

Functional High-Definition Imaging of EEG Brain Dynamics



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Klaus Gramann



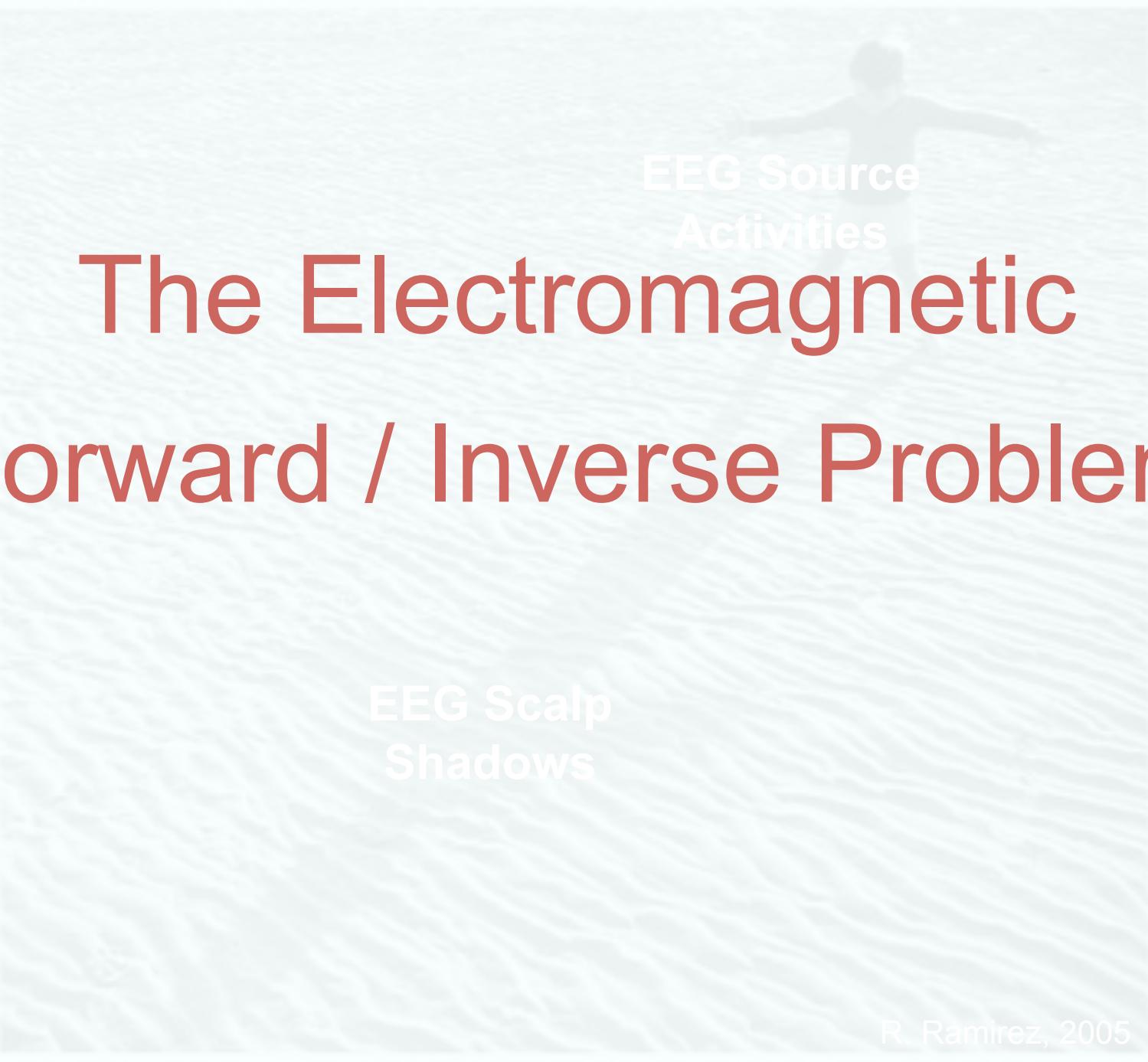
Tony Bell



Zeynep
Akalin Acar



Nima Bigdely
Shamlo



EEG Source
Activities

The Electromagnetic Forward / Inverse Problem

EEG Scalp
Shadows

R. Ramirez, 2005



**EEG Source
Activities**

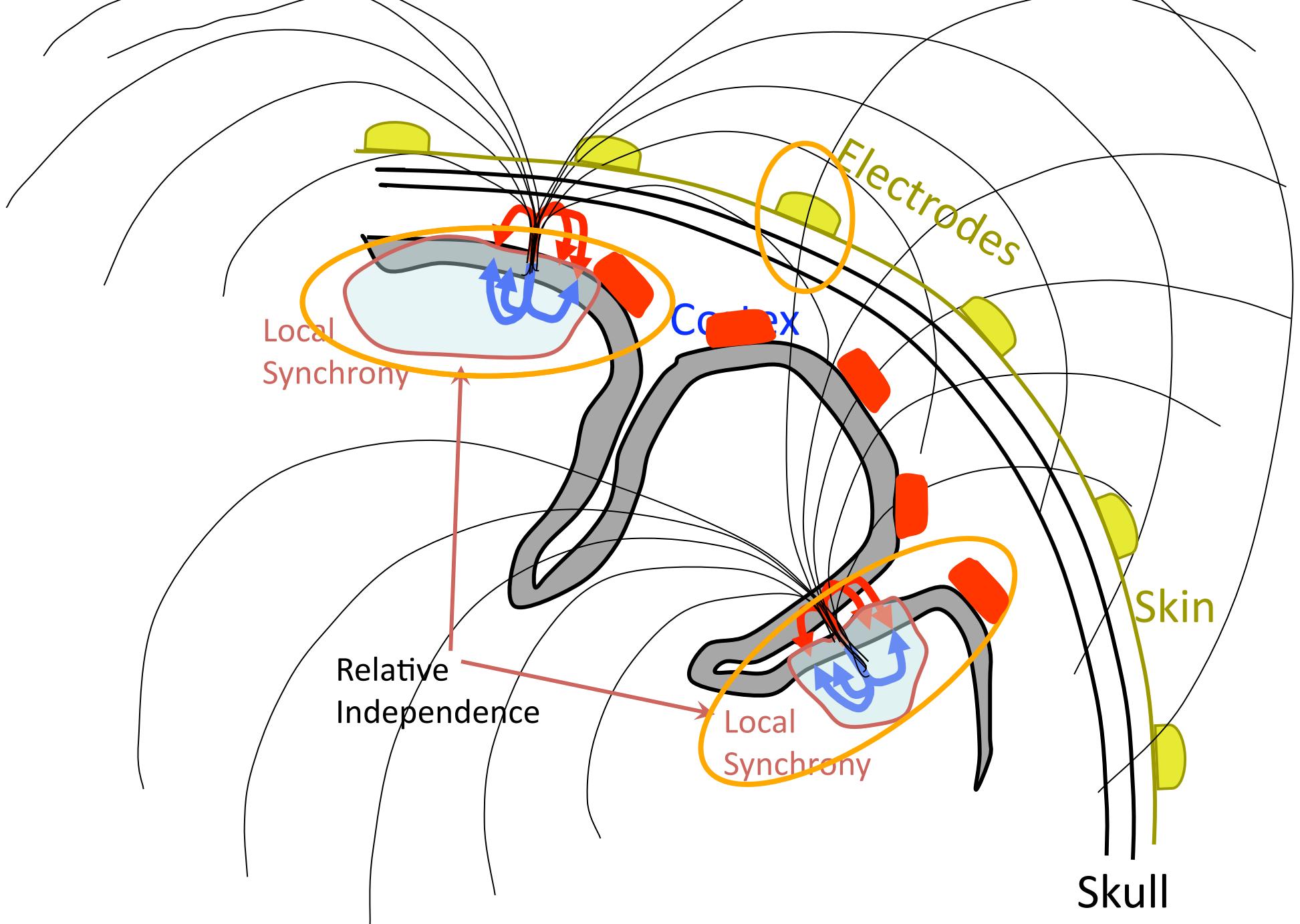
**EEG Scalp
Shadows**

R. Ramirez, 2005

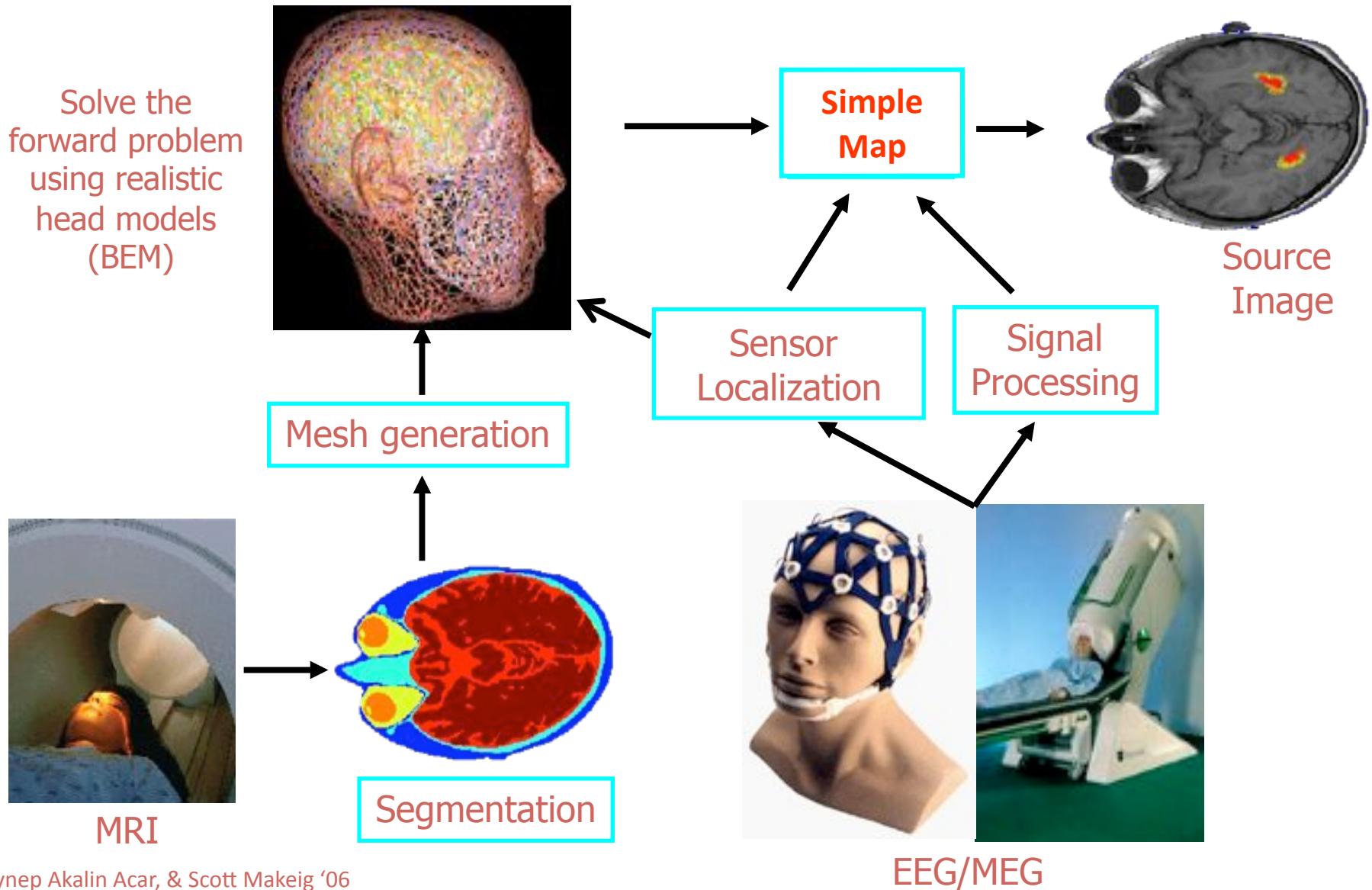
Phase cones (Freeman)

Avalanches (Plenz)

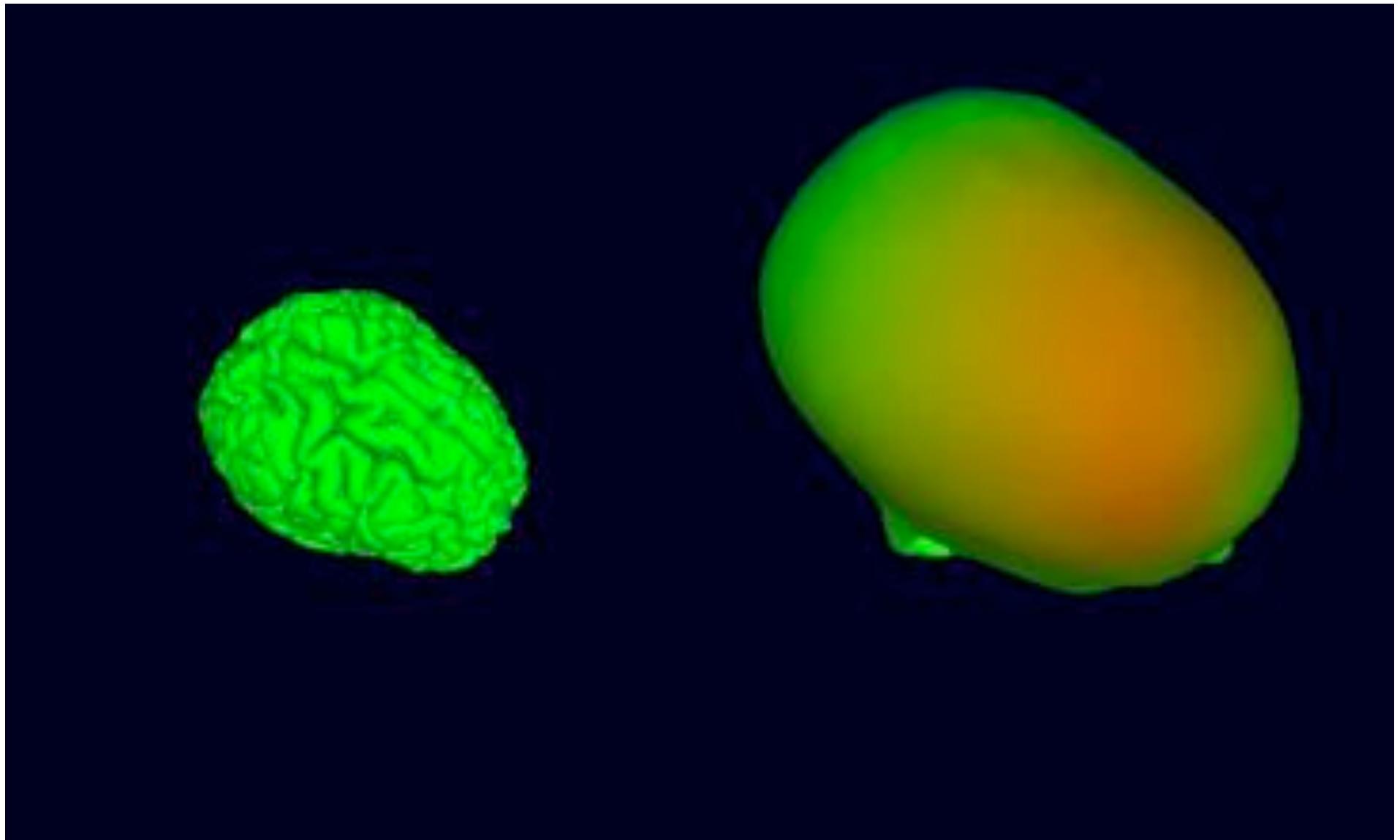




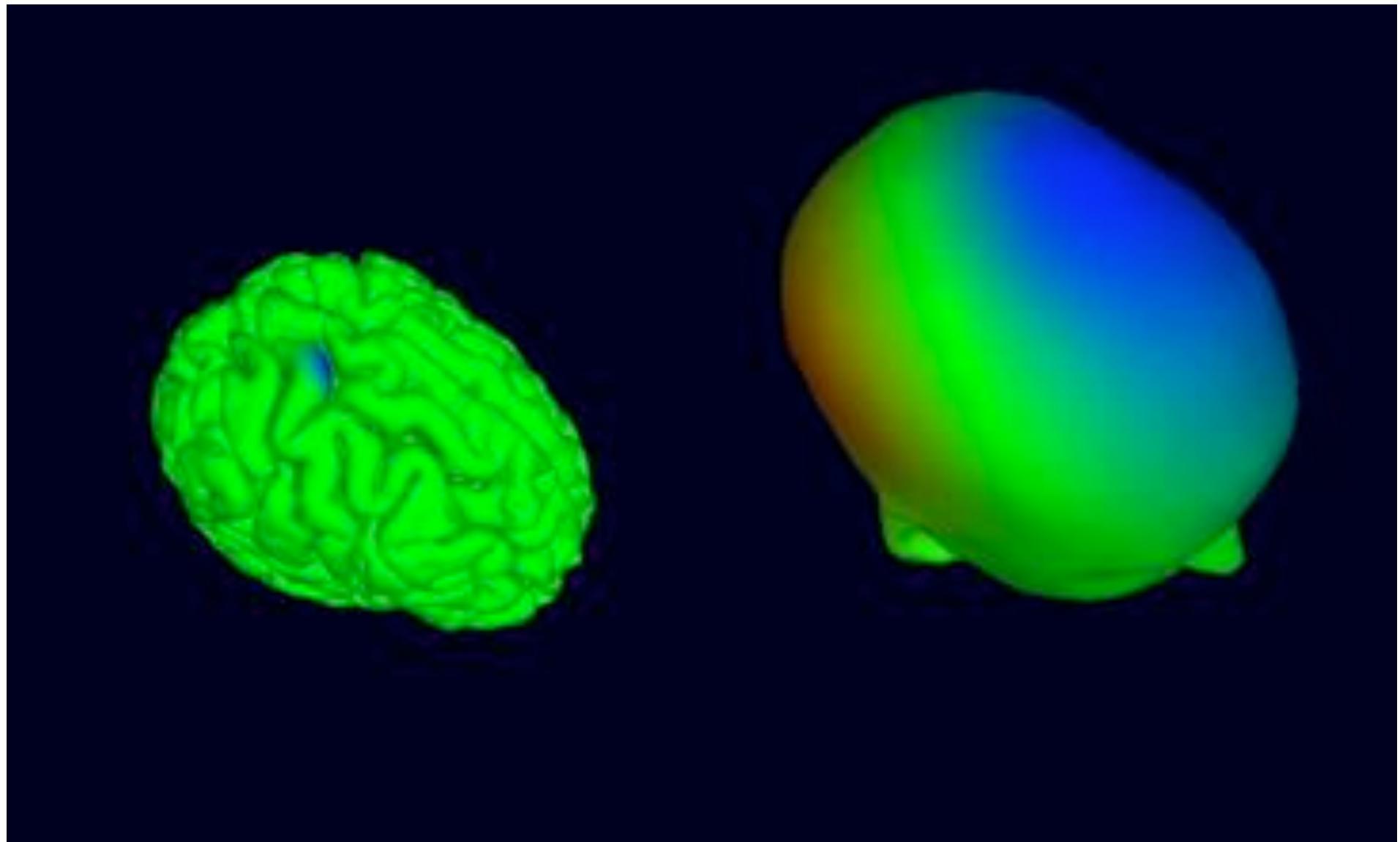
Electromagnetic source localization using realistic head models – the NFT toolbox



The very broad EEG point-spread function



The very broad EEG point-spread function

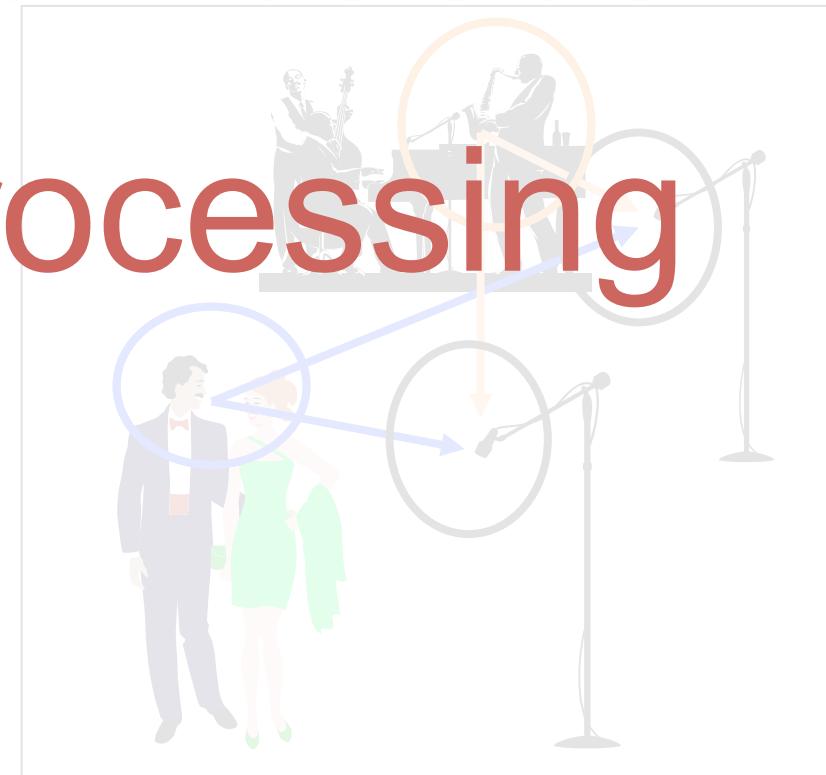
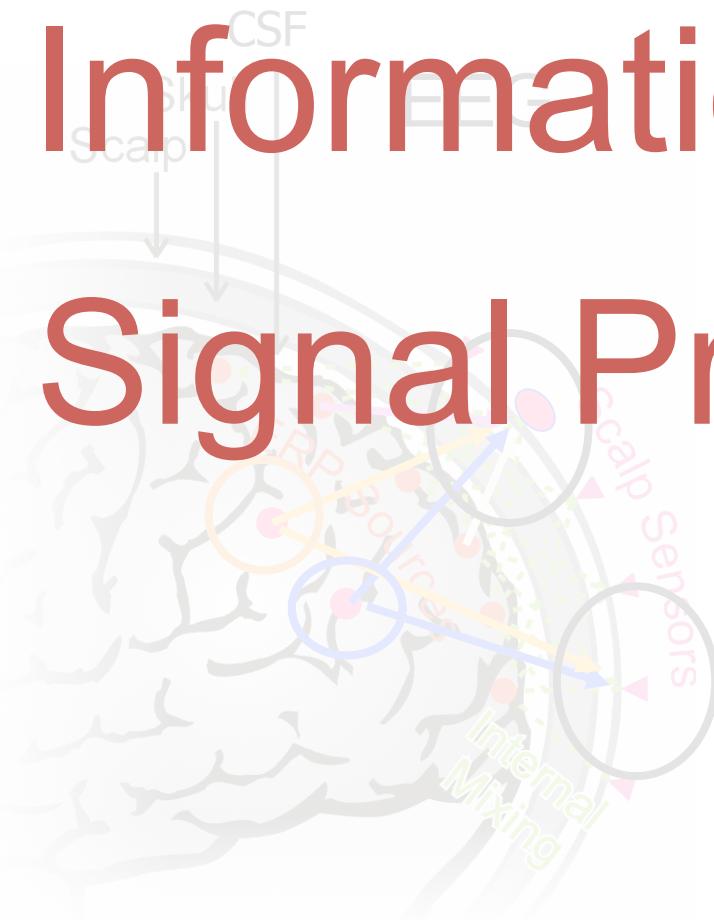


Simulated spatially labile parietal source activity

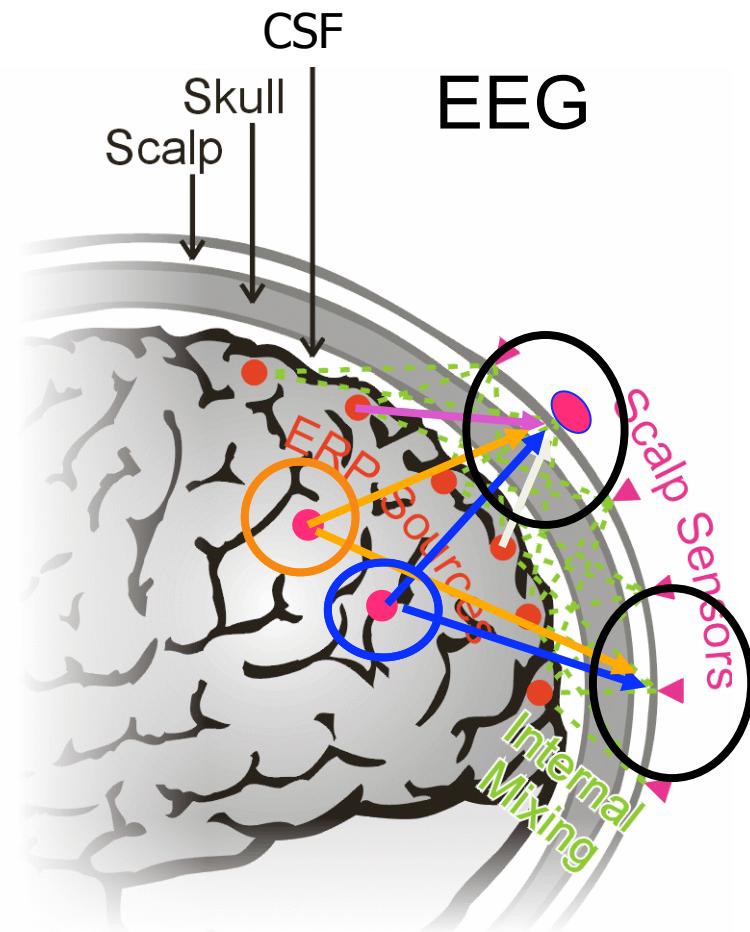
Akalin Acar & Makeig 2010

Blind EEG Source Separation by ICA

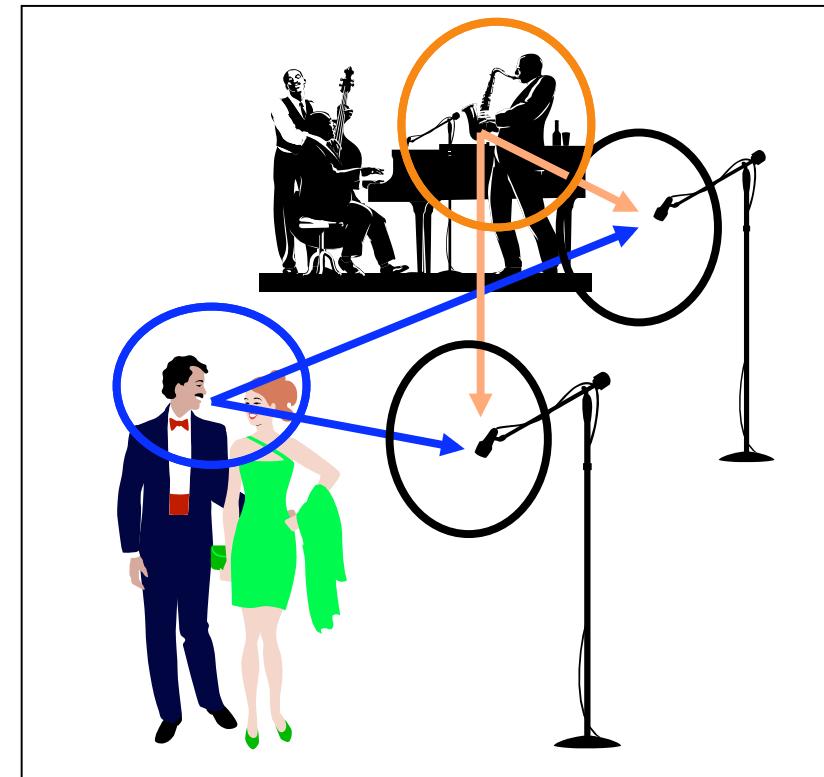
Information-based Signal Processing

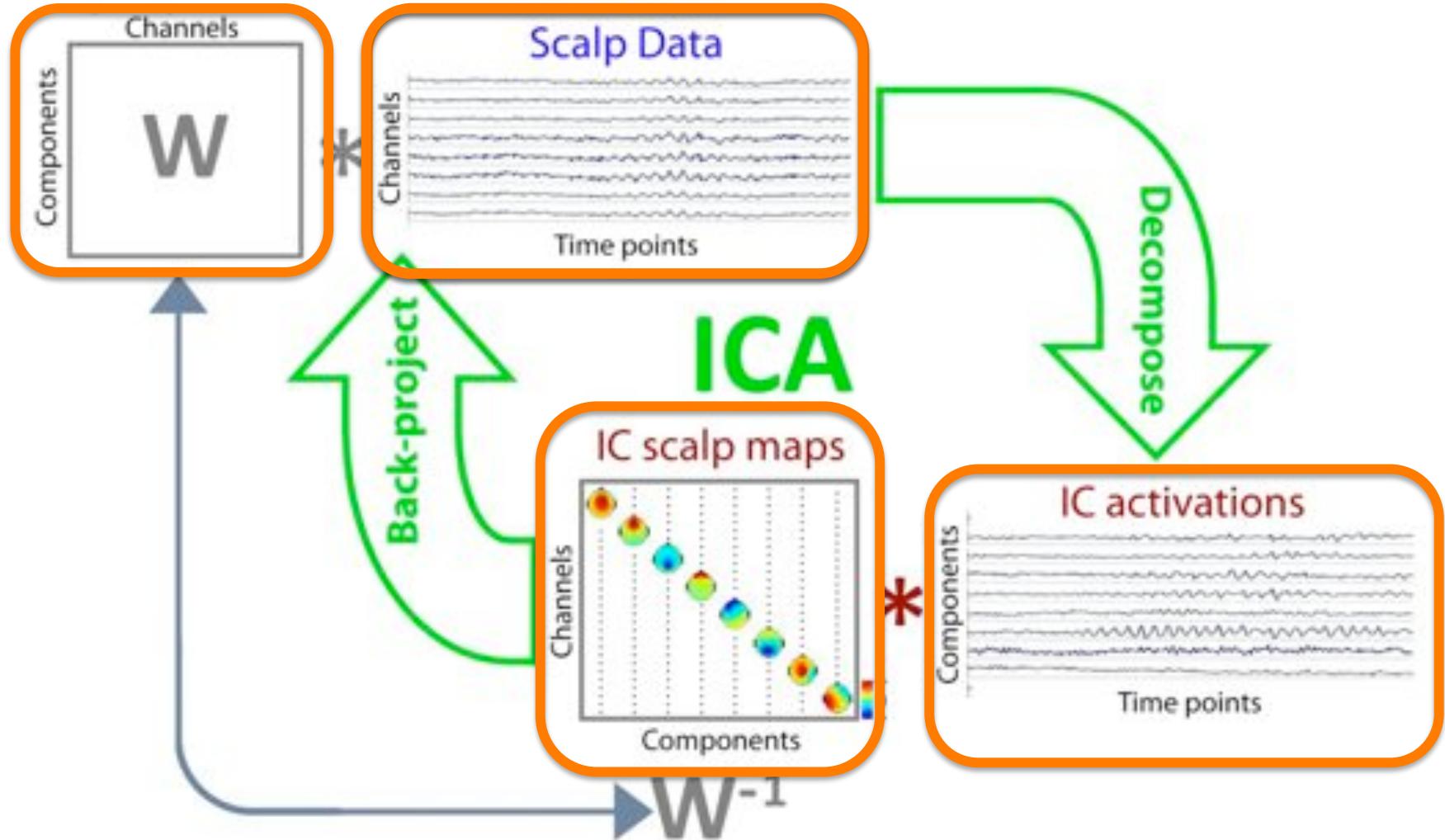


Blind EEG Source Separation by ICA



Cocktail Party





Independent Component Analysis of Electroencephalographic Data



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Abstract

Because of the differences between the left and right and their different responsibilities, electroencephalographic (EEG) data collected from any point on the human scalp includes activity generated within a large brain area. This makes processing of EEG data by volume conduction due to muscle significant time delays. However, suggesting that the Independent Component Analysis (ICA) algorithm of Bell and Sejnowski [1] is suitable for performing blind source separation on EEG data. The ICA algorithm separates the position of source identification from that of source localization. Thus, similar to applying the ICA algorithm to fMRI and magnetoencephalogram (MEG) data collected during a sustained auditory detection task shown [2], ICA is able to distinguish 16 different random walks. (2) ICA may be used to segregate obvious artifacts (EEG components that are clearly noise, eye movements) from other sources. (3) ICA is capable of isolating overlapping EEG phenomena, including alpha and theta bands and spindles against the MEG components, no separate ICA channels. (4) Nonstationarities in EEG and behavioral tasks can be tracked using ICA via changes in the structure of mutual information between ICA filtered output channels.

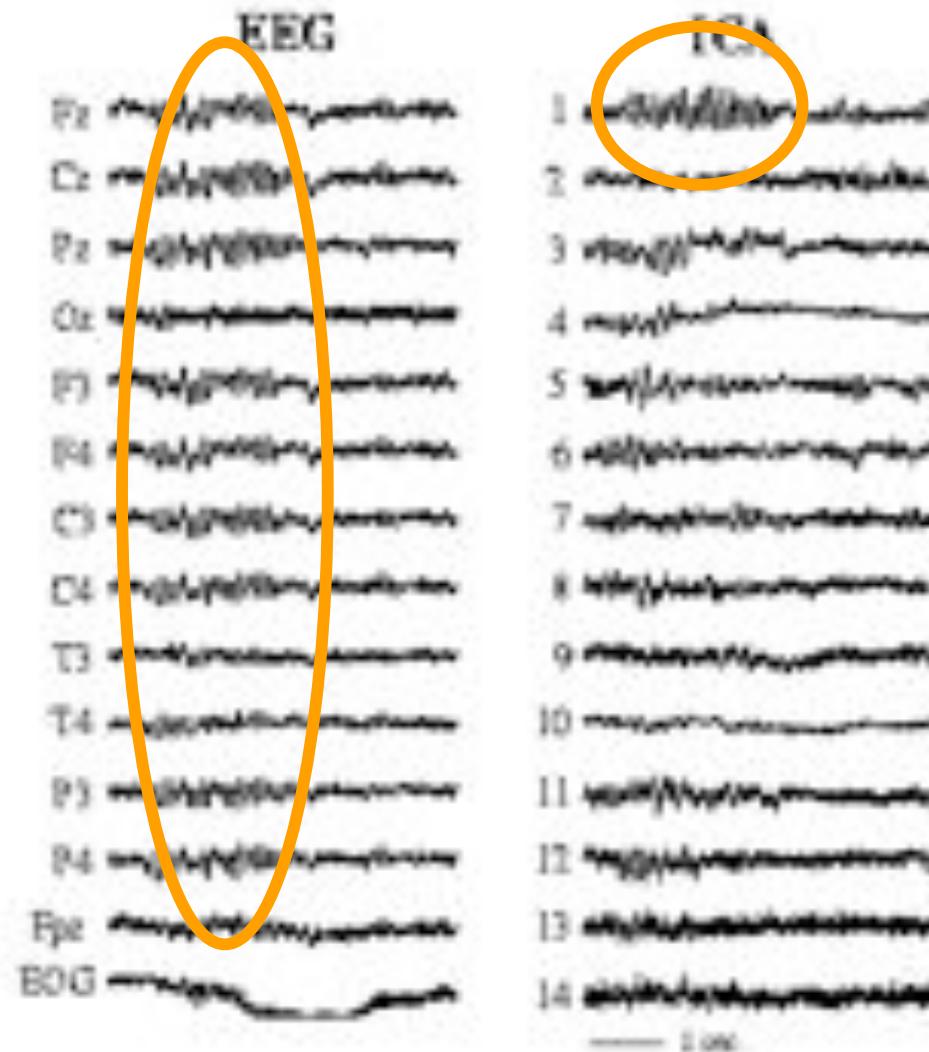
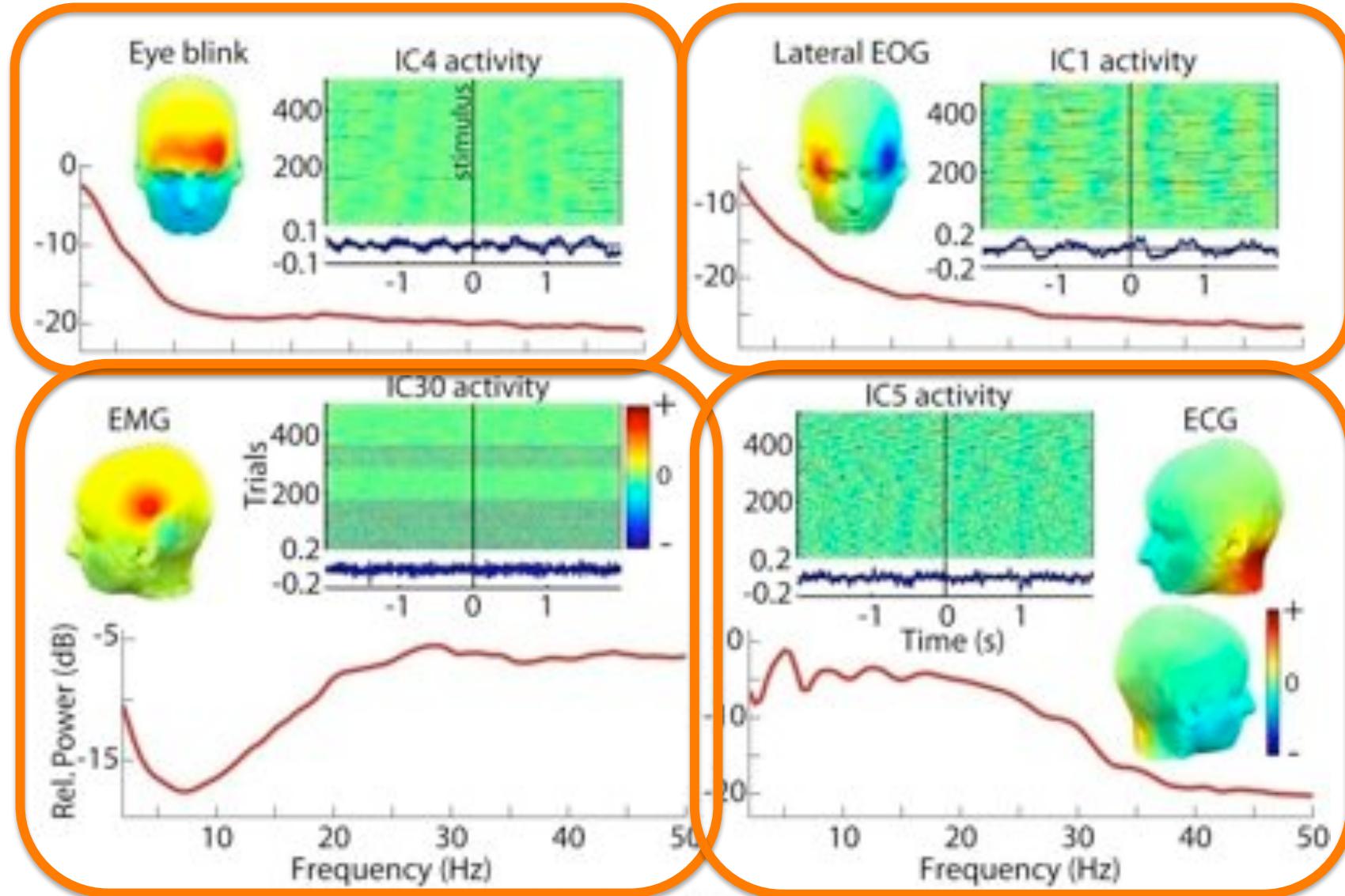


Figure 3. Left: 6.5 seconds of 16-channel EEG data. Right: an ICA transform of the same data, using weights trained on 6.5 minutes of similar data from the same session.

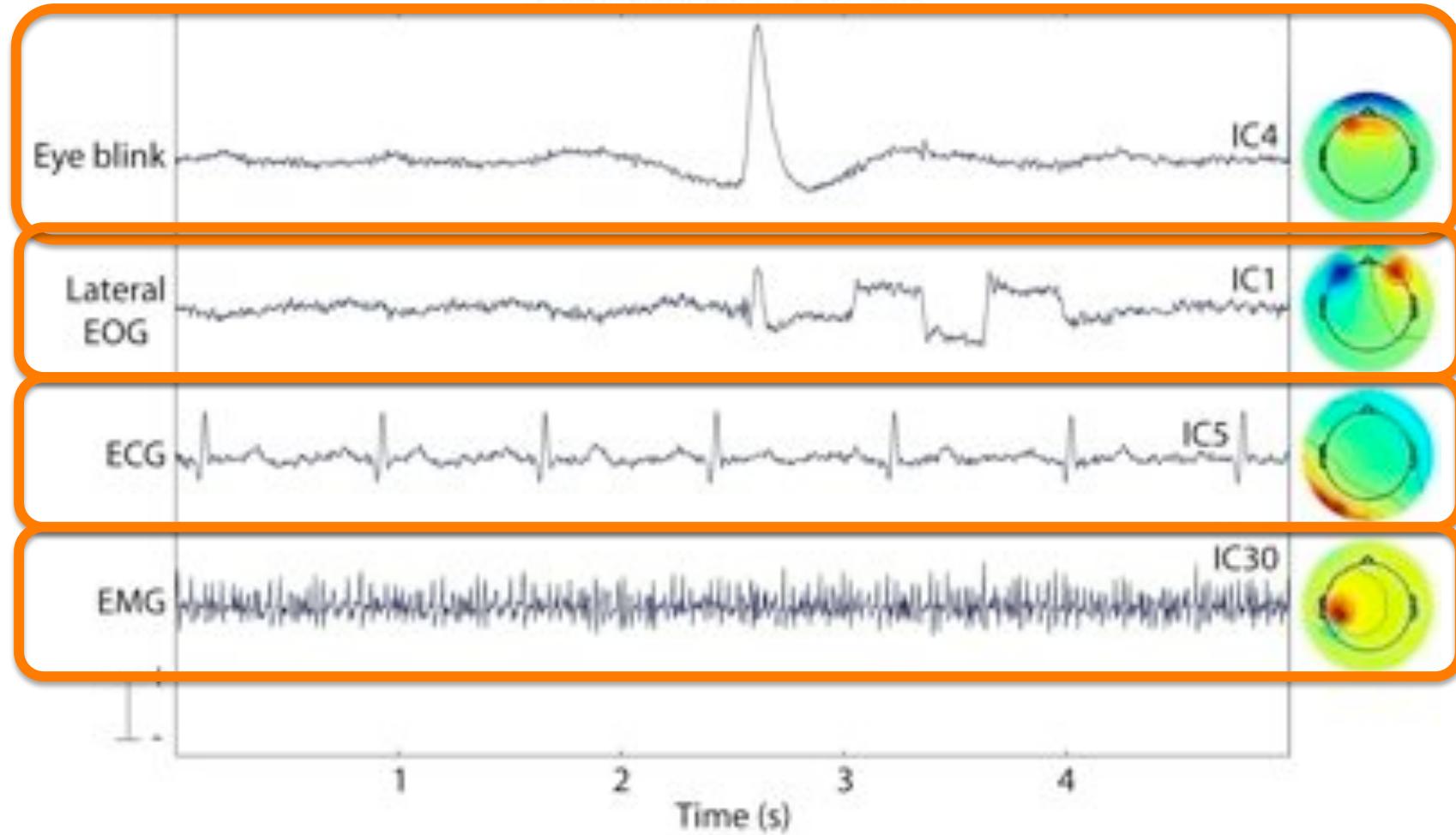
1

“ICA may be used to segregate obvious artificial EEG component (line and muscle noise, eye movements) from other sources.”

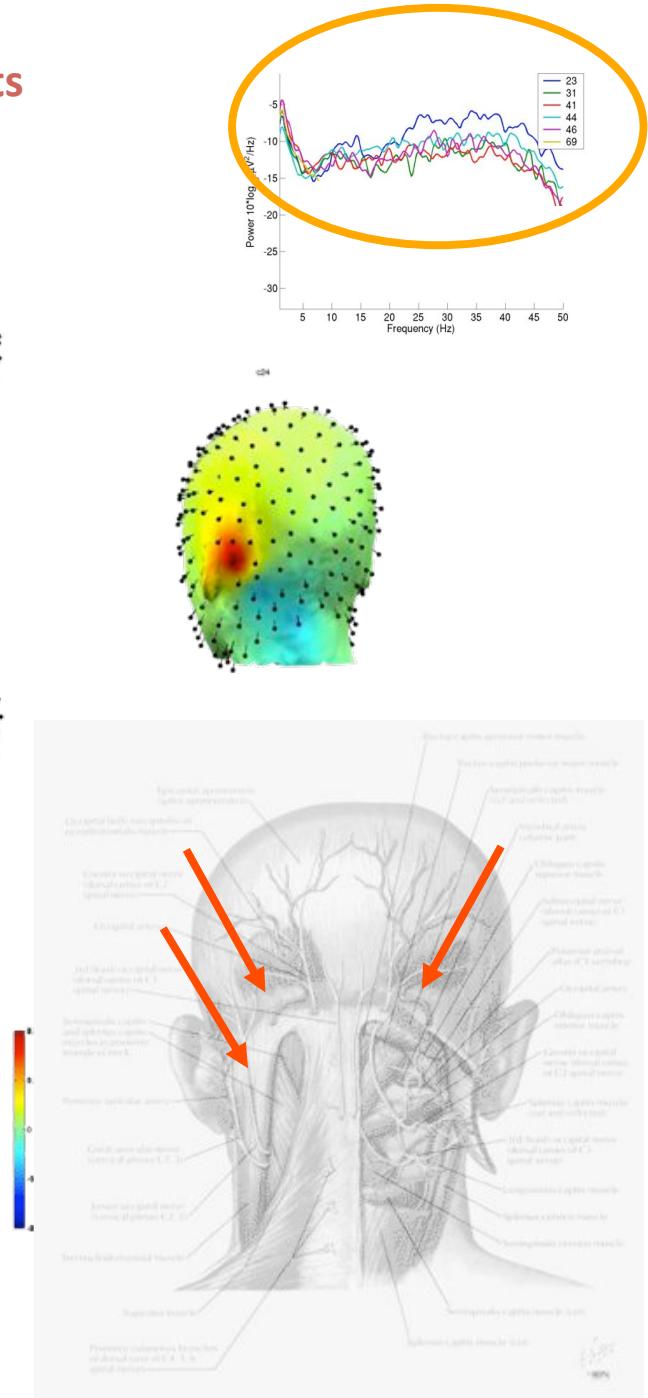
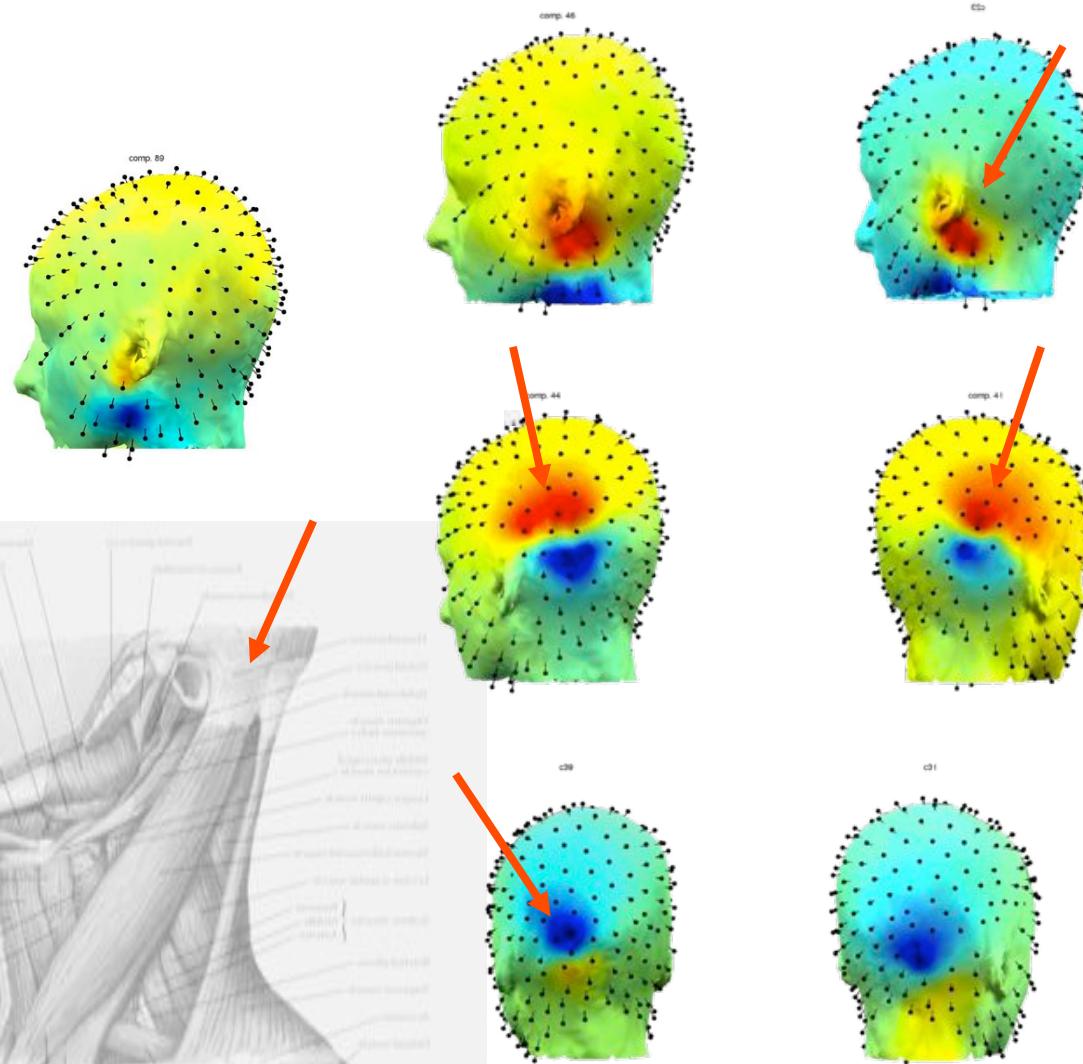
- Makeig et al., 1996



IC activation time courses



Independent muscle components



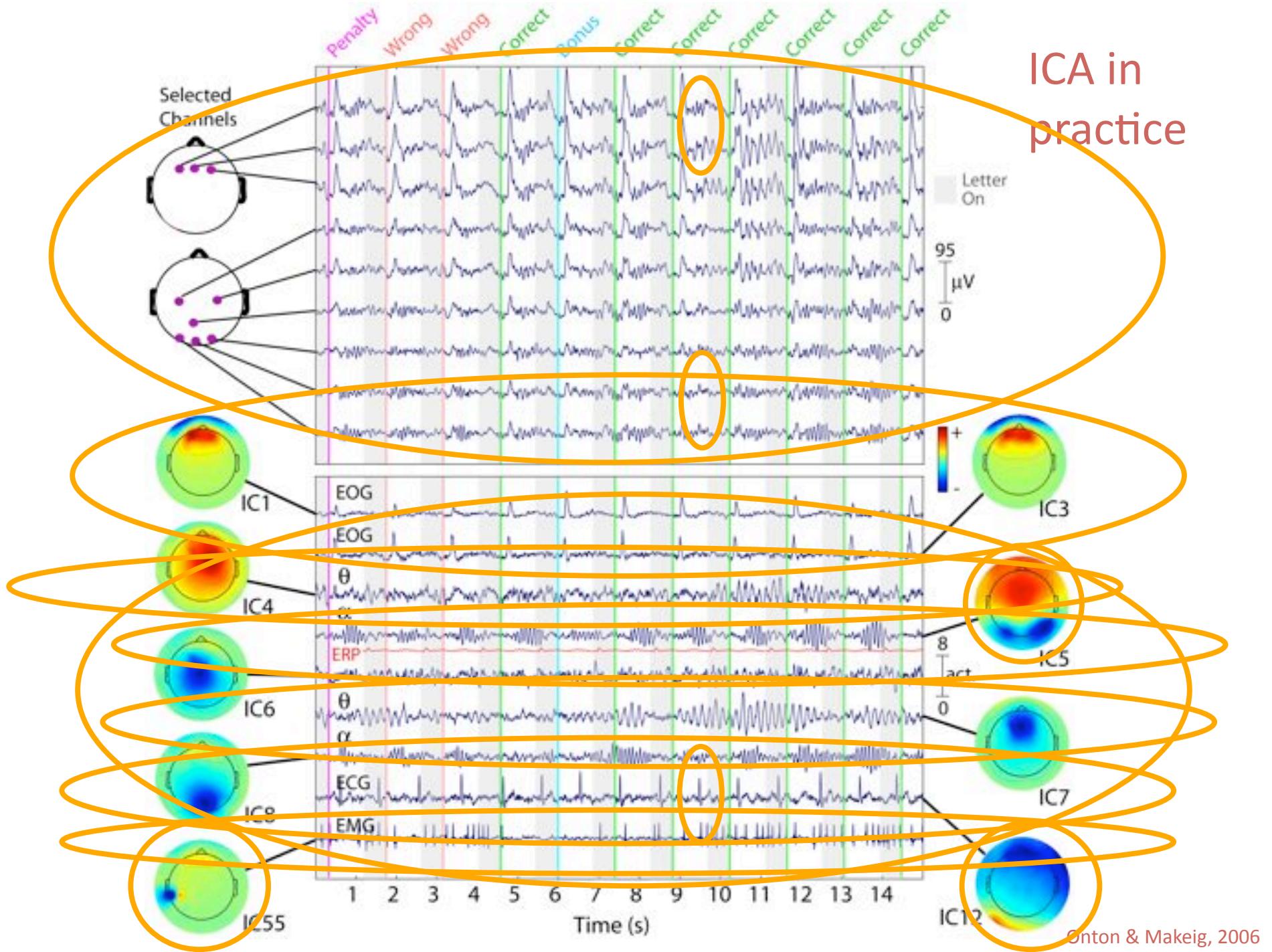
S. Makeig, 2005

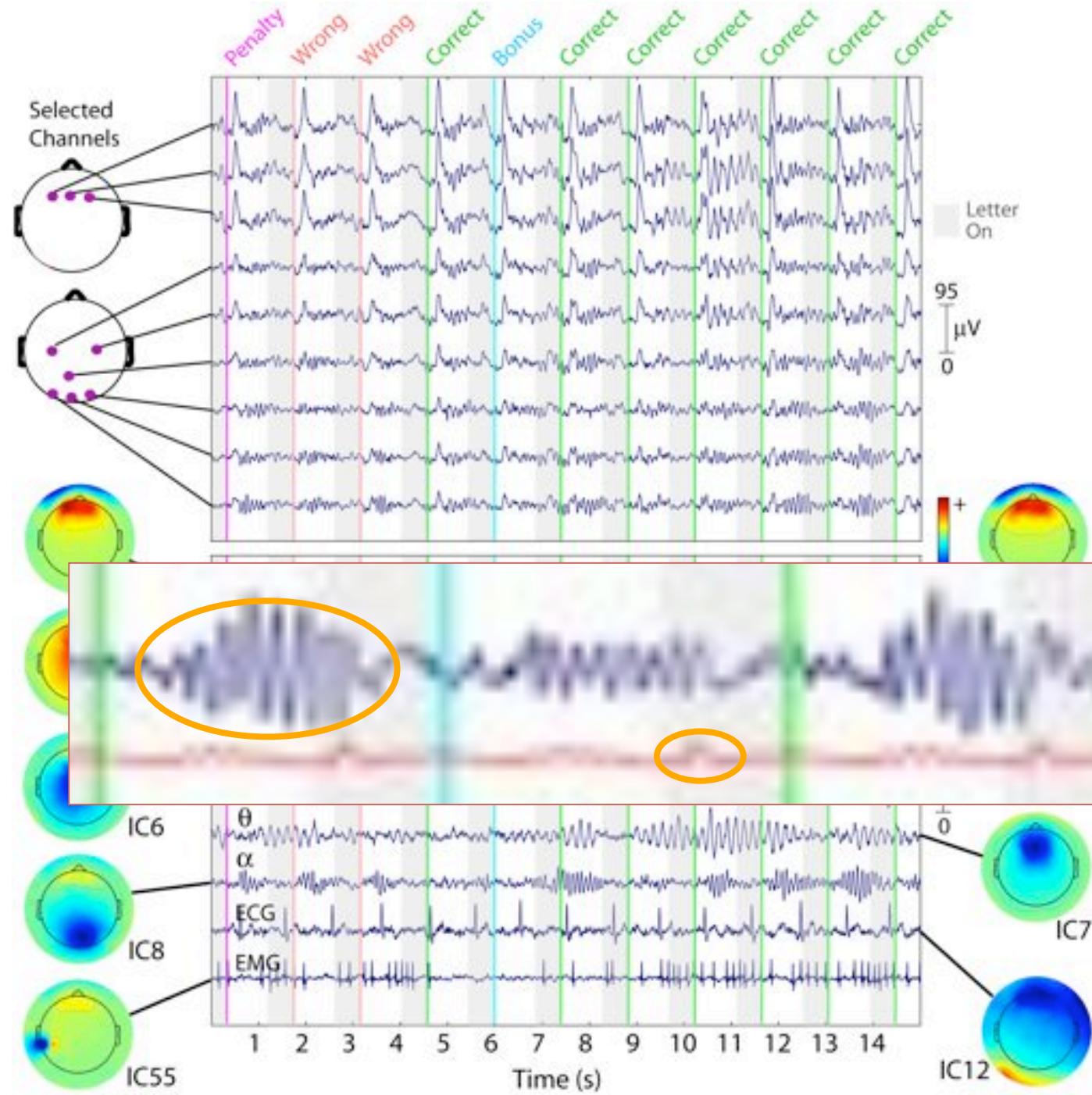
2

“ICA is capable of isolating overlapping EEG phenomena including alpha and theta bursts and spatially separable ERP components, to separate [ICs].”

- Makeig et al., 1996

ICA in practice





Onton, Makeig (2006)

3

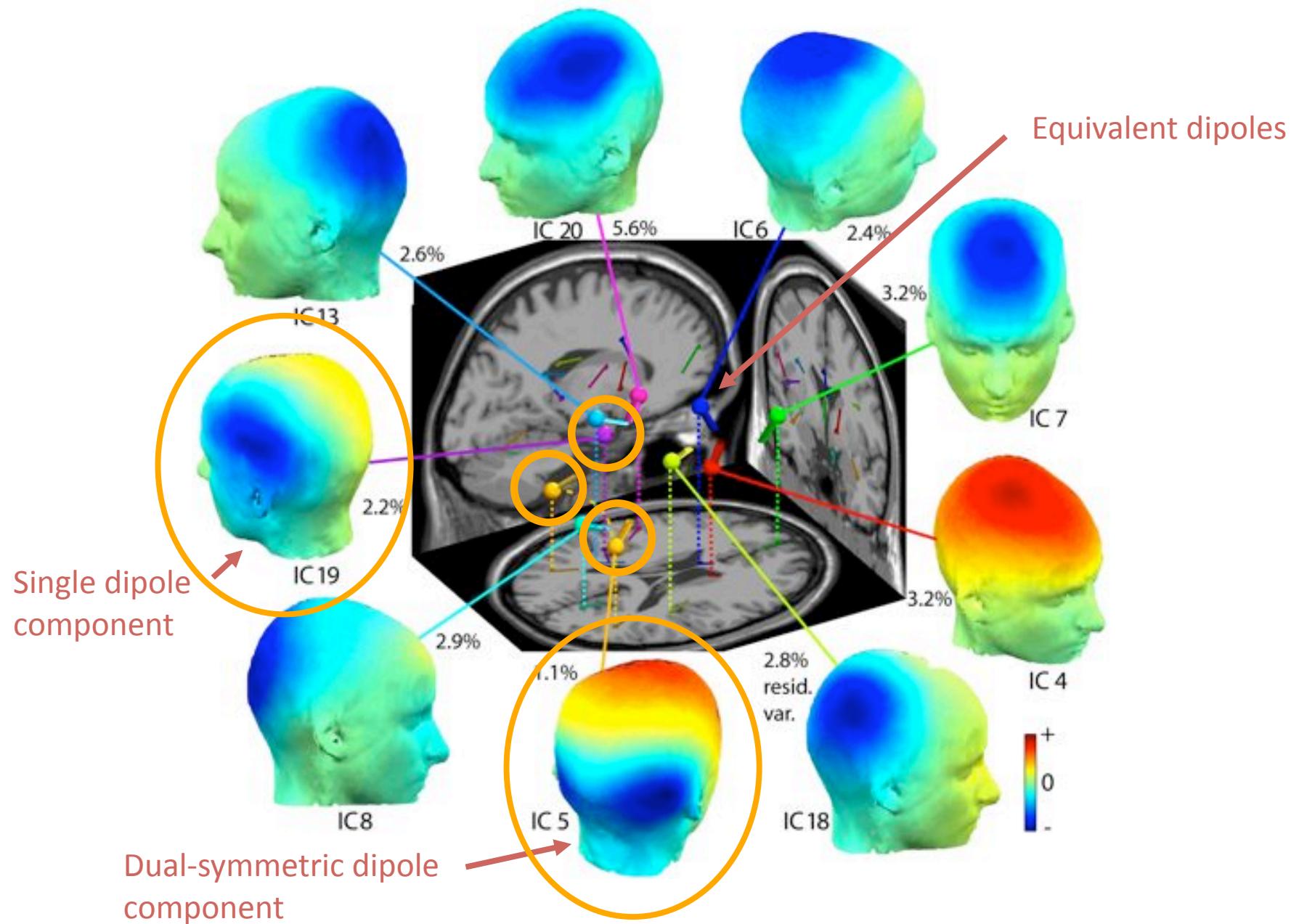
“ICA training is insensitive to
different random seeds,”
... and can separate out
independent components of
data with hundreds of channels.

- Makeig et al., 1996

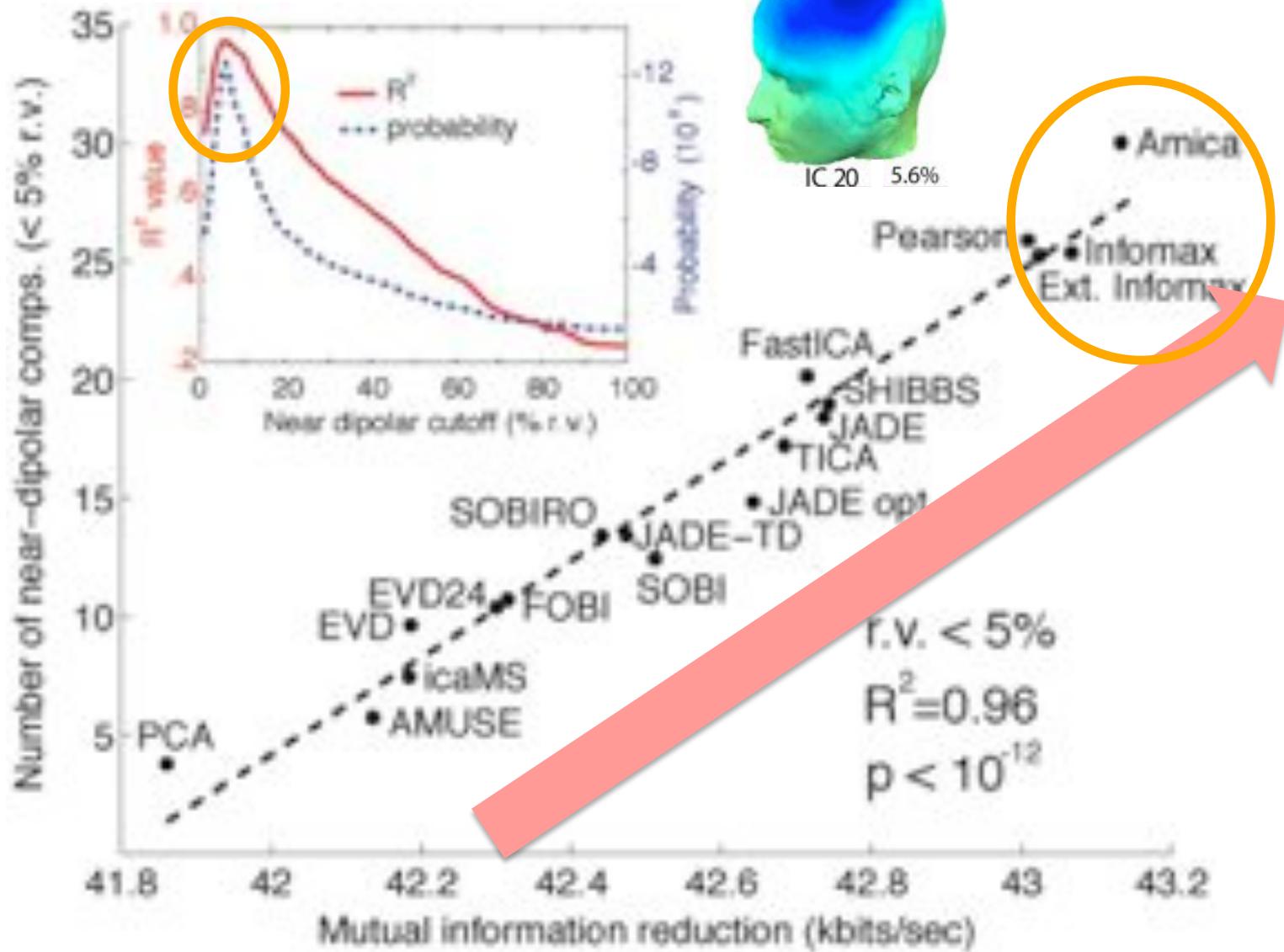
4

Brain-based, ‘dipolar’
independent components of
EEG data are projections of
single (dual) cortical patches.

Independent cortical components



Julie Onton & S. Makeig (2006)

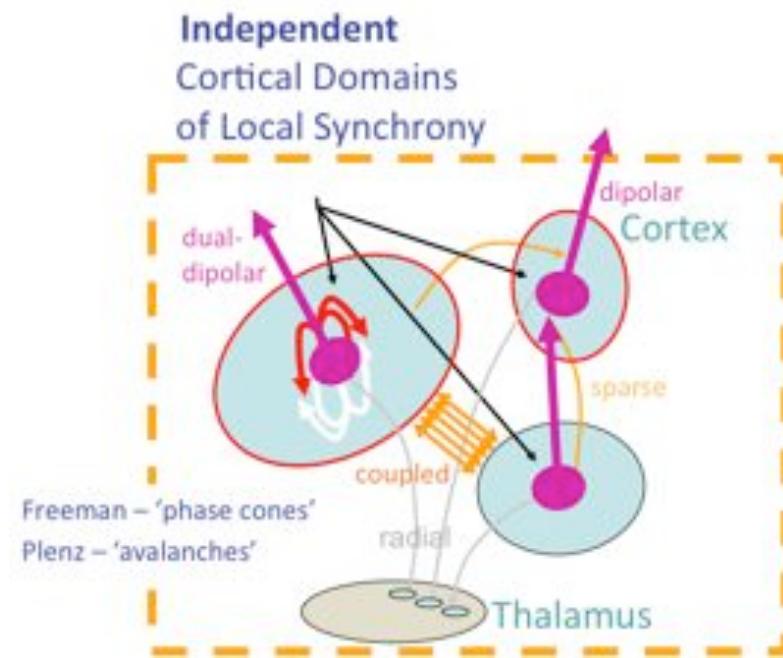


THUS → ICA (BSS) decompositions that
find components whose time courses are **more**
independent
→ also find **more** components whose scalp maps
are '**dipolar**'!

Thus, the two approaches to
constraining the EEG inverse problem,
biophysical and ***statistical***,
are directly interlinked.

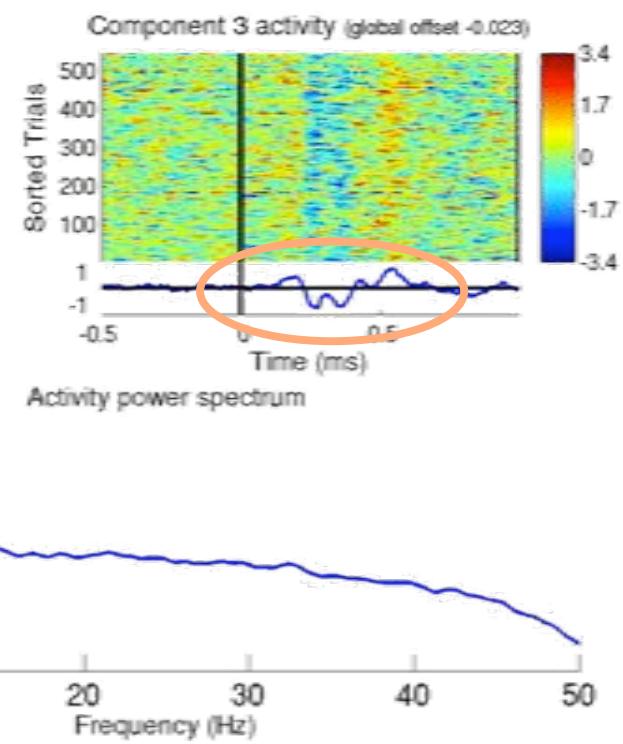
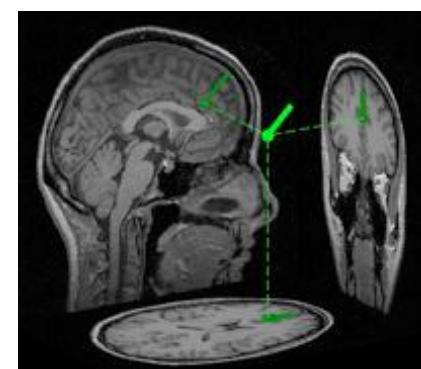
Why?

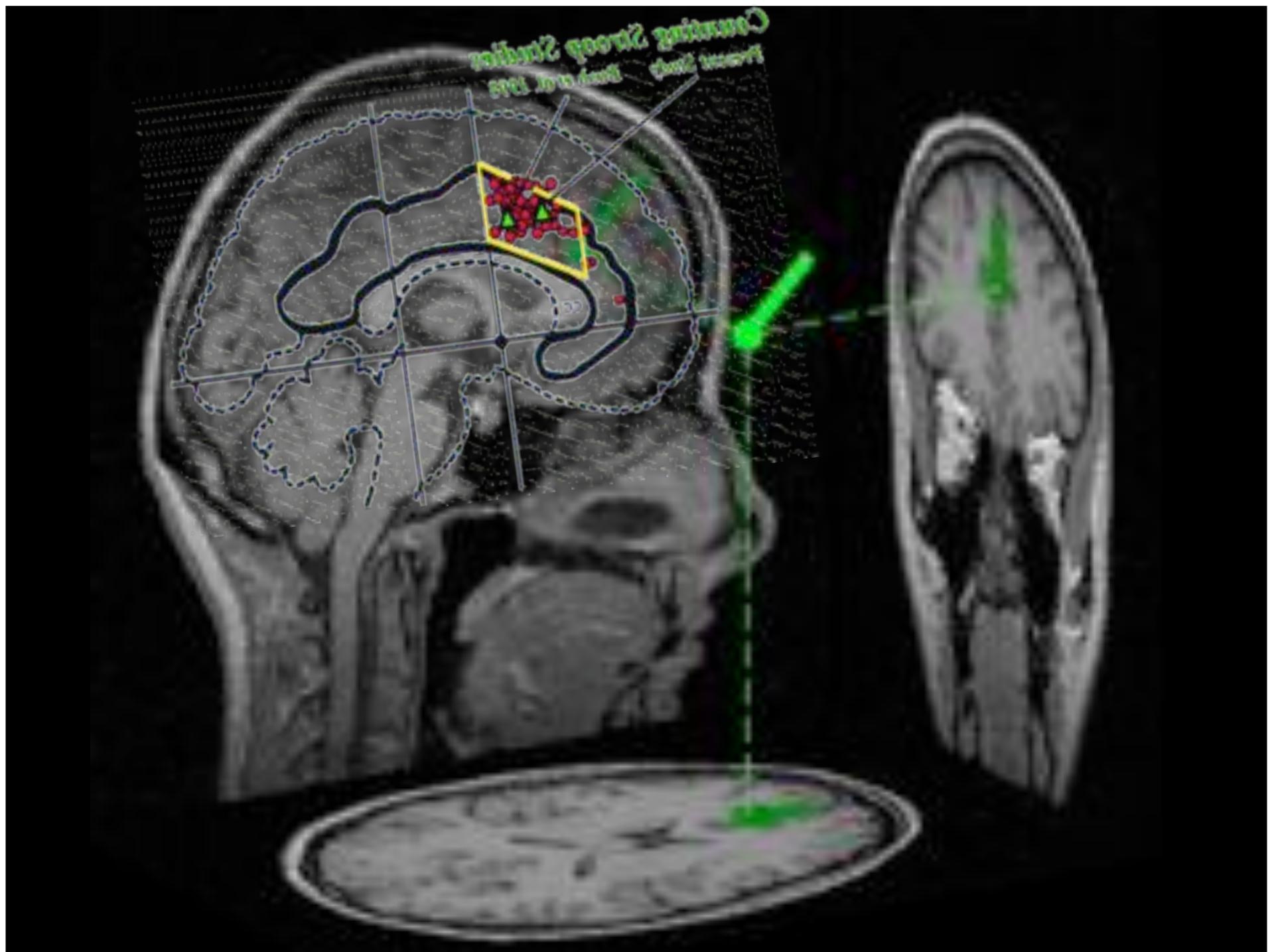
Very likely because the physiological assumptions motivating the use of ICA for EEG data are *substantially* correct...





Frontal Midline Theta Process

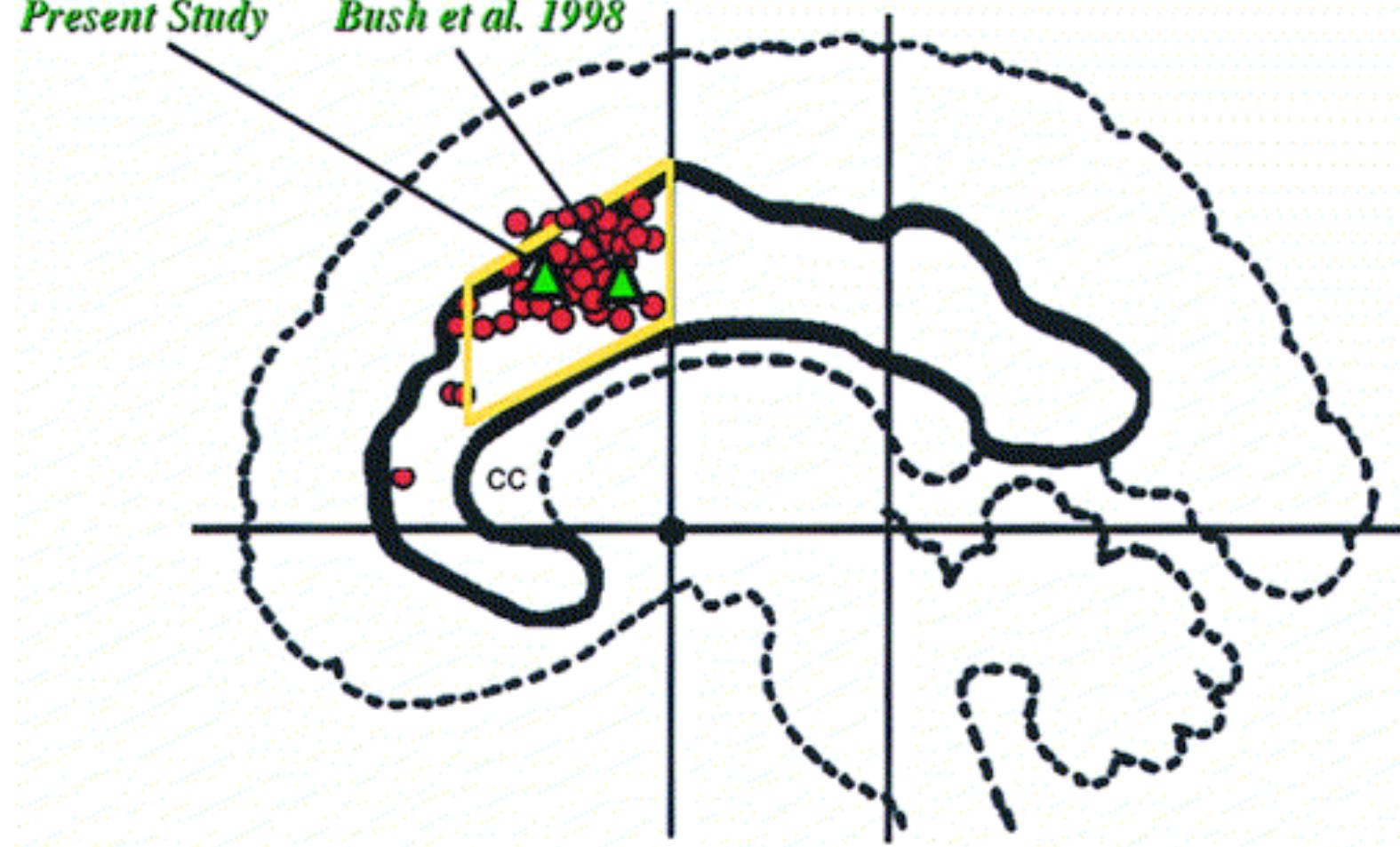




Anterior Cingulate Cognitive Division

Counting Stroop Studies

Present Study Bush et al. 1998

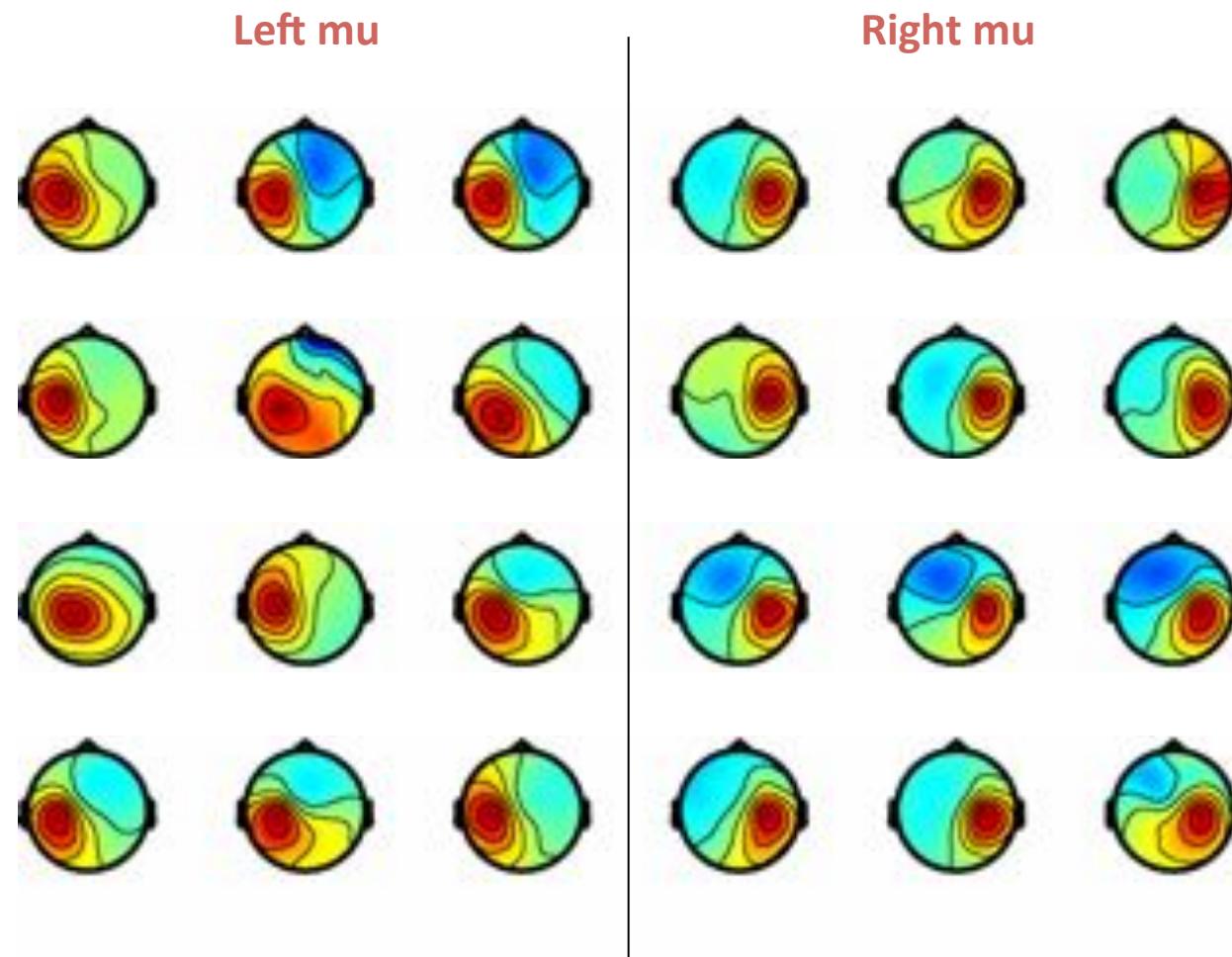


Bush et al., 1999

5

Similar independent components tend to
reappear in different subjects performing the
same task.

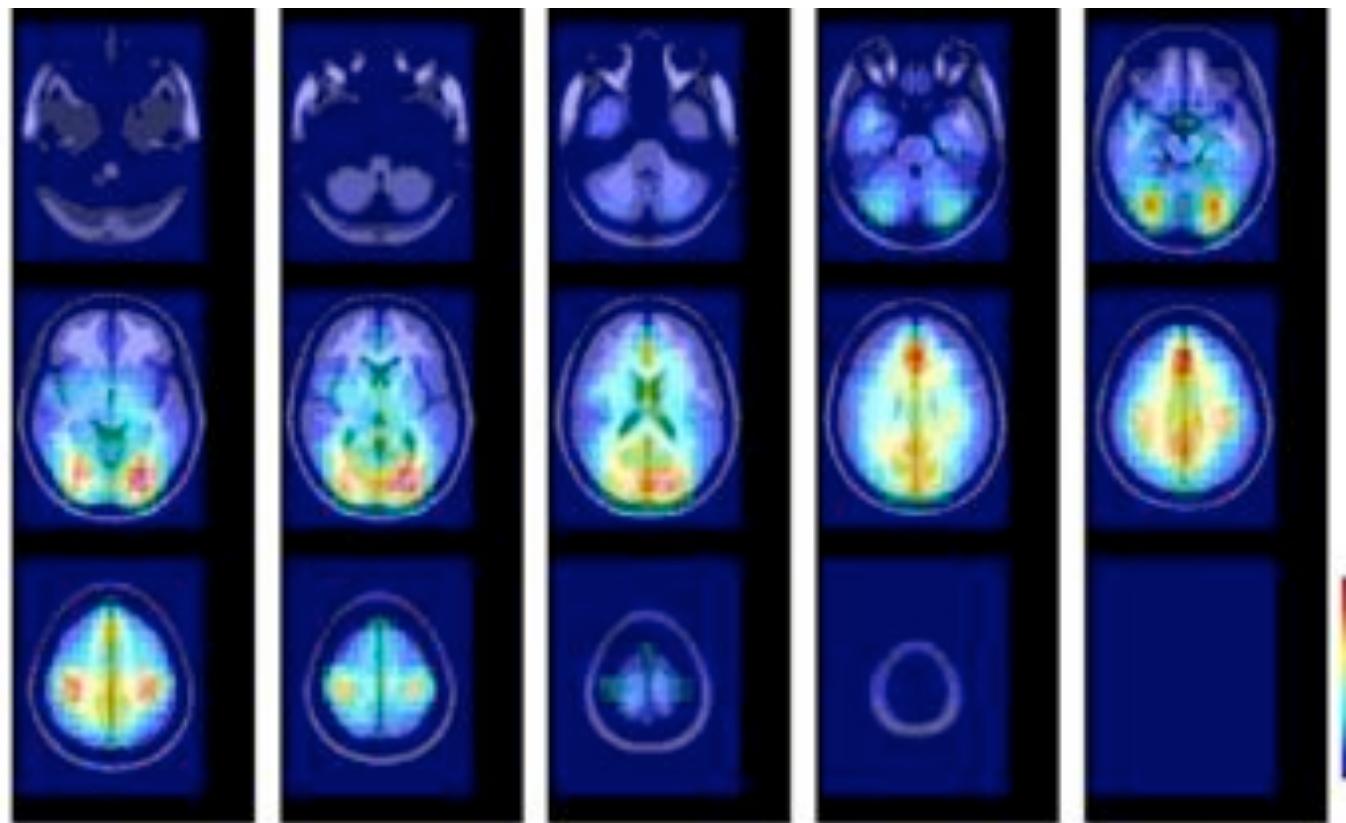
Clustering ICA components



Makeig et al., 2003

Equivalent dipole density

Visual Working Memory



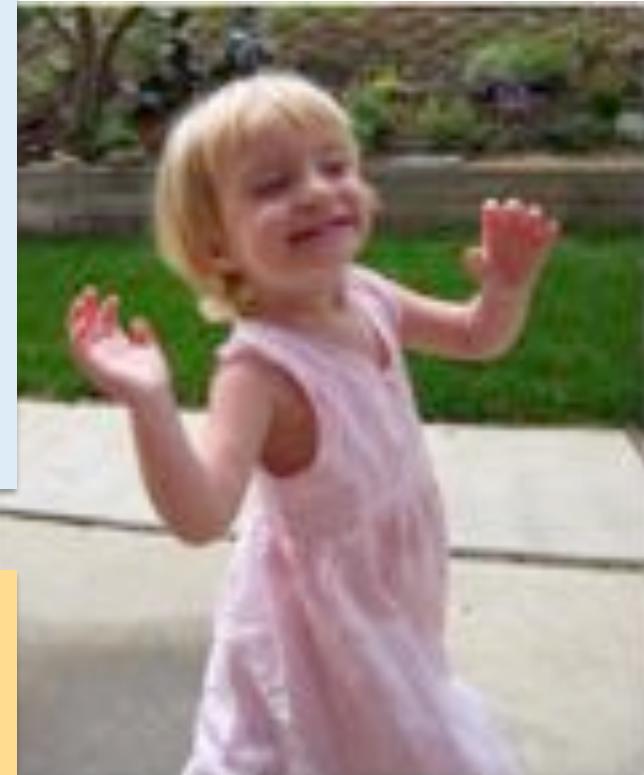
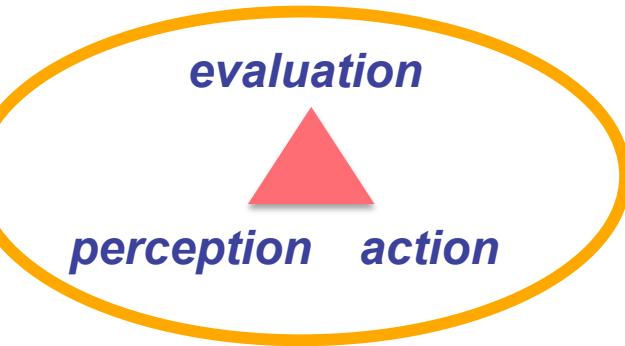
Sternberg
letter
memory
task

6

Independent components of EEG data tend to
be **functionally** independent –
changes in their activity patterns tend to reflect
‘top-down’ changes in cognitive state and/or
cognitive appraisal.

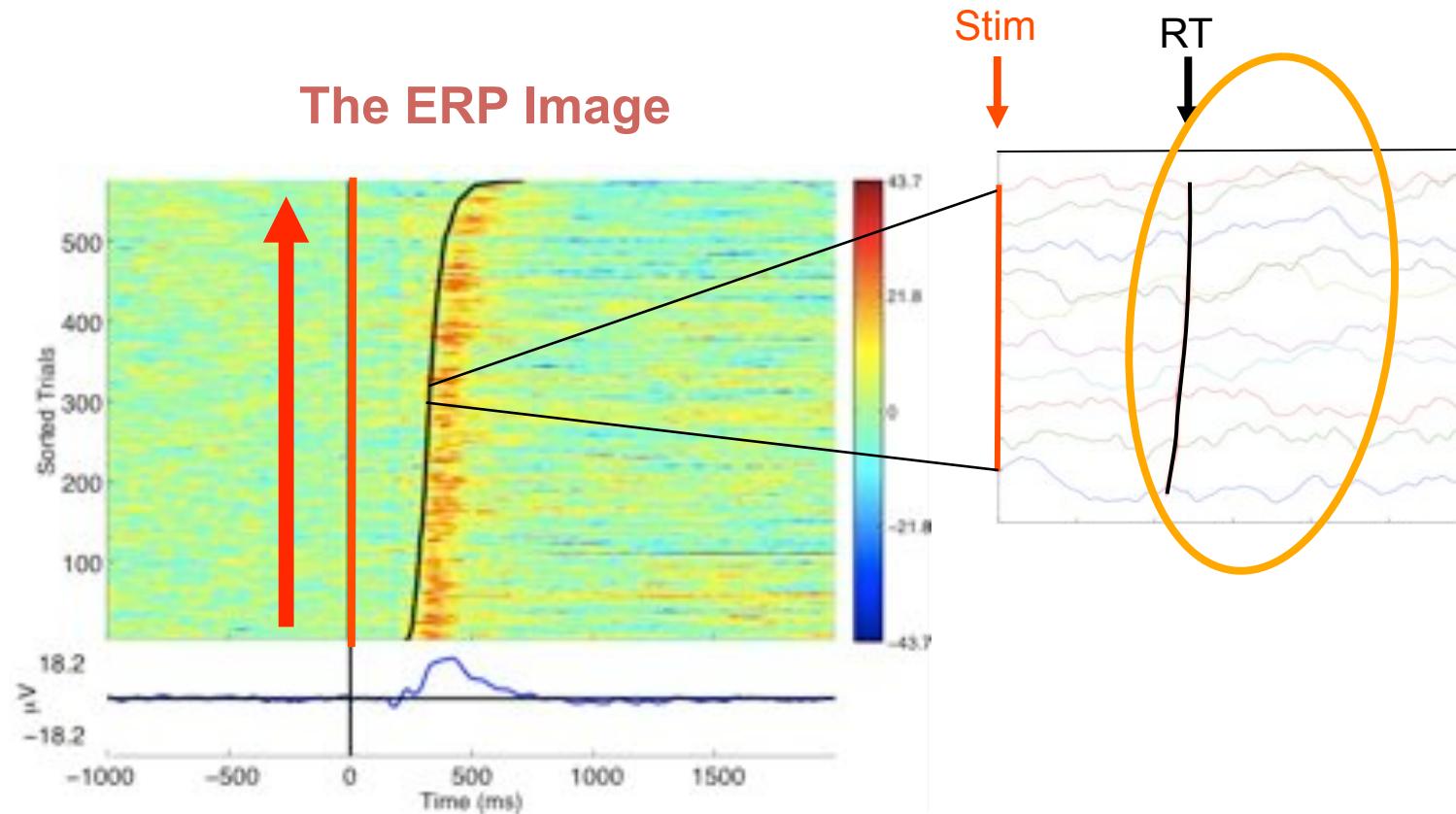
Embodied Cognition & Agency

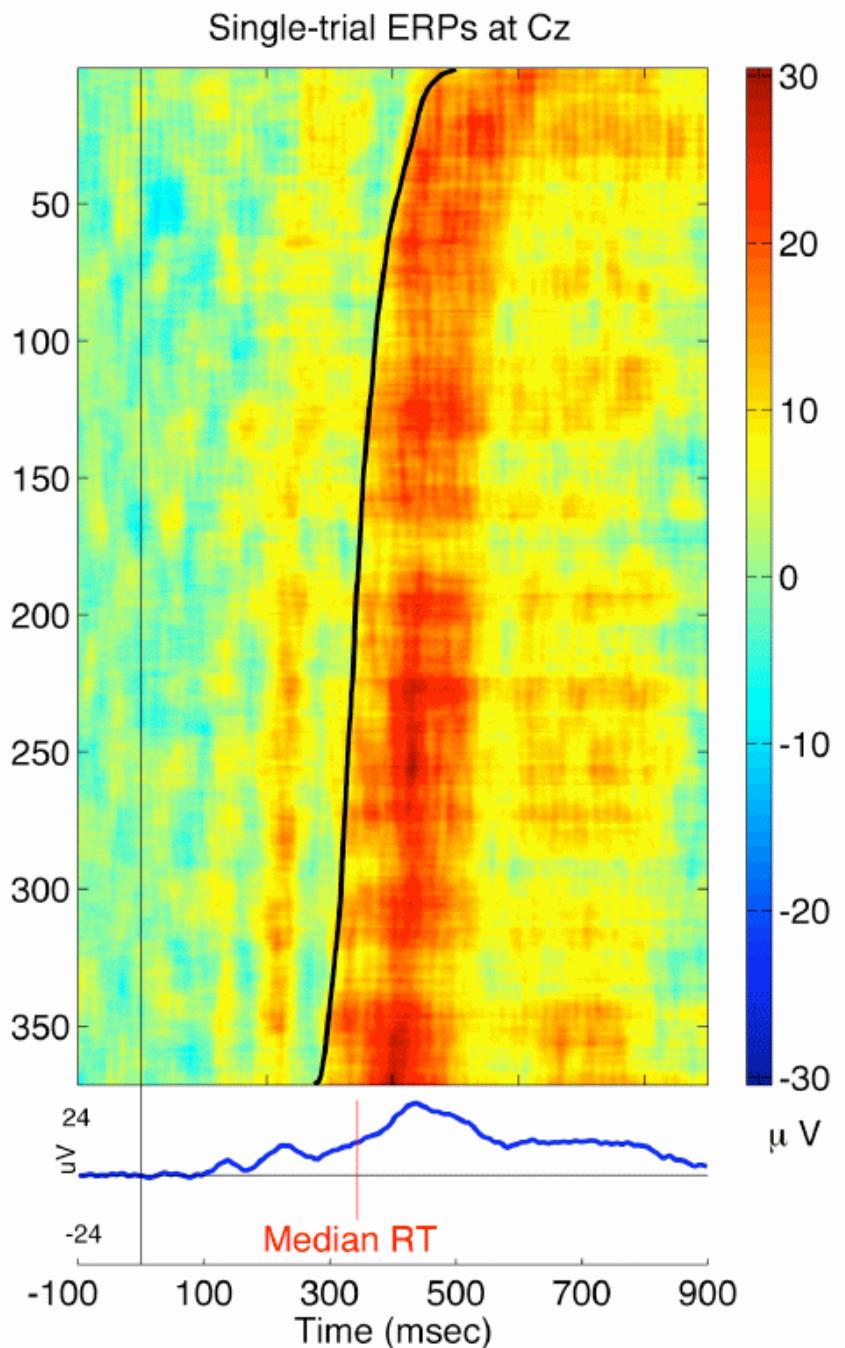
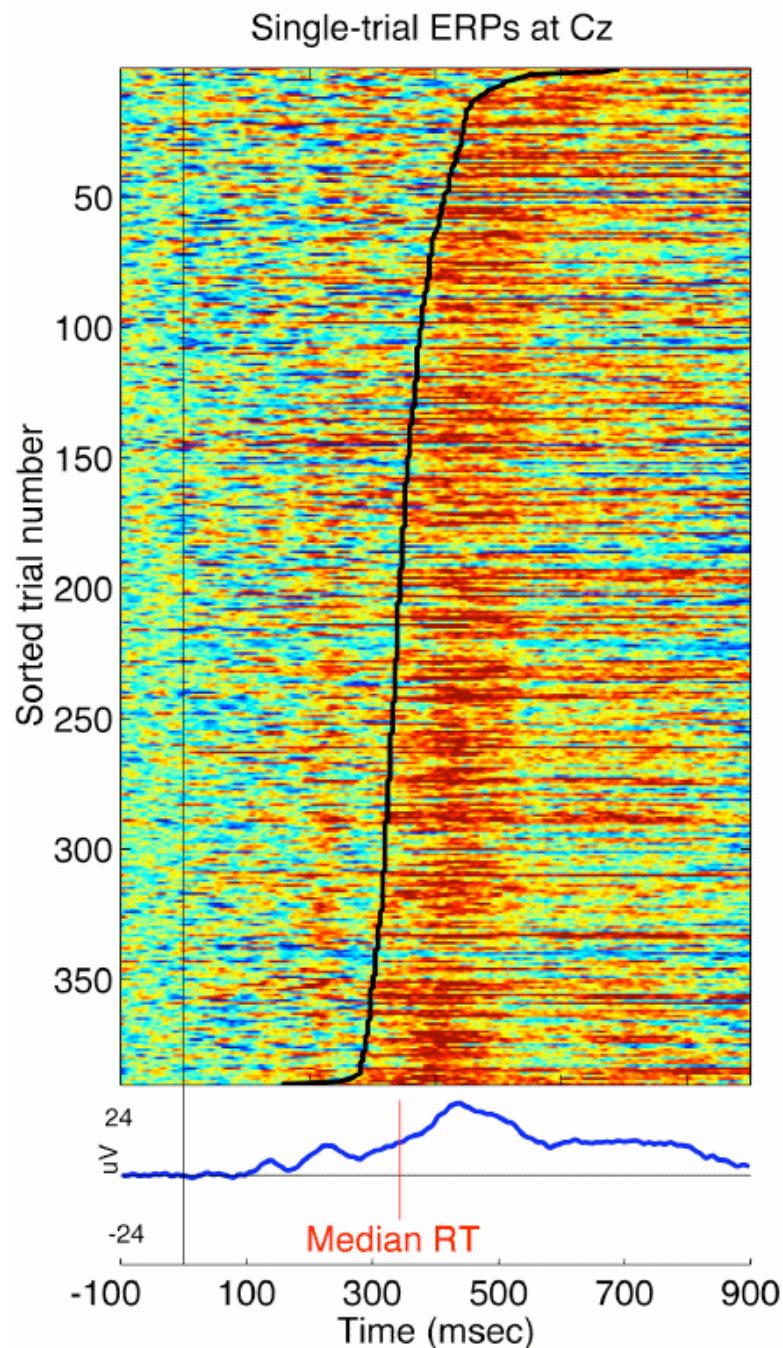
Brain processes
have evolved and function
*to optimize the outcome
of the behavior*
the brain organizes
in response to
*perceived challenges
and opportunities.*



**Brains meet the challenge of
the moment!**

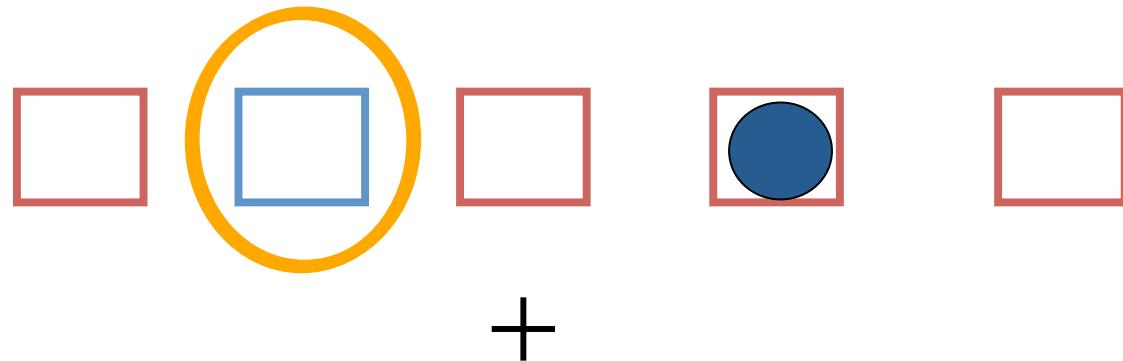
Collections of single trials, even at the source level, are regular, but in multiple ways – so they *appear* noisy!



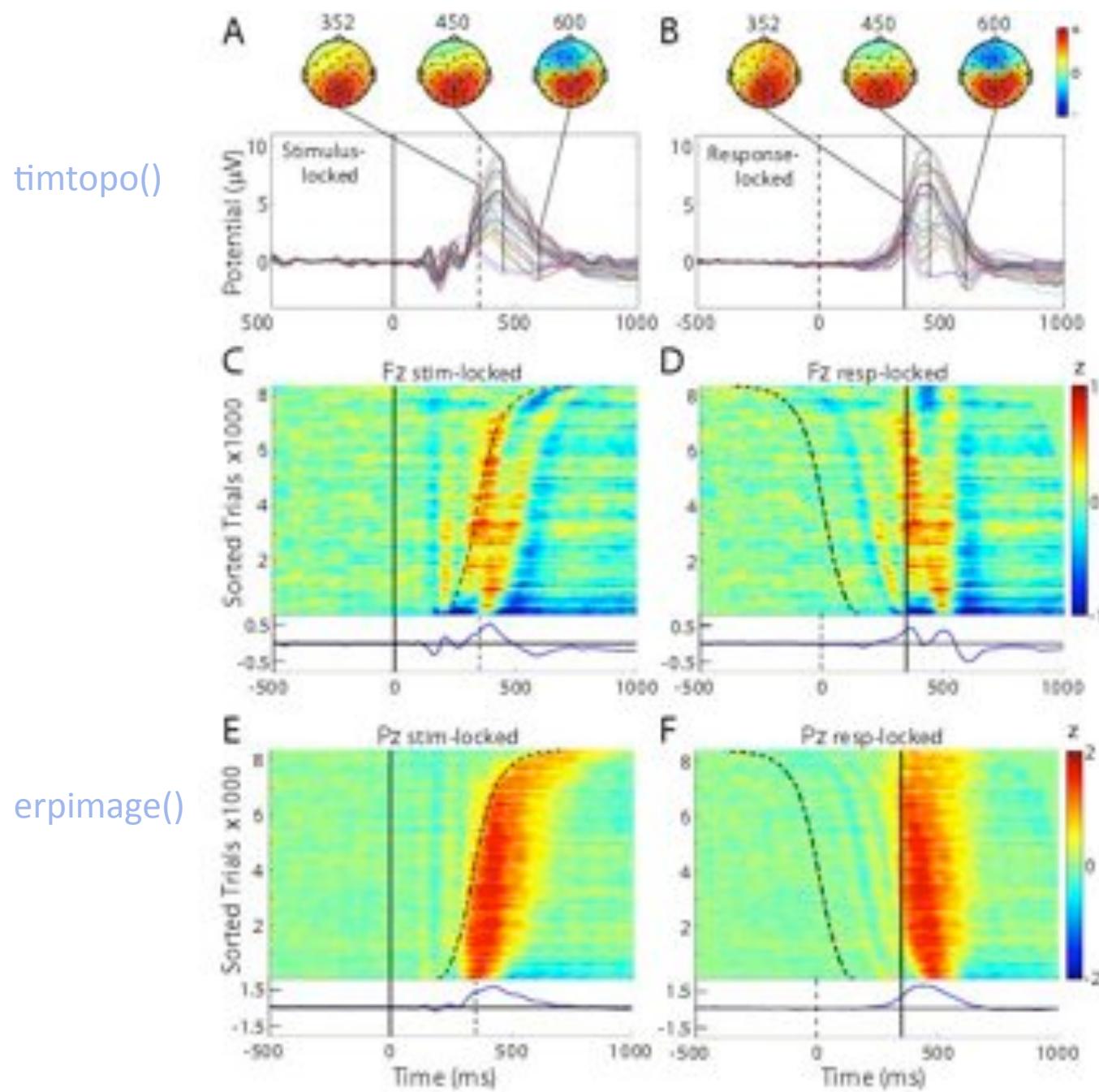


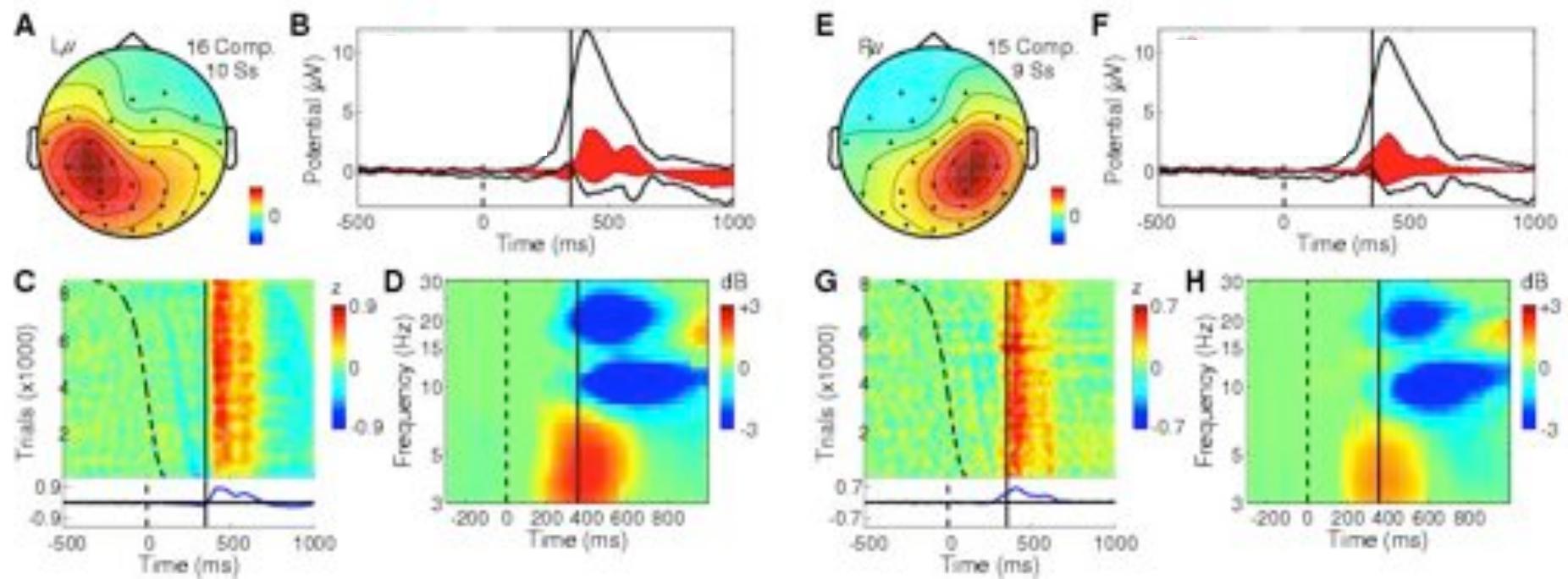
Jung et al., *Human Brain Mapping*, 2001.

Visual Selective Attention Task



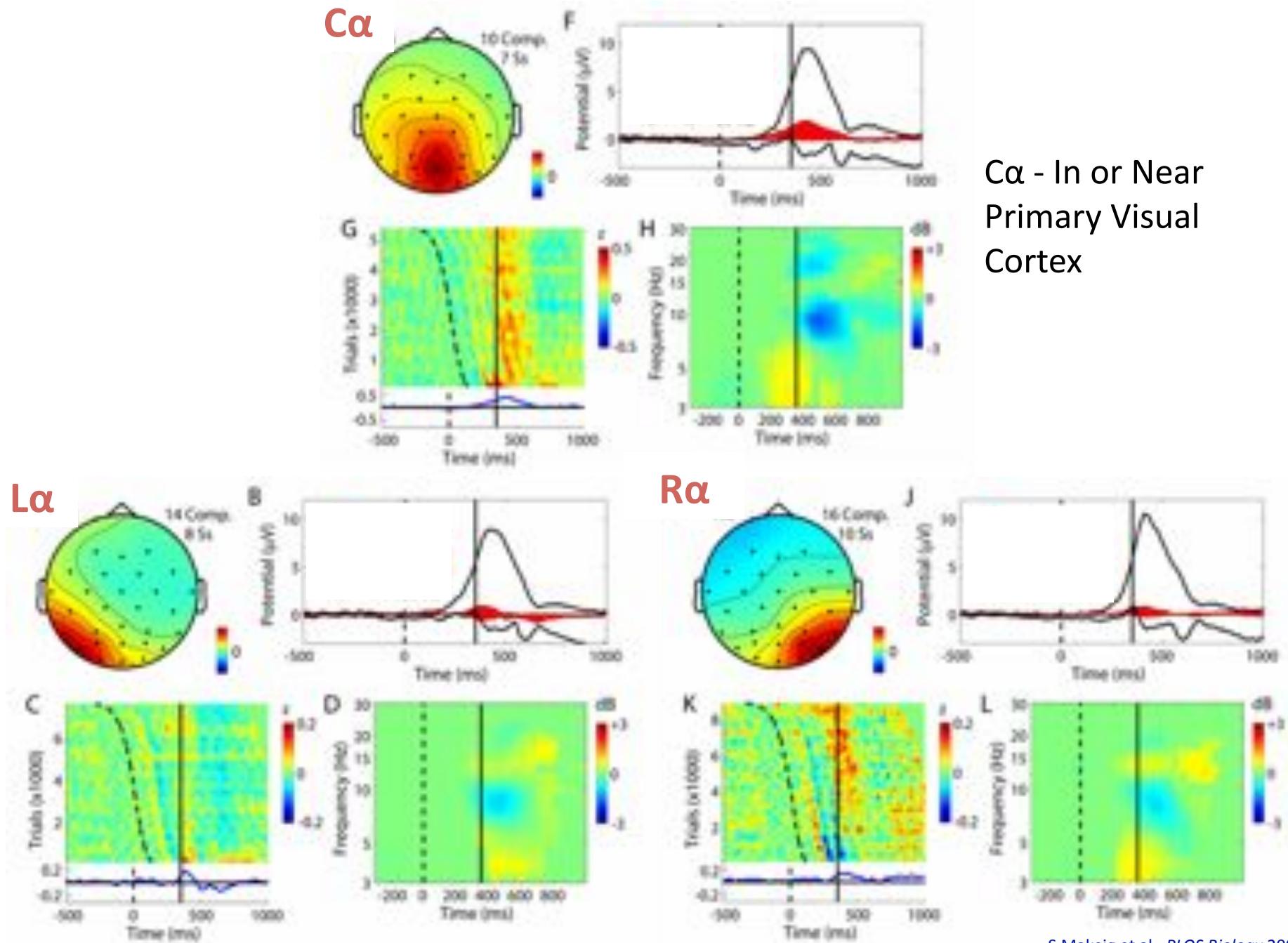
15 subjects



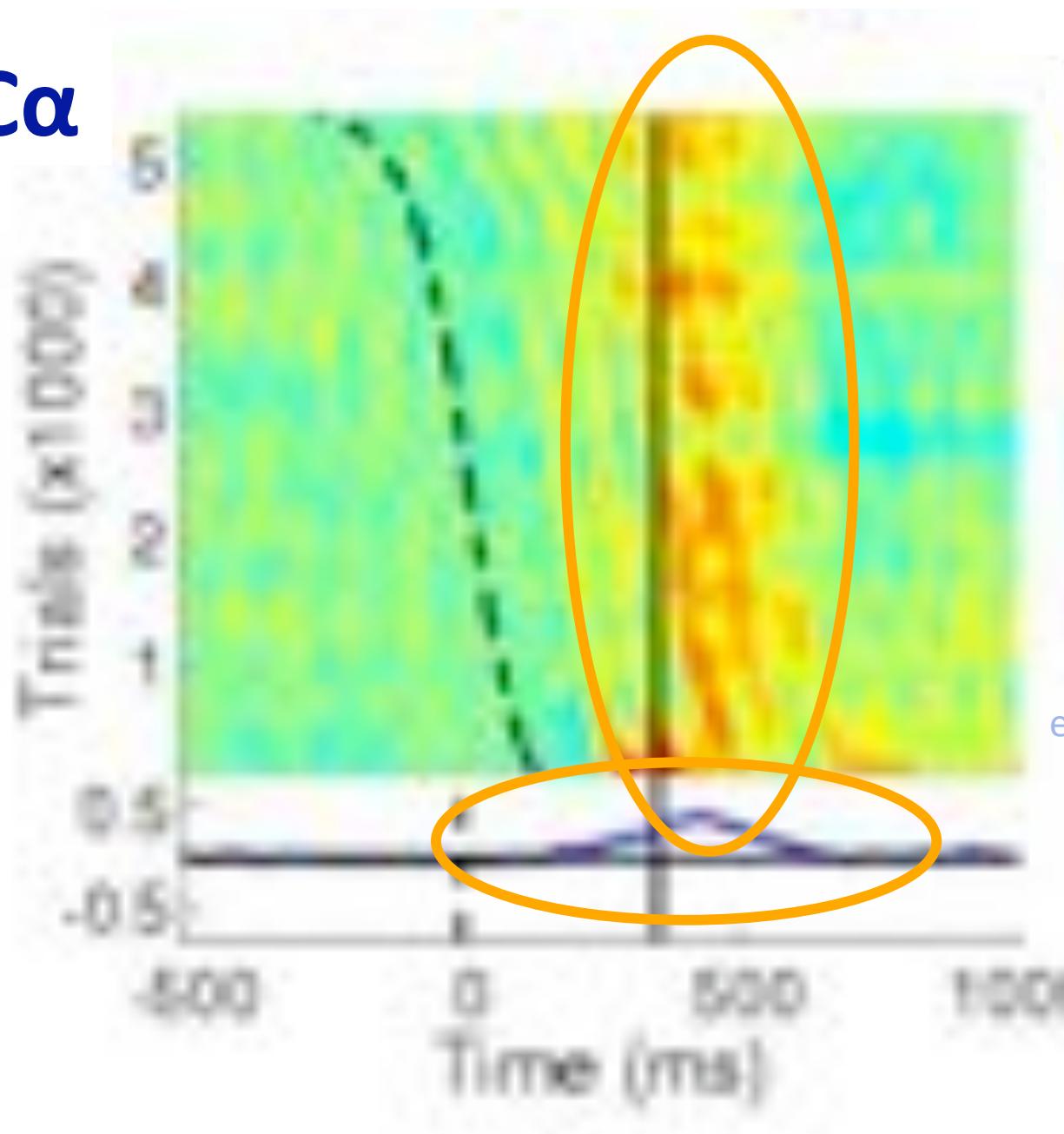


L μ - In or Near
Right Hand
Somatomotor
Cortex

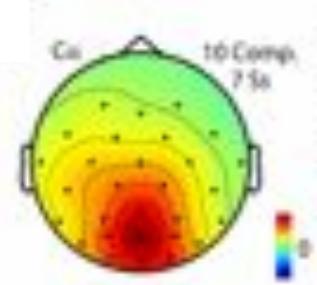
R μ - In or Near
Left Hand
Somatomotor
Cortex

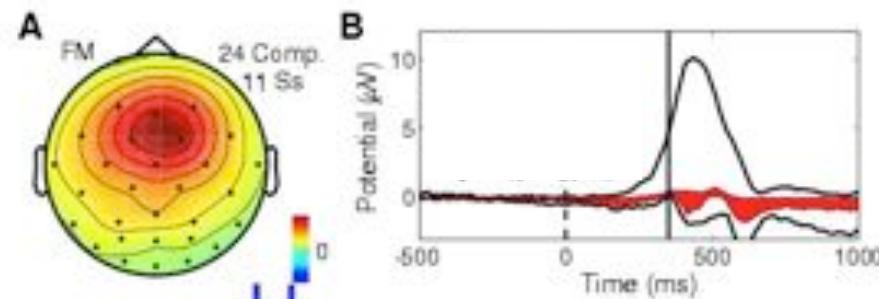


Ca

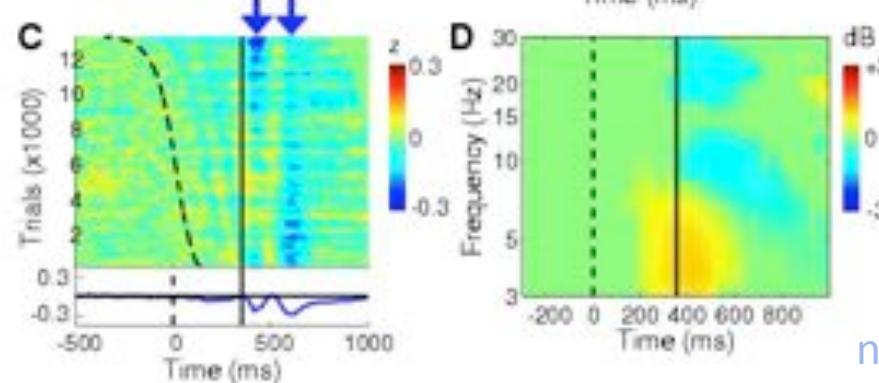


erpimage()



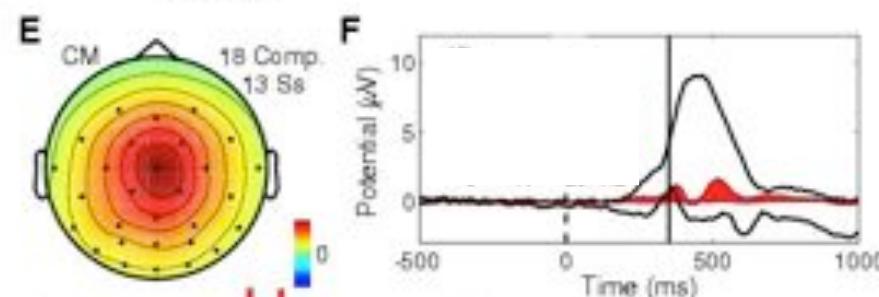


`envtopo()`
`std_envtopo()`

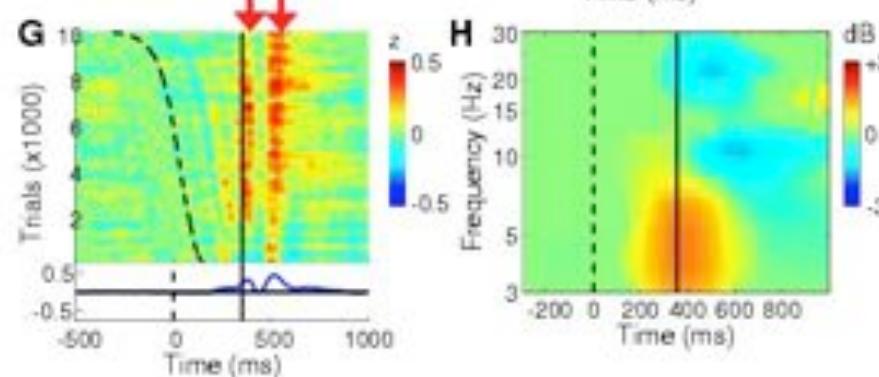


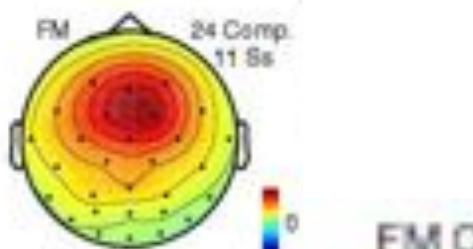
FM - In or Near
Rostral
Cingulate
Zone
(dACC)

`newtimef()`

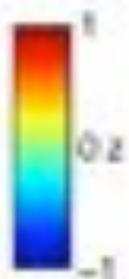
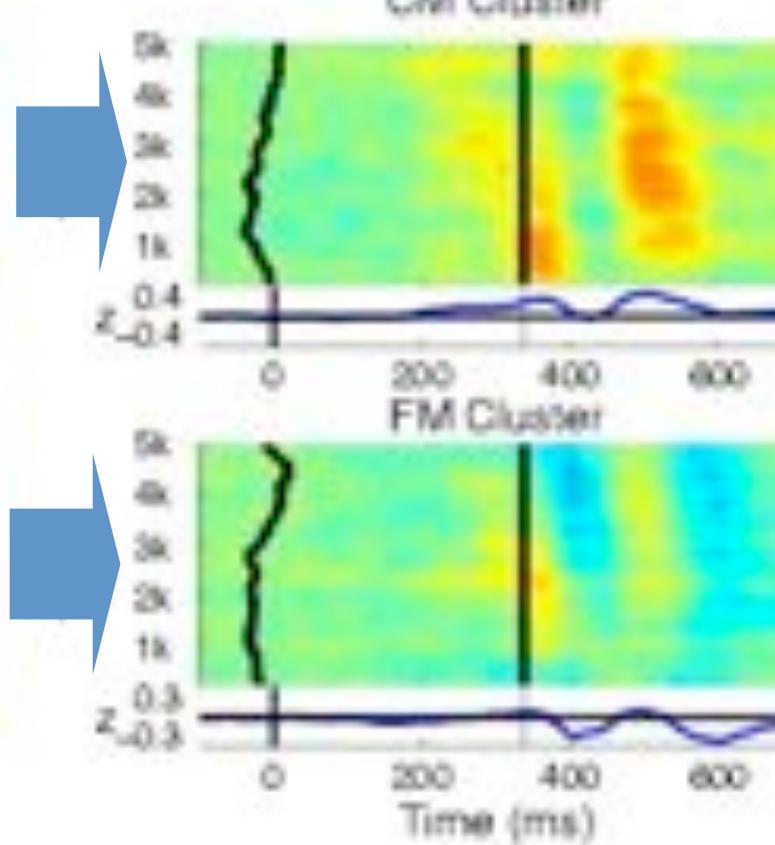
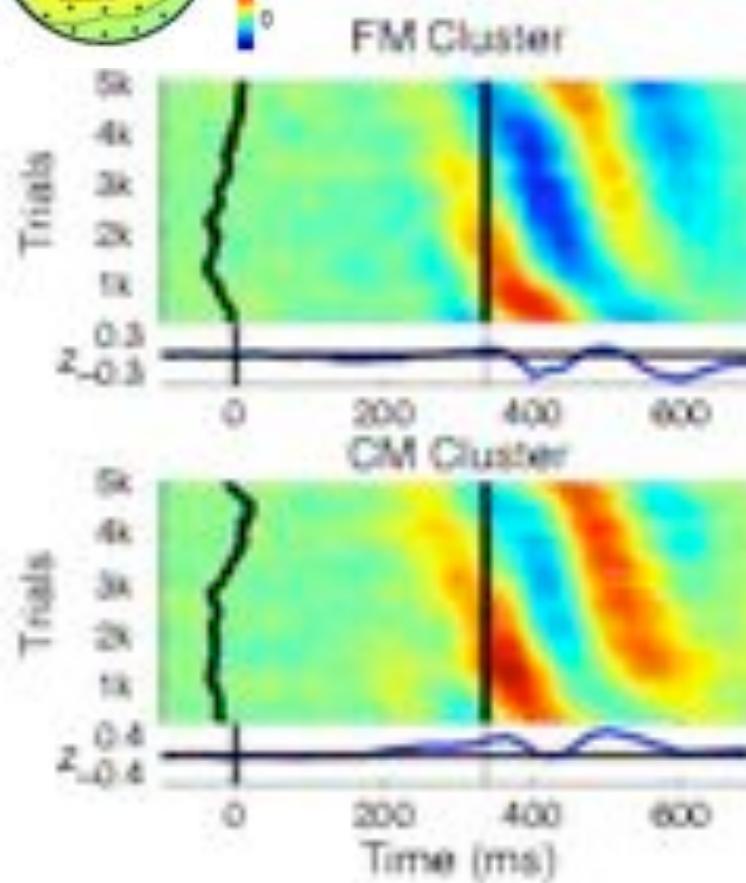
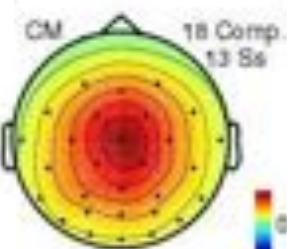


CM - In or Near
Motor Cingulate
/ Supplementary
Motor Cortex

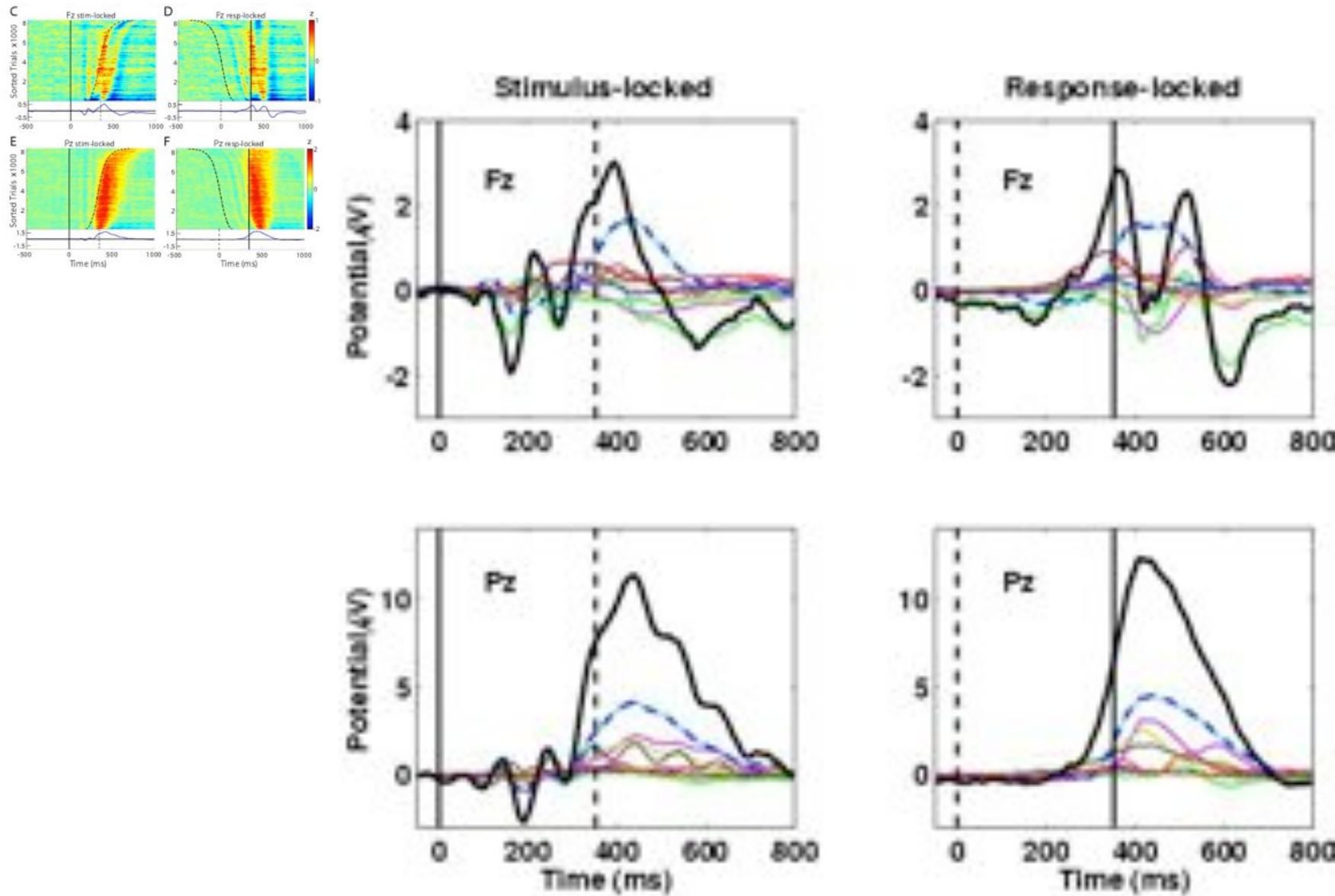




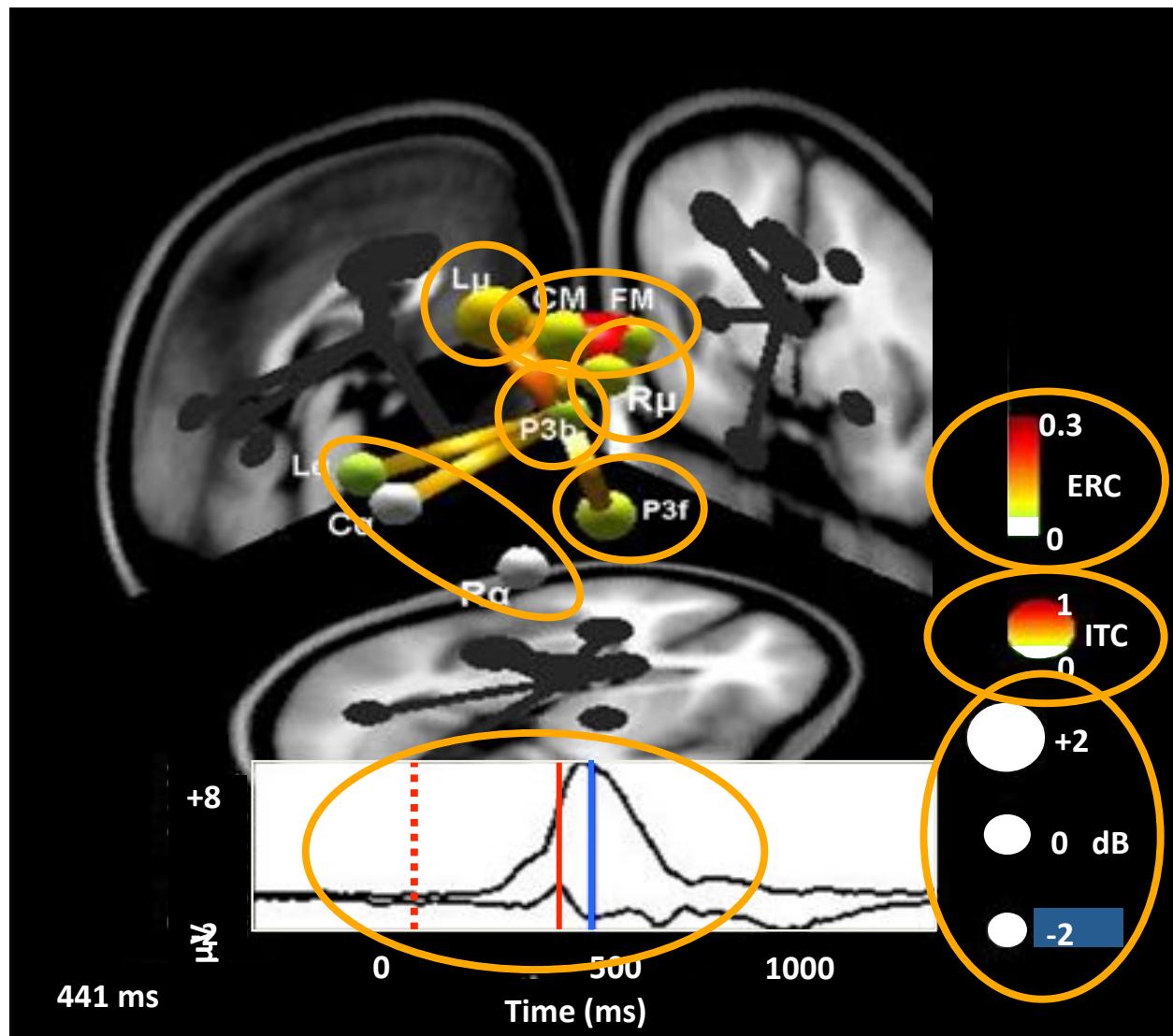
Partial Phase Coherence of FM and CM Clusters



Complex event-related dynamics sum to ‘the’ P300



ICA-modeled theta-band event-related dynamics accompanying the speeded manual target responses



brainmovie3d()

S Makeig et al., *PLOS Biology* 2004

