

Estimating transient phase-amplitude coupling using local mutual information

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Outline

Intro to theory

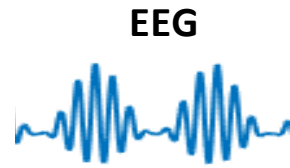
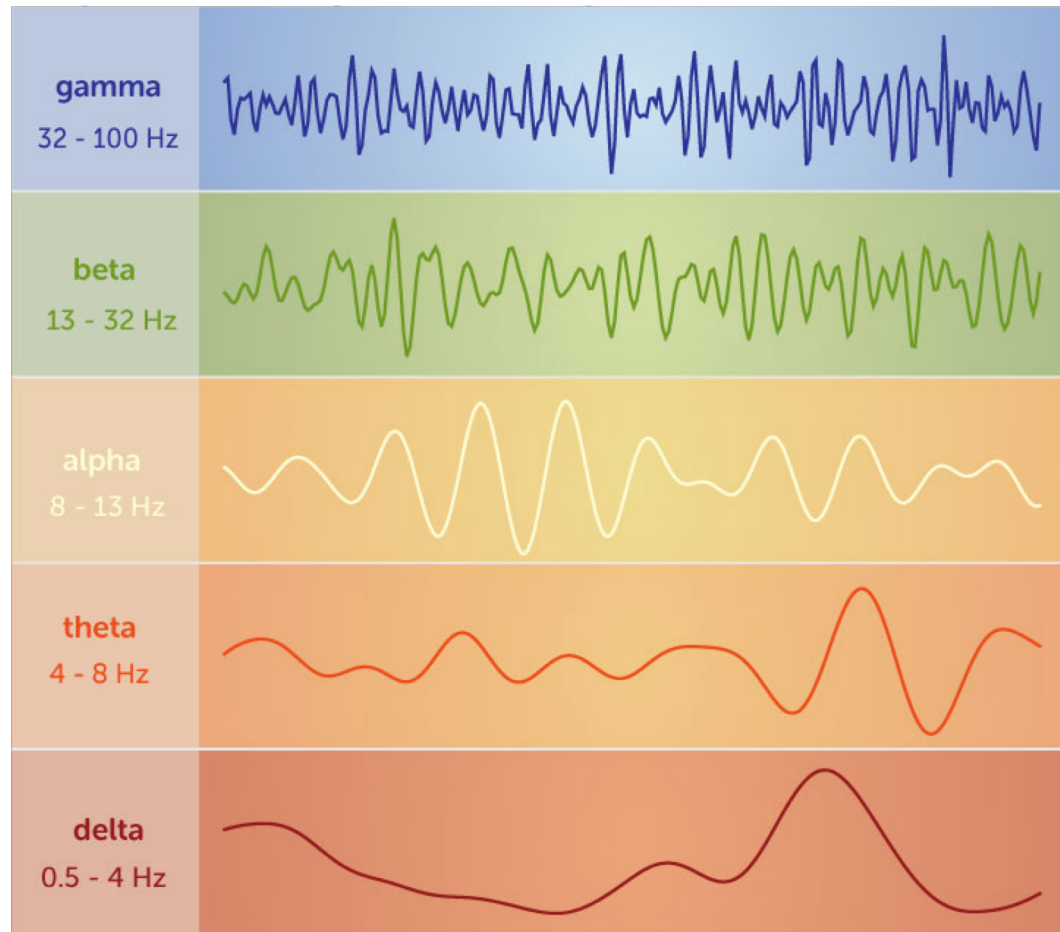
- Intro to Phase-Amplitude Coupling (PAC)
- Local (pointwise) Information Theory Measures
- Estimating PAC with Local Mutual Information

Results

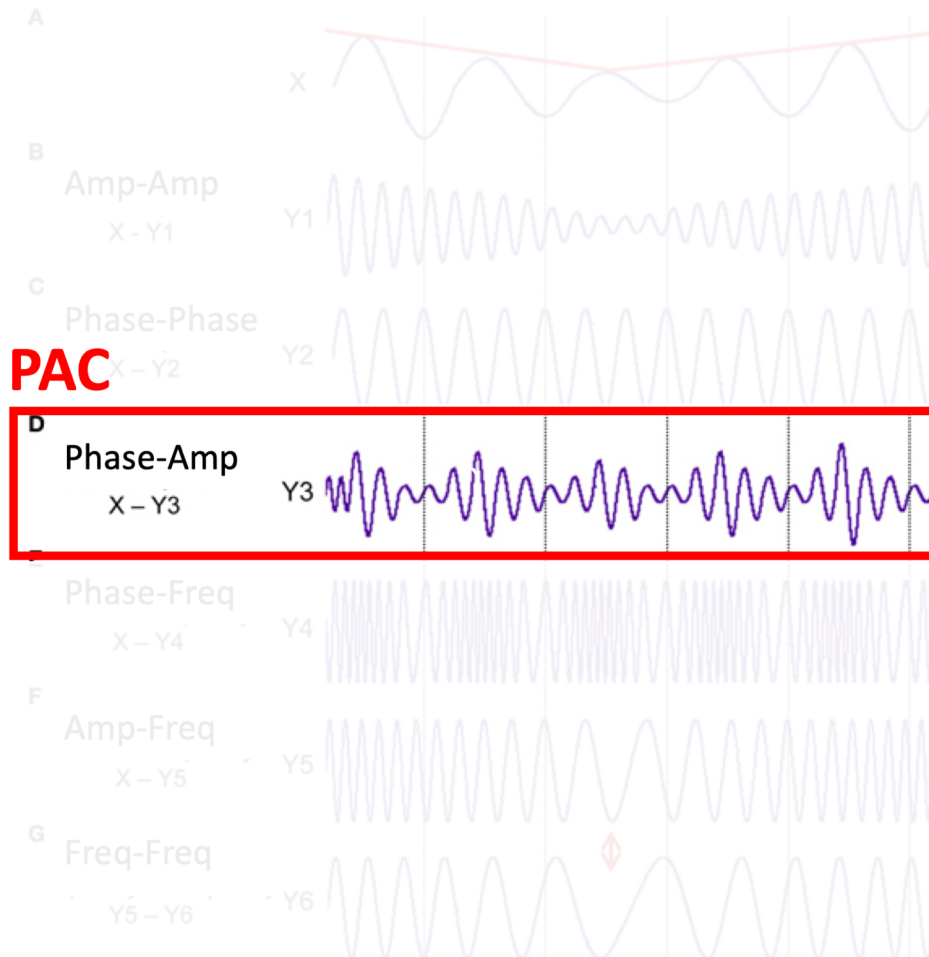
- Simulations
- ECoG data analysis

Demo

Brain oscillations



Cross-Frequency Coupling



Found both in **animals** and **humans**

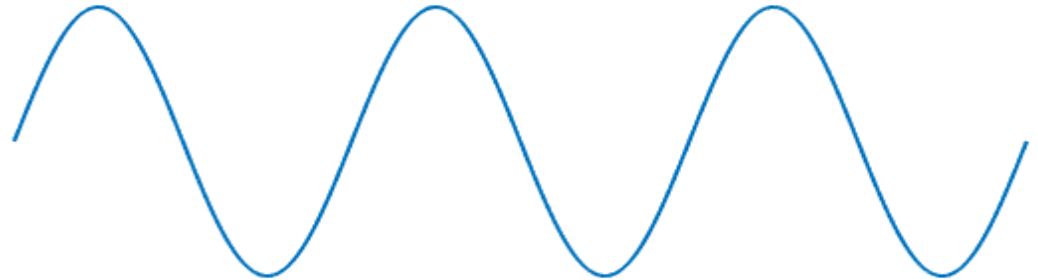
Associated to epilepsy, Parkinson's disease, Alzheimer's disease, schizophrenia, obsessive-compulsive disorder and mild cognitive impairment.

(Mormann et al., 2005; Cohen, 2008; Osipova et al., 2008; Tort et al., 2008, 2009, 2010; Cohen et al., 2009a,b; Colgin et al., 2009; Axmacher et al., 2010a,b; Voytek et al., 2010)

Amplitude Modulation Fundamentals

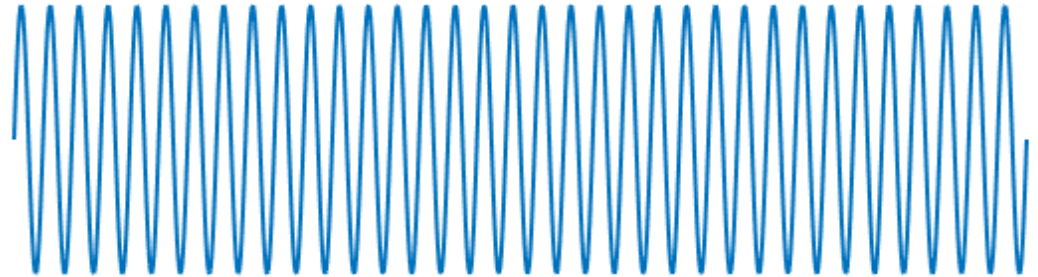
Modulator

$$v_{\text{mod}} = V_{\text{mod}} \sin(2\pi f_{\text{mod}} t)$$



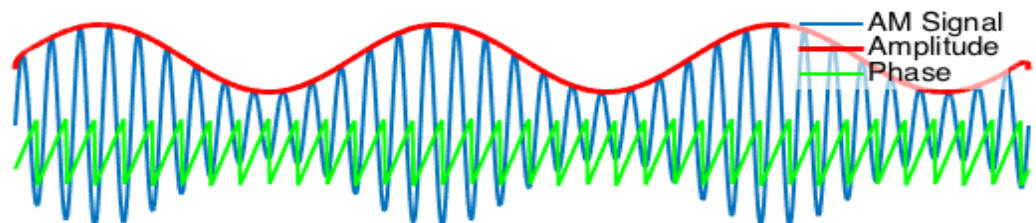
Carrier

$$v_{\text{carr}} = V_{\text{carr}} \sin(2\pi f_{\text{carr}} t)$$



AM Signal

$$v_{\text{AM}} = V_{\text{carr}} \sin(2\pi f_{\text{carr}} t) + [V_{\text{mod}} \sin(2\pi f_{\text{mod}} t)] \sin(2\pi f_{\text{carr}} t)$$



Instantaneous Phase and Amplitude

$$S_t = s_{m_t} e^{i\phi_t}$$

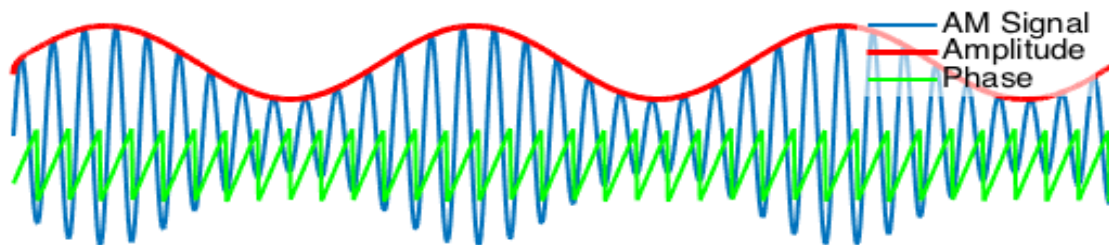
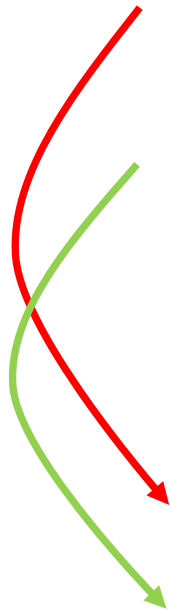
By means of the **Hilbert transform** a signal can be expressed as its **analytic signal**

$$s_{m_t} = |S_t|$$

Instantaneous amplitude (or the envelope)

$$\phi_t = \arg[S_t]$$

Instantaneous phase.



AM Signal
Amplitude
Phase

$\leftarrow abs(hilbert(S_t))$
 $\leftarrow angle(hilbert(S_t))$

Computing PAC

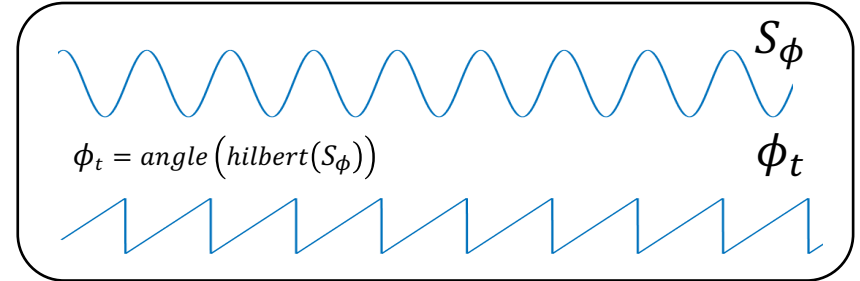
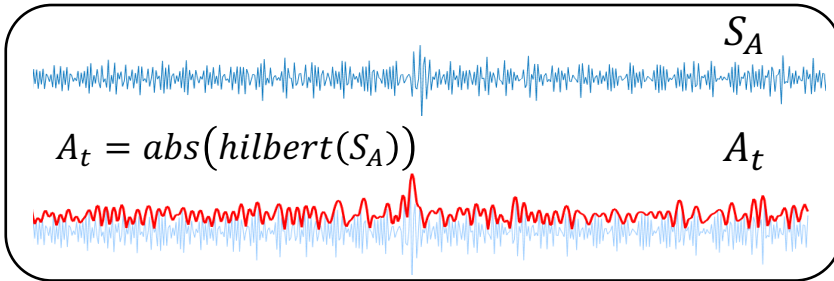
Electrophysiological signal



High frequency band f_{Amp} (e.g: 30-50Hz)

Low frequency band f_{phase} (e.g: 5-12Hz)

Band-pass Filter

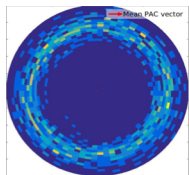


Mean Vector Length

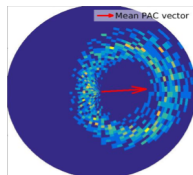
Canolty et al. 2006

- Composite vectors $z_t = A_t e^{i\phi_t}$
- Mean vector length

$$MVLmi = \left| \frac{1}{N} \sum_{t=1}^N z_t \right|$$



No Coupling



Coupling

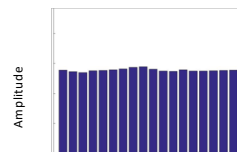
Kullback-Leibler Modulation Index

Tort et al, 2010

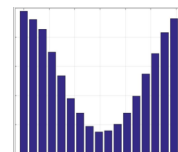
$$P(j) = \frac{\langle A_{f_A} \rangle \phi_{f_p}(j)}{\sum_{k=1}^N \langle A_{f_A} \rangle \phi_{f_p}(k)}$$

$$MI = \frac{D_{KL}(P,U)}{\log N}$$

Compute the Kullback-Leibler with a uniform distribution



No Coupling



Coupling

GLM Measure

Penny et al. 2008

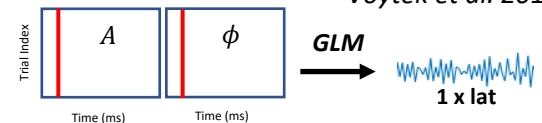
$$A_t = X\beta + e$$

$$X = \begin{bmatrix} \cos\phi_1 & \sin\phi_1 & 1 \\ \vdots & \vdots & \vdots \\ \cos\phi_N & \sin\phi_N & 1 \end{bmatrix}$$

Explained variance as an index of PAC

ERPAC

Voytek et al. 2013



Time resolved 'average' PAC by applying **GLM Measure** for each latency in event related data

Computing PAC

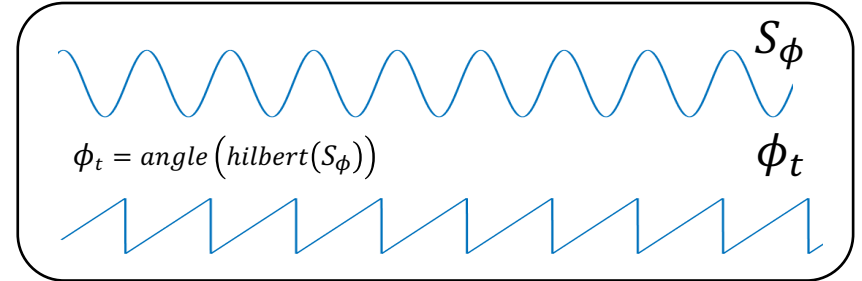
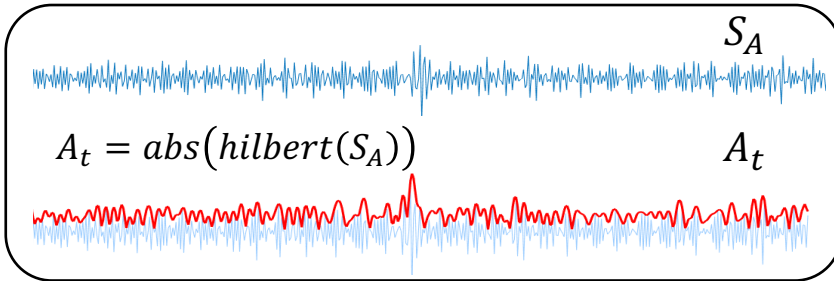
Electrophysiological signal



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Band-pass Filter

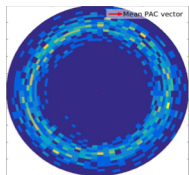


Mean Vector Length

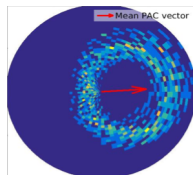
Canolty et al. 2006

- Composite vectors $z_t = A_t e^{i\phi_t}$
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No Coupling



Coupling

Kullback-Leibler Modulation Index

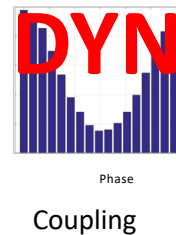
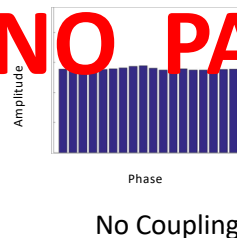
Tort et al, 2010

$$P(j) = \frac{\langle A_{f_A} \rangle \phi_{f_p}(j)}{\sum_{k=1}^N \langle A_{f_A} \rangle \phi_{f_p}(k)}$$

$$MI = \frac{D_{KL}(P,U)}{\log N}$$

Compute the Kullback-Leibler with a uniform distribution

NO PAC DYNAMIC



GLM Measure

Penny et al. 2008

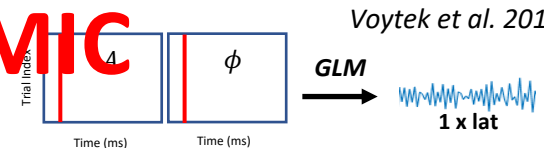
$$A_t = X\beta + e$$

$$X = \begin{bmatrix} \cos\phi_1 & \sin\phi_1 & 1 \\ \vdots & \vdots & \vdots \\ \cos\phi_N & \sin\phi_N & 1 \end{bmatrix}$$

Explained variance as an index of PAC

ERPAC

Voytek et al. 2013



Time resolved 'average' PAC by applying **GLM Measure** for each latency in event related data

Can we do better than this?

YES WE CAN

Goal:
Estimating PAC temporal dynamics

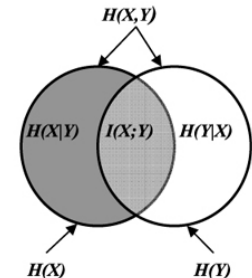
Information Theory Definitions

Shannon Entropy: average amount of uncertainty associated to any measure x of X

$$H(X) = -\sum_x p(x) \log_2 p(x)$$

Mutual Information: average reduction in uncertainty about X given the knowledge of the value of Y

$$I(X, Y) = H(X) - H(X|Y)$$



Non-linear form of correlation !!!!!!!

$$I(X, Y) = -\sum p(x, y) \log_2 \frac{p(x, y)}{p(x)p(y)}$$

KSG Mutual Information Estimator

(Kraskov, Stogbauer and Grassberger)

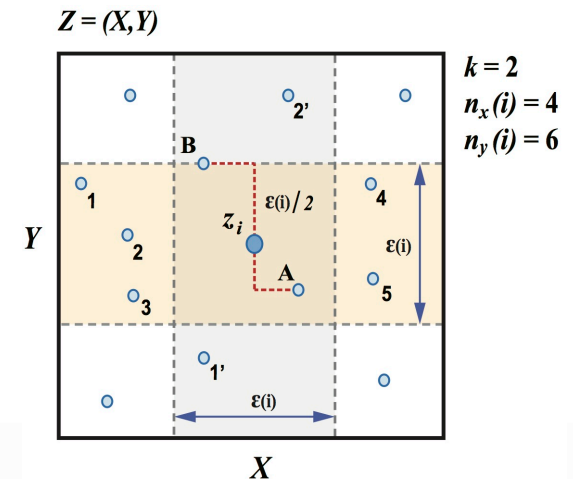
- Extension of Kozachenko-Leonenko estimator of Entropy
- Non-parametric estimator
- Data efficient
- Minimal bias

Assume the joint space $Z = (X, Y)$

Determining k -nearest neighbors for each z_i

$$\|z - z'\| = \max\{\|x - x'\|, \|y - y'\|\}$$

- Find k -nearest neighbor of z_i (a distance $\frac{\varepsilon}{2}$)
- Count the number of points $n_x(i)$ and $n_y(i)$ in the marginal space within a row (and column) of width ε



Estimate Mutual Information

$$I(X, Y) = \psi(k) - \langle \psi(n_x + 1) + \psi(n_y + 1) \rangle + \psi(N)$$

Estimating local Mutual Information

Lizier et al. 2008, considered the estimation of Local MI from the KSG estimator

Estimate Mutual Information

Kraskov et al. 2004

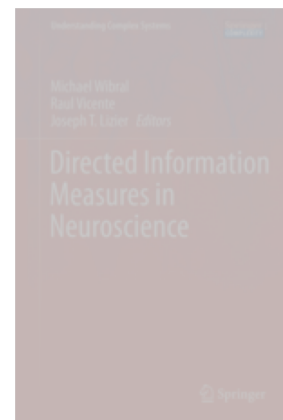
$$I(X,Y) = \psi(k) - \langle \psi(n_x + 1) + \psi(n_y + 1) \rangle + \psi(N)$$

Unrolling expectation

Estimating Local Mutual Information

$$i(x,y) = \psi(k) - \psi(n_x + 1) - \psi(n_y + 1) + \psi(N)$$

Lizier, J. T. *Directed Information Measures in Neuroscience*. Springer, 2014



Goal:

Estimating PAC using local Mutual Information

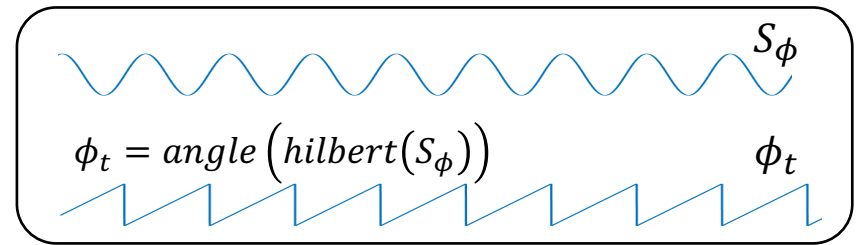
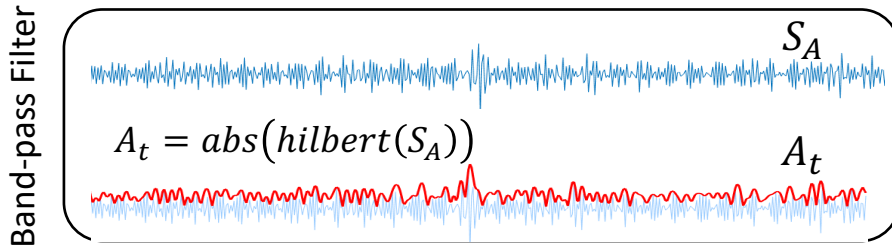
Instantaneous MIPAC

Data model: Continuous data ($1 \times N_{lat}$)



High frequency band f_{Amp} (e.g: 30-50Hz)

Low frequency band f_{phase} (e.g: 5-12Hz)



Assume the joint space $Z = (A_t, \phi_t)$

$$\|z - z'\| = \max\{\|\phi - \phi'\|, \|A - A'\|\}$$

Circular norm color: green; Euclidean norm

$$i(x, y) = \psi(k) - \psi(n_x + 1) - \psi(n_y + 1) + \psi(N)$$

Inst. MIPAC

% Single trials or continuous

$\Delta_{var} = \text{Inf}$; % Initialize Percentage variance reduction
 $c = 1$;

while $\Delta_{var_threshold} < \Delta_{var}$

Estimate $i(A_t, \phi_t)$ for $k=c$;

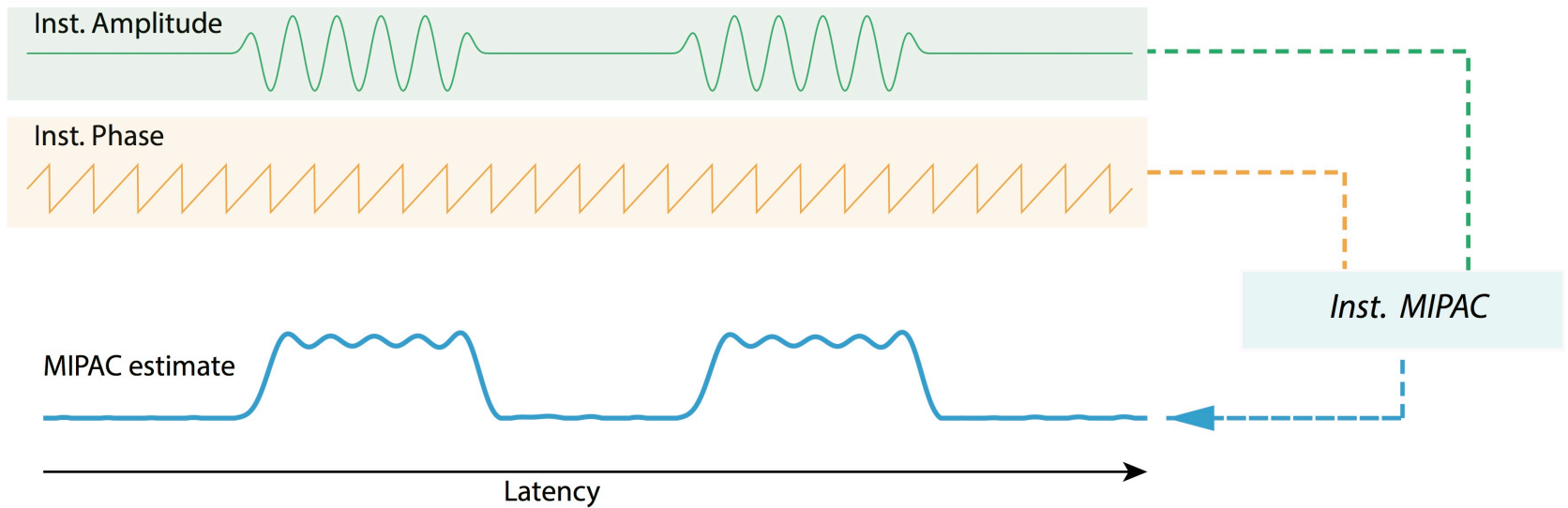
Compute Δ_{var} ;

$c = c+1$;

End

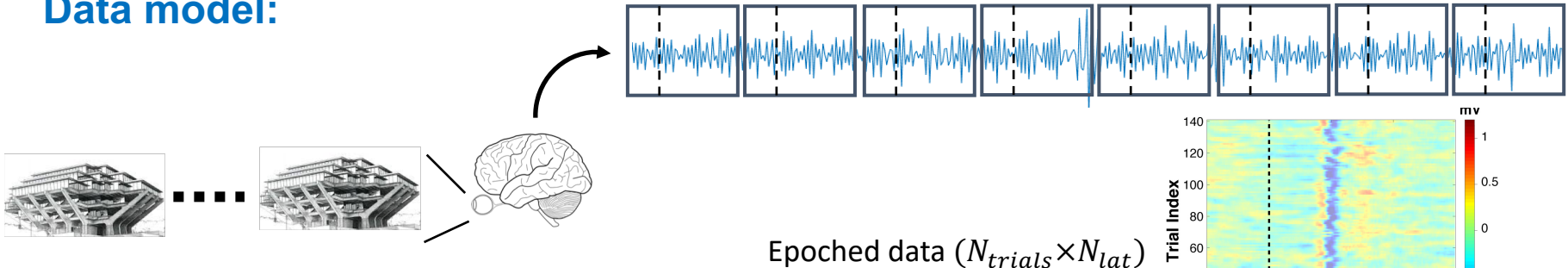
MIPAC = Low-pass filter $i(A_t, \phi_t)$ at f_{phase} ;

Inst. MIPAC in a nutshell



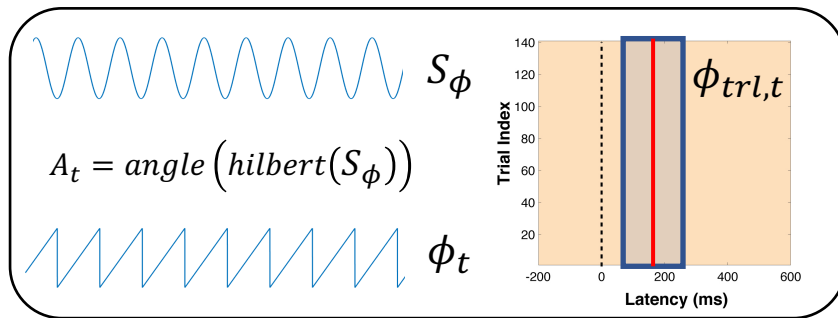
Event-related MIPAC

Data model:

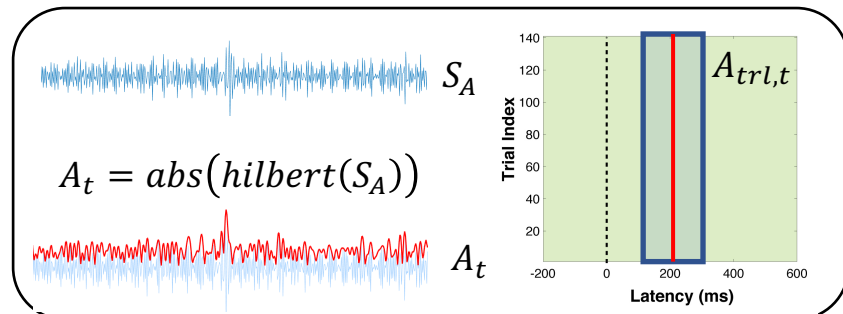


Low frequency band (f_{phase})

Full cycle of f_{phase}



High frequency band (f_{amp})



Event Related MIPAC (cyclostationary)

% Epoches data

for $t = 1:N_{lat}$

$\Delta_{var} = \text{Inf}$; % Initialize Percentage variance reduction
 $c = 1$;

while $\Delta_{var_threshold} < \Delta_{var}$

Estimate $i(A_{trl,t}(:, t), \phi_{trl,t}(:, t))$ for $k=c$;

(Neighbors are count in a latency window)

Compute Δ_{var} ;

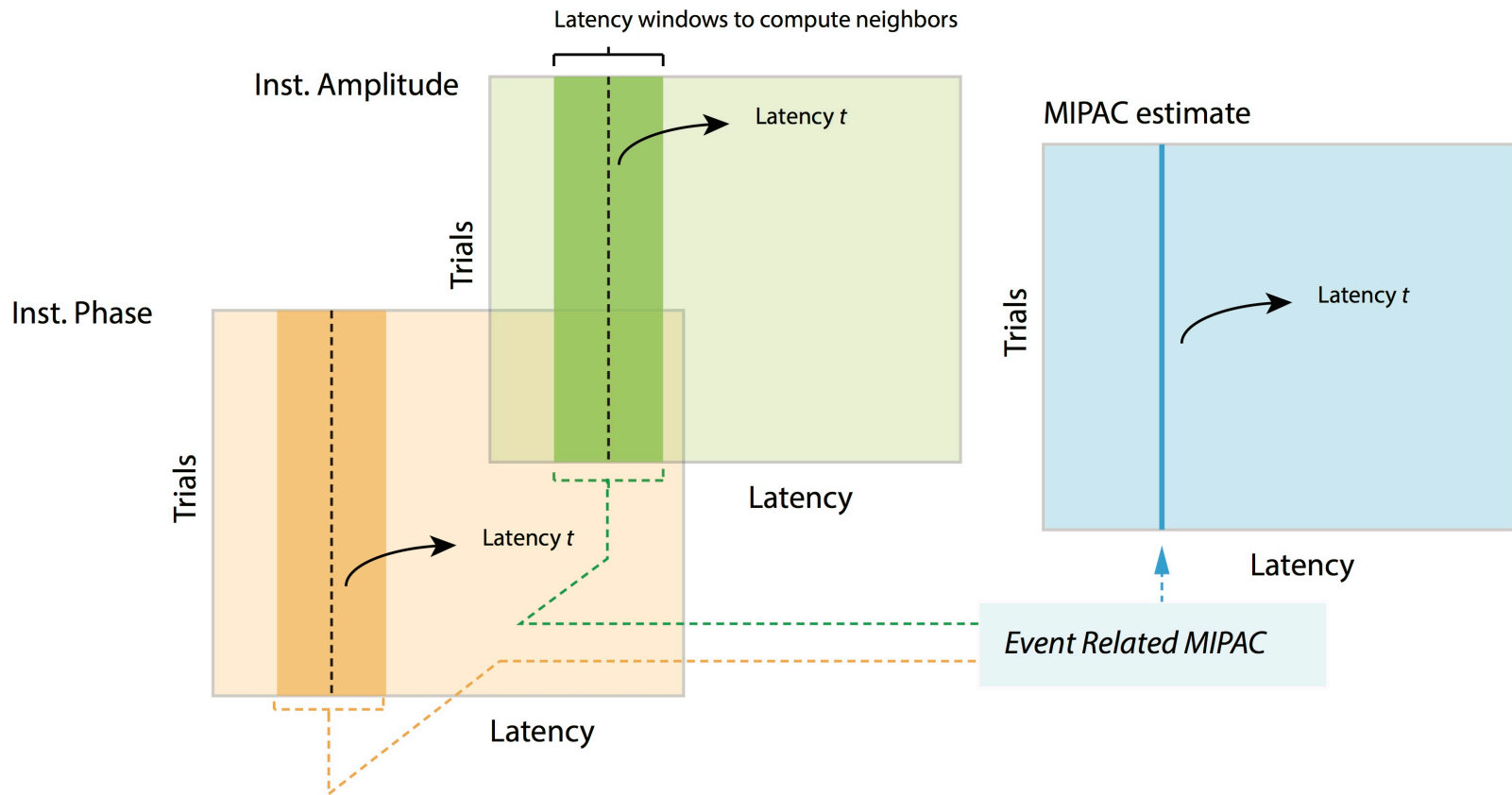
$c = c+1$;

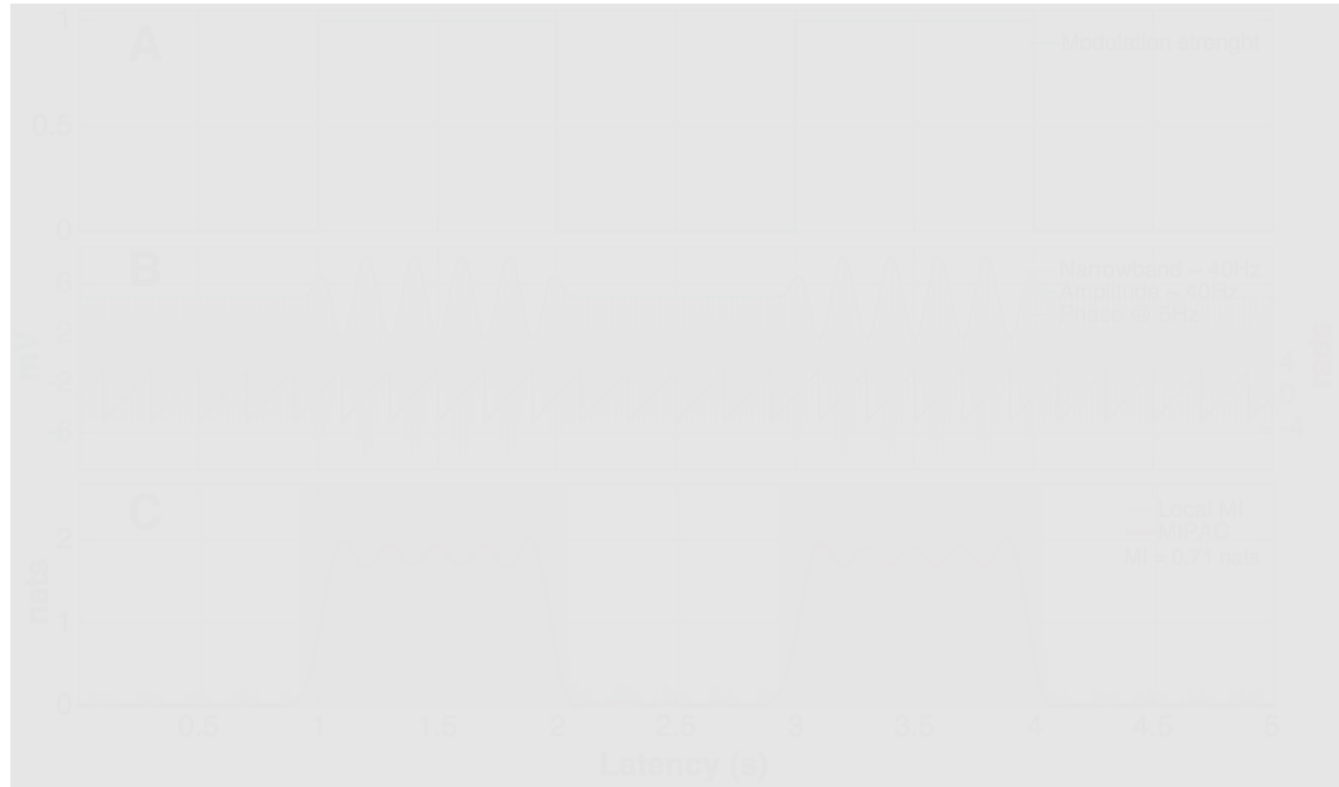
end

end

MIPAC = Low-pass filter $i(A_{trl,t}, \phi_{trl,t})$ at f_{phase} .

Event-related MIPAC in a nutshell





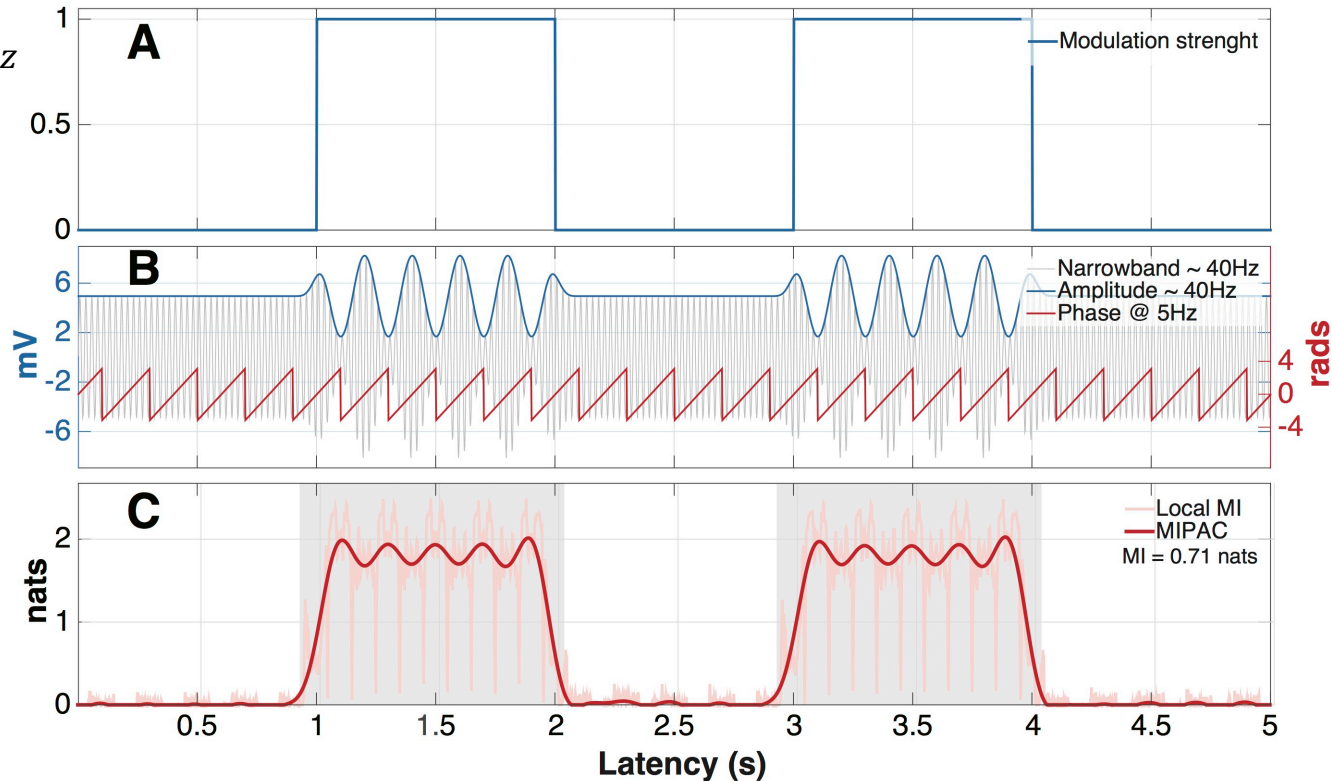
MIPAC Simulations

Simulation 1.1: Instantaneous MIPAC

$$f_{mod} = 5\text{Hz}$$

$$f_{carr} = 40\text{Hz}$$

$$S_{rate} = 500\text{Hz}$$



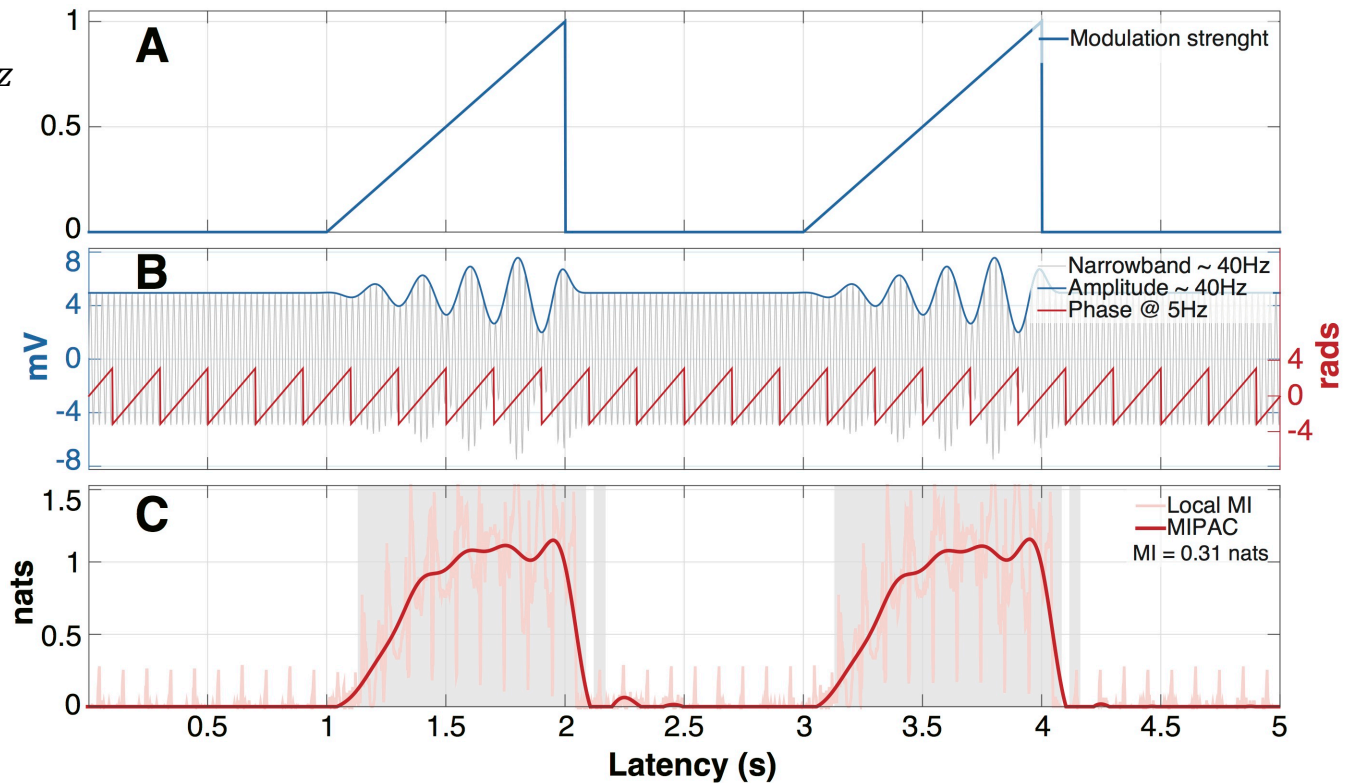
- (A) Block-shaped waveform modulation strength.
 (B) Simulated signal
 (C) Estimated MIPAC (red), and local MI (light red)

Simulation 1.2: Instantaneous MIPAC

$$f_{mod} = 5\text{Hz}$$

$$f_{carr} = 40\text{Hz}$$

$$S_{rate} = 500\text{Hz}$$



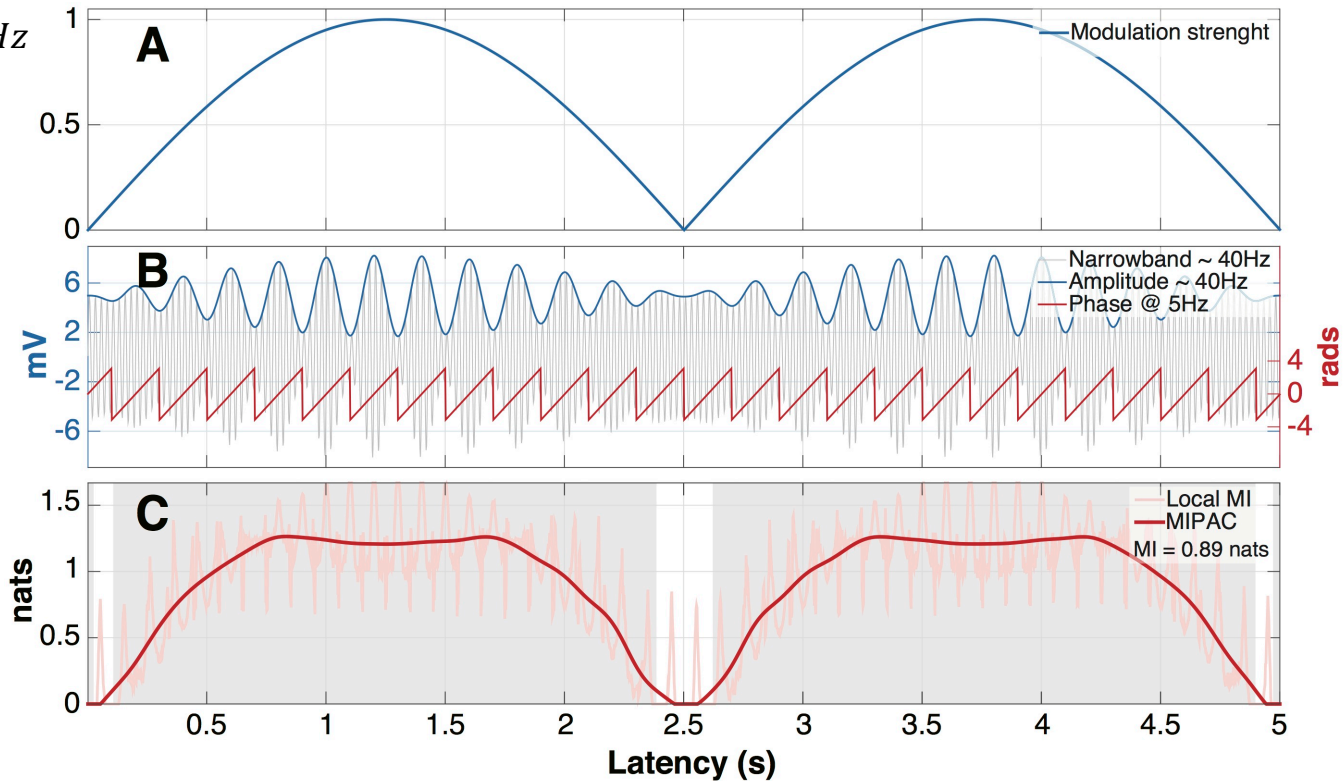
- (A) Saw-tooth shape waveform modulation strength.
- (B) Simulated signal
- (C) Estimated MIPAC (red), and local MI (light red)

Simulation 1.3: Instantaneous MIPAC

$$f_{mod} = 5\text{Hz}$$

$$f_{carr} = 40\text{Hz}$$

$$S_{rate} = 500\text{Hz}$$



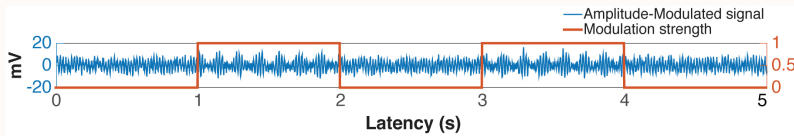
(A) Absolute value of a sinusoid used as modulation strength.

(B) Simulated signal

(C) Estimated MIPAC (red), and local MI (light red)

Simulation 2: Event-related MIPAC

ER PAC data simulation



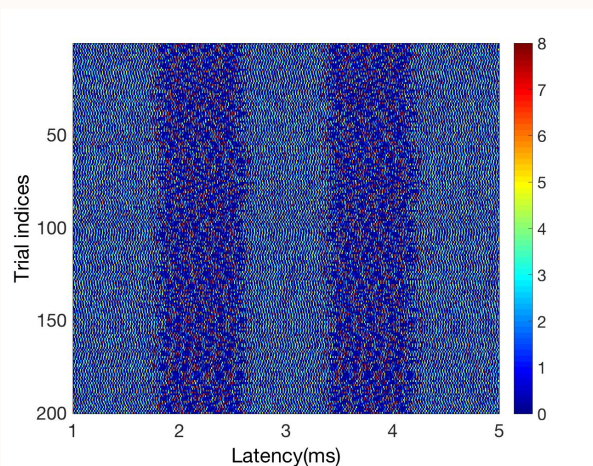
$$f_{mod} = 5\text{Hz}$$

x200

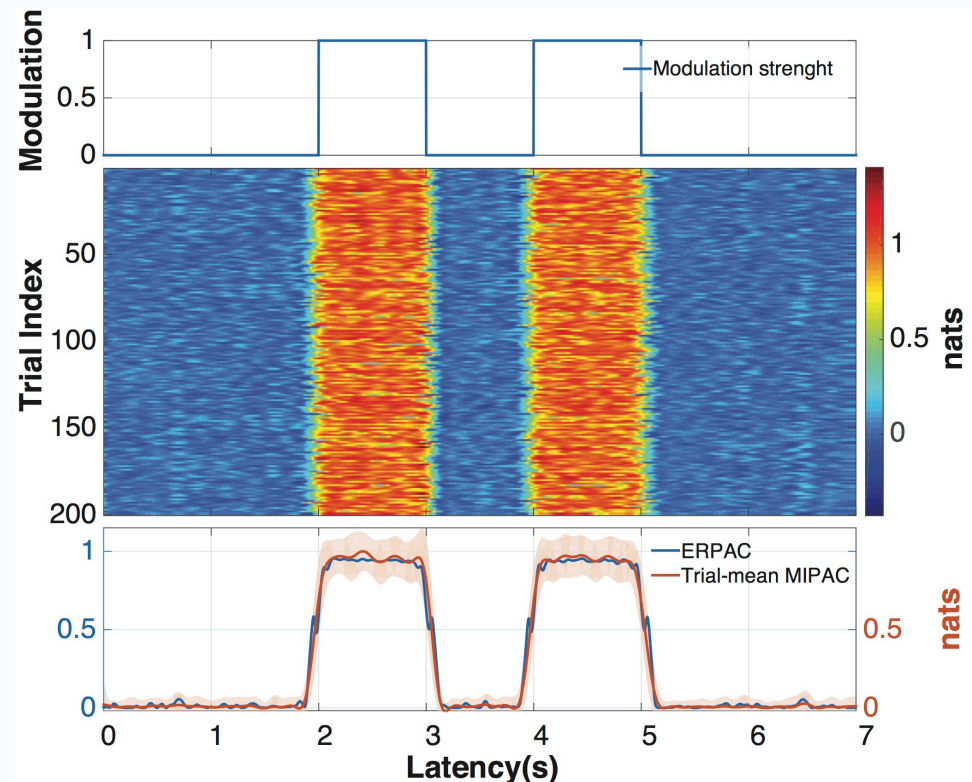
$$f_{carr} = 40\text{Hz}$$

$$S_{rate} = 500\text{Hz} \quad SNR = 10$$

Each trial was shifted 1-100 pts

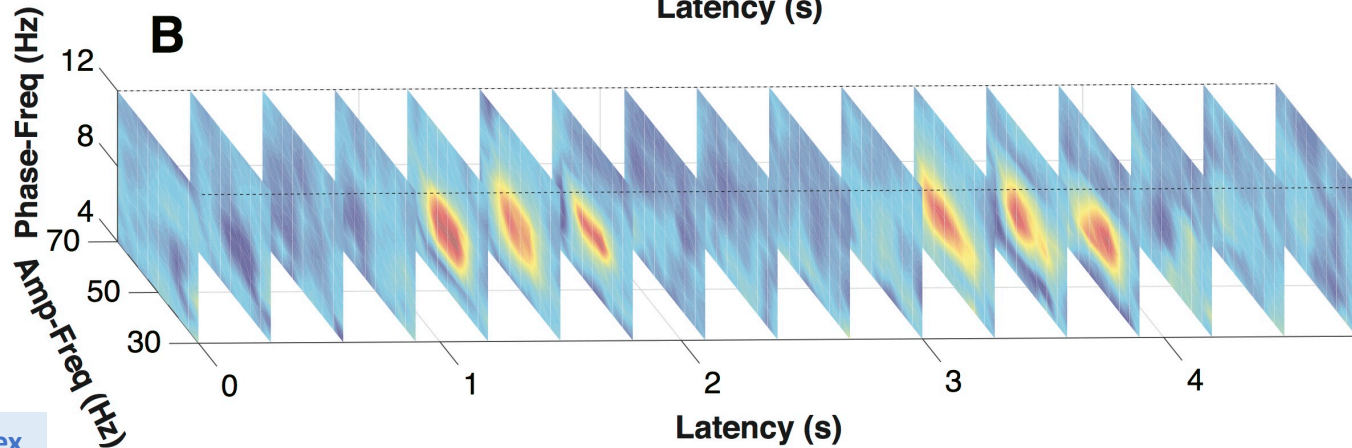
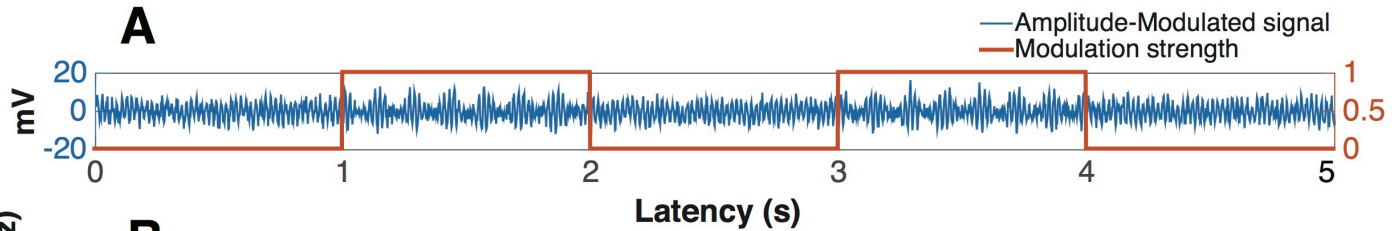


Event related MIPAC and **ERPAC** (Voytek et al, 2013) were used to estimate PAC



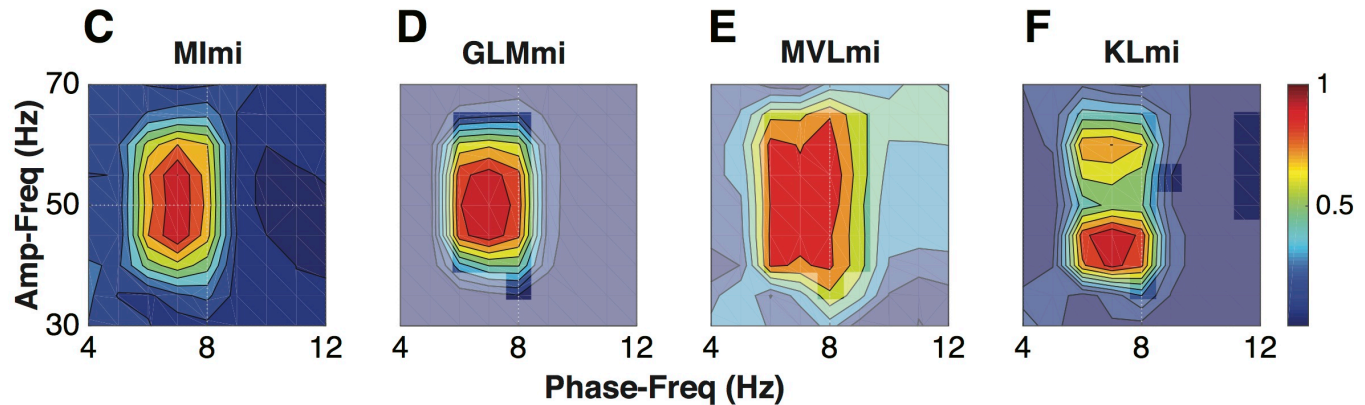
Simulation 4: MIPAC & MI mi

$f_{mod} = 7\text{Hz}$
 $f_{carr} = 50\text{Hz}$
 $S_{rate} = 500\text{Hz}$



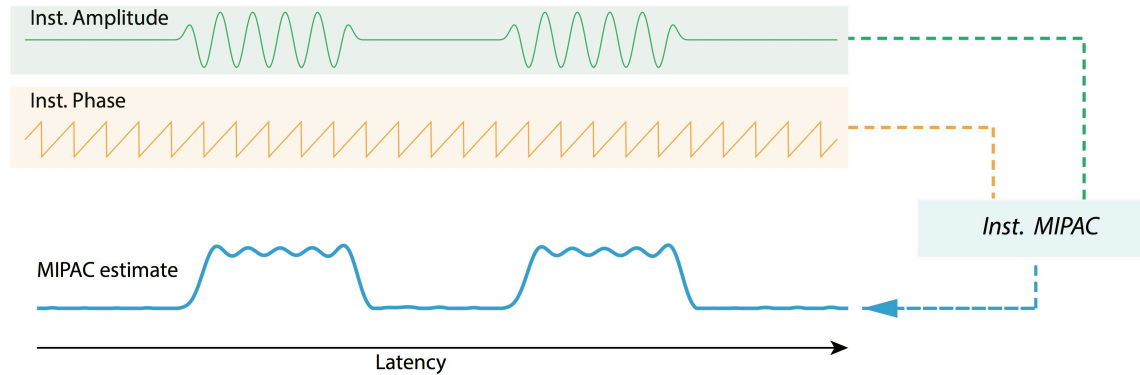
Grand Mean

MI modulation index

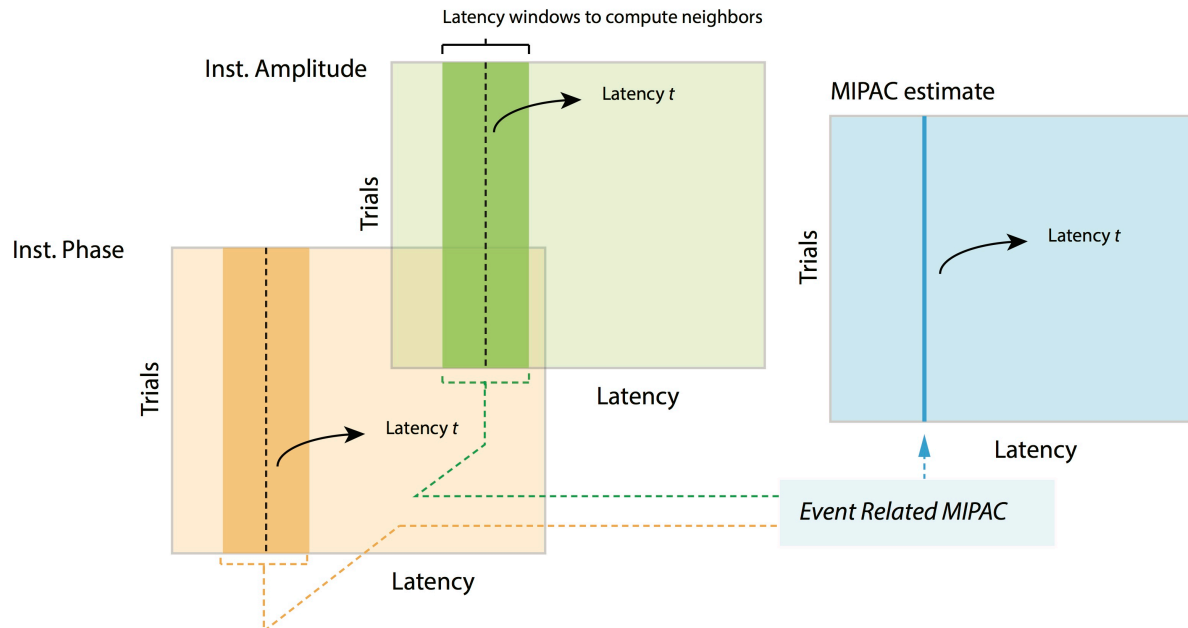


Inst. MIPAC and Event-related MIPAC

MIPAC



Event-related MIPAC





MIPAC application to real data

ECoG Data

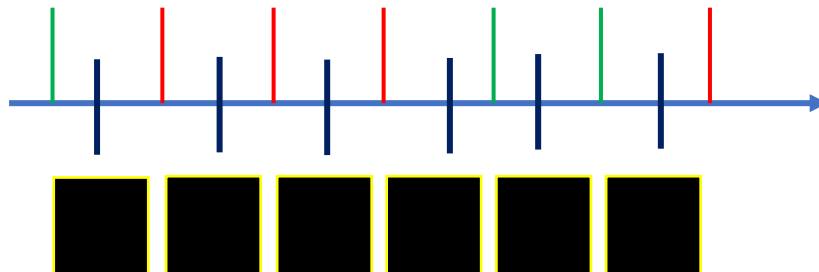
Subject

- Clinical monitoring and localization of seizure foci
- 1 subject (mv)
- ECoG channels in: Inf. Temp. Gyrus
Lingual Gyrus
Fusiform Gyrus

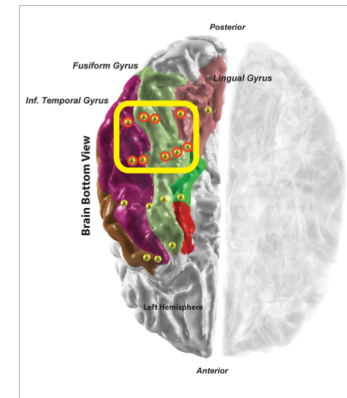
Experimental design

- Images of Houses and Faces were presented randomly
- 3 runs 100 presentations each (50 H / 50F)

400 ms



400 ms



Preprocessing

Performed in EEGLAB (*Delorme and Makeig, 2004*)

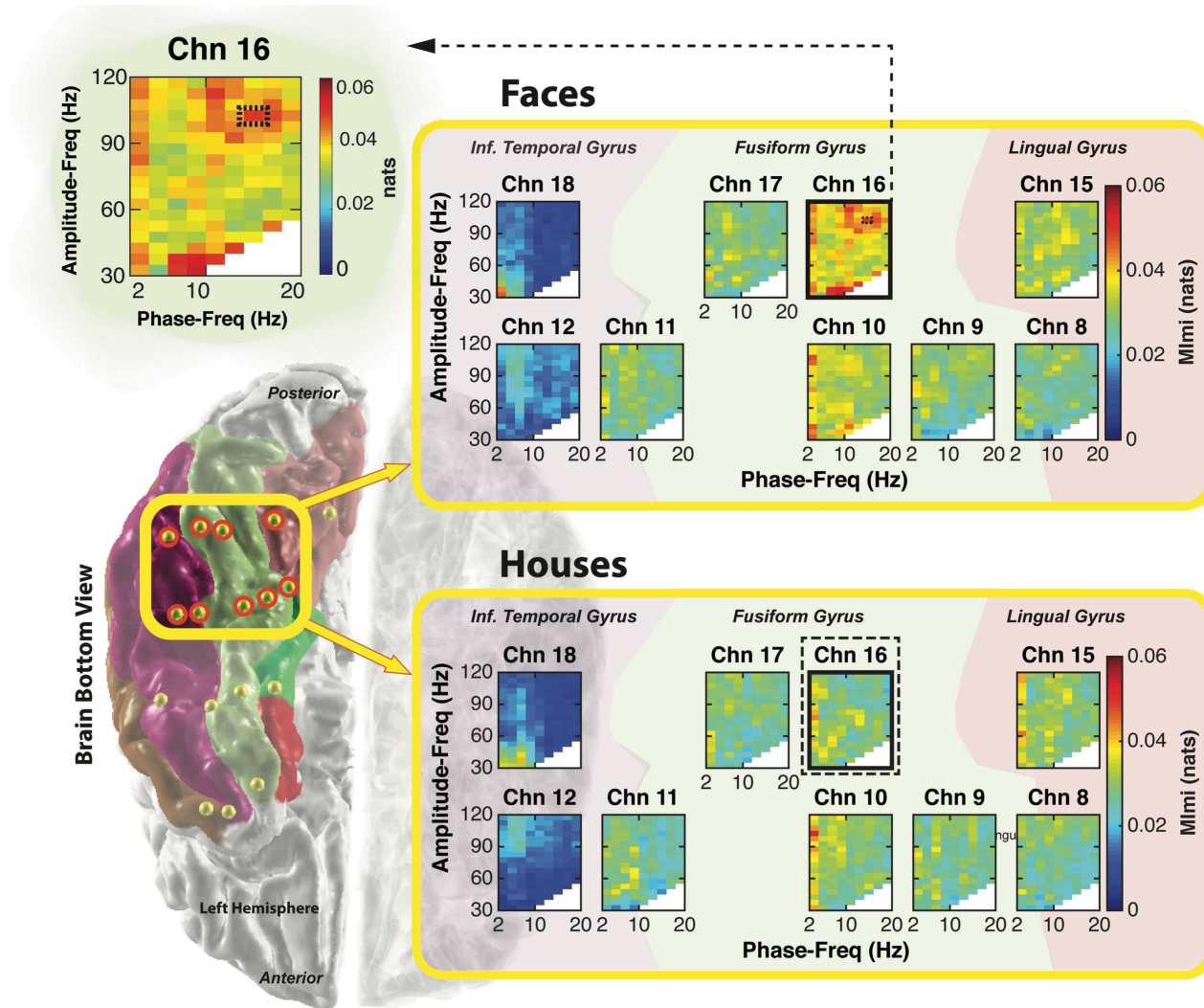
1. Artifact removal
2. CAR
3. Resampling to 512Hz
4. Line noise removal $\sim(60, 120)$ Hz
Hamming-windowed FIR notch filter
5. Extract epochs time-locked to stimulus presentations $[-400, 800]$ ms

Original publication:

The physiology of perception in human temporal lobe is specialized for contextual novelty

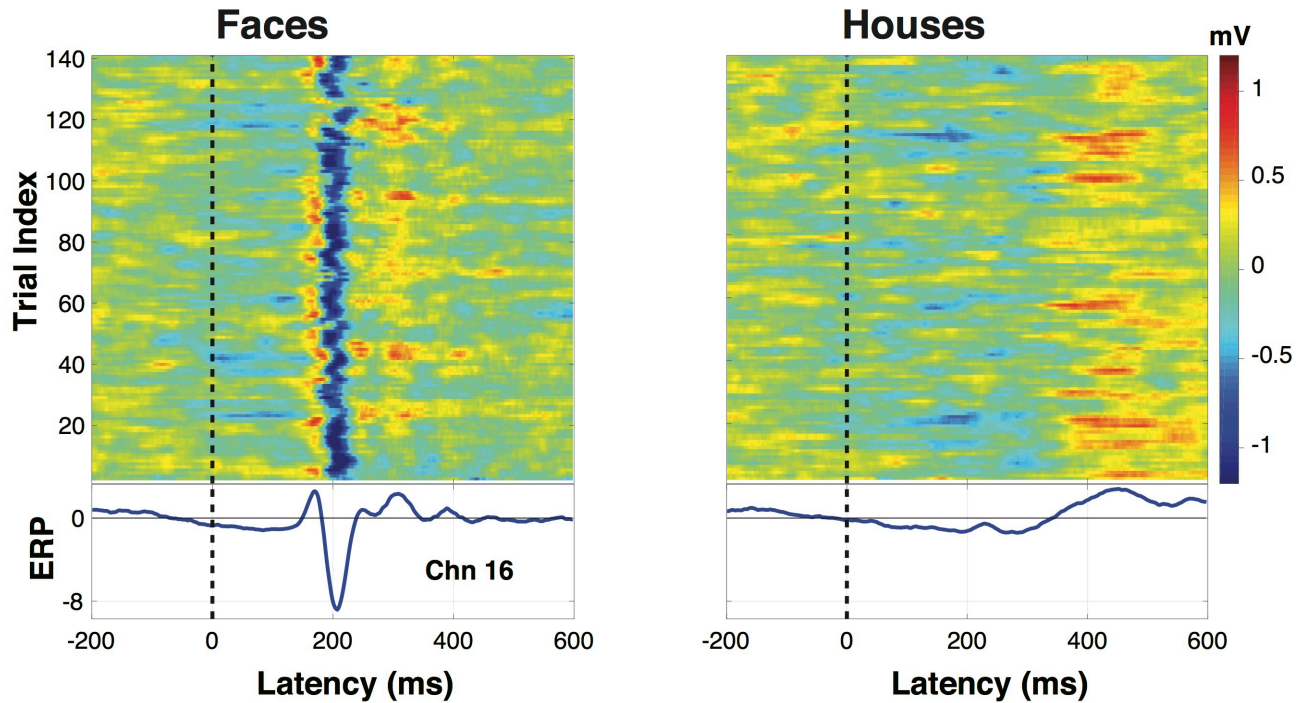
Kai J. Miller, Dora Hermes, Nathan Witthoft, Rajesh P. N. Rao, Jeffrey G. Ojemann

ECoG Data: Mimi in action



ECoG Data: Event Related Potential Image

Channel 16

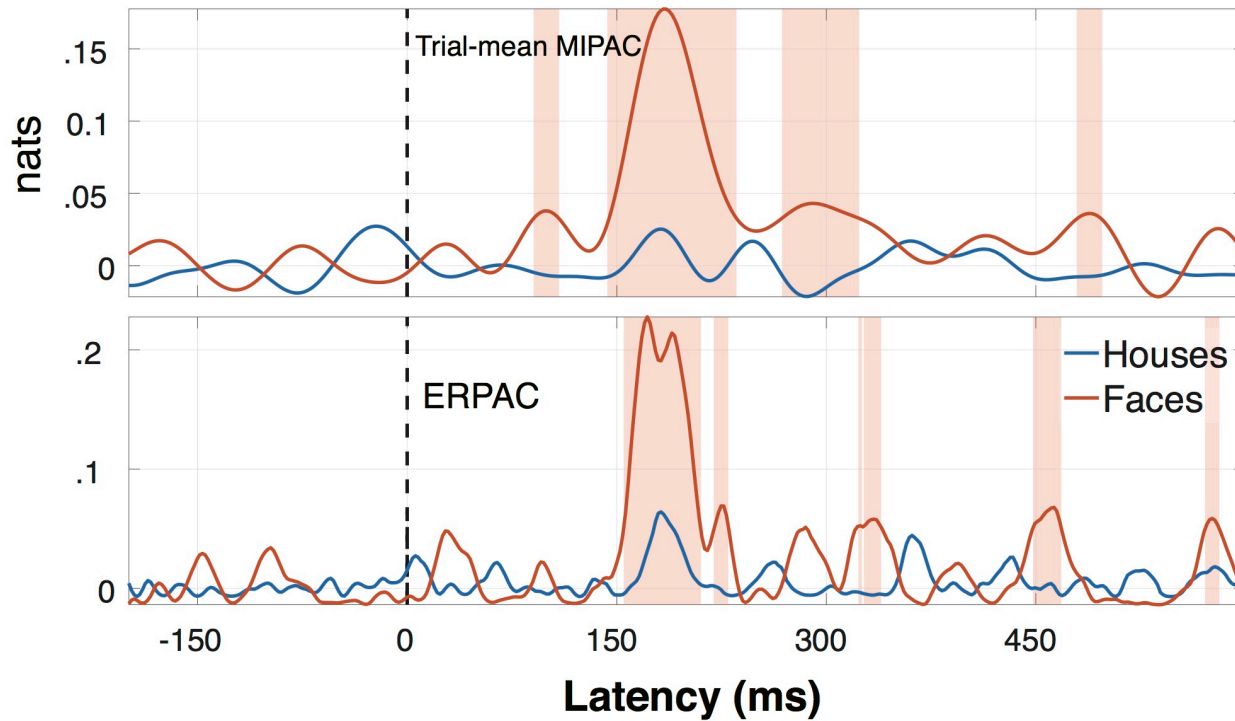


ECoG Data: MIPAC vs ERPAC

Event-related MIPAC and ERPAC (Voytek et al. 2014) were computed

$$f_{phase} = 16 \text{ Hz}$$

$$f_{amp} = 95 \text{ Hz}$$

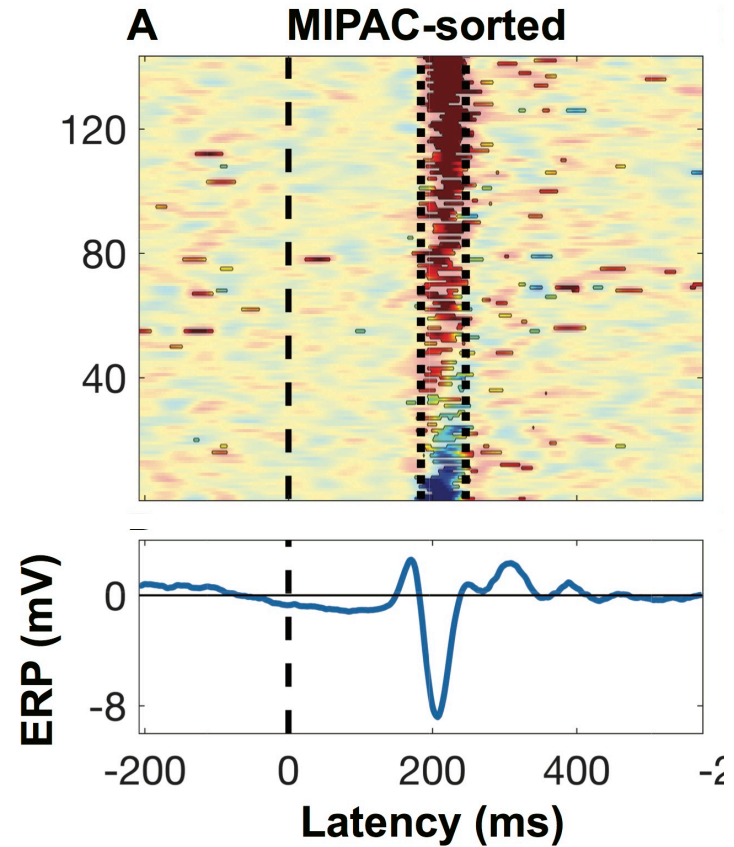


ECoG Data: MIPAC Image

ER-MIPAC computed for **Faces** presentation

$$f_{phase} = 16 \text{ Hz}$$

$$f_{amp} = 95 \text{ Hz}$$

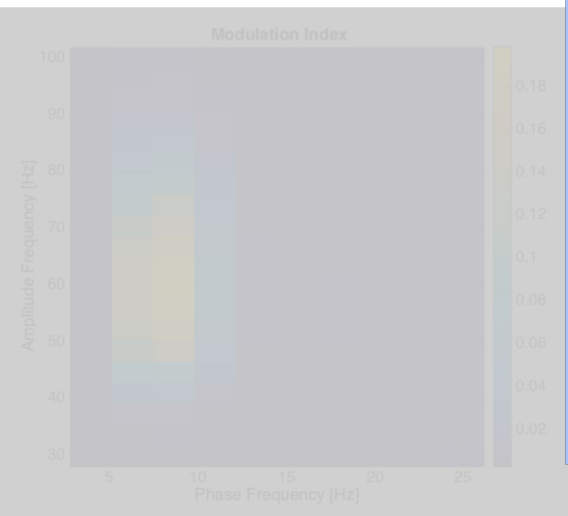
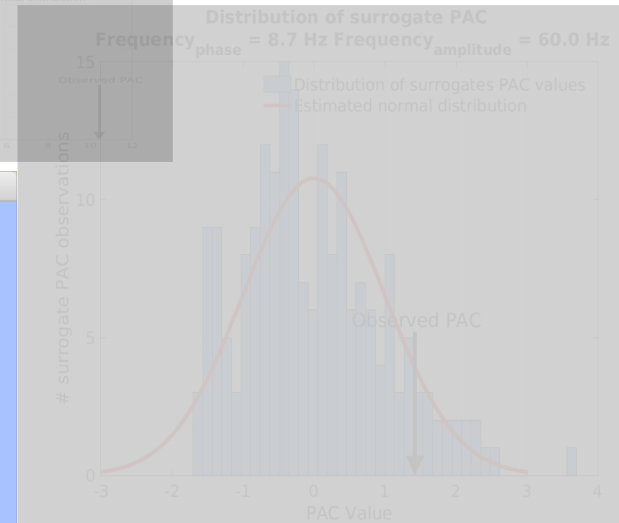
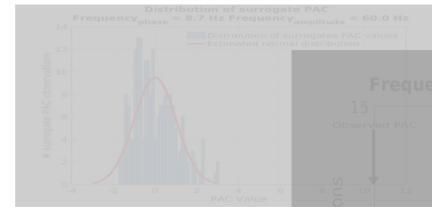
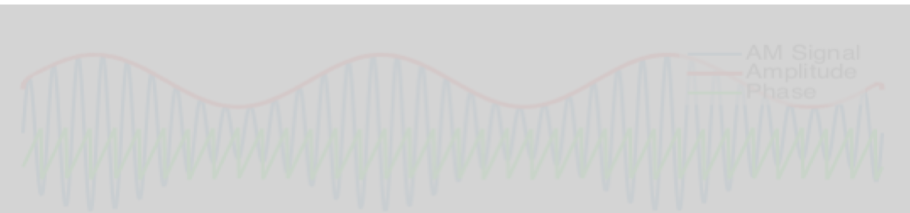


Conclusions

- The method was validated on simulated PAC signals
- Application to human ECoG data showed positive results

Future Direction

ERPAC Tools



pop_pac() - Test for event-related Phase/Amplitude Coupling (PAC)

PAC data type: Components

	Comp/chan indices	Freq range [lo hi] Hz	# Frequencies
Phase data	2 3 4	4 15	6
Amp data	4 5	20 64	15

PAC method: Mean vector length modulation index (Canolty et al.)

PAC statistics

# Surrogates	200
Significance threshold (0<p<1)	0.05

Buttons: Help, Cancel

pop_plotpac()

Method: kmi Chan/Comp. Indx: 1 1

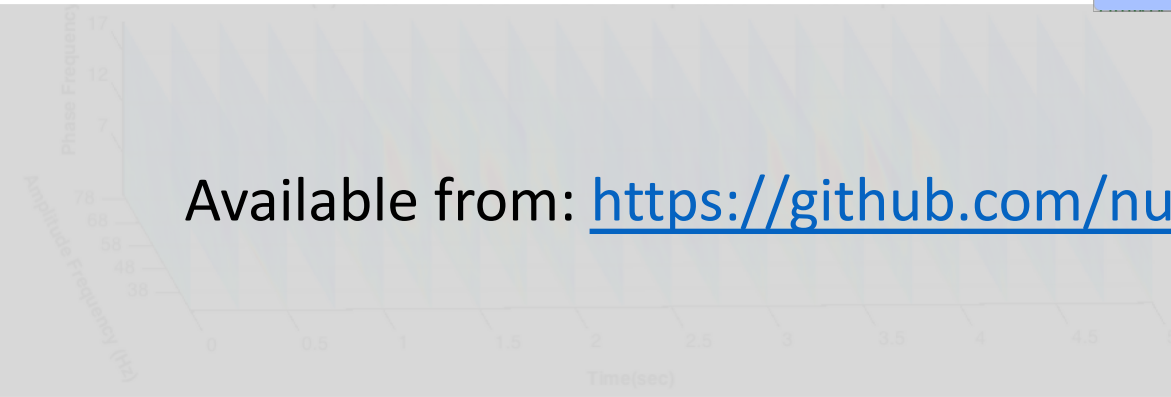
Plot type: Comodulogram

Phase freq. (Hz): Amp freq. (Hz): Time (s):

Command line options:

Buttons: Help, Cancel, Ok

Available from: https://github.com/nucleuscub/pop_pac



Acknowledgments

Coauthors



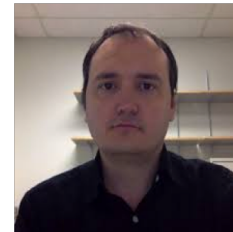
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