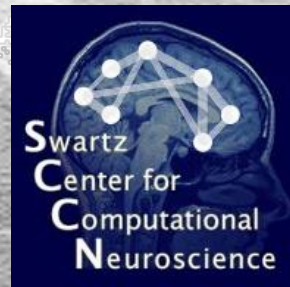


# Clustering Independent Components of EEG Data



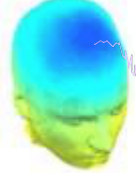
**Scott Makeig**

Institute for Neural Computation  
University of California San Diego

**25<sup>th</sup> EEGLAB Workshop**

Tokyo, Japan

September, 2017



# Why cluster independent components across subjects or sessions?



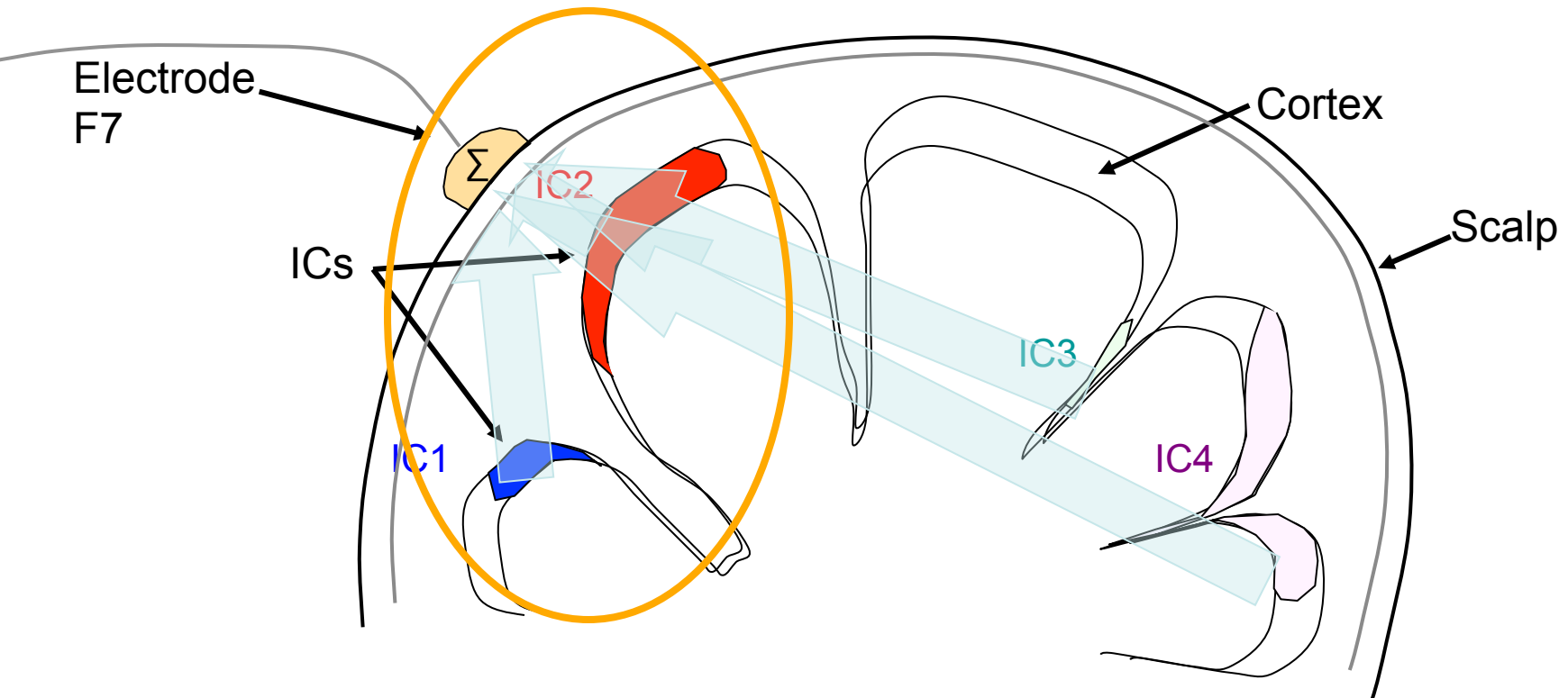
- ICA transforms the data from a channel basis (activity recorded at each channel)
  - to a component basis (activity computed at each IC).
- Normally, EEG researchers assume that, for example, electrode channel F7 == F7 == F7 ... in each subject – and then ‘cluster’ their data assuming channel equivalence.
- This amounts to the simple assumption

***“Your Cz is My Cz!”***

- But this is only ***roughly*** correct !



# Example: First Subject





# ICs

## Cortex

Scalp



IC1

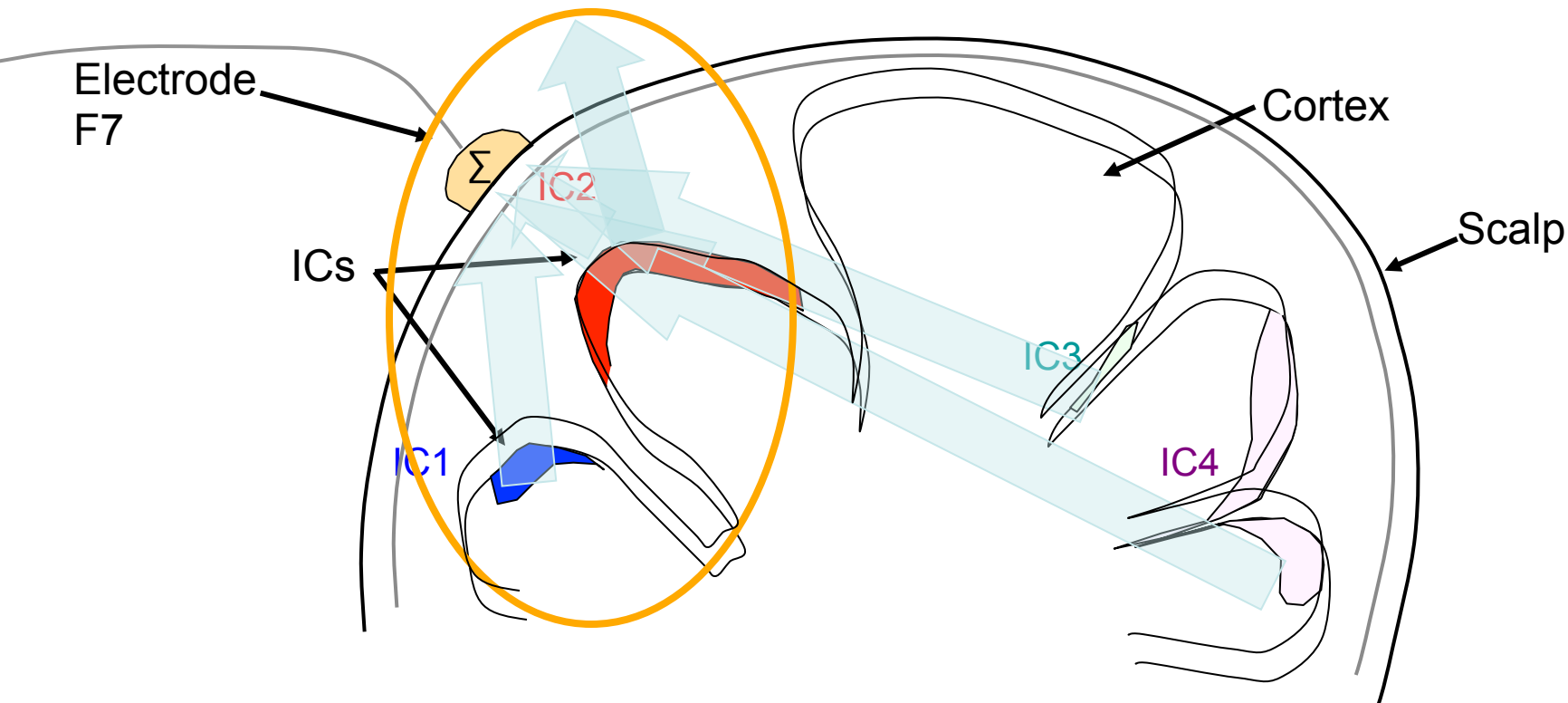
IC3

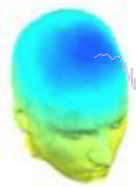
## IC4



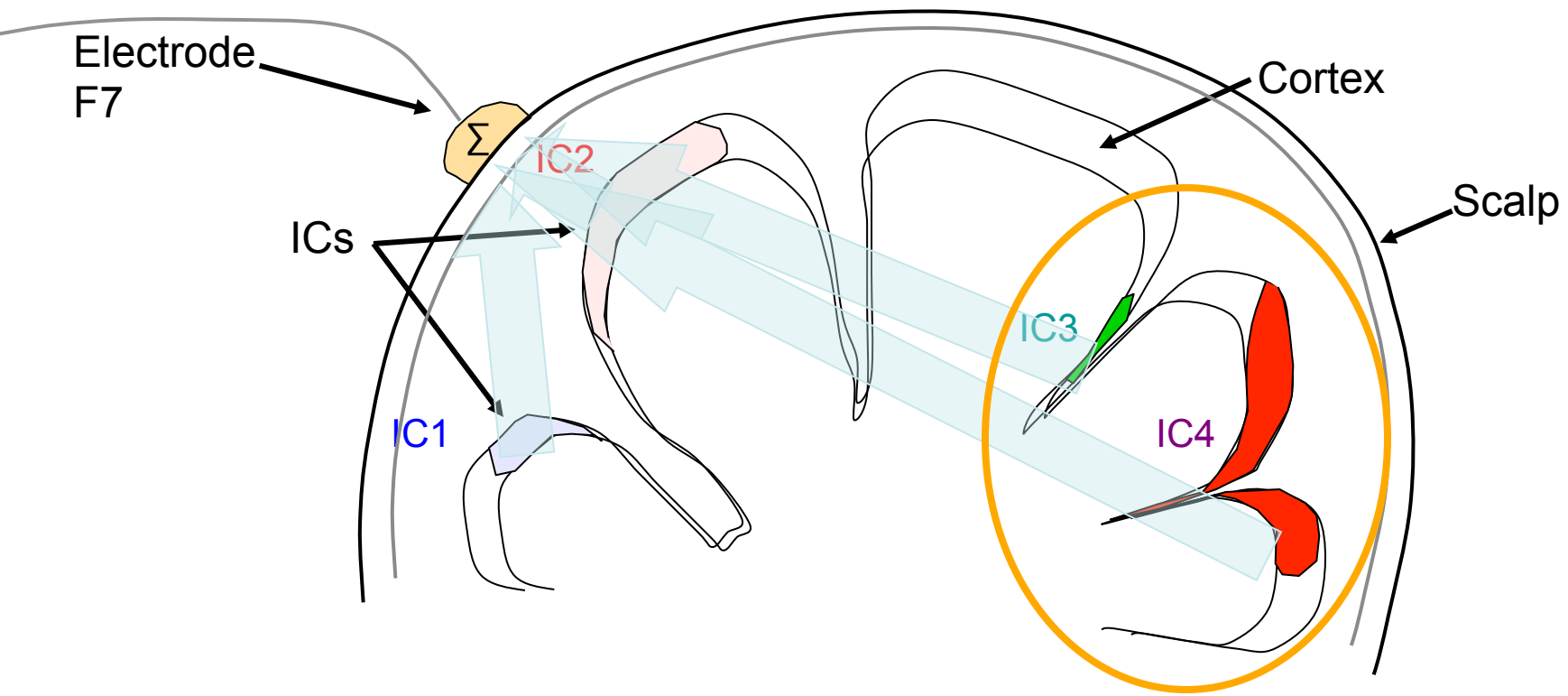


# Third Subject





# Fourth Subject

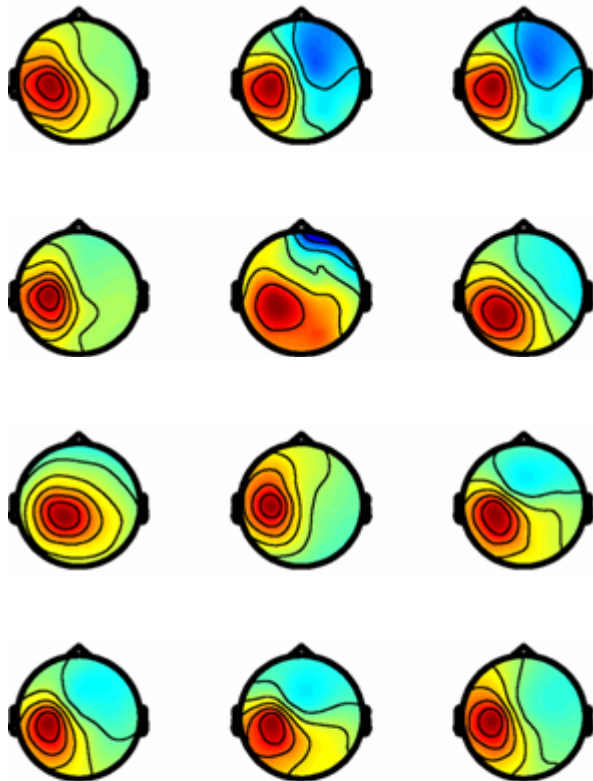




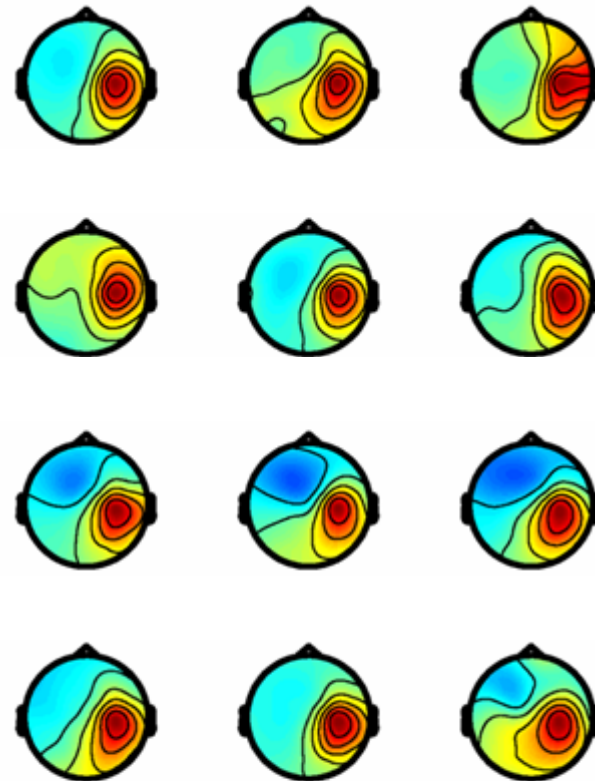
# Clustering ICA components by eye

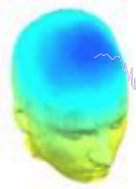


Left mu



Right mu





# So how to cluster components?

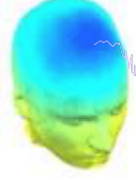


## The same problems hold for clustering independent components

Across Ss, components don't even have “the same” scalp maps!

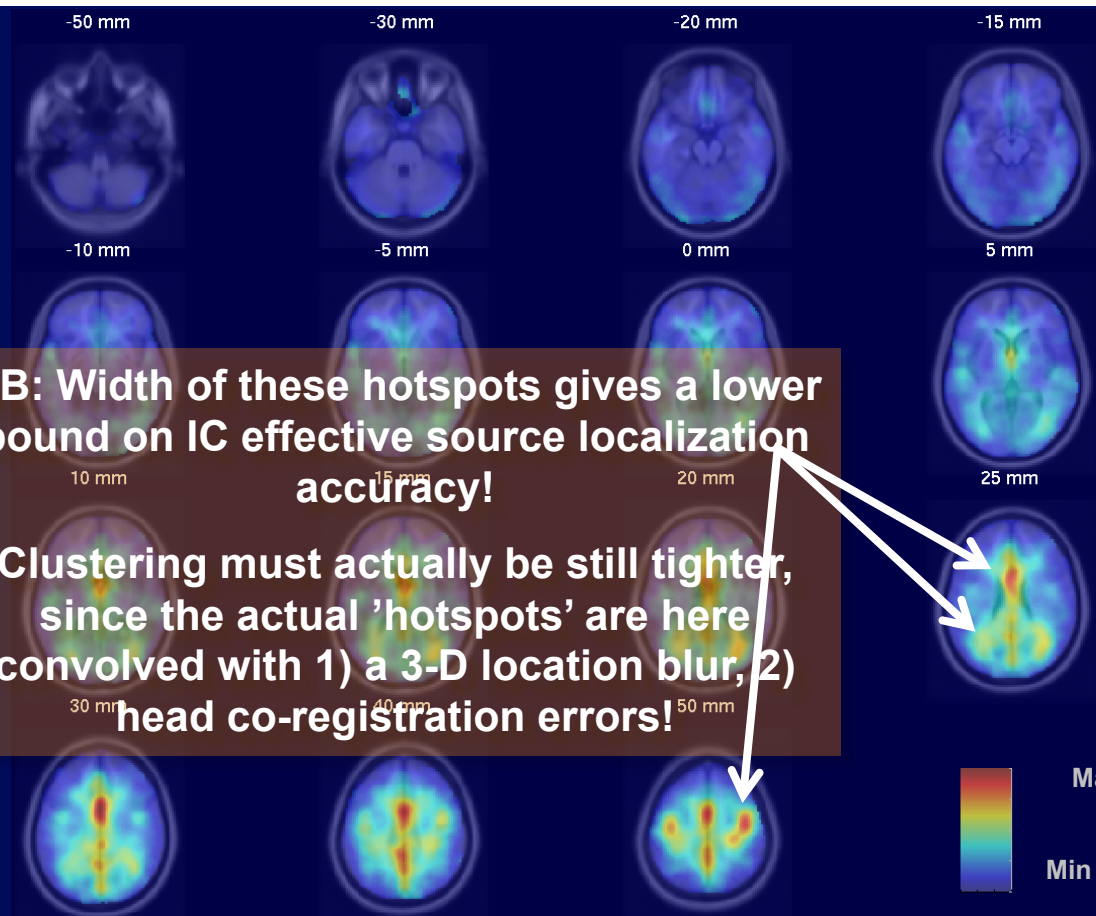
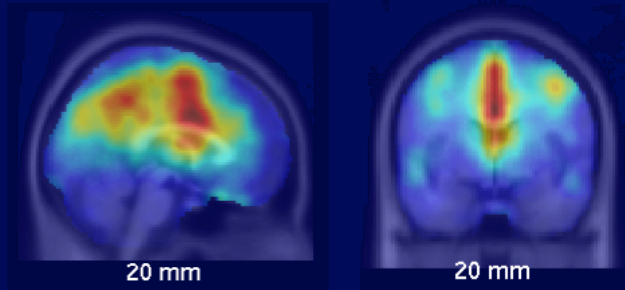
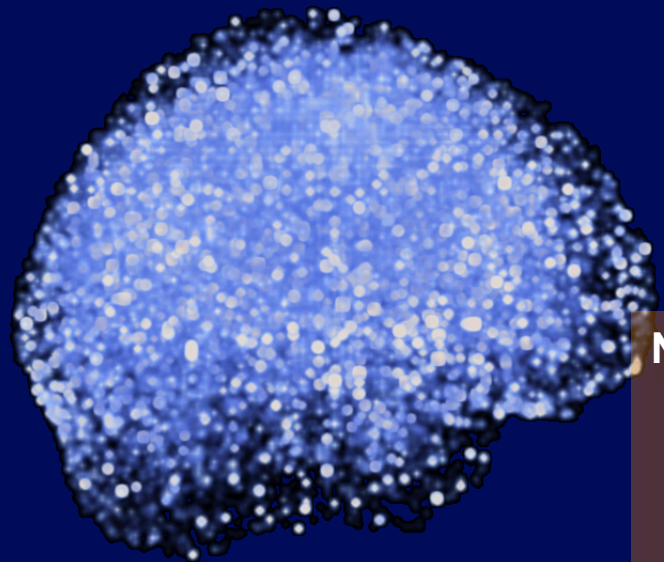
→ Are “the same” components found across subjects?

- What should define “*the same*” (i.e., “*component equivalence*”)?:
  - Similar scalp maps?
  - Similar cortical or 3-D equivalent dipole locations?
  - Similar activity power spectra?
  - Similar ERPs?
  - Similar ERSPs?
  - Similar ITCs?
  - Or similar *combinations* of the above?? ...

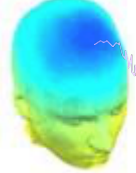


# EEG IC Source Locations

(135,794 IC equivalent dipoles!)



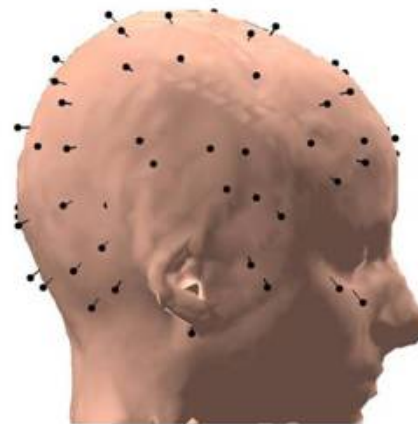
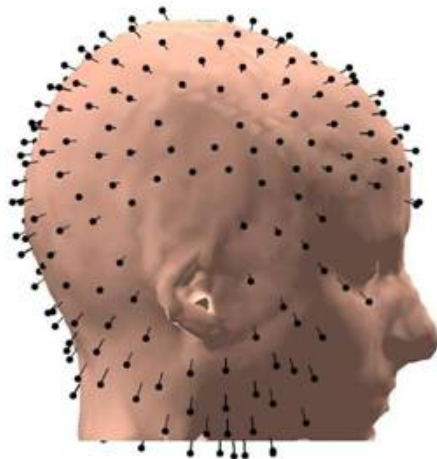


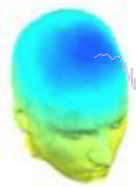


## ... Some caveats

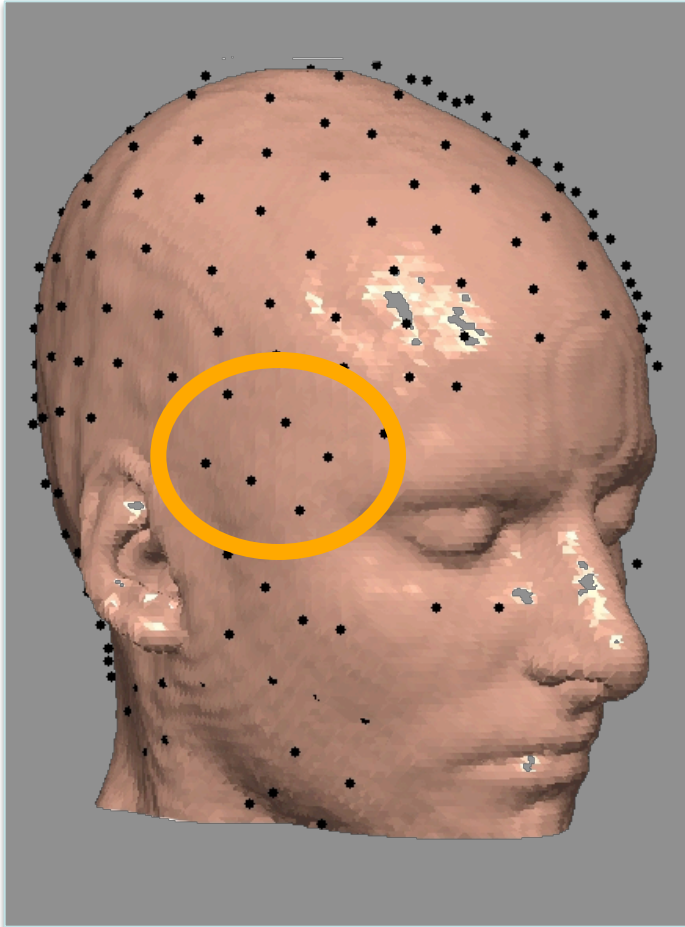
### In this *dipoledensity()* assay ...

- MR head images were not available → brain co-registration crude.
- Single versus dual-dipole model selection was subjective.
- Different electrode montages → mis-localization effects.
- Electrode locations were not all digitized – some ‘guestimated’ !
- Brain geometries differ!





# Co-Registration of Electrodes with MR Image



**MR + EEG**



**EEG**

# Arthur Tsai – Topological source clustering

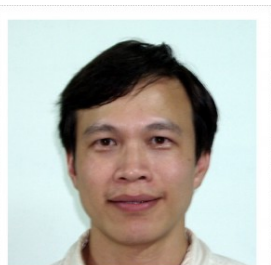
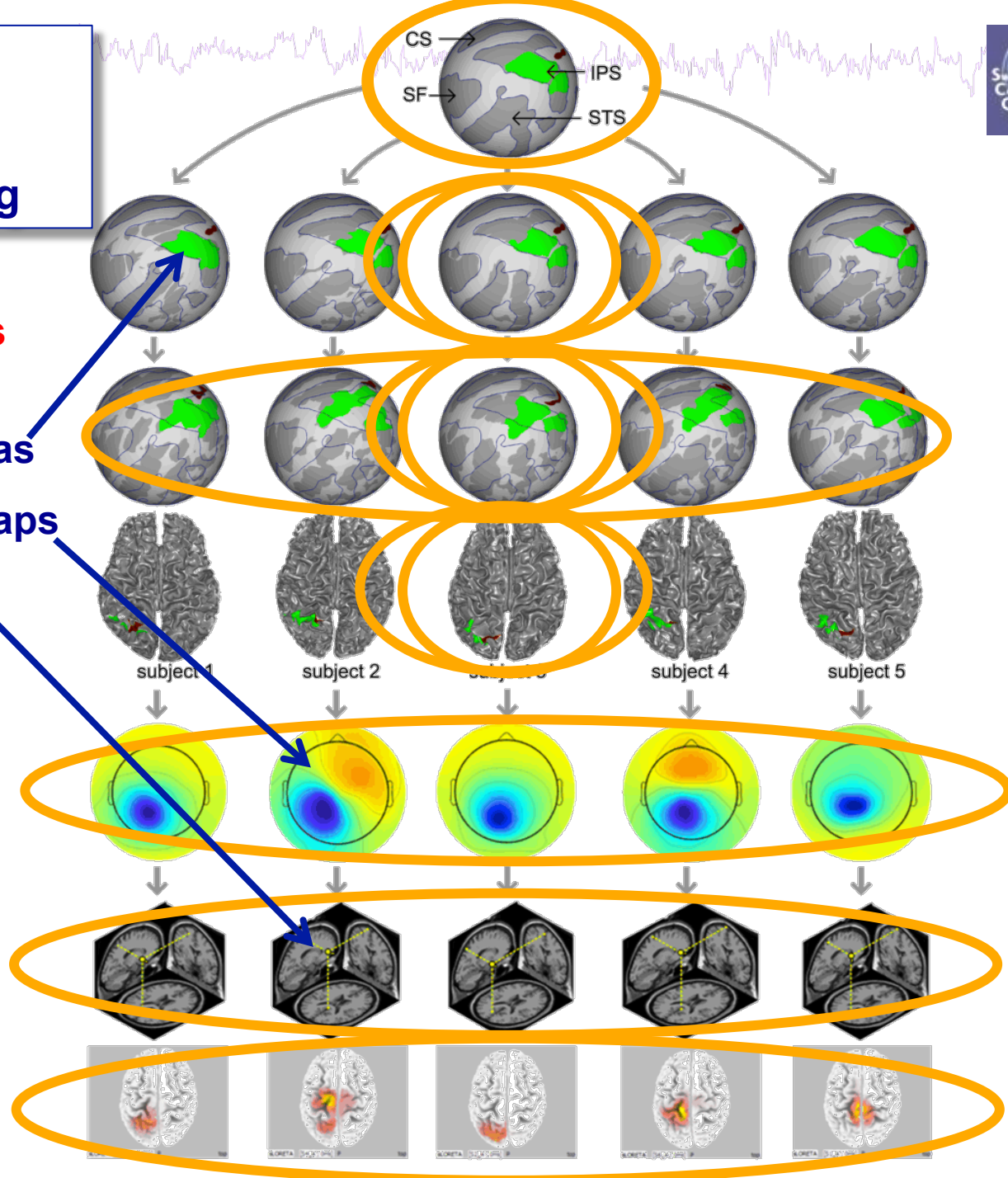


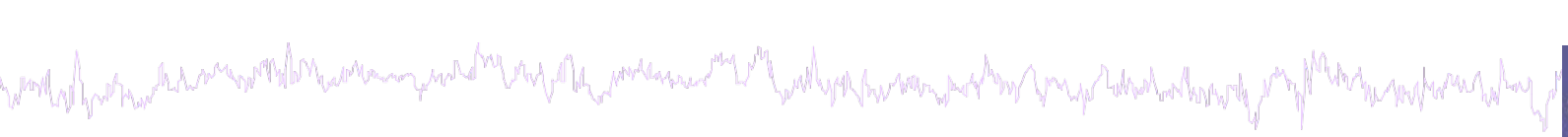
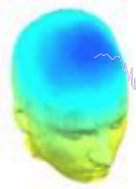
Why should IC clusters  
have breadth?

Equivalent cortical areas

Have different scalp maps

And dipole locations!





**Does the spatial distribution of IC  
equivalent dipole source locations  
depend on the task the subject  
performs?**

i.e.

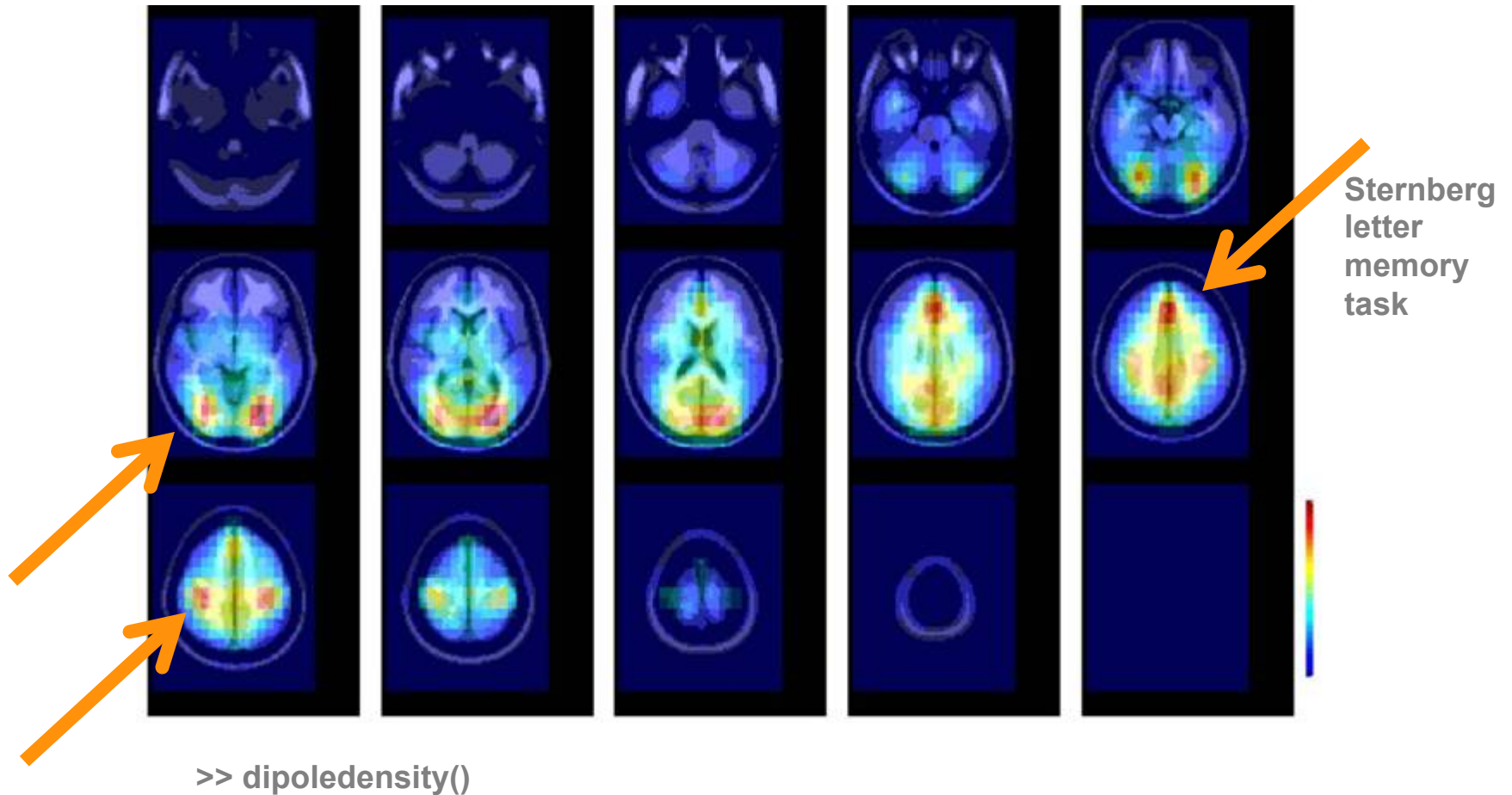
**Do “the same” ICs (and IC clusters)  
appear for every task?**







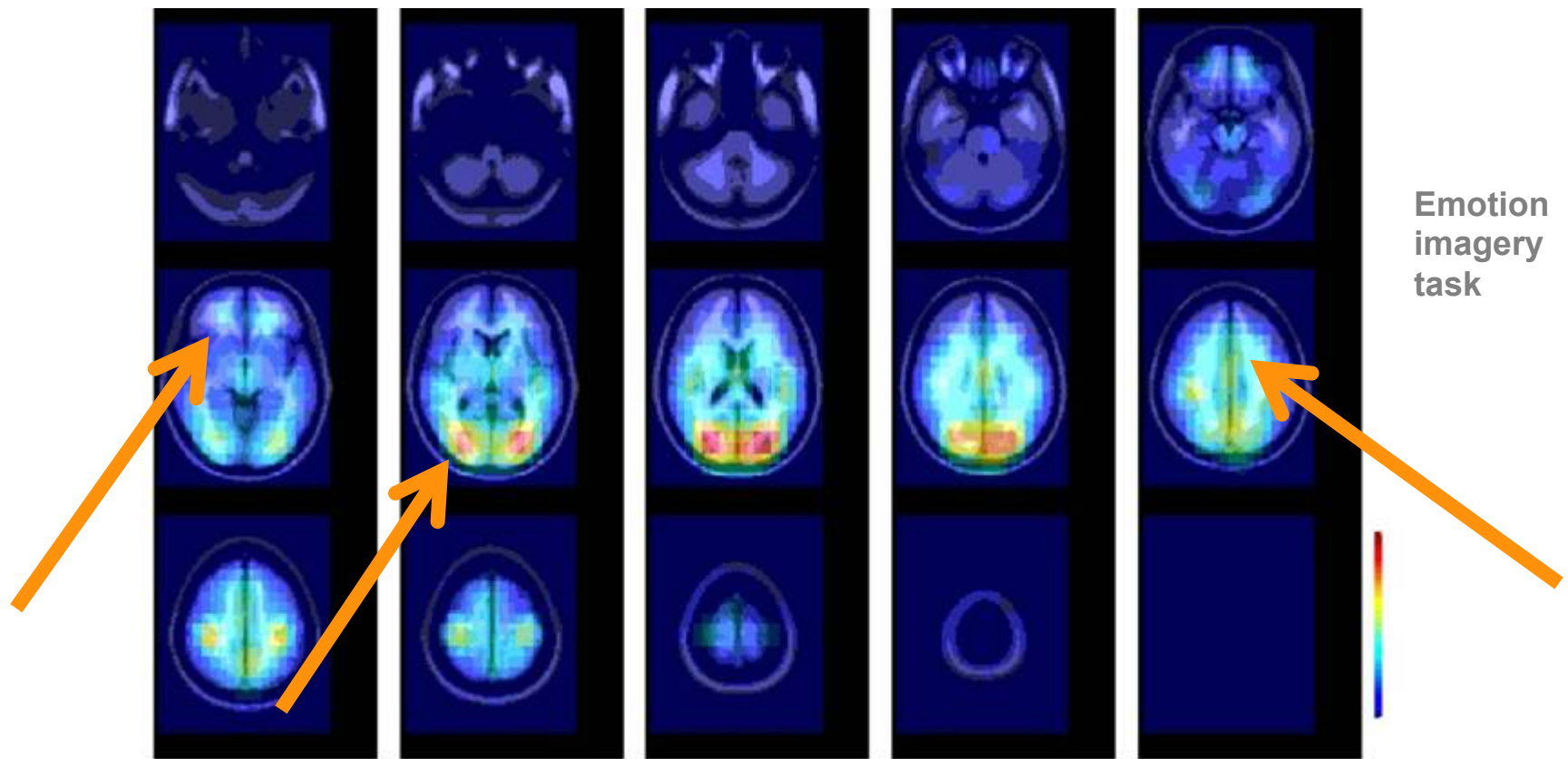
# Equivalent dipole density







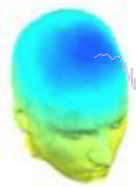
# Equivalent dipole density



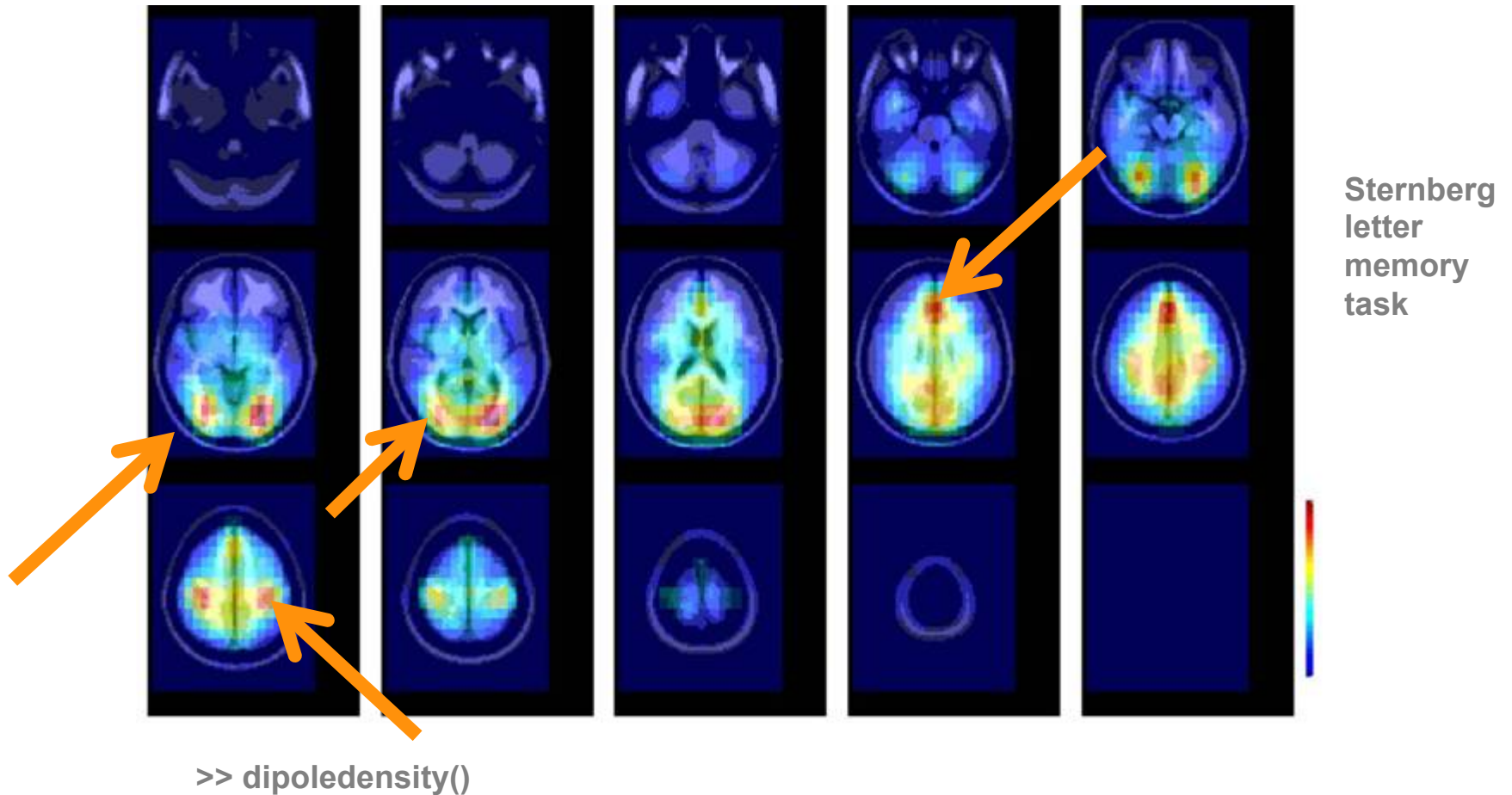
Emotion  
imagery  
task

>> dipoledensity()



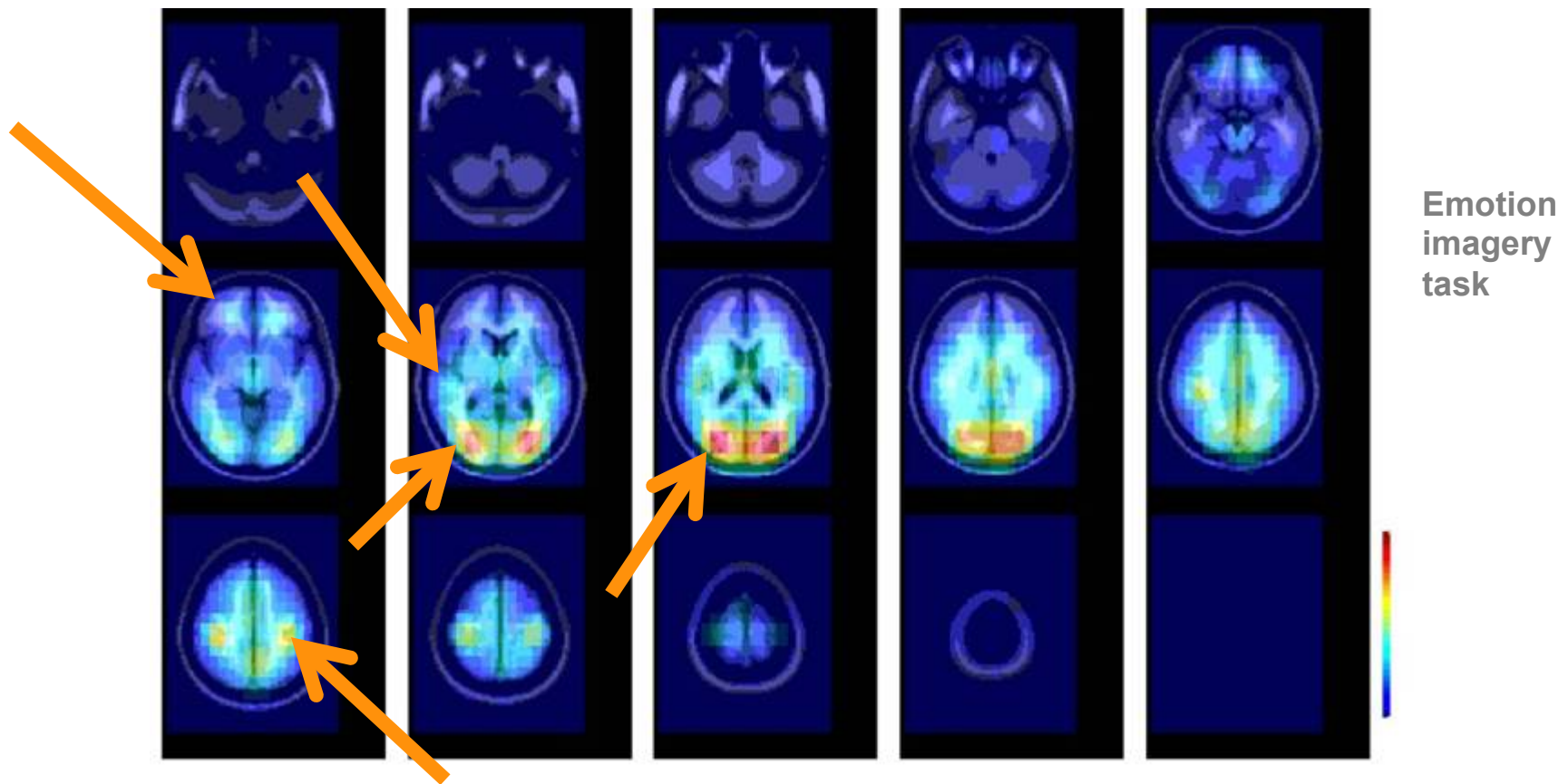


# Equivalent dipole density





# Equivalent dipole density



>> dipoledensity()



# So how to cluster components?

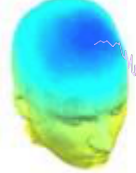


## The same problems hold for clustering independent components

Across Ss, components don't even have “the same” scalp maps!

→ Are “the same” components found across subjects?

- What should define “the same” (i.e., “component equivalence”)?
  - Similar scalp maps?
  - Similar cortical or 3-D equivalent dipole locations?
  - Similar activity power spectra?
  - Similar ERPs?
  - Similar ERSPs?
  - Similar ITCs?
  - Or similar ***combinations*** of the above?? ...
- **EEGLAB clustering supports all these possibilities.**

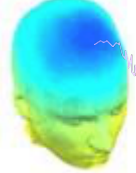


# Study IC Clustering: Assumptions

- Assumes there are *functionally equivalent* ICs across most subjects.
- Assumes these ICs have *similar responses* to experimental conditions across **a set** of measures (ERP, ERSP, ITC...)
- Creates ***non-overlapping IC partitions*** making each IC belong to only one cluster.

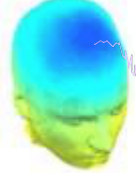




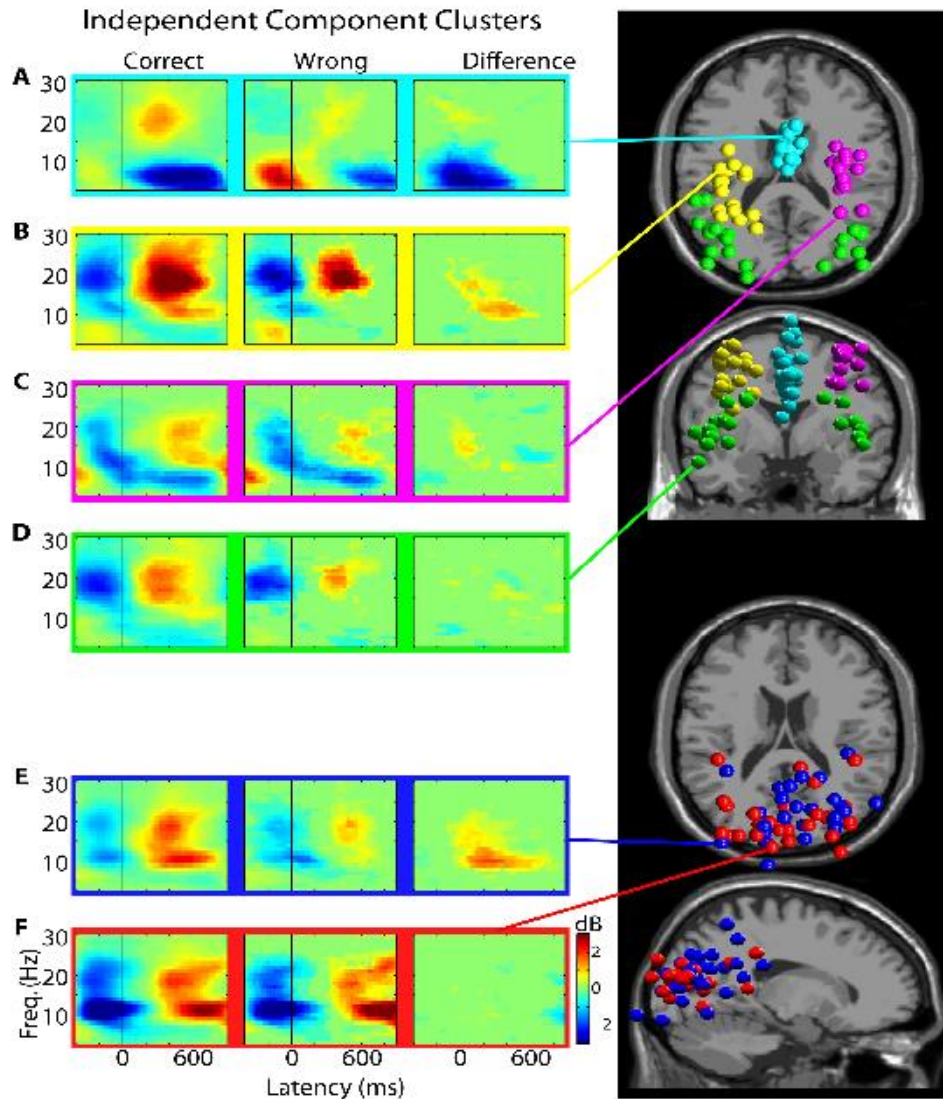


# EEGLAB Study Clustering strategy

1. Cluster on **multiple measures** (**dipole locations**, scalp maps, spectra, ERPs, ITCs, ERSPs, ...) **in one or more conditions**.
2. **Reduce the dimension** of each measure to a principal component subspace.
3. Compose a PCA-reduced **position vector** for each component.
4. **Cluster** the composed component vectors using k-means or other.
5. Use the computed component measures (not PCA-reduced) to **visualize the activities and spatial properties** of the clustered components.
6. Compute and visualize the **cluster-mean measures**.
7. Use **clustered Study set data** as input into 'std\_???' functions.

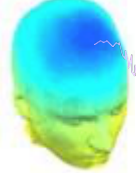


# Study IC Clustering



Sometime  
clusters are  
spatially separate  
AND have distinct  
responses.

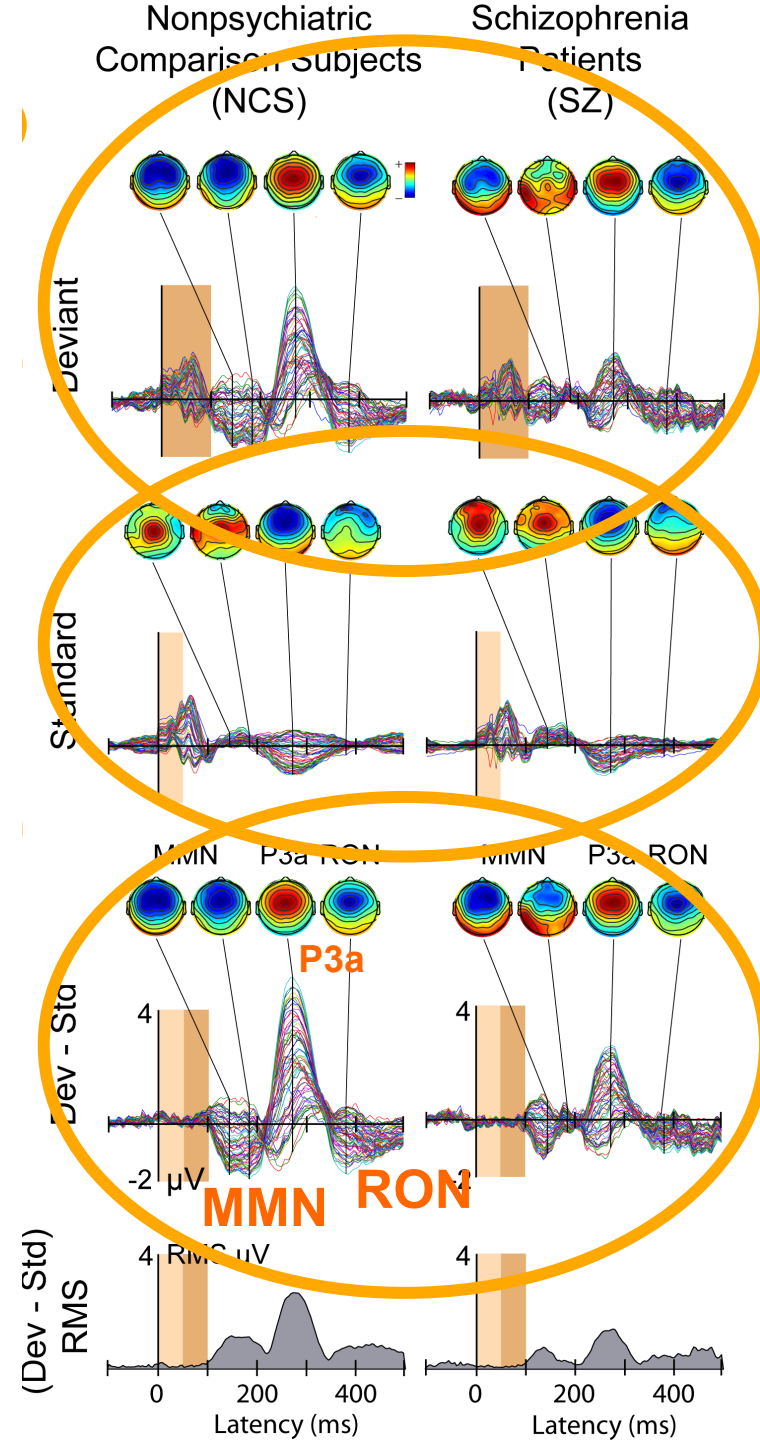
In other cases, they  
may have similar  
responses or may  
overlap spatially.

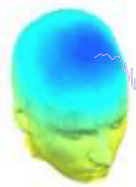


# EEGLAB Study Clustering procedure

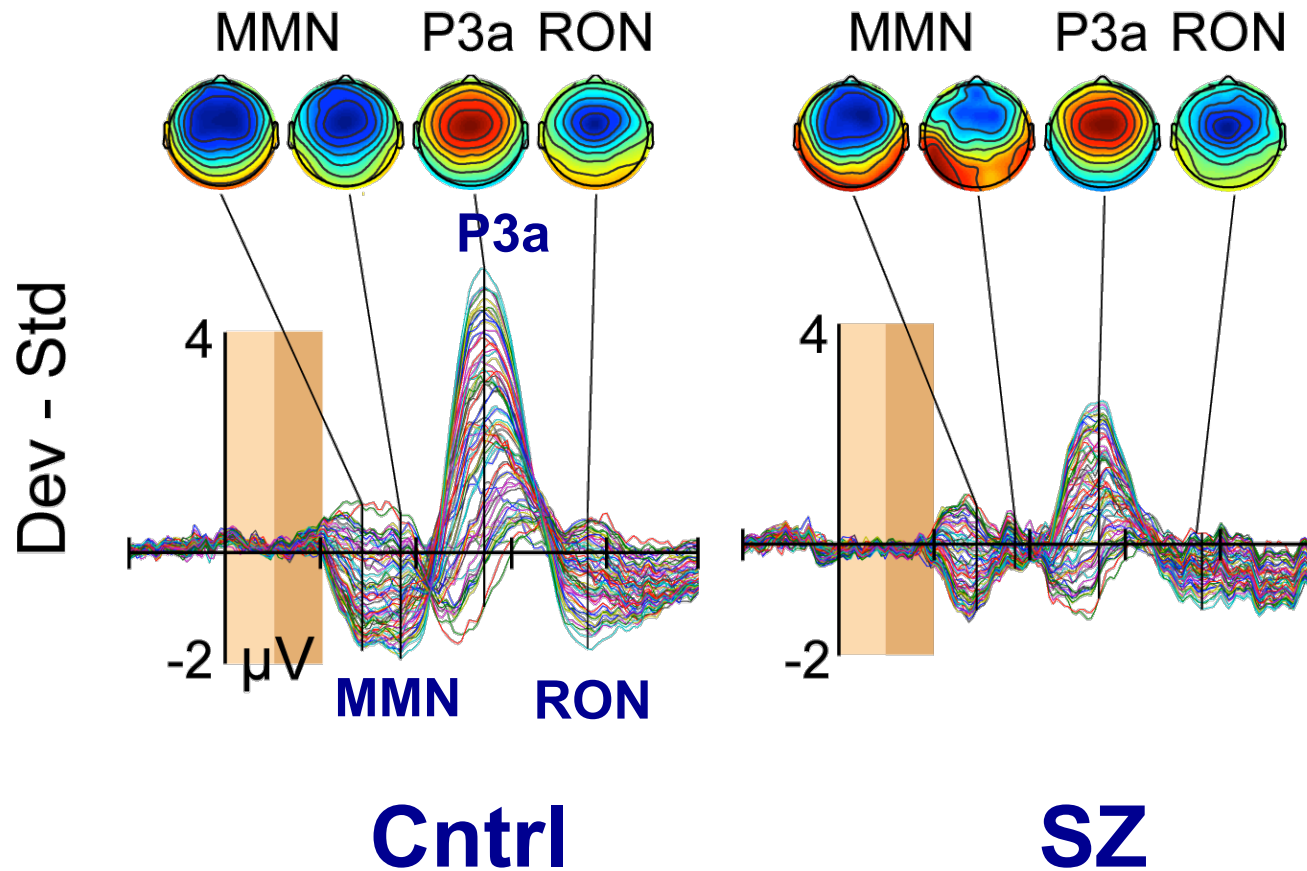


1. Identify a set of datasets as an **EEGLAB Study**.
2. Specify the **subject** code, subject **group**, **condition** and/or **session** for each dataset in the Study.
3. Identify **components to cluster** in each Study dataset.
4. Decide on **component measures** to use in clustering the Study and/or to evaluate the obtained component clusters.
5. **Compute the component measures** for each Study dataset.
6. **Cluster the components on these component measures.**
7. **Review the obtained clusters** (e.g., their scalp maps, dipoles, and activity measures).
8. **Edit the clusters** (manually remove/shift components, make sub-clusters, merge clusters, re-cluster).
9. **Statistically test differences** within or between selected clusters.





# Auditory Deviance Response

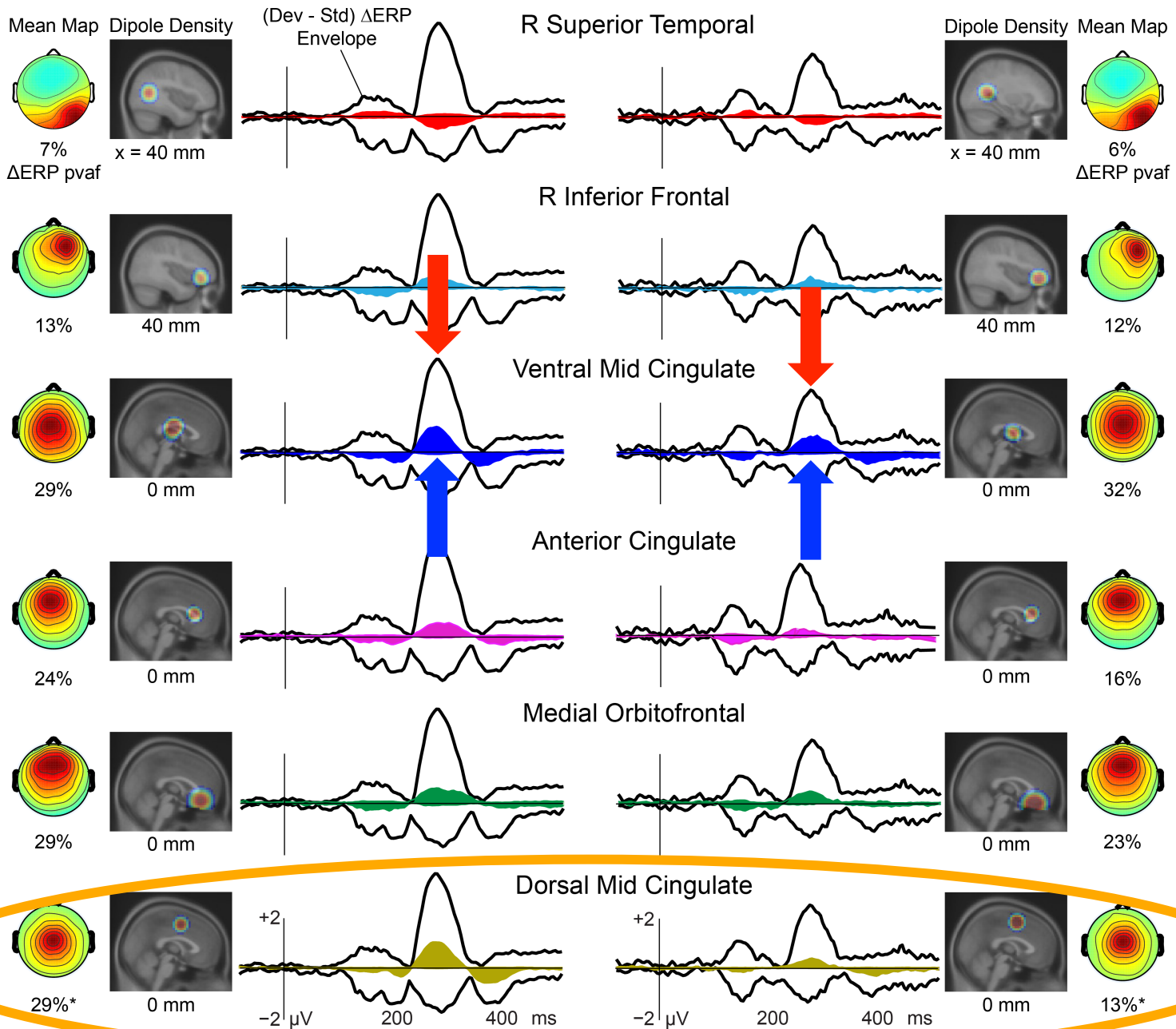


The deepest mental trap in electrophysiology  
lies in the word "THE" !!!



## Nonpsychiatric Comparison Subjects (NCS)

## Schizophrenia Patients (SZ)



# PEAK AMPLITUDES

ERP

$r^2$



## ADR

### Scalp Electrode (Fz)

Verbal IQ (WRAT)

P3a

0.11

Functional Capacity (UPS

RON

0.12

### R Superior Temporal

Working Memory (LNS Reorder)

RON

0.15

Verbal IQ (WRAT)

RON

0.15

**Immediate Verbal Memory (CVLT)**

**RON**

**0.28**

Delayed Verbal Memory (CVLT)

RON

0.26

**Functional Capacity (UPSA)**

**MMN**

**0.48**

Functional Capacity (UPSA)

RON

0.26

### R Inferior Frontal

**Negative Symptoms (SANS)**

**RON**

**0.36**

Psychosocial Functioning (SOF)

RON

0.24

**Auditory Attention (LNS Forward)**

**MMN**

**0.38**

**Working Memory (LNS Reorder)**

**MMN**

**0.30**

**Verbal IQ (WRAT)**

**MMN**

**0.46**

### Ventral Mid Cingulate

**Positive Symptoms (SAPS)**

**RON**

**0.29**

**Negative Symptoms (SANS)**

**P3a**

**0.36**

**Immediate Verbal Memory (CVLT)**

**RON**

**0.41**

Delayed Verbal Memory (CVLT)

RON

0.24

**Verbal IQ (WRAT)**

**RON**

**0.29**

Executive Functioning (WCST)

RON

0.24

### Anterior Cingulate

Functional Status (GAF)

MMN

0.18

Functional Status (GAF)

RON

0.17

Immediate Verbal Memory (CVLT)

RON

0.25

Delayed Verbal Memory (CVLT)

RON

0.17

### Medial Orbitofrontal

**Positive Symptoms (SAPS)**

**P3a**

**0.40**

**Negative Symptoms (SANS)**

**P3a**

**0.54**

**Psychosocial Functioning (SOF)**

**P3a**

**0.37**

**Functional Capacity (UPSA)**

**P3a**

**0.32**

### Dorsal Mid Cingulate

Verbal IQ (WRAT)

P3a

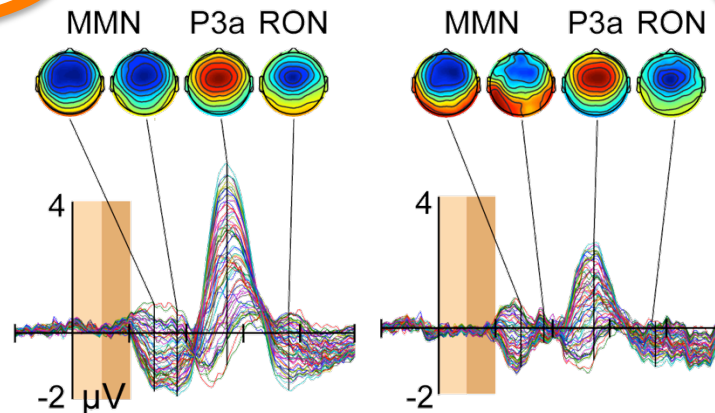
0.15

Executive Functioning (WCST)

MMN

0.18

Dev - Std



## Cntrl

## SZ

# PEAK LATENCIES

ERP

r<sup>2</sup>

ADR



## Scalp Electrode (Fz)

---n/a---

## R Superior Temporal

Functional capacity (UPSA)

MMN

0.25

Delayed Verbal Memory (CVLT)

MMN

0.17

## R Inferior Frontal

**Negative Symptoms (SANS)**

RON

0.51

Psychosocial Functioning (SOF)

RON

0.25

**Executive Functioning (WCST)**

MMN

0.30

**Executive Functioning (WCST)**

P3a

0.28

## Ventral Mid Cingulate

**Negative Symptoms (SANS)**

P3a

0.33

**Negative Symptoms (SANS)**

RON

0.33

**Psychosocial Functioning (SOF)**

P3a

0.31

Verbal IQ (WRAT)

MMN

0.25

**Executive Functioning (WCST)**

P3a

0.30

## Anterior Cingulate

Functional Capacity (UPSA)

RON

0.17

Verbal IQ (WRAT)

MMN

0.24

Auditory Attention (LNS-Forward)

MMN

0.17

## Medial Orbitofrontal

**Negative Symptoms (SANS)**

RON

0.41

**Positive Symptoms (SAPS)**

RON

0.40

**Auditory Attention (LNS-Forward)**

MMN

0.29

**Executive Functioning (WCST)**

P3a

0.32

## Dorsal Mid Cingulate

Negative Symptoms (SANS)

MMN

0.20

Negative Symptoms (SANS)

P3a

0.17

Global Functioning (GAF)

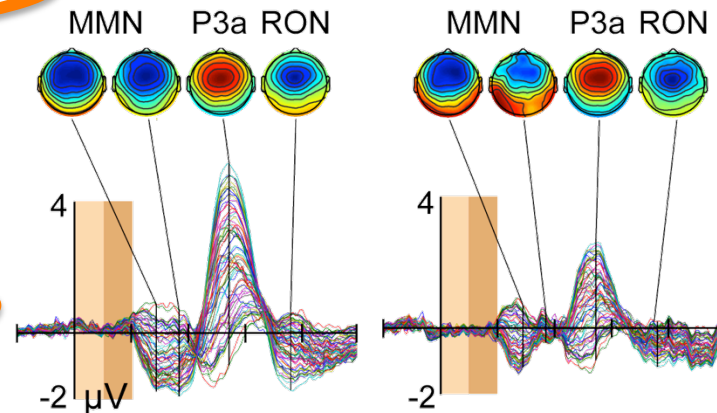
RON

0.24

Functional Capacity (UPSA)

P3a

0.13



Cntrl

SZ



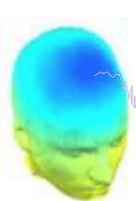
# Should every subject be included in every cluster?

**Not all subjects contribute components to each cluster.**

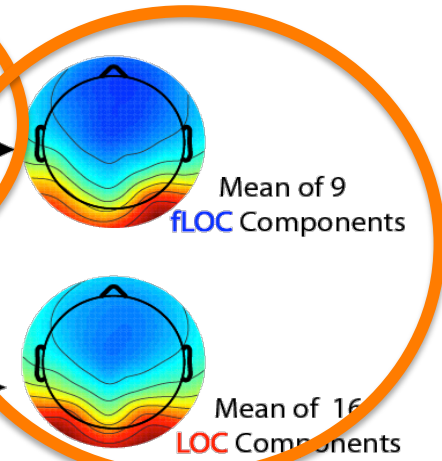
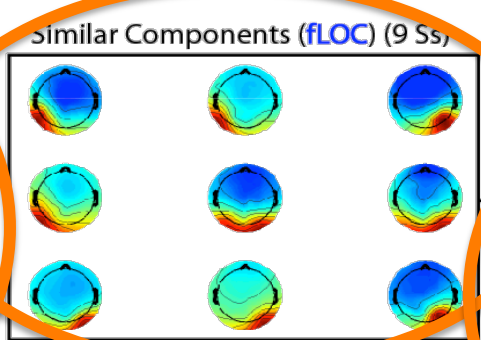
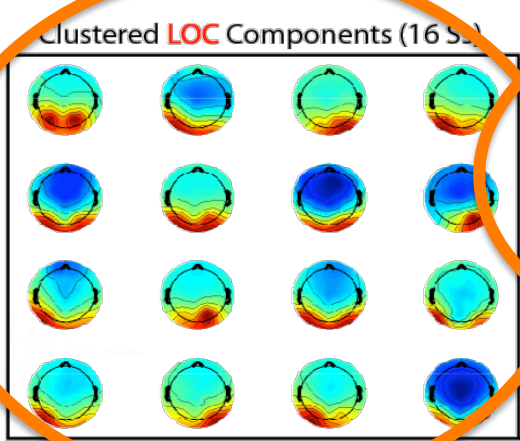
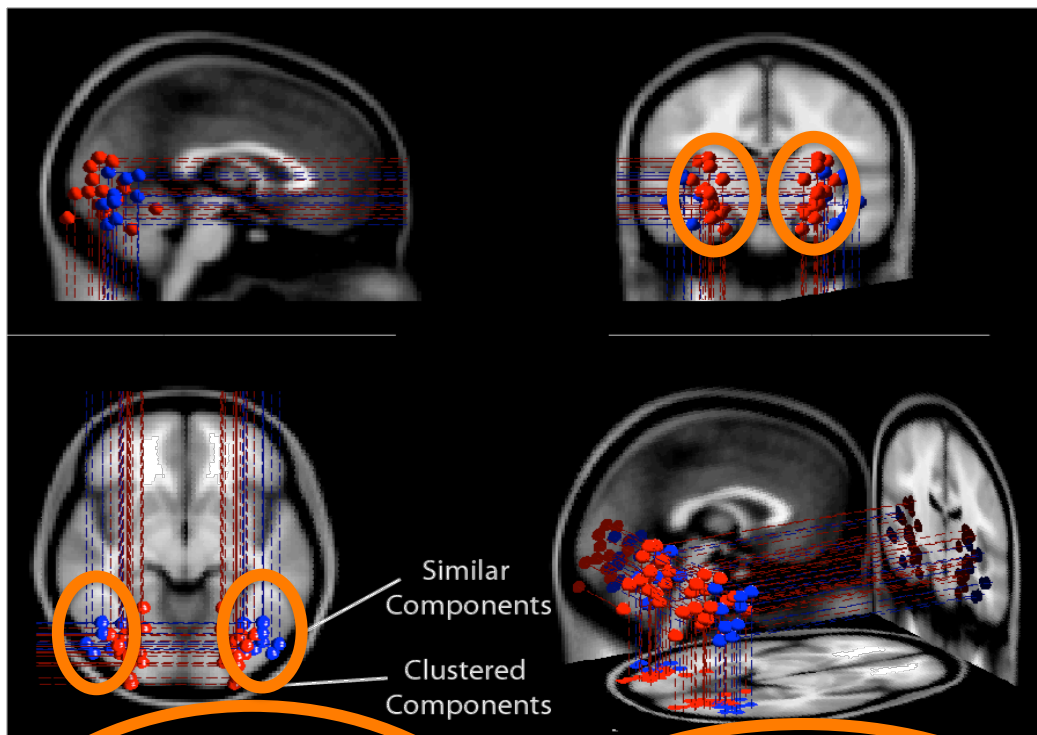
**Why not?**

- Different numbers of artifact components
- Subject differences!?
- Does my subject group really exhibit a Gaussian cloud of individual differences around 'a mean subject' in 'subject space' ??



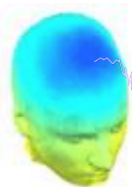


# Why aren't all participants in every IC cluster?

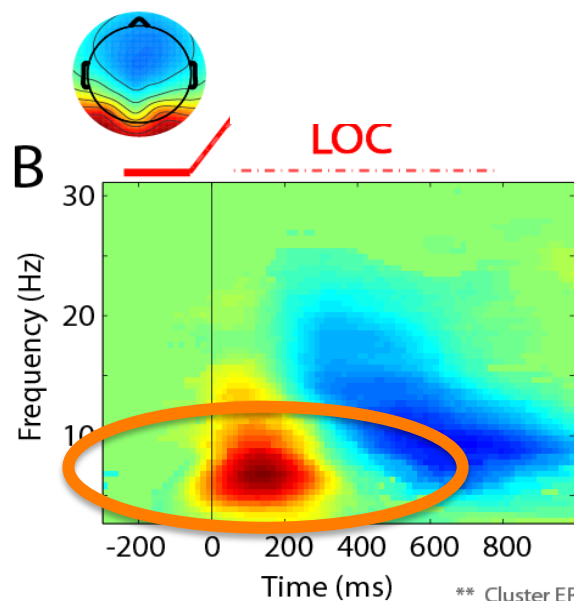
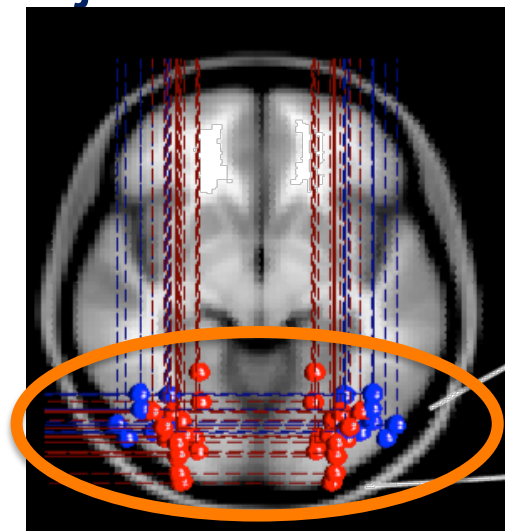




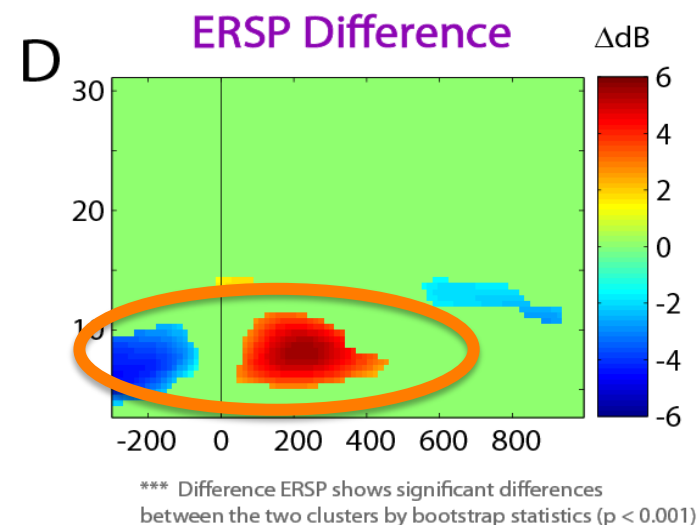
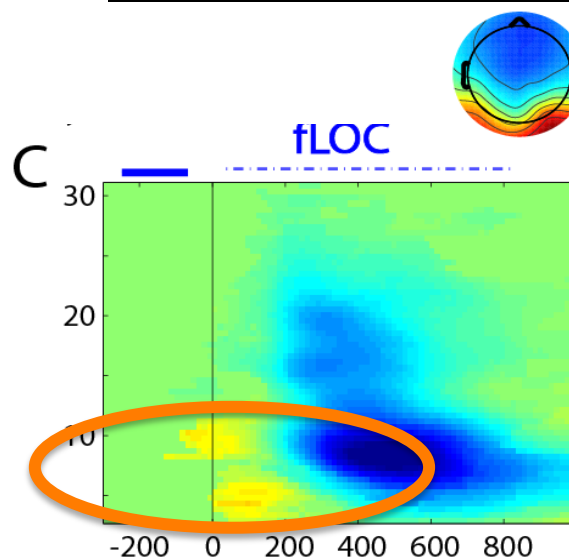




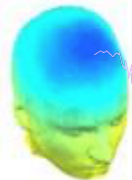
# Subject differences?



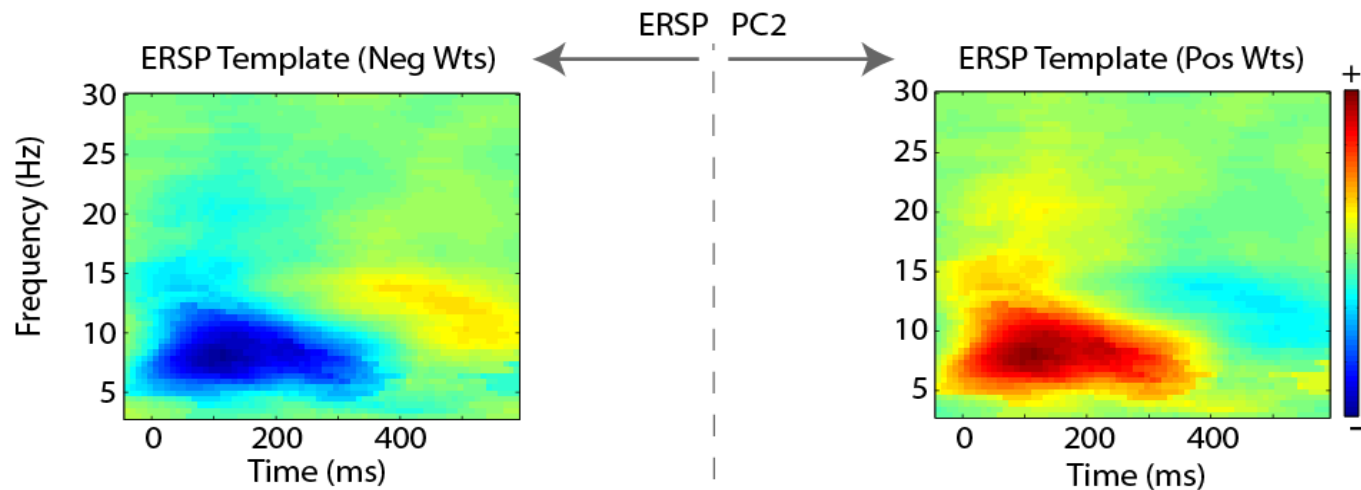
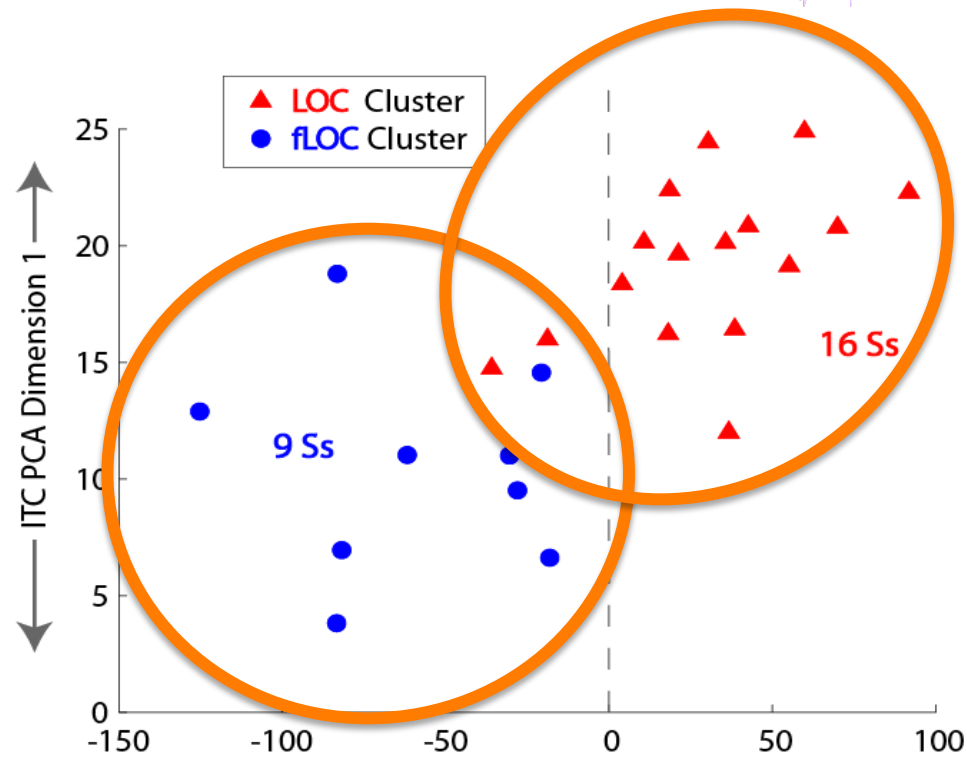
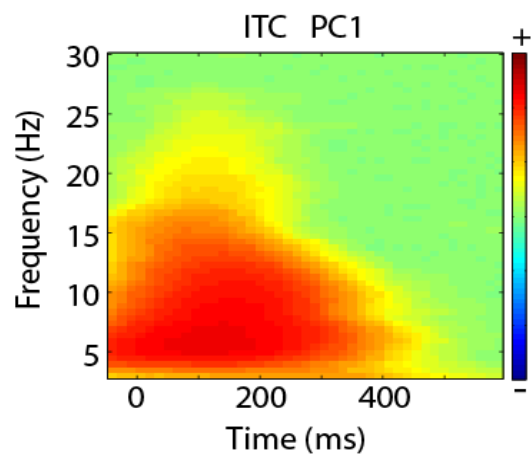
\*\* Cluster ERSPs show significant activity determined by bootstrap statistics within subject and binomial probability between subjects ( $p < 0.01$ )

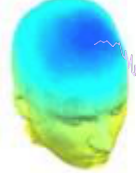


\*\*\* Difference ERSP shows significant differences between the two clusters by bootstrap statistics ( $p < 0.001$ )



# Subject differences?

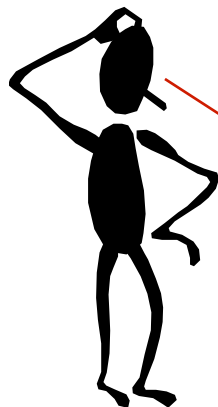




# STUDY IC Clustering: Practical Problems

Large parameter space problem: many different clustering solutions can be produced by changing parameters and measure subsets. Which one should we choose?

EEGLAB clustering  
has ~12 parameters



Select and compute component measures for later clustering – pop\_preclust()

Pre-compute measures on which to cluster components from study 'N400STUDY'  
Select the cluster to refine during sub-clustering (any existing sub-hierarchy will be overwritten)

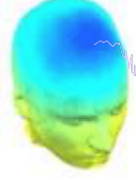
ParentCluster 1 (151 ICs)

Pre-compute or Load	Dims.	Norm.	Rel. Wt.
<input checked="" type="checkbox"/> spectra	10	<input checked="" type="checkbox"/> 1	Frequency range [Hz]
<input checked="" type="checkbox"/> ERPs	10	<input checked="" type="checkbox"/> 1	Latency range in ms [lo hi]
<input checked="" type="checkbox"/> dipoles	3	<input checked="" type="checkbox"/> 10	
<input checked="" type="checkbox"/> scalp maps	10	<input checked="" type="checkbox"/> 1	Use channel values <input type="checkbox"/>
<input checked="" type="checkbox"/> ERSPs	10	<input checked="" type="checkbox"/> 1	Time/freq. parameters
<input checked="" type="checkbox"/> ITCs	10	<input checked="" type="checkbox"/> 1	Time/freq. parameters
<input checked="" type="checkbox"/> Final dimensions	10	Help	

Frequency range [Hz] 3 25  
Latency range in ms [lo hi] -2100 1995  
Time/freq. parameters [3 25], 'cycles', [3 0.5], 'pa  
Time/freq. parameters [3 25], 'cycles', [3 0.5], 'pa

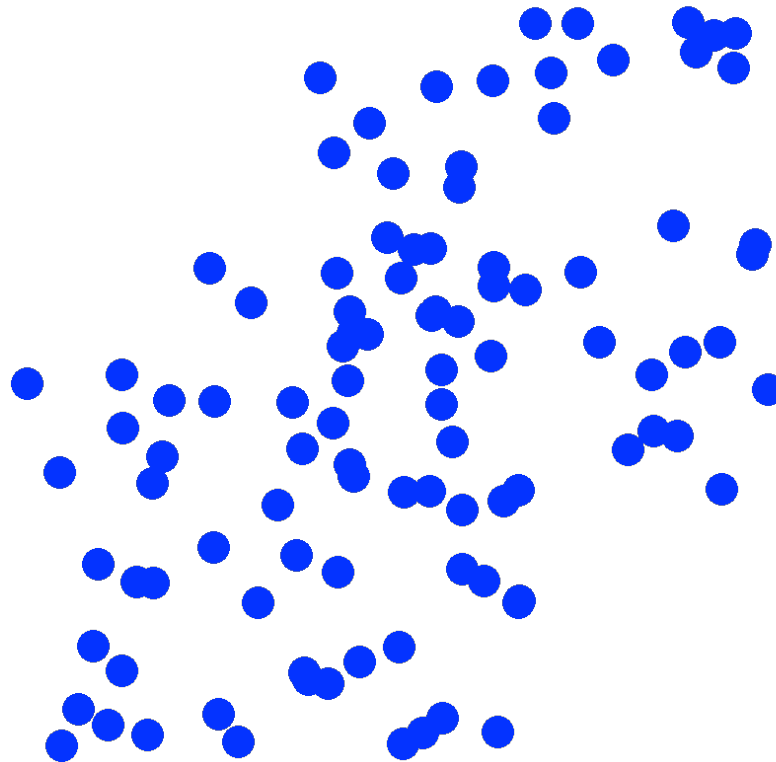
☐ Save STUDY to file /data/common4/amer/5subjects/N400precluststudy ...

Cancel Help Ok

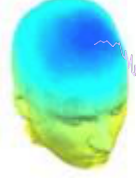


# Problems with multi-measure clustering

In a uniform density distribution,  
where are the clusters by location?

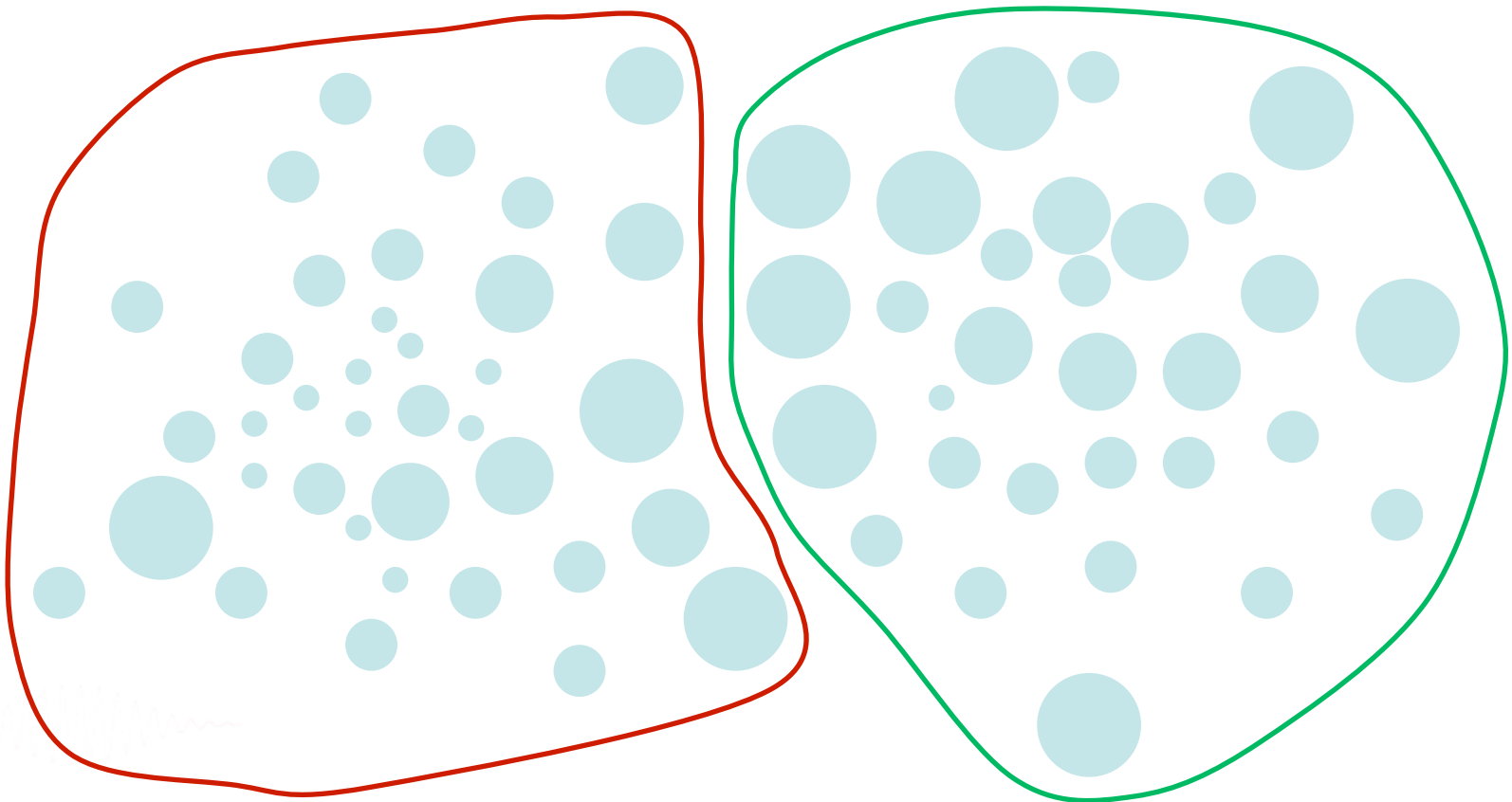


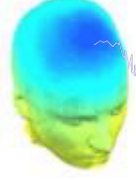




# Problems with multi-measure clustering

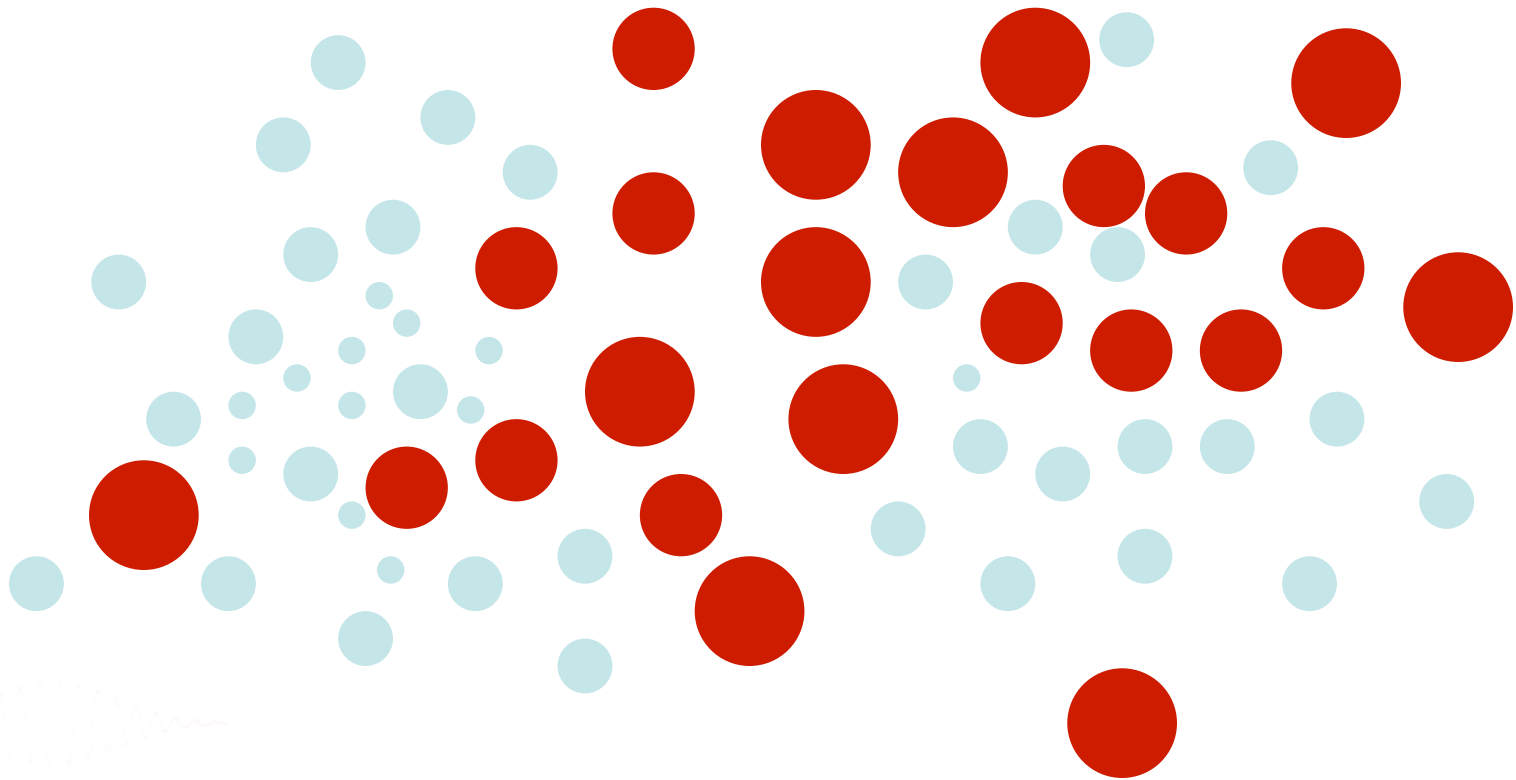
What are the clusters according to location?

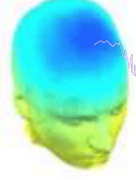




# Problems with multi-measure clustering

What are the clusters according to size ?

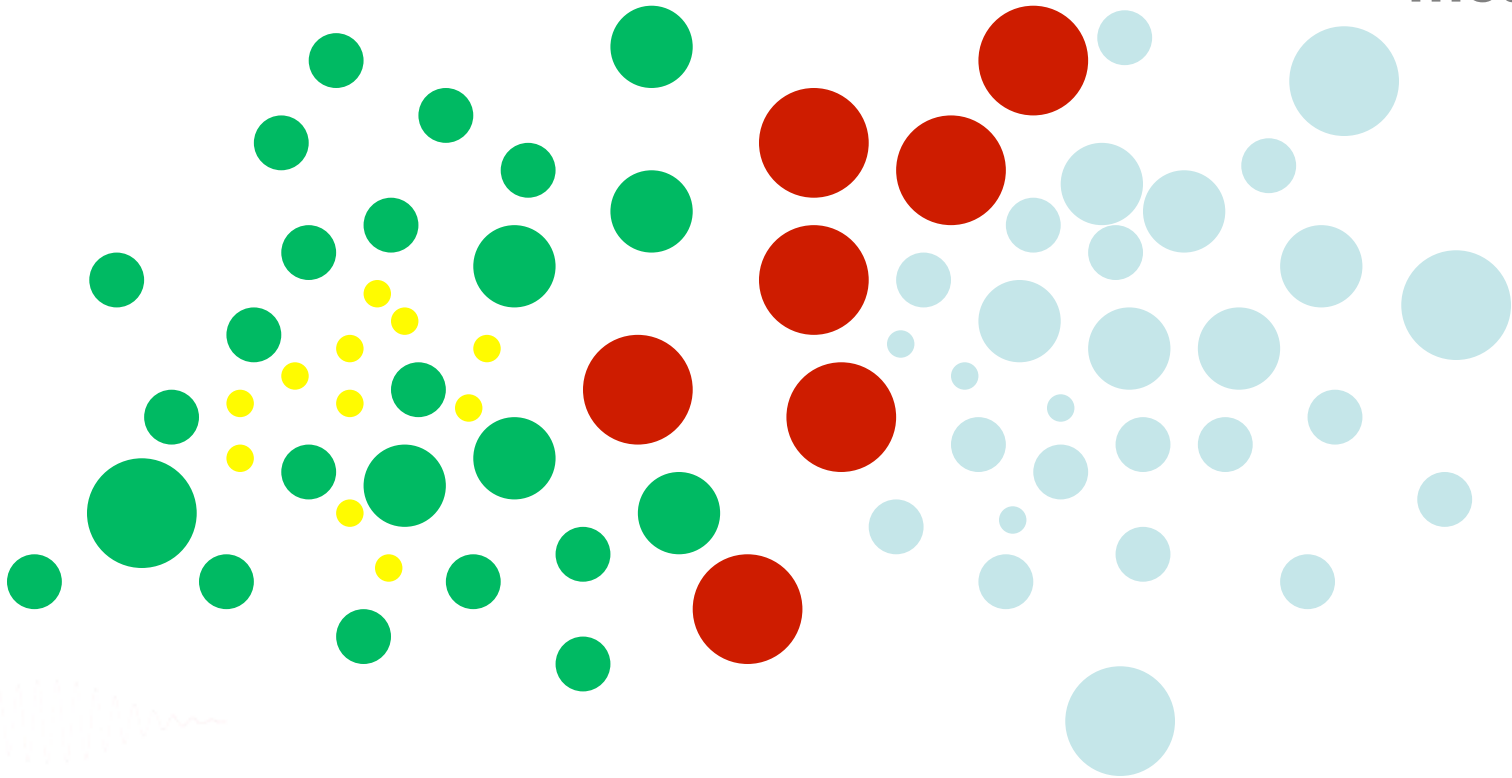


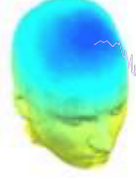


# Problems with multi-measure clustering

What are the clusters according to location and size?

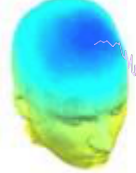
Well, it depends on how much weight we give each measure...





- With either clustering method, we basically mix together distances for a subset of EEG measures (ERP, ERSP, ITC, mean spectrum, dipole location).
- This may make clustering distance less interpretable.





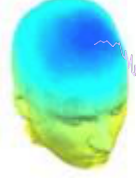
# Study IC Clustering by Measure Projection

- **Instead**, we can directly work on pair-wise similarity matrices and prevent ICs with similarities less than certain threshold (e.g., ERSP corr.  $< 0.5$ ) to be clustered together.
- The most important measure is **equivalent dipole location**.
- Assuming a certain variability estimate for dipole location (due to error in localization and subject variability), one can also estimate an optimum number of clusters.

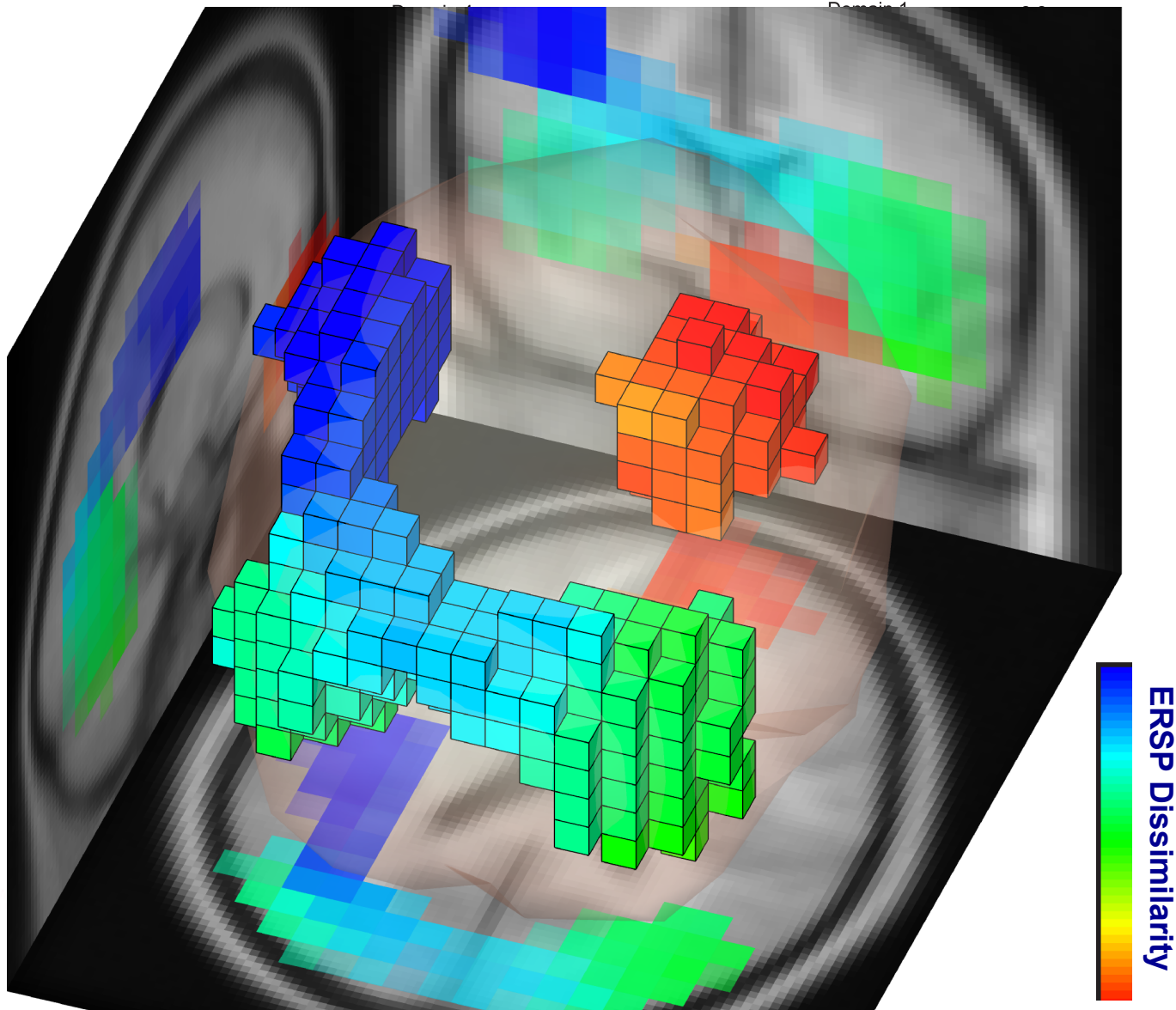
## Measure Projection asks:

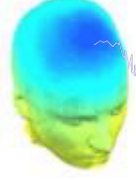
1. Where in 'template brain space' does our data have evidence that our measure of interest is consistent across nearby ICs?
2. Which such brain space voxel *domains* show consistent differences?





# Measure Projection: RSVP Task Example



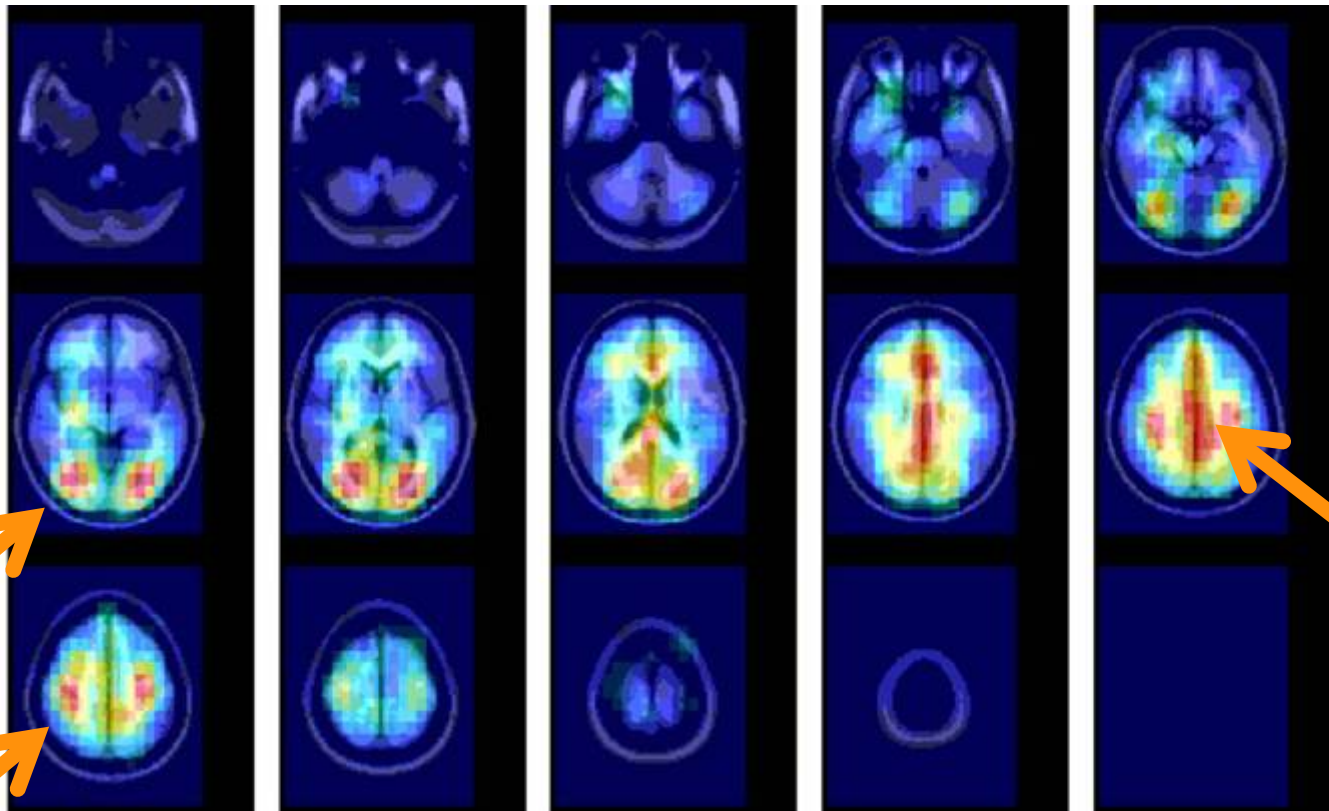


# Questions?





# Equivalent dipole density

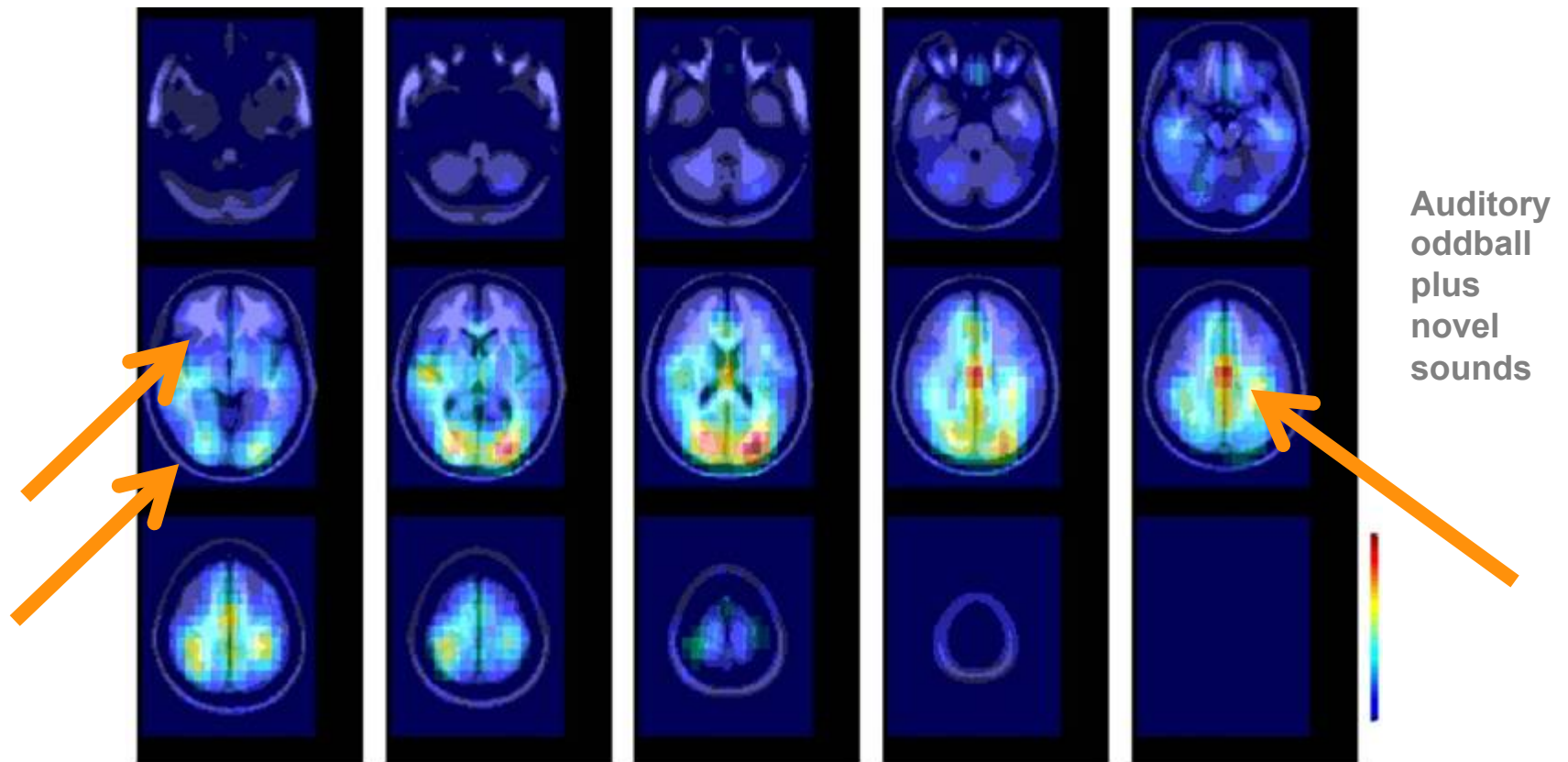


Letter  
two-back  
with  
feedback

>> dipoledensity()

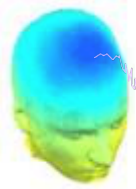


# Equivalent dipole density

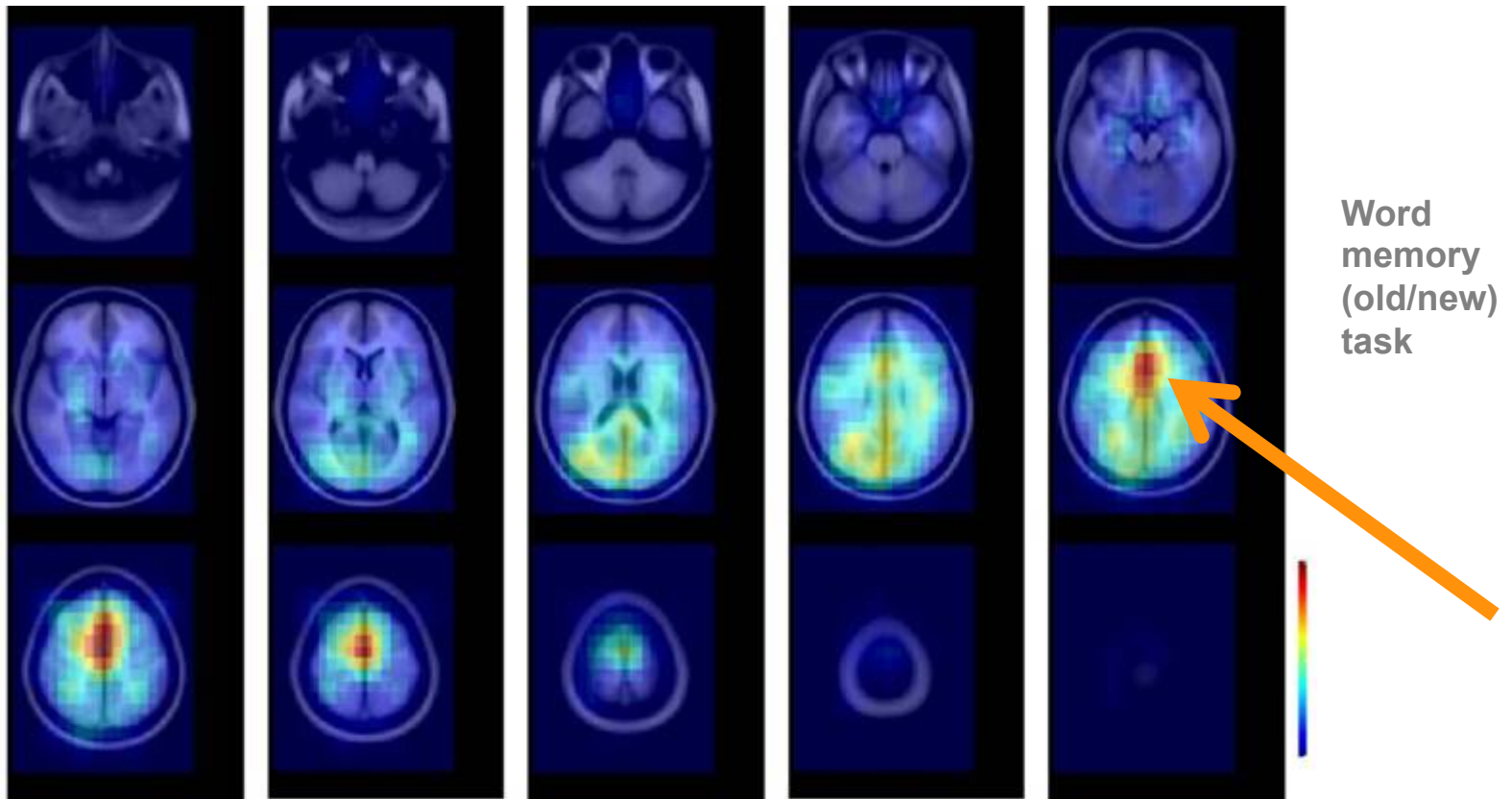


>> dipoledensity()





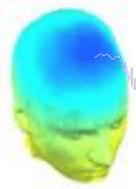
# Equivalent dipole density Exp I



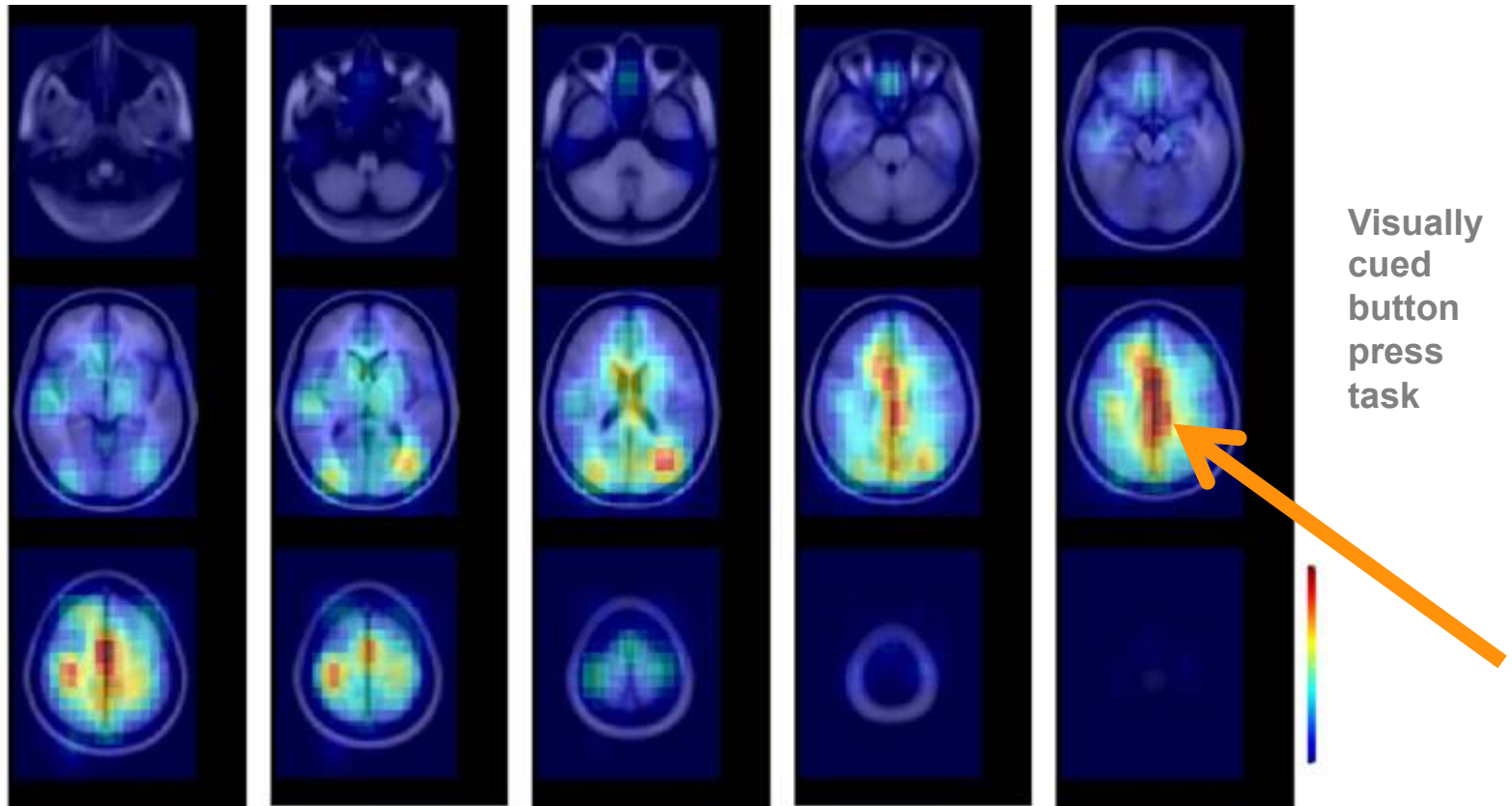
>> dipoledensity()





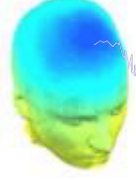


# Equivalent dipole density Exp II



>> dipoledensity()

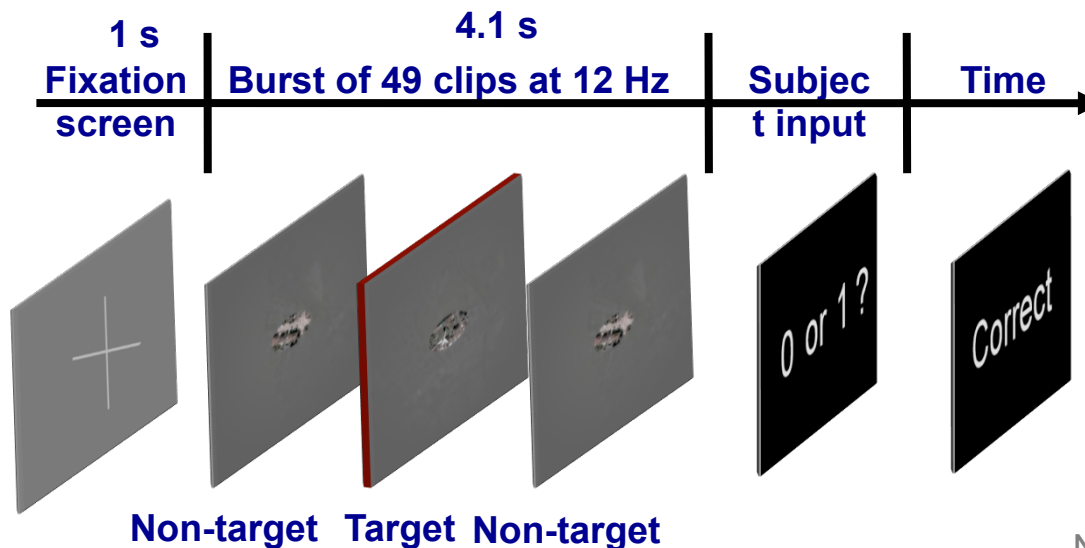


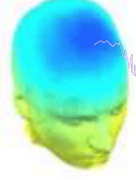


# Measure Projection: RSVP Example

## Rapid Serial Visual Presentation Experiment

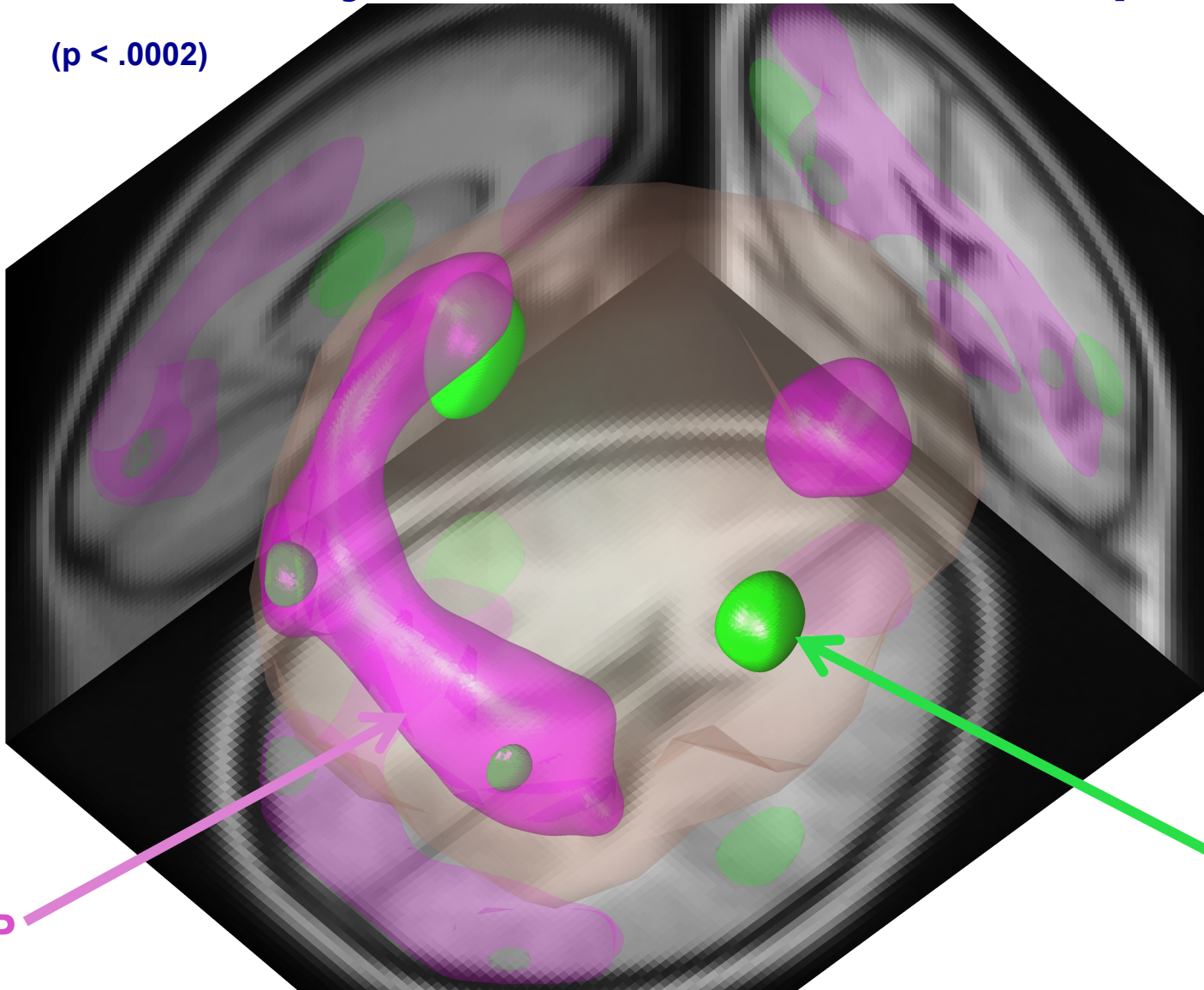
- 8 subjects
- 15 Sessions
- Visual target detection
- 257 components with equiv. dipoles inside the brain





# Measure Projection: RSVP Task Example

( $p < .0002$ )



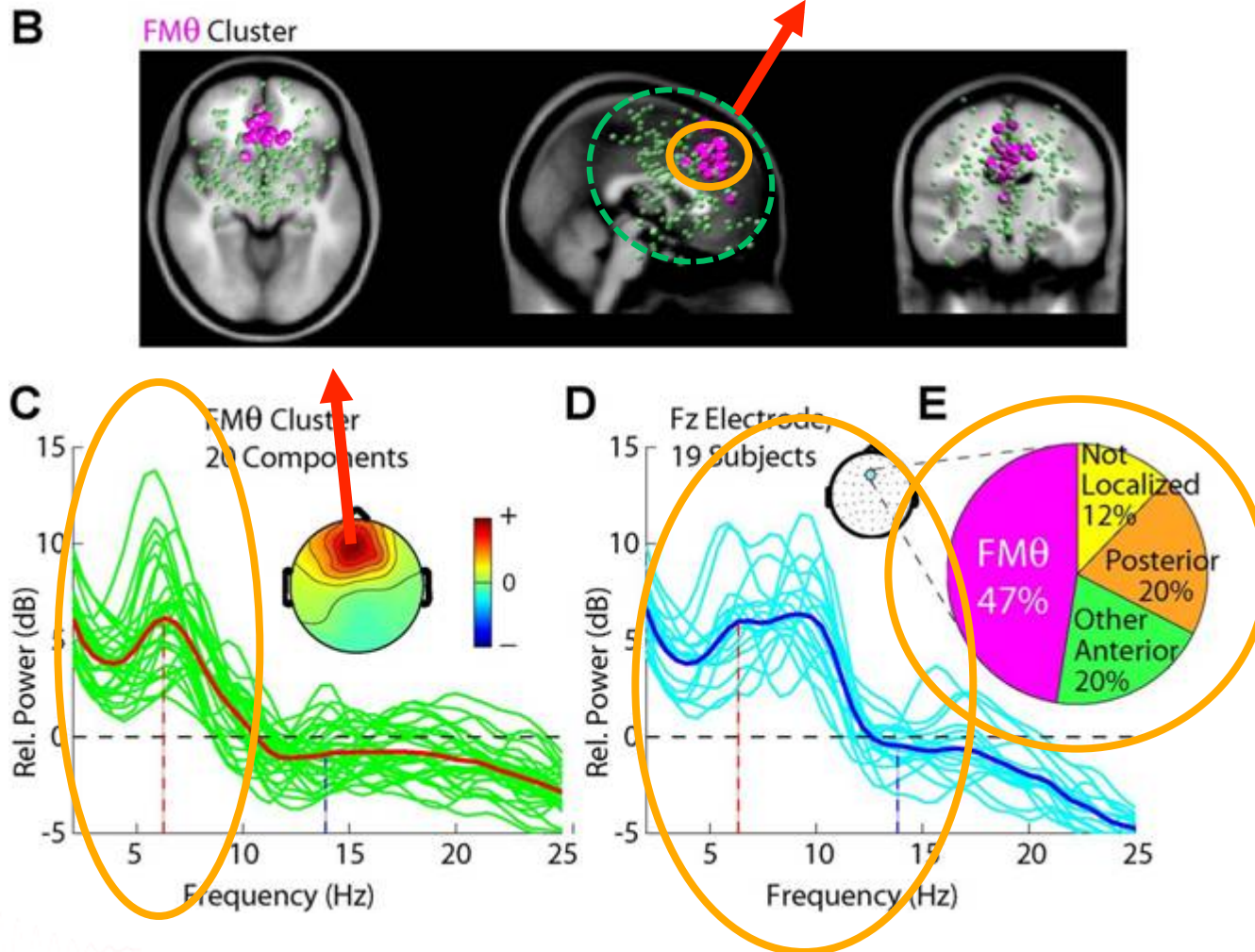
ERSP

ERP

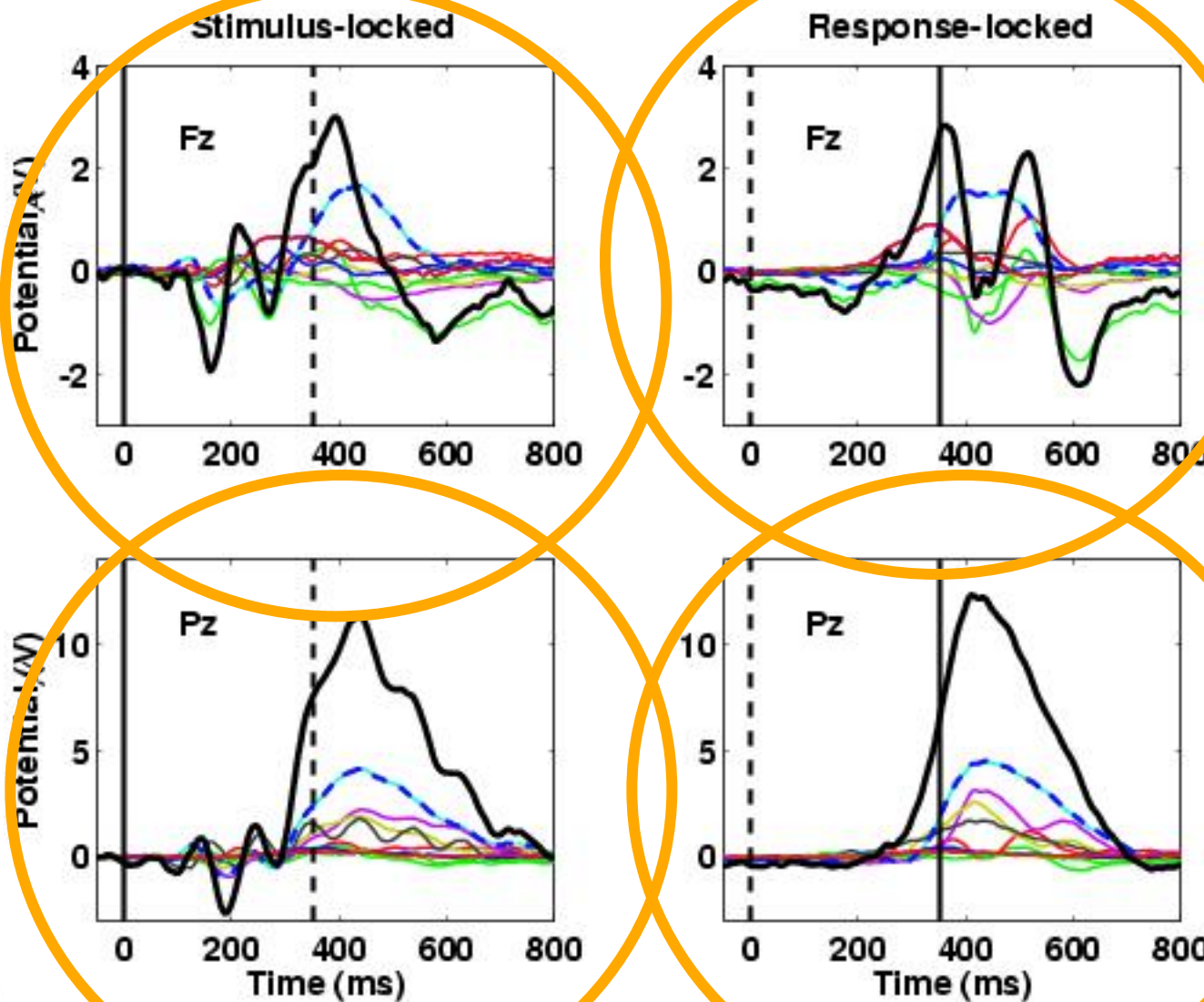




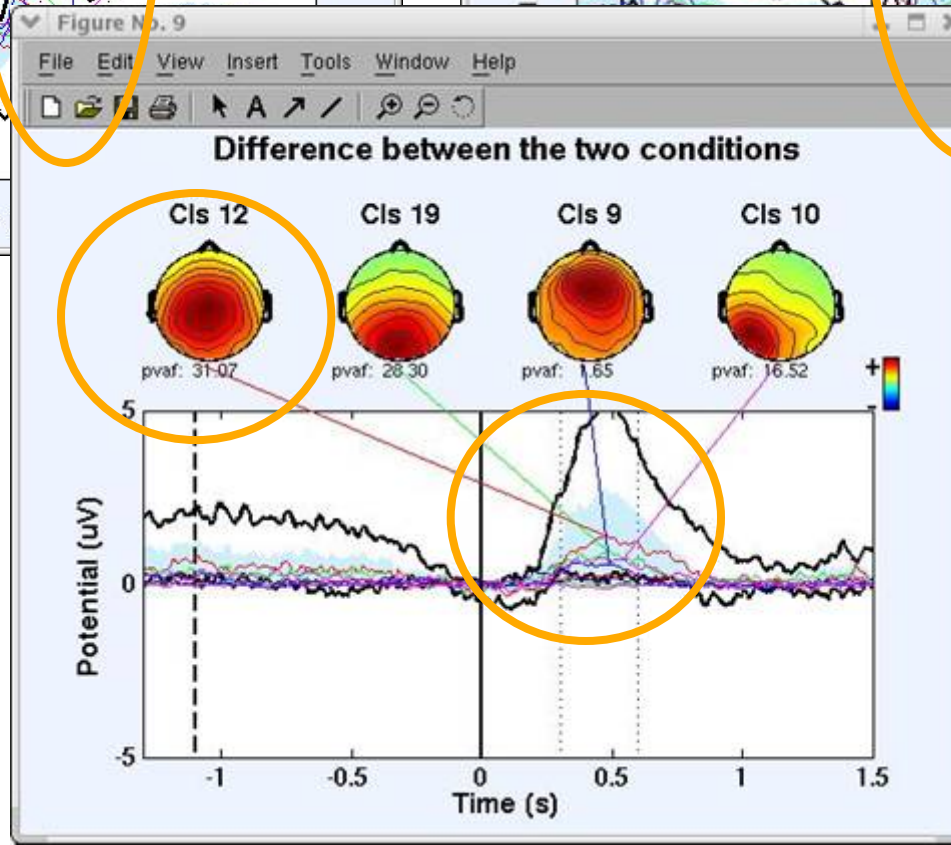
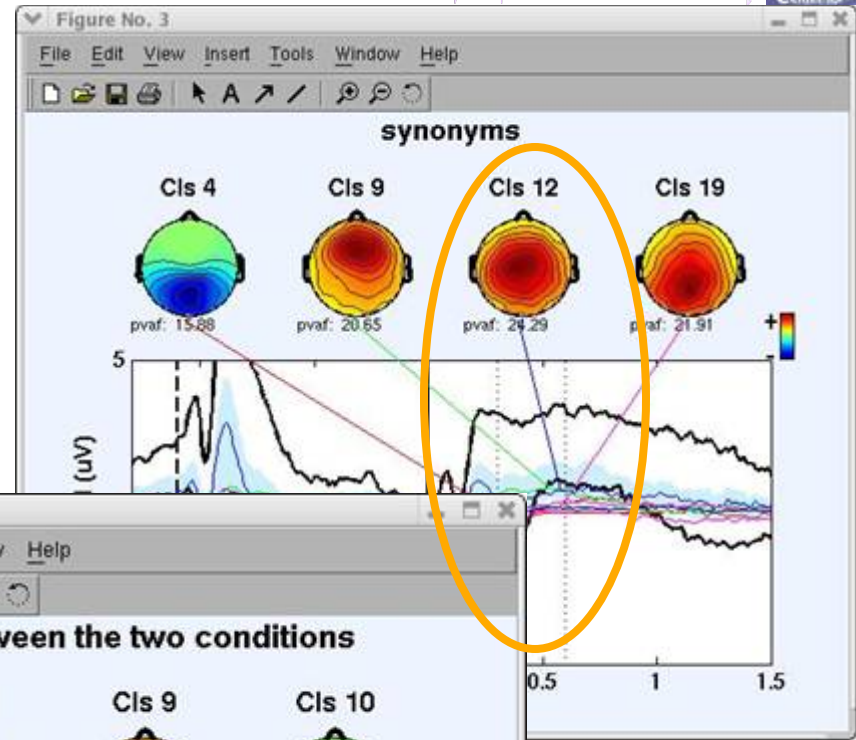
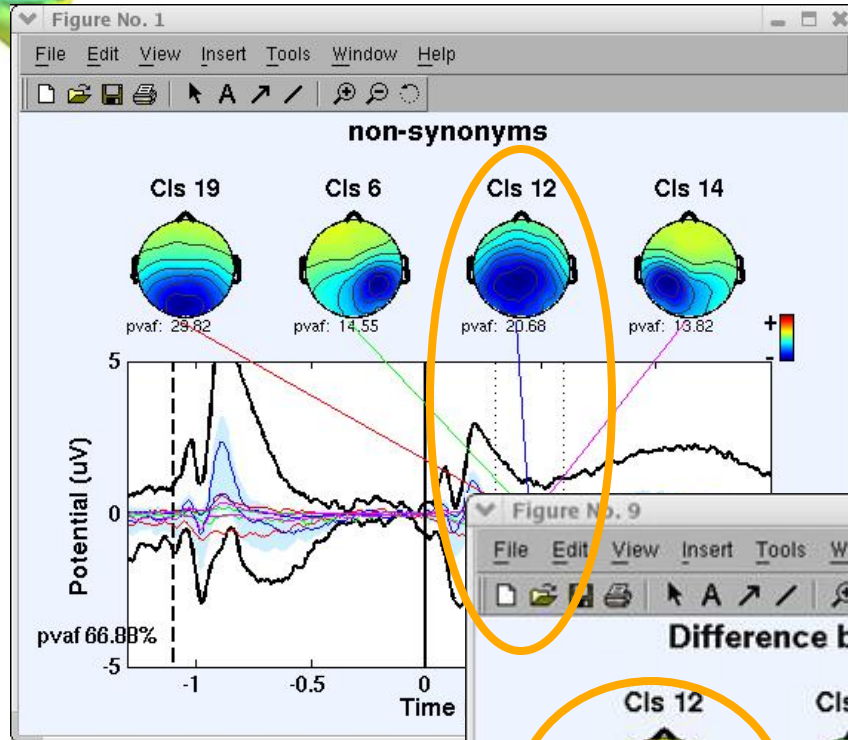
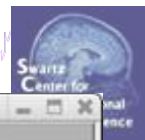
# An FM-theta IC cluster In a working memory task



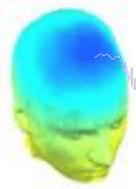
# Complex event-related dynamics produce "the" P300



# Cluster ERP contributions – `std_envtopo()`



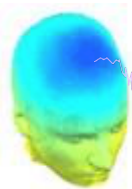




# IC clustering of LPC data



- Clustered components from 15 Ss using a IC distance metric incorporating differences between their (weighted) scalp maps, dipole locations, spectra, ERP, ERSP, and ITC patterns.
- Hand-adjusted clusters to remove outliers.
- Determined time/frequency regions of significant ERSP and ITC for each component using permutation-based statistics.
- Used binomial statistics to highlight time/frequency regions significantly active within clusters.

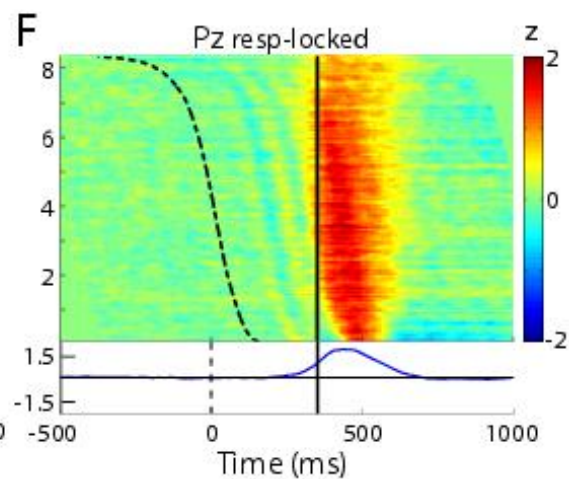
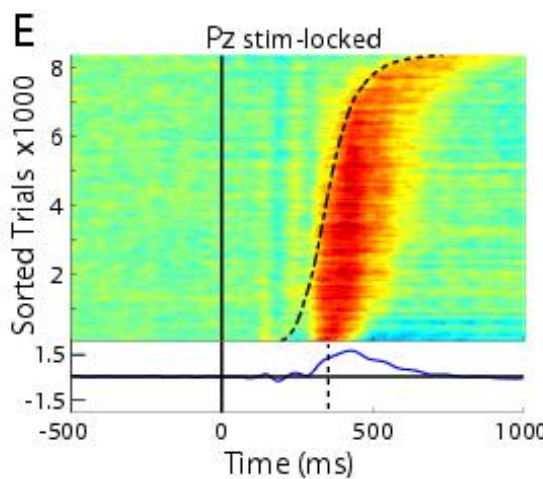
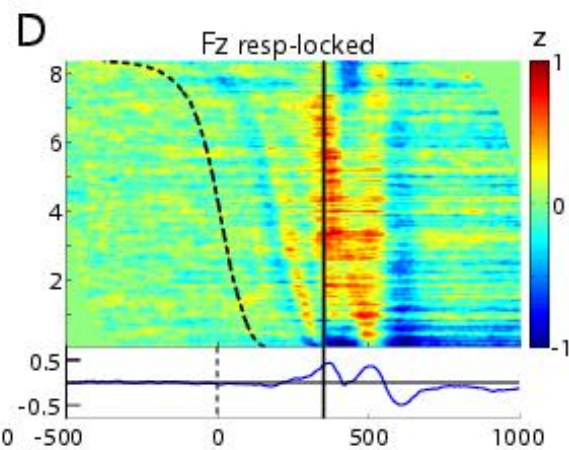
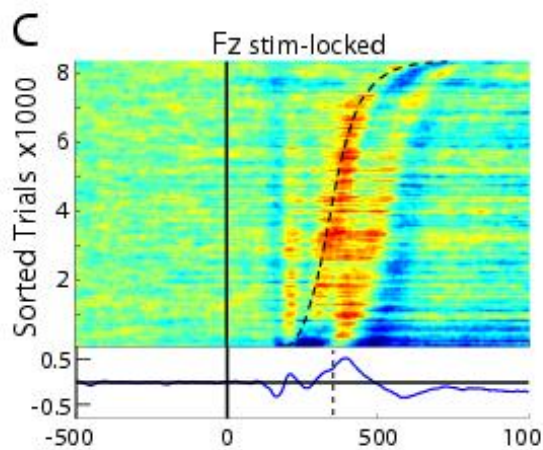
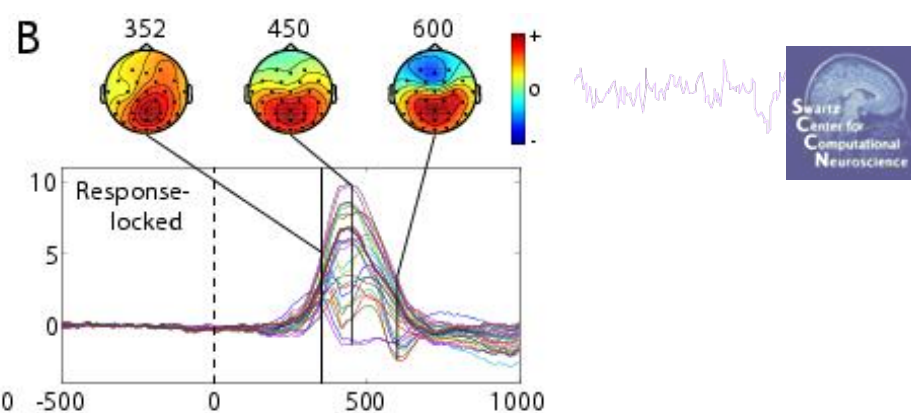
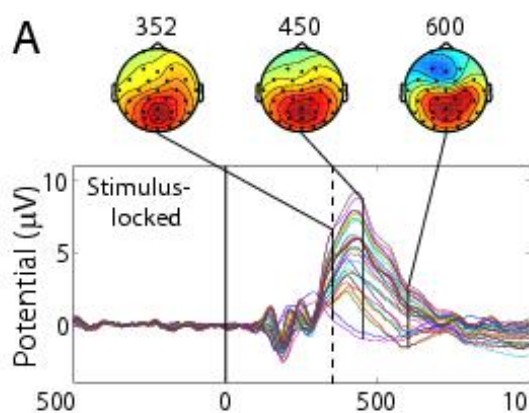
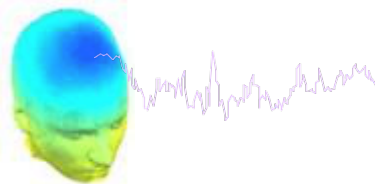


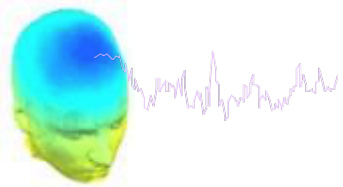
# Visual Selective Attention Task



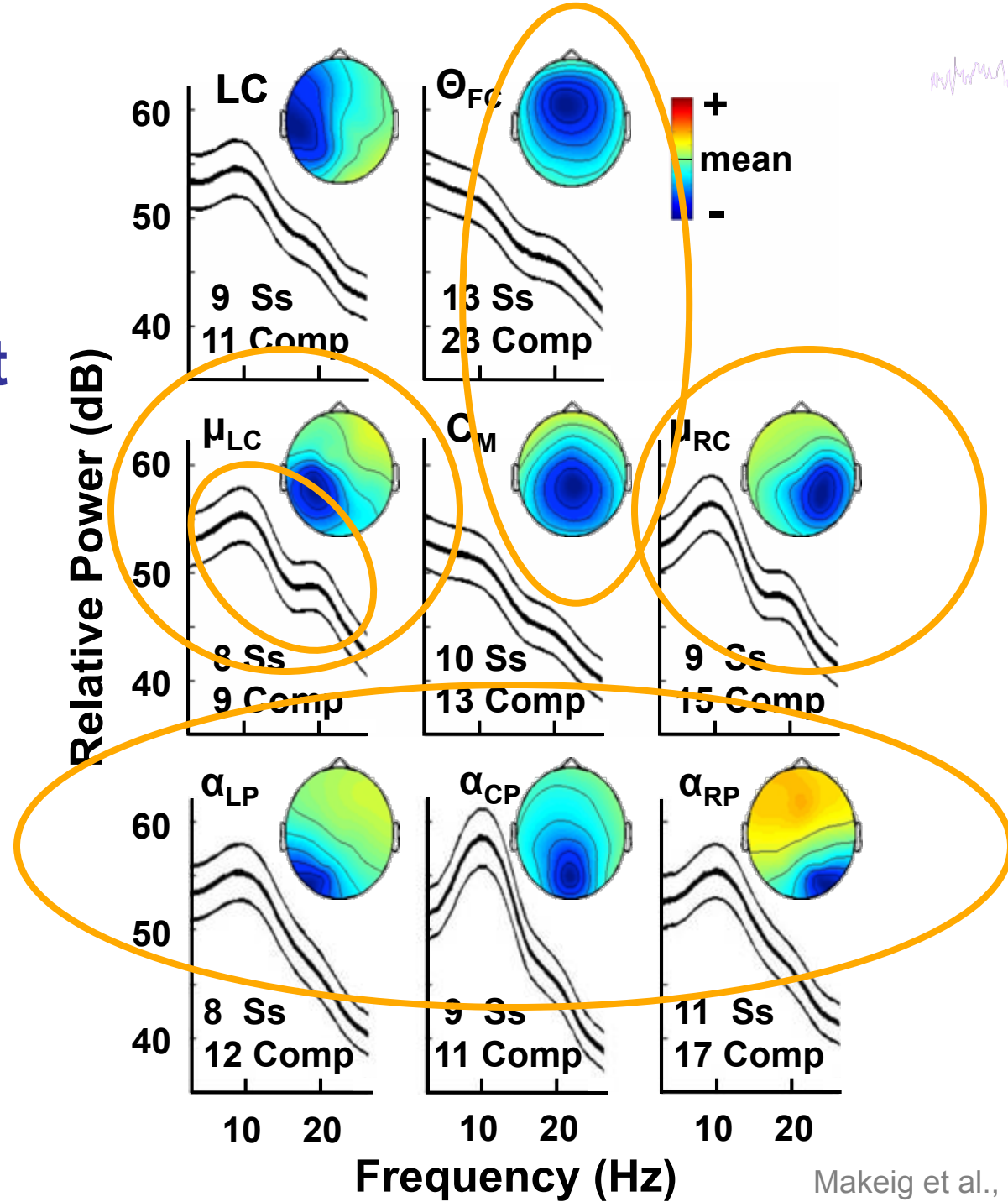
+

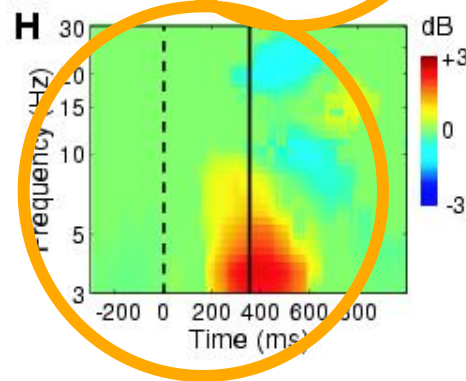
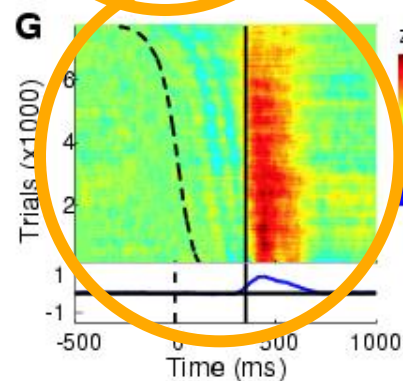
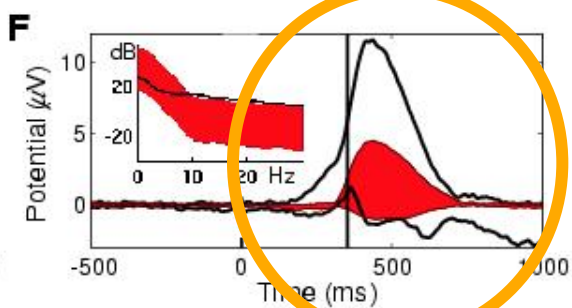
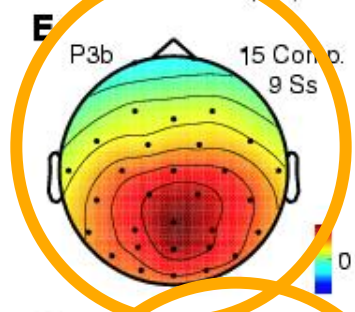
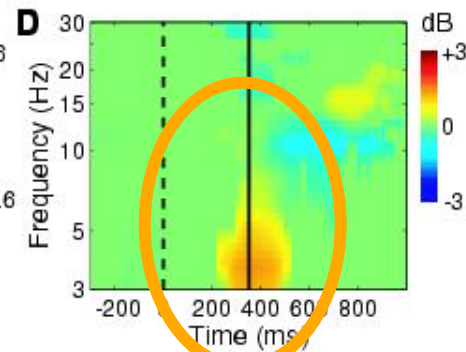
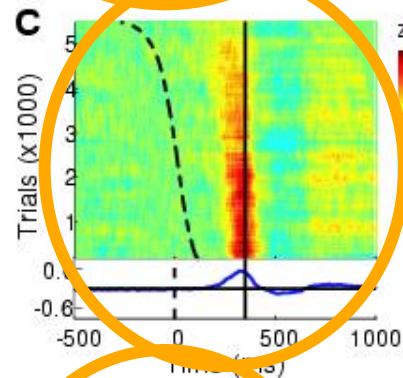
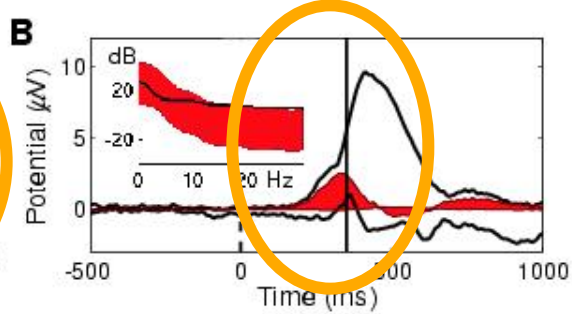
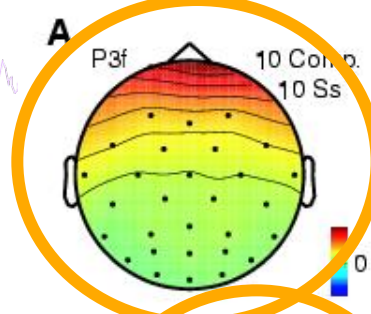
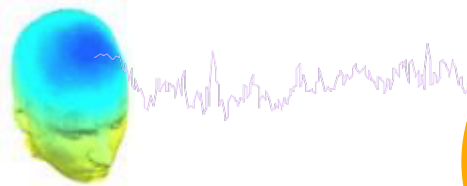
**15 subjects**



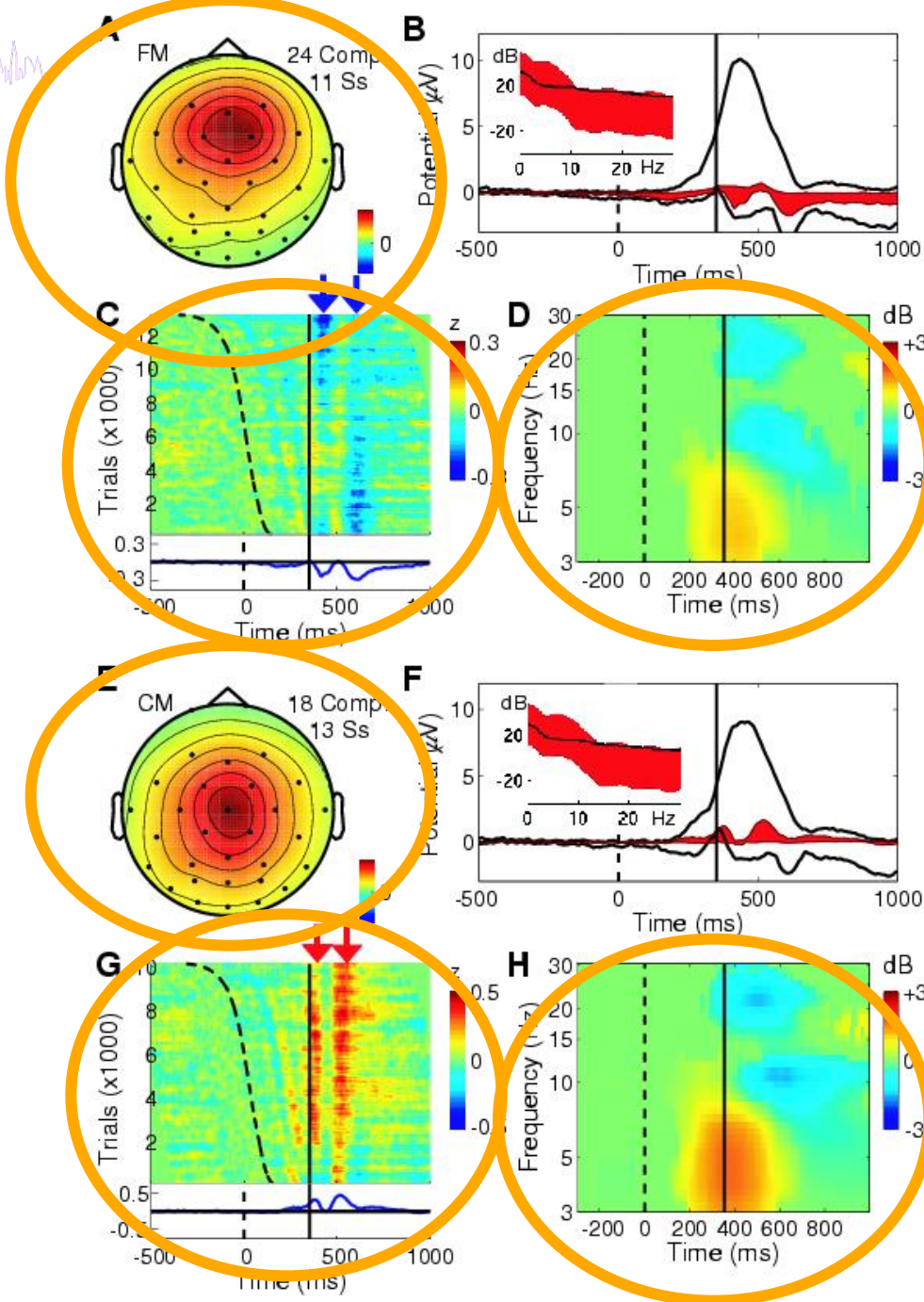
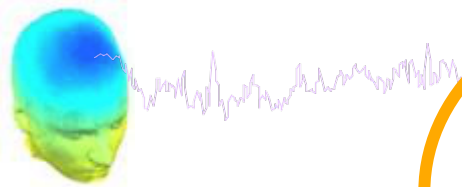


# N1 Component Clusters

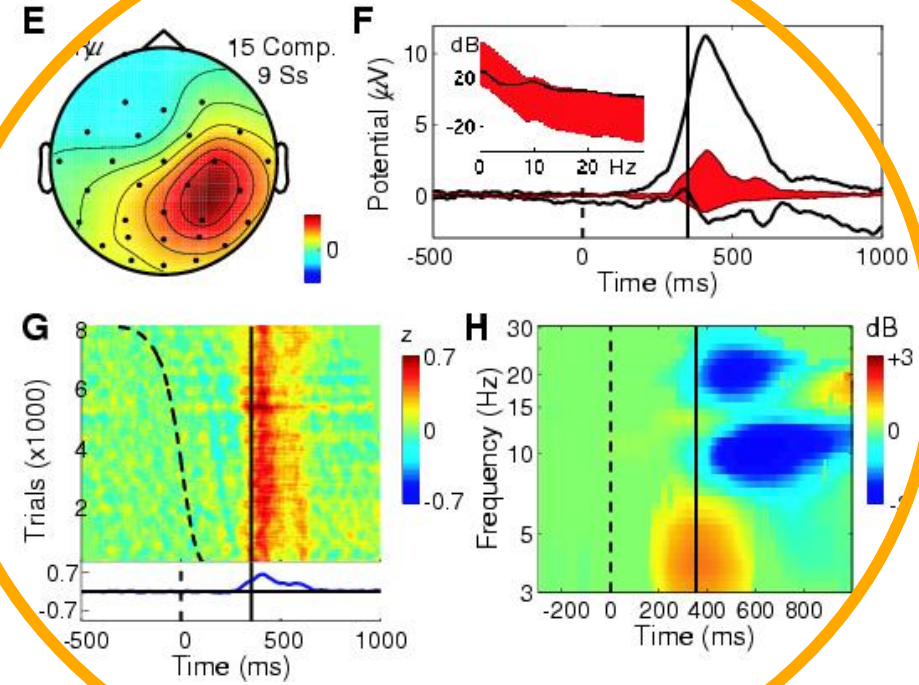
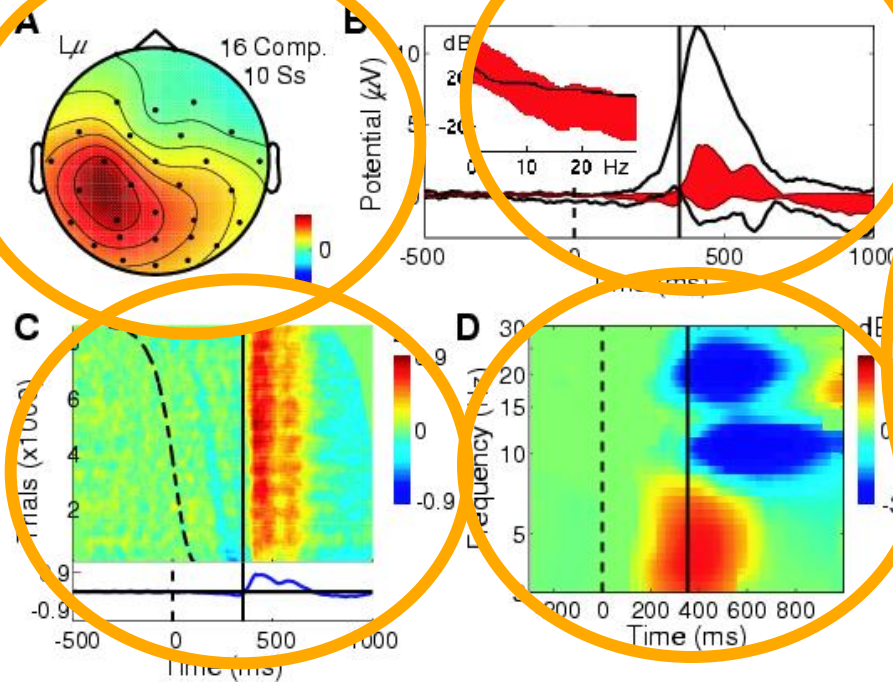


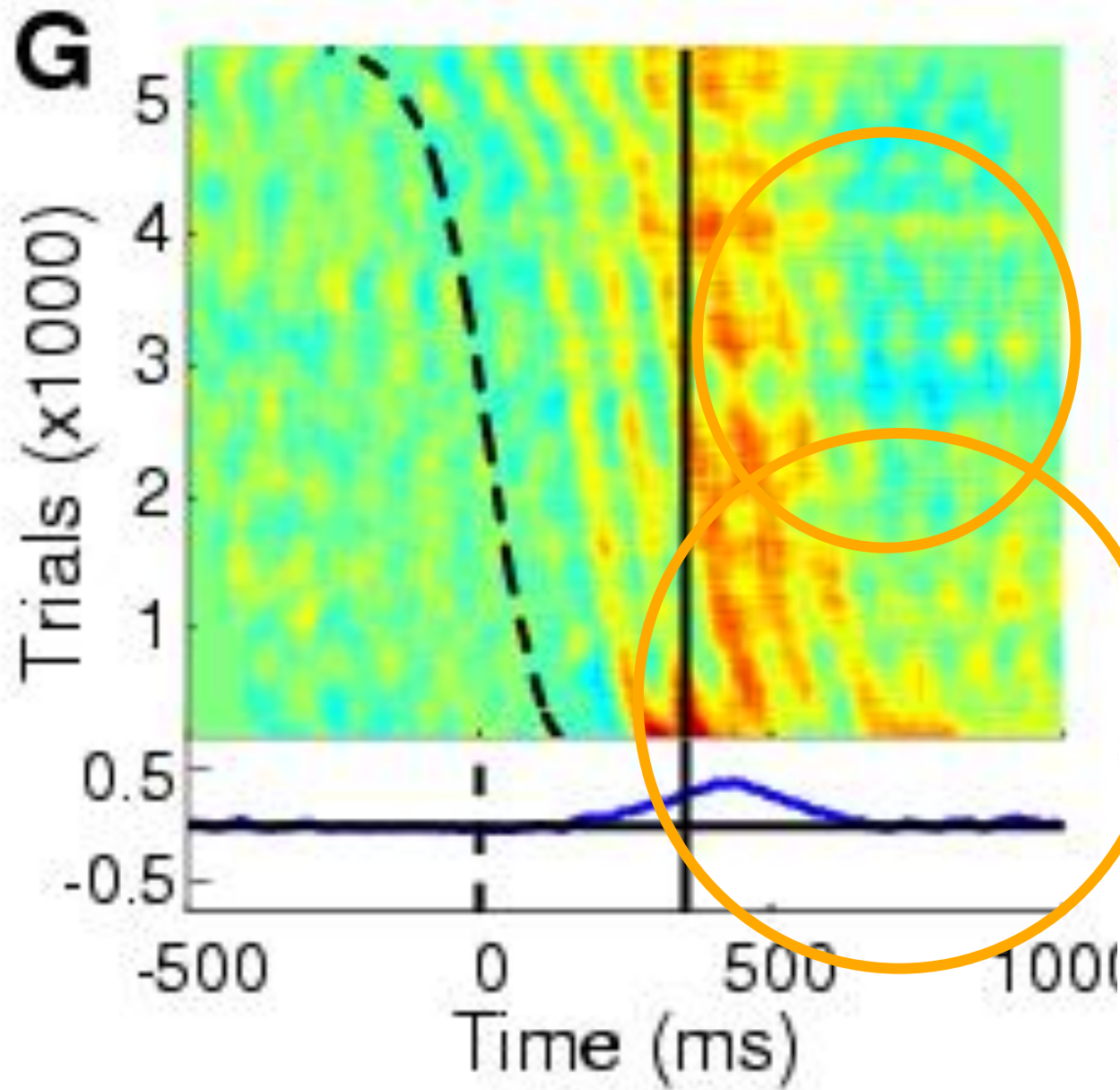
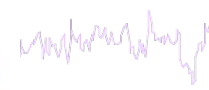
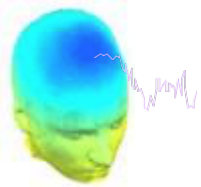


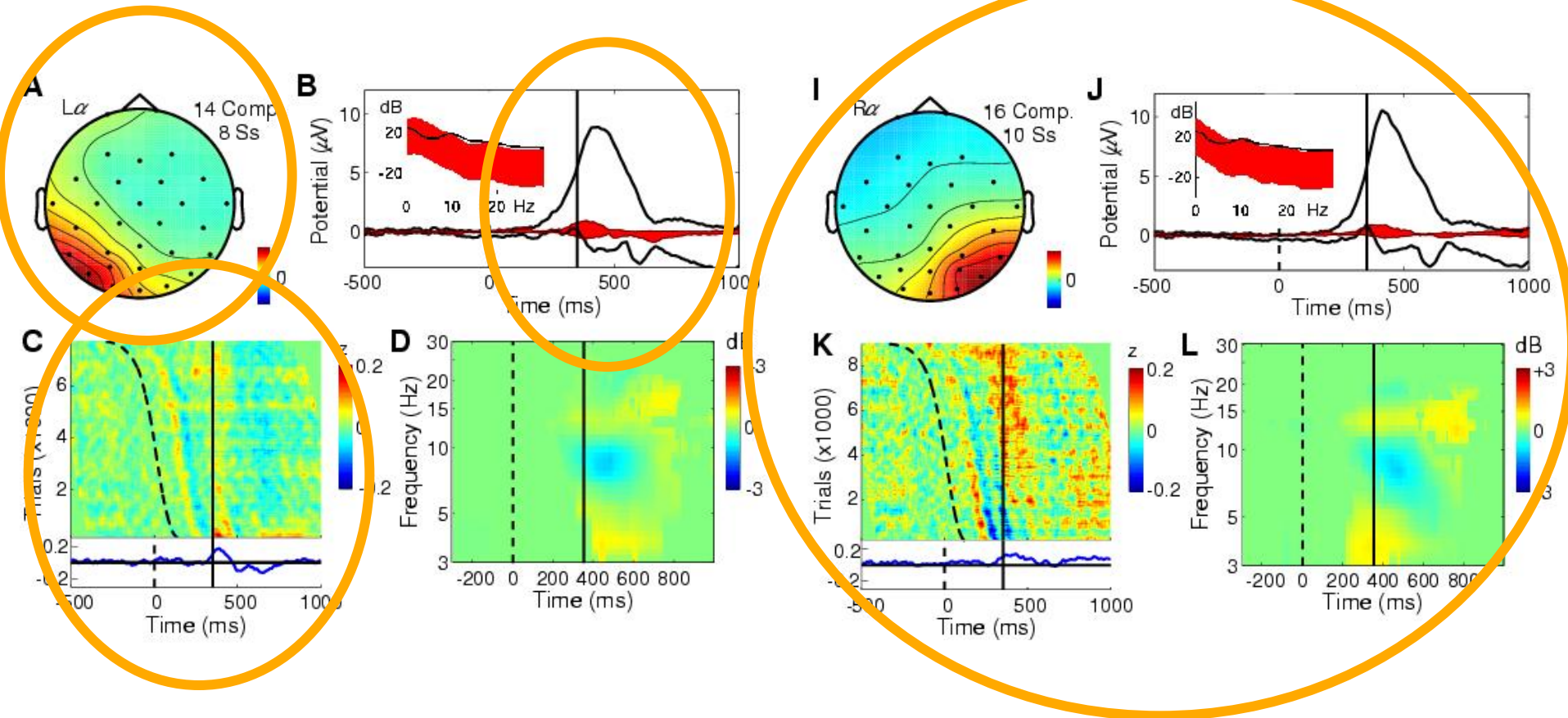














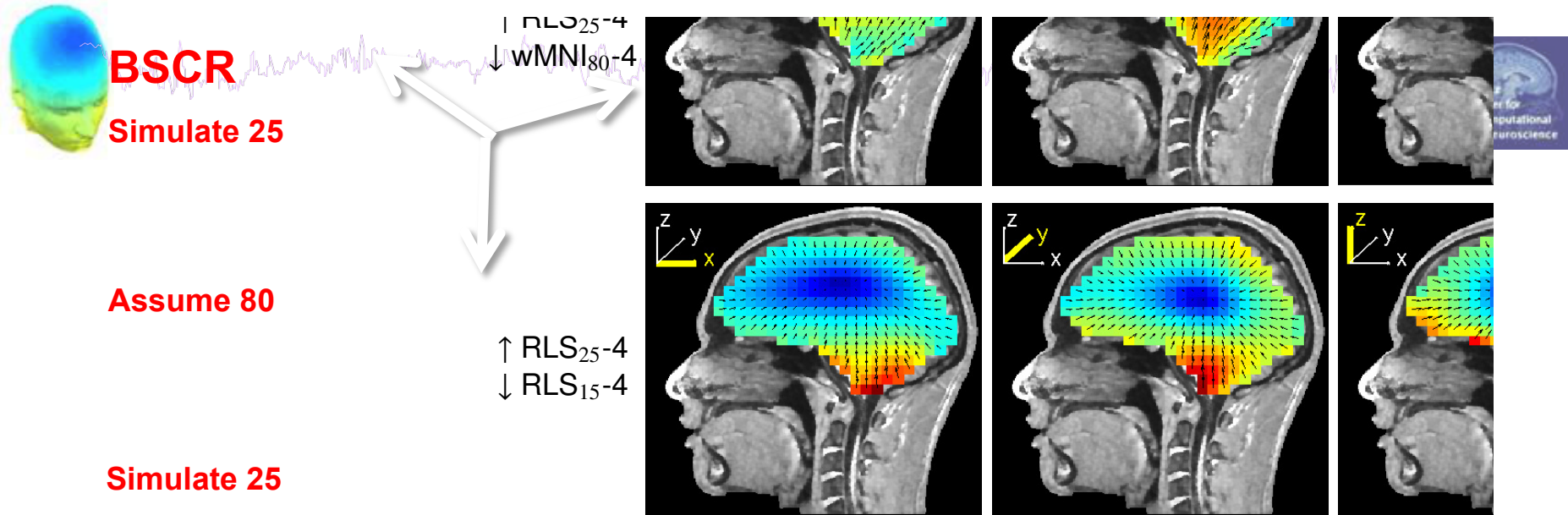


Figure 13: Equivalent dipole source localization error directions (arrows) and magnitudes (colors) for model dipoles in a head model when the brain-to-skull conductivity ratio was mis-estimated as 80:1 (top row) or as 15:1 (bottom row) relative to the forward-model value (25:1). The middle row shows errors when source localization was performed using a warped template head model where the forward model brain-to-skull ratio was again mis-estimated as 80:1. Note that, maximum error shown was 20 mm for the top row to use the same scaling while retaining some contrast for the lower-error plots. Maximum localization errors were shown in Figure 3.

## Effects of Mis-Estimating Skull Conductivity