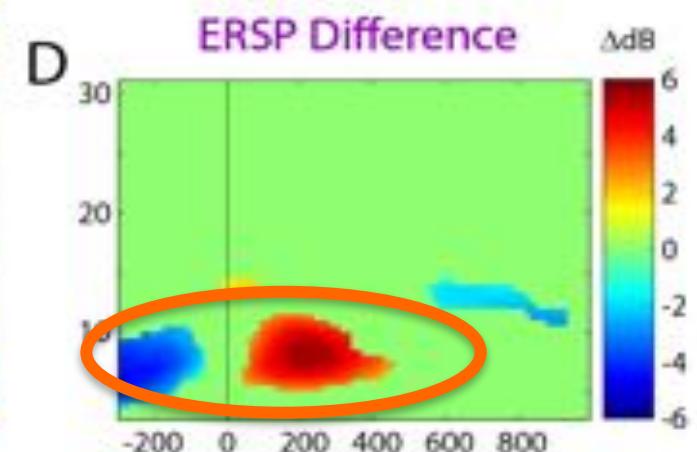
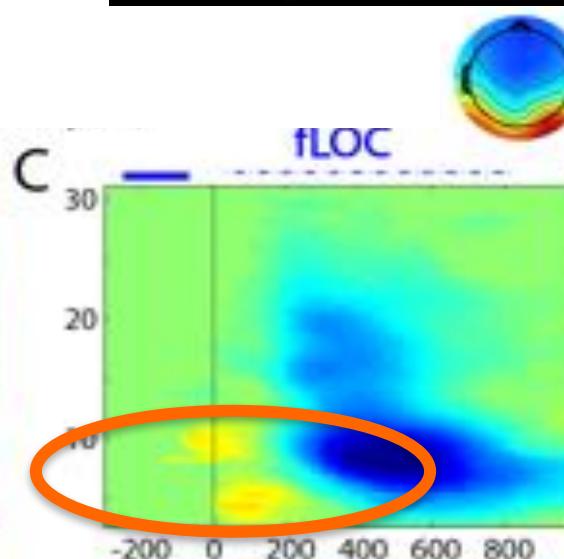
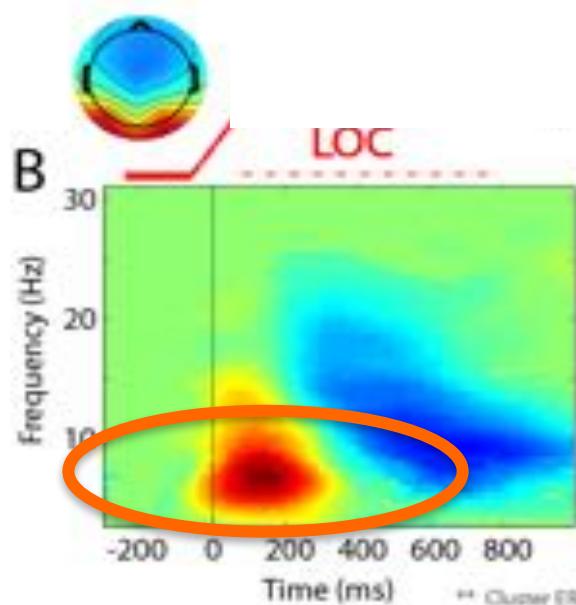
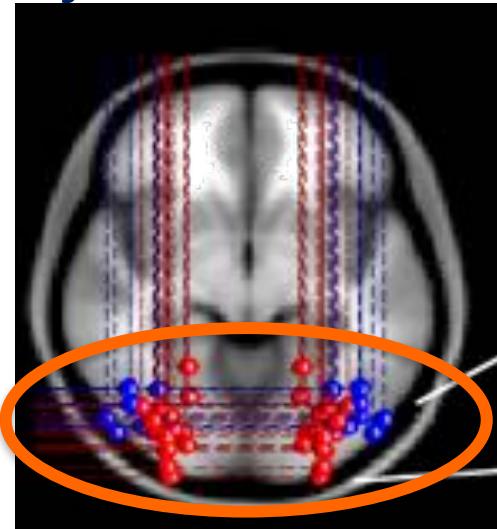


Mean of 16 LOC Components

# Subject differences?



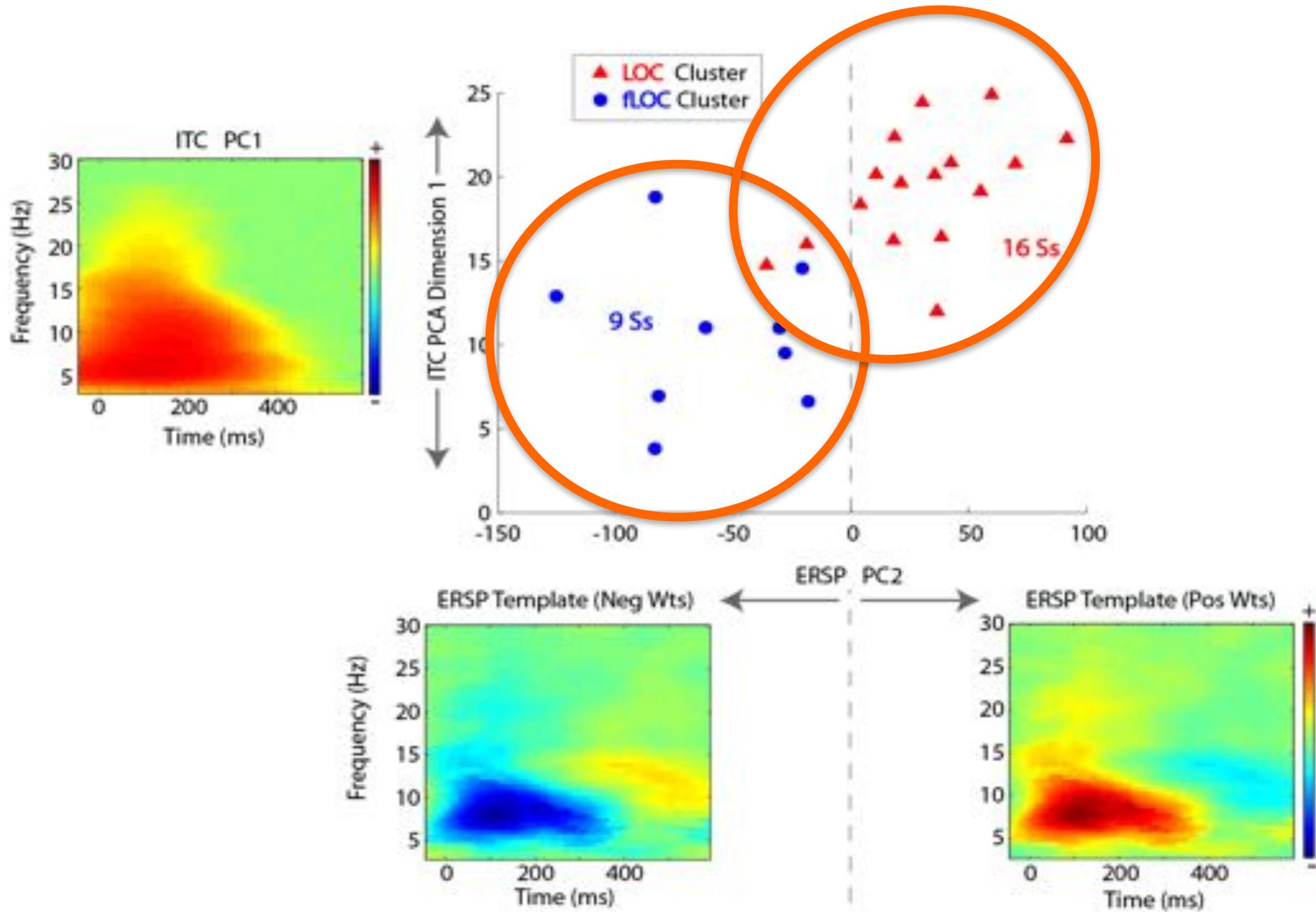
# Subject differences?



\*\* Cluster ERSPs show significant activity determined by bootstrap statistics within subject and binomial probability between subjects ( $p < 0.01$ )

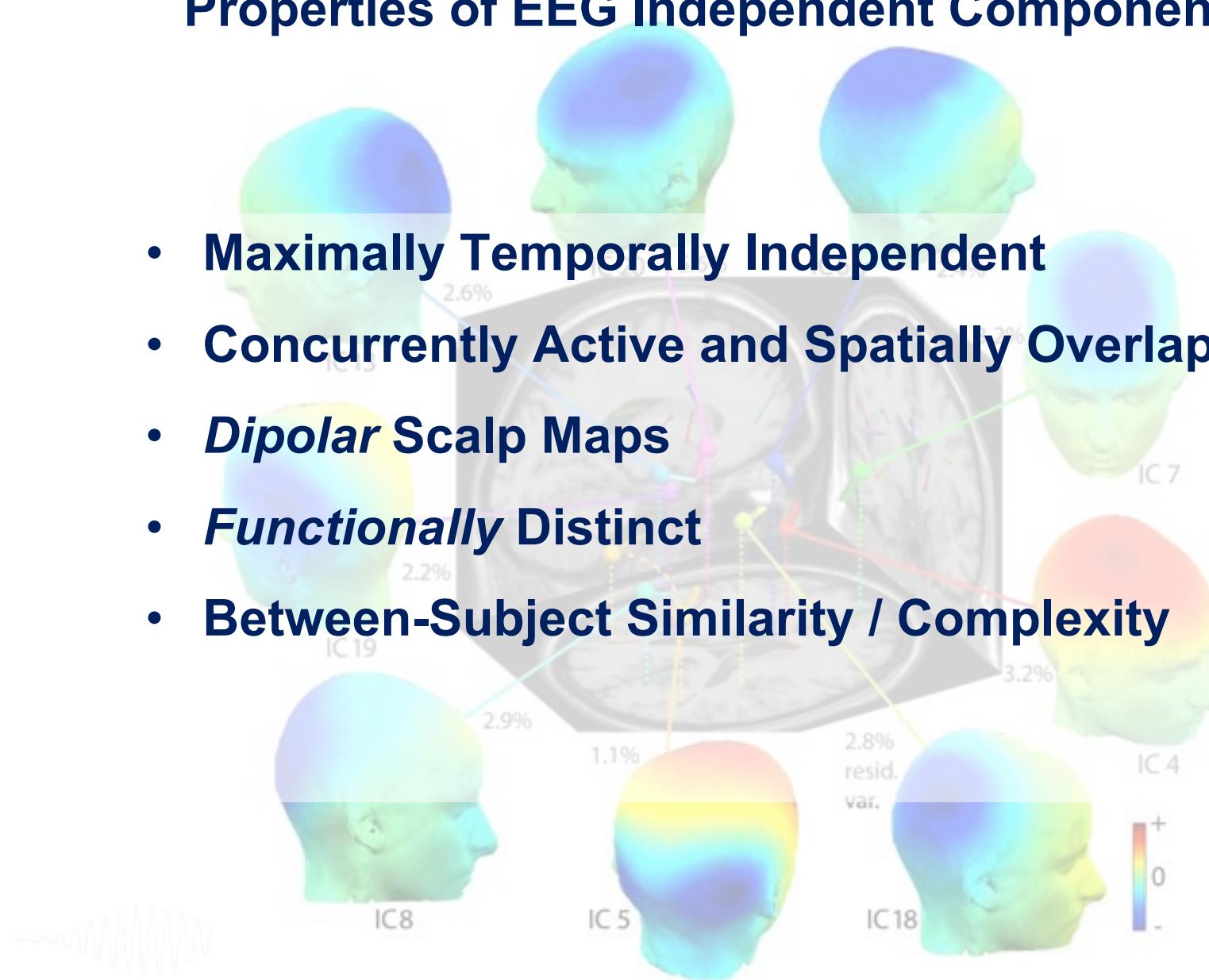
\*\*\* Difference ERSP shows significant differences between the two clusters by bootstrap statistics ( $p < 0.001$ )

# Subject differences?



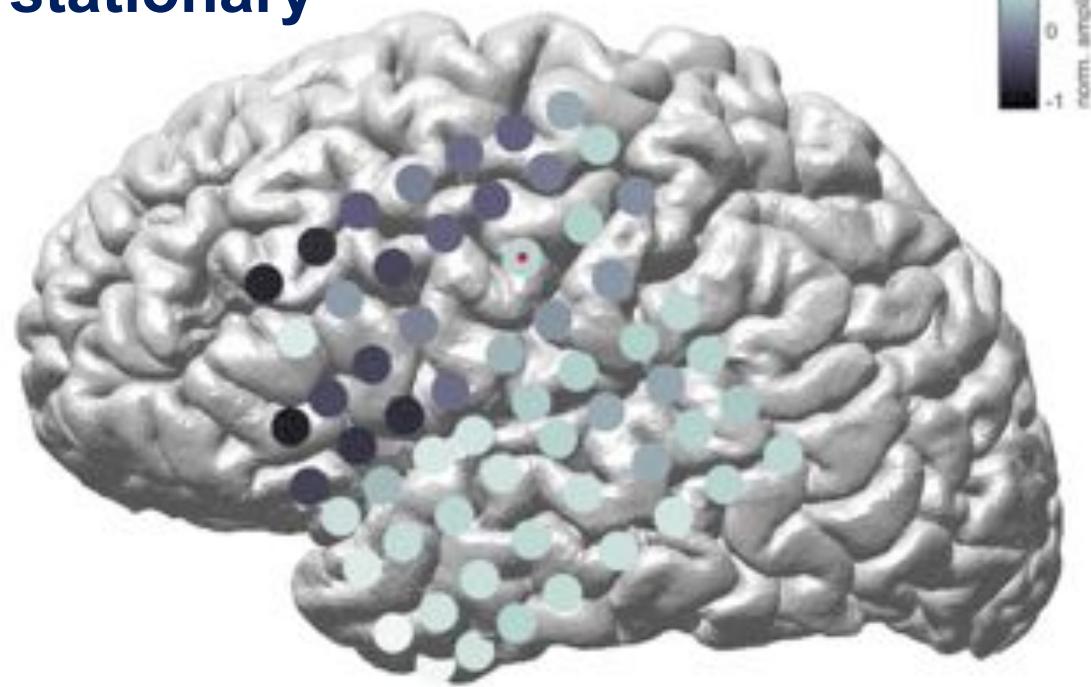
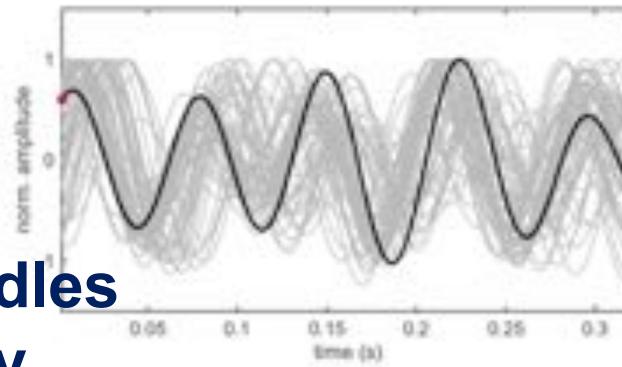
# Properties of EEG Independent Components

- **Maximally Temporally Independent**
- **Concurrently Active and Spatially Overlapping**
- ***Dipolar Scalp Maps***
- ***Functionally Distinct***
- **Between-Subject Similarity / Complexity**



**But ...**

**NB: Sleep spindles  
are *not* spatially  
stationary**





*More ...*