

# Sleep in the Unresponsive Wakefulness Syndrome and Minimally Conscious State

Victor Cologan,<sup>1</sup> Xavier Drouot,<sup>2,3</sup> Silvia Parapatics,<sup>4,6</sup> Arnaud Delorme,<sup>5</sup> Georg Gruber,<sup>4,6</sup> Gustave Moonen,<sup>7</sup> and Steven Laureys<sup>1,7</sup>

## Abstract

The goal of our study was to investigate different aspects of sleep, namely the sleep-wake cycle and sleep stages, in the vegetative state/unresponsive wakefulness syndrome (VS/UWS), and minimally conscious state (MCS). A 24-h polysomnography was performed in 20 patients who were in a UWS ( $n = 10$ ) or in a MCS ( $n = 10$ ) because of brain injury. The data were first tested for the presence of a sleep-wake cycle, and the observed sleep patterns were compared with standard scoring criteria. Sleep spindles, slow wave sleep, and rapid eye movement sleep were quantified and their clinical value was investigated. According to our results, an electrophysiological sleep-wake cycle was identified in five MCS and three VS/UWS patients. Sleep stages did not always match the standard scoring criteria, which therefore needed to be adapted. Sleep spindles were present more in patients who clinically improved within 6 months. Slow wave sleep was present in eight MCS and three VS/UWS patients but never in the ischemic etiology. Rapid eye movement sleep, and therefore dreaming that is a form of consciousness, was present in all MCS and three VS/UWS patients. In conclusion, the presence of alternating periods of eyes-open/eyes-closed cycles does not necessarily imply preserved electrophysiological sleep architecture in the UWS and MCS, contrary to previous definition. The investigation of sleep is a little studied yet simple and informative way to evaluate the integrity of residual brain function in patients with disorders of consciousness with possible clinical diagnostic and prognostic implications.

**Key words:** brain injury; coma; minimally conscious state; sleep; vegetative state

## Introduction

MEDICAL PROGRESS HAS led to an increase in the number of brain-injured patients in a vegetative state/unresponsive wakefulness syndrome (VS/UWS) or minimally conscious state (MCS) after coma (European Task Force on Disorders of Consciousness 2010). Wakefulness and awareness are the two main components of consciousness.<sup>1</sup> The UWS is, therefore, defined as a state of wakefulness without awareness, whereas the MCS corresponds to uncommunicative patients showing basic conscious behavior. Clinical practice and research, relying mainly on behavioral, electrophysiological, and neuroimaging studies, have shown how challenging it can be to establish the diagnosis and prognosis in such disorders of consciousness (DOC).<sup>1</sup> In particular, “active” paradigms evaluating residual cognitive function and command following are measures made for short and defined

periods. It is well known, however, that vigilance and awareness fluctuate in such patients, resulting in variable behaviors and cognitive performances.<sup>2–4</sup> At present, there is no standard description of the different vigilance states in VS/UWS and MCS patients.

Together with evidence of eye opening, the presence of a sleep-wake cycle defines the threshold between a comatose state and the UWS or MCS. Although it is well known that sleep abnormalities are common in critically ill patients, there is little empirical evidence that brain-injured patients actually exhibit electrophysiological sleep phenomena or display a circadian rhythm.<sup>5–9</sup> In DOC, sleep-wake cycles are typically inferred by behavioral observations of periods of eye closure, but their underlying mechanisms remain poorly understood and their fine-grained characterizations are still unknown.

Our objective is, therefore, to describe the large variety of sleep patterns existing in VS/UWS and MCS patients and to test their potential clinical interest. To our knowledge, this is the first study specifically

<sup>1</sup>Coma Science Group, Cyclotron Research Center, University of Liège, Belgium.

<sup>2</sup>Sleep Center, Henri Mondor Hospital, Paris, France.

<sup>3</sup>EA 4391, University Paris 12, Paris, France.

<sup>4</sup>The Siesta Group, Vienna, Austria.

<sup>5</sup>National Center of Scientific Research, CERCO, Toulouse, France.

<sup>6</sup>Department of Psychiatry and Psychotherapy, Medical University of Vienna, Vienna, Austria.

<sup>7</sup>Department of Neurology, Liege University Hospital, Liege, Belgium.

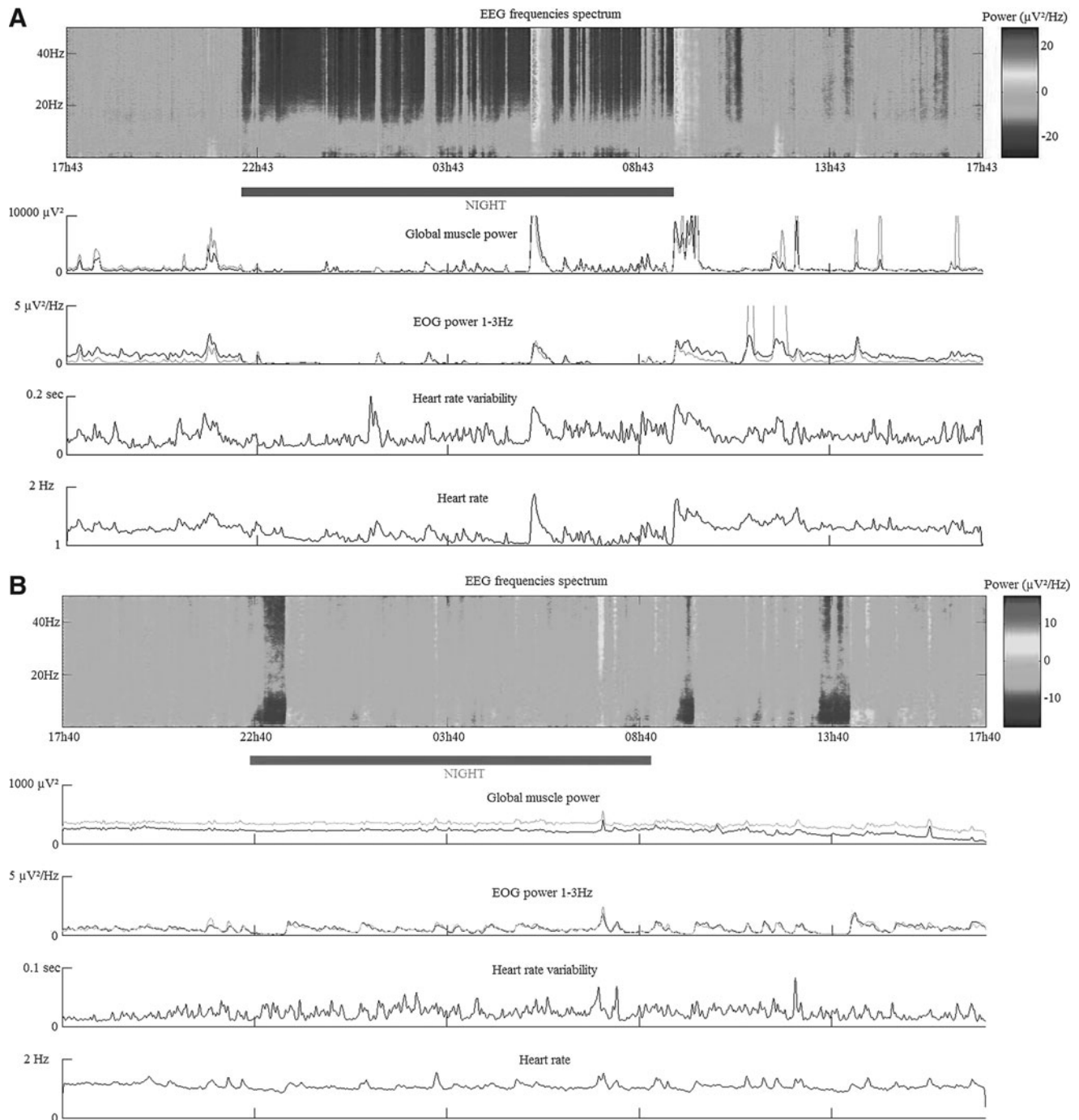
designed for the analysis of sleep in the vegetative and minimally conscious states and based on 24-h recordings of brain activity.

## Methods

### Patients

A 24-h polysomnography was performed in sub-acute (1–12 months after brain injury), unsedated, and spontaneously breathing DOC patients in their usual clinical environment. Clinical assessment

and diagnosis were made using the recommended Coma Recovery Scale-Revised (CRS-R), performed the day before and after the recording by the first author.<sup>10,11</sup> Patients also received a diagnosis from the neurologists and neuropsychologists of the Coma Science Group. Patients with continuous epileptiform activity, suppression, or burst-suppression patterns were excluded from the present study. Outcome was measured at a 6-month follow-up using the CRS-R. The study was approved by the Ethics Committee of the Faculty of Medicine of the University of Liège, and written informed consent was obtained from the patients' legal representatives.



**FIG. 1.** (A) Cycled pattern of brain activity. The night period is represented by the blue bar and was determined from the video. (B) Uncycled pattern of brain activity. Note the almost monotonous activity pattern and the rarity of rest periods. (C) Ultradian cycle of brain activity. Note the relatively rhythmic four cycles of brain de-/activation. (continued)

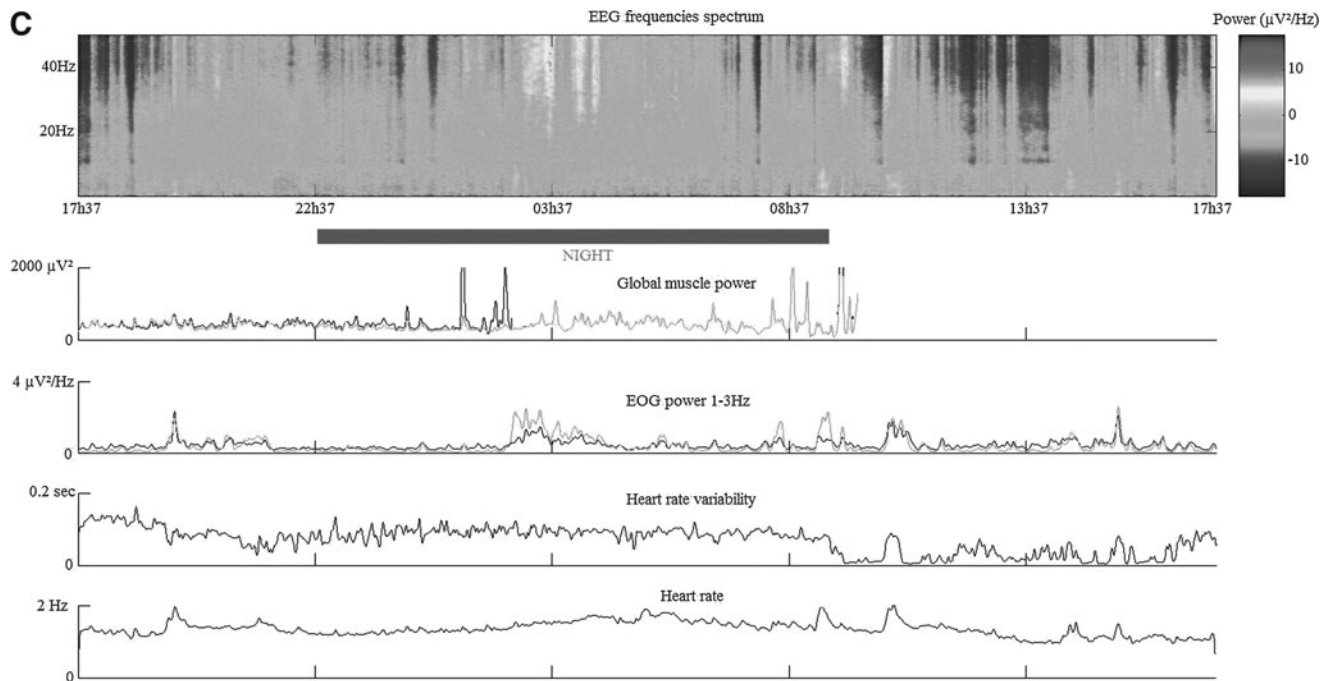


FIG. 1. (Continued).

#### Data acquisition and analysis

**Recordings.** The 24-h polysomnography was performed with a V-Amp16 amplifier (Brain Products) with infrared video monitoring. We used 12 electroencephalography (EEG) channels localized according to the conventional 10–20 system, chin-electromyography (EMG), electro-oculography (EOG in crossed montage), and electrocardiography (ECG). We applied an analog band pass filter of (0.1–200 Hz), (10–100 Hz), (0.3–35 Hz), and (0.3–70 Hz) to the respective data channels. Impedance of all channels was kept  $<5\text{ k}\Omega$  at the start and  $<20\text{ k}\Omega$  at the ending of all recordings. Analyses were performed using a 64-bit Linux workstation and EEGLAB freeware running in Matlab.<sup>12</sup> Raw data were sampled at 250 Hz and filtered using 1 Hz high-pass and 45 Hz low-pass thresholds. Epochs containing electrode movement artifacts were visually rejected (1% in average). During the recording, patients experienced their usual environmental conditions.

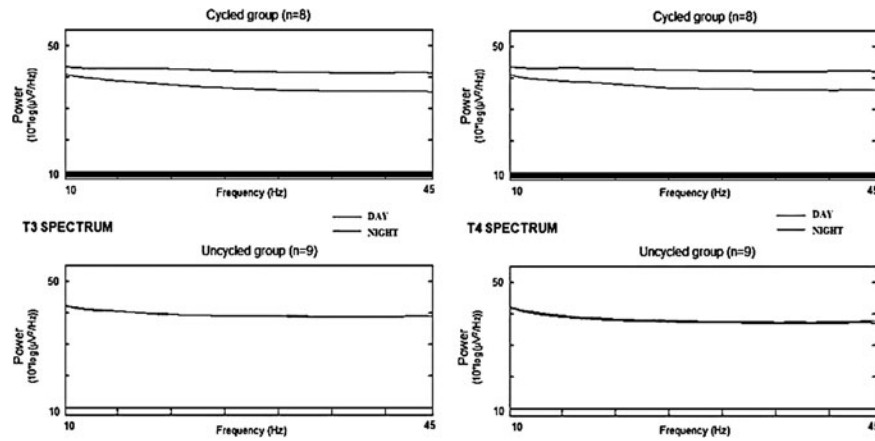
**Chronobiology.** To locate the rest periods of patients, we built a map of each recording. EEG relative power spectrum, muscle tonus, eyes movements, heart-rate variability, and heart rate were plotted over time (Fig. 1). The spectrogram of the EEG activity was computed using standard Fast Fourier Transform decomposition in EEGLAB, and missing data segment containing artifacts were interpolated. For eyes movements, we plotted the average power of the EOG channels in the 1–3 Hz frequency band, because eye channels have most power within these frequency bands at wake. For muscle activity, no artifactual data were removed from the 24-h period, because paroxysmal muscle activity can be interpreted as movement. For heart rate, we applied a band-pass filter between 1.5 Hz and 30 Hz and extracted heart beats by applying an automatic threshold, depending on the standard deviation of the recorded ECG signal. Heart beat intervals falling outside of the physiological range of 0.3–1.35 sec were considered artefactual and were removed ( $<1\%$  for each recording). Finally, all data measures were finally smoothed over time using a Gaussian filter.

On these chronobiological plots, a “rest pattern” was defined as a simultaneous slowing of the EEG relative spectrum and decrease of the global muscle power, EOG power, heart rate, and heart-rate variability,

because this is the case in healthy subjects. The problem: as yet, there is no empirical description of the EEG frequencies spectrum in the UWS and MCS. Moreover, the muscular artifacts contaminate the EEG channels in the 10–100 Hz band. An EEG slowing was therefore defined here as a reduction of the muscular frequencies from positive (hot colors) to negative (cold colors) relative power values. Indeed, even if standard background and cognitive high frequencies (12–40 Hz) are preserved in brain-injured patients, these are not visible in data unfiltered for muscular artifacts because these are of much higher amplitude. As for slow wave activity during the wake and rest phases, this was found to vary too much both individually and across our sample to be used as a proven sleep criterion.

Once the chronobiological figures were plotted, we noticed three recurrent patterns. Patients were classified as “cycled” if the patient was at rest during at least 80% of the nighttime and awake during at least 80% of the daytime (Fig. 1A), or “uncycled” if this distinction was absent (Fig. 1B). Patients showing at least two periodic rest-wake patterns were classified as “ultradian” (Fig. 1C). Nighttime corresponds to the time a patient is left alone with the light off to the time he is woken by the nurse or family with the light on (10 pm  $\pm$  1 h to 9 am  $\pm$  1 h). During the day, the room ambient lighting was normalized using the room lamps when the weather was dark. We also compared the mean value of the muscular spectral power between the day and night in cycled and uncycled patients using the paired *t* test corrected for multiple comparisons ( $p < 0.01$ ) to provide an objective and quantified marker of sleep-wake cycling (Fig. 2). Because one of the two EMG channels was unreliable during the last hours of recording for 9/20 patients, we calculated the 10–100 Hz power on the EEG temporal channels (T3, T4) as an EMG proxy measurement.

**Visual scoring.** Sleep analysis was performed by three independent, experienced scorers (VC, XD, and SP). The visual scoring of sleep patterns was performed using the EEGLAB visualization window. The first scorer reiteratively explored the data and listed the different standard and alternative sleep patterns encountered. Next, the other scorers assessed the presence of the reported patterns using a blind method. Ambiguous scoring conflicts were resolved by



**FIG. 2.** Muscular spectrum of the T3 (left) and T4 (right) channels during day and night in cycled (upper panel) and uncycled (lower panel) patients. The black bar represents significant difference between the two groups at a paired *t* test corrected for multiple comparisons ( $p < 0.01$ ). Note that the 10–100 Hz spectrum is cut at 45 Hz because of the data preprocessing.

common consensus, and standard spindles, slow wave sleep (SWS) and rapid eye movement sleep (REMS) were calculated.

**Definition of standard sleep scoring criteria.** The waking state is characterized by a high-frequency ( $> 10$  Hz) desynchronized EEG, a high muscular tone in EMG channels, and eye blinks in EOG channels. Stage 1 is defined by a slower and synchronized EEG, a low muscular tone, the absence of eye blinks, and the occurrence of slow eye movements. The  $\alpha$  waves, occurring when eyes are closed, progressively slow down toward  $\theta$  activity. Persons aroused from this stage often believe that they have been awake. Sleep spindles were initially defined as 12–15 Hz bursts under  $50\mu\text{V}$  amplitude, lasting 0.5–2 sec, having a typical sinus-like shape, best visible in the central channel, and generally occurring during the sleep stage 2 preceding SWS.<sup>13</sup> Later, it was shown that spindles can have a larger frequency band (10–16 Hz) and topography.<sup>14</sup>

SWS is defined by a high amplitude (75–140  $\mu\text{V}$ ) synchronized EEG in the  $\delta$  band including at least 20% (stage 3) or 50% (stage 4) slow waves that are most visible in the frontal channels, a low muscular tone close to atonia, and the absence of eye blinks and movements. Paradoxical sleep—or REMS—is characterized by a synchronized EEG in the  $\theta$  band, a muscular atonia, and the presence of phasic events such as REM and muscular twitches. It is generally preceded by SWS (night start) or stage 1 (night end) and interrupted by an awakening.

## Results

We included 20 patients (10 VS/UWS and 10 MCS) of traumatic ( $n=9$ ) and non-traumatic etiology (anoxia,  $n=6$  and cerebrovascular accident [CVA],  $n=5$ ). Demographic, clinical, and outcome data are summarized in Table 1.

A polysomnographic sleep-wake cycle was found in 3/10 VS/UWS and 5/10 MCS. An ultradian pattern was found in one VS/UWS and two MCS patients. In the cycled patients' group, the mean of the muscular spectral power was significantly higher ( $p < 0.01$ ) during the day (10 am–10 pm data segment) than during the night (10 pm–10 am) according to the paired *t* test with false discovery rate correction for multiple comparisons in EEGLAB (Fig. 2).

### Comparison of the observed sleep patterns to the standard criteria

The wake EEG of brain-injured patients is generally described as “slowed” (i.e., from standard  $\alpha$ – $\beta$  to predominant  $\delta$ – $\theta$  activity under

75  $\mu\text{V}$  amplitude) and showing phasic or tonic high amplitude epileptiform bursts that reflect the brain injury (Supplementary Fig. 1; see online supplementary material at <http://www.liebertonline.com>).<sup>15</sup> In our recordings, epileptiform waves appeared during the waking state, the stage 1, and SWS in very variable quantities. They can be distinguished from sleep slow waves because they are monomorphic and more symmetrical and spike shaped. We also noted that the muscular tone was generally higher during periods including epileptiform activity than during periods without. Epileptiform patterns are suggestive of the degree of impairment in DOC and may vary with the patient's state of consciousness.<sup>15</sup> Indeed, epilepsy can be considered as a transient vegetative state in epileptic patients, so it probably abolishes consciousness in MCS patients as well.<sup>16,17</sup> Otherwise, there is still no empirical description of the wake EEG frequency spectrum in the UWS and MCS. Abnormal muscular, ocular and epileptic activities generally contaminate different EEG channels according to their amplitude and source, which are variable in brain-injured patients. So it is challenging to isolate the brain signal.

This clinical population is by definition generally non-cooperative and can hardly be forced to relax their muscles and eyes without using drugs. Another difficulty concerning these patients is that being awake doesn't mean being “aware” for these patients, and there is also no evidence of any electrophysiological difference between an aware and an unaware waking state in the literature. In consequence, the only possible scoring criteria for the waking state in polysomnography of brain-injured patients are the presence of eye blinks and, of course, the absence of sleep patterns.

Similarly, stage 1 was defined as the absence of eye blinks (i.e., eyes closed), spindles, SWS, and REMS (Supplementary Fig. 2; see online supplementary material at <http://www.liebertonline.com>) in brain-injured patients. As for the waking state, the standard description of stage 1 does not match with the altered behavior and polysomnography of patients with DOC. This stage, however, mixes two different vigilance states in the MCS, the first corresponding to the “resting state” in healthy subjects, which is a state in which one is still conscious.<sup>18,19</sup> The second corresponds to the standard sleep stage 1 itself, in which one is unwittingly losing consciousness and starting to sleep.

Standard sleep spindles and SWS were detected in some of our recordings. We also found some spindles in the 6–9 Hz frequency range which were defined as “slow spindles” (Supplementary Fig. 3; see online supplementary material at <http://www.liebertonline.com>).



TABLE 1. DESCRIPTION OF THE RECORDED PATIENTS

Patient ID		Etiology	Glasgow Liege score	Coma recovery scale revised	Outcome +6 months	Sleep-wake cycle	Standard sleep stages		
Code	Age						Spindles	SWS	REM sleep
VS1	62	itCVA	E4VtM1-5	A0 V1 M0 OV1 C0 W2	Death	None		<75µV	
VS2	44	Anoxia	E4V1M3-5	A0 V0 M2 OV1 C0 W2	Death	Cycled		<75µV	44.7'
VS3	54	Anoxia	E4V1M2-4	A1 V0 M1 OV1 C0 W2	UWS	None	<10Hz	<75µV	
VS4	37	Anoxia	E4V1M3-5	A1 V0 M1 OV1 C0 W2	UWS	Cycled	<10Hz	<75µV	61.7'
VS5	21	Trauma	E4V2M3-4	A1 V0 M2 OV1 C0 W2	UWS	None	7 <10Hz	177.7'	
VS6	61	Anoxia	E4VtM4-5	A1 V1 M2 OV1 C0 W2	UWS	None		<75µV	
VS7	16	Trauma	E4V2M3-5	A1 V0 M1 OV2 C0 W2	UWS	Cycled	<10Hz	128.5'	38.7'
VS8	61	stCVA	E4V1M3-3	A0 V1 M2 OV1 C0 W2	MCS	Ultradian	3 <10Hz	CAP	
VS9	74	Trauma	E3VtM1-3	A0 V0 M1 OV1 C0 W1	MCS+	None	30	<75µV	
VS10	16	Trauma	E4VtM4-5	A1 V1 M2 OV1 C0 W2	EMCS	None	550	212.7'	
MCS1	36	Trauma	E4V1M1-5	A0 V3 M0 OV1 C0 W2	MCS	Cycled	3 <10Hz	39.0'	42.3'
MCS2	62	Trauma	E4V1M3-5	A0 V3 M2 OV1 C0 W2	MCS	Cycled	<10Hz	386.3'	Primes
MCS3	34	Anoxia	E4V2M4-5	A1 V1 M2 OV2 C0 W2	MCS	Ultradian	2 <10Hz	176.1'	79.8'
MCS4	48	Trauma	E4V1M5-5	A3 V0 M3 OV2 C1 W2	MCS	Ultradian	1 <10Hz	76.3'	4.7'
MCS5	61	Anoxia	E4V2M4-5	A2 V3 M2 OV1 C0 W2	MCS+	Cycled	61	229.6'	20.3'
MCS6	31	stCVA	E4V2M3-4	A2 V3 M2 OV2 C0 W2	MCS+	None	<10Hz	<75µV	19.9'
MCS7	20	Trauma	E4V2M4-5	A2 V3 M2 OV2 C1 W3	MCS+	Cycled	25	233.6'	16.2'
MCS8+	66	stCVA	E4V1M6-5	A4 V2 M1 OV1 C0 W2	MCS+	None	<10Hz	<75µV	15.5'
MCS9+	43	Trauma	E4V4M6-5	A4 V5 M5 OV3 C1 W3	MCS+	None	2 <10Hz	110.5'	8.1'
MCS10+	48	mCVA	E4V1M6-5	A3 V5 M5 OV2 C1 W2	EMCS	Cycled	125	248.7'	5.9'

SWS, slow wave sleep; REM, rapid eye movement; itCVA, infratentorial cerebral vascular accident; UWS, unresponsive wakefulness syndrome; stCVA = supratentorial cerebral vascular accident; MCS, minimally conscious state; mCVA = meningeal hemorrhage.

CRS-R: A = Auditory, V = Visual, M = Motor, OV = Oralmotor/Verbal, C = communication, W = Wakefulness. MCS+ = The MCS+ describes a clinical subpopulation with high-level behavioral responses (command following, intelligible verbalizations, or non-functional communication) and a higher degree of recovery compared with the MCS.<sup>36</sup>

CAP: Cyclical alternating pattern of frontal cortical synchronization arousals >75µV (318.0 min in VS/UWS8).

.com). We also detected SWS under 75µV amplitude which was defined as “attenuated SWS” (Supplementary Fig. 4; see online supplementary material at <http://www.liebertonline.com>). In VS8, a cyclical alternating pattern (CAP) of frontal cortical synchronization arousals >75 µV was observed. This activity was so different from the standard SWS patterns encountered in the other patients that it was classified as “CAP,” as proposed in a previous article.<sup>8</sup>

Finally, paradoxical sleep did match with the standard scoring criteria (Supplementary Fig. 5; see online supplementary mate-

rial at <http://www.liebertonline.com>). We noted that the standard temporal progression of sleep stages (wake → stage 1 → stage 2 (spindles) → stages 3–4 → REMS → awakening) was standard during the rest periods except in two patients. VS7 showed a fragmented episode containing a mix of NREMS alternating with REMS without any awakening during his nocturnal sleep period. MCS2 had REM sleep primes lasting less than 40 sec and being interrupted by an awakening at the first or second REM iteration.

TABLE 2. DIFFERENCES IN STANDARD SLEEP STAGES BETWEEN SCORERS

Sleep reference	First scorer		Second scorer		Third scorer	
	Occurrence	Quantity (min)	Occurrence	Quantity (min)	Occurrence	Quantity (min)
REMS in VS4	10	73.7	7	61.7	8	58.6
REMS in VS7	11	48.9	8	38.7	8	38.7
Spindles in VS9	30	–	27	–	30	–
Spindles in VS10	539	–	550	–	542	–
SWS in MCS1	1	28.0	1	39.0	1	28.0
REMS in MCS1	7	40.9	7	42.3	7	40.9
SWS in MCS2	12	76.1	17	386.3	12	76.1
SWS in MCS3	18	176.1	18	175.7	18	176.1
REMS in MCS3	11	79.8	10	78.6	10	78.6
Spindles in MCS7	20	–	24	–	25	–
SWS in MCS7	10	228.1	11	233.6	10	228.1
REMS in MCS7	3	16.2	2	12.0	2	12.0
SWS in MCS4	20	68.8	22	76.3	20	68.8
Spindles in MCS10	125	–	121	–	124	–
SWS in MCS10	15	131.5	5	248.7	15	131.5

REMS, rapid eye movement sleep; SWS, slow wave sleep.

TABLE 3. NUMBER OF PATIENTS WITH PRESERVED STANDARD SLEEP STAGES

Standard sleep stages	Spindles sleep		Slow waves sleep		REM sleep	
	UWS	MCS	UWS	MCS	UWS	MCS
Number of traumatic patients	3/4	4/5	4/4	5/5	1/4	5/5
Number of anoxic patients	0/4	2/2	0/4	2/2	2/4	2/2
Number of vascular patients	1/2	0/2	0/2	0/2	0/2	2/2

REM, rapid eye movement, UWS, unresponsive wakefulness syndrome, MCS, minimally conscious state.

### Interscorer rate

The scorers' qualitative analysis (presence or absence of sleep patterns) matched except on the following points and these cases were then discussed before reaching a common agreement: (1) The existence of rare standard spindles ( $n < 10$ ) in VS5, VS8, MCS1, MCS3, MCS4, MCS9; (2) The CAP of VS8; (3) The REMS primes of MCS2.

The quantitative analysis matched between the scorers except for the cases seen in Table 2.

The quantitative study confirms the general rule that there is always a difference between the visual scorings of several independent sleep specialists. It also raises an important point that SWS and REMS can be easily definable in some patients but not others. Indeed, we noted that SWS could have clear boundaries and good stability in some cases (especially in UWS patients), while in other cases, the limits are progressive and the slow waves' amplitude unstable, making the interscorers quantification less consistent (especially in MCS patients). As for REMS, interscorers discrepancies show that the first scorer tended to overestimate the number of episodes. This confirms that the scorer's experience affects the scoring of sleep but also suggests that brain-injured patients may have episodes resembling REMS. Nevertheless, from a clinical point of view, we argue that it is more important to know what sleep stages are preserved rather than their exact quantities in brain-injured patients.

### Sleep stages

All patients showed sleep stage 1. Three MCS patients had preserved spindles ( $n > 10$ ), SWS, and REMS. Standard spindles were found in 4/10 VS/UWS and 7/10 MCS patients; number varied between 1 and 539. Slow spindles were found in 5/10 VS/UWS and 7/10 MCS patients. Six patients did have both standard ( $n < 10$ ) and slow spindles. Standard SWS was found in 3/10 VS/UWS and 8/10 MCS patients. On average, the number of epochs was  $5.3 \pm 2.1$  and the duration  $36.0 \text{ min} \pm 21.0 \text{ min}$  in the VS/UWS;  $11.5 \pm 6.9$  and  $16.4 \text{ min} \pm 10.3 \text{ min}$  in the MCS. Attenuated SWS was found in 6/10 VS/UWS and 2/10 MCS. REMS was found in 3/10 VS/UWS and 10/10 MCS patients. On average, the number of epochs was  $6.3 \pm 2.9$  and the duration  $9.0 \text{ min} \pm 5.2 \text{ min}$  in the VS/UWS;  $4.9 \pm 3.2$  and  $4.4 \text{ min} \pm 2.0 \text{ min}$  in the MCS. All these amounts of standard sleep stages

(Table 3) cannot be statistically compared yet, because the number of patients showing them is too small. The persistence of REMS is correlated with MCS patients:  $\chi^2 = 10.8$ ,  $p = 0.005$  (Pearson uncorrected).

Concerning the outcome study, a low number of spindles ( $n < 10$ ) was found in four persistent patients; in one MCS patient who recovered occasional command following; and in one VS/UWS patient who improved to the MCS. An intermediate number of spindles (in the  $10^1$  range) was found in one VS/UWS and two MCS patients who improved to the MCS+. A high number of spindles (in the  $10^2$  range) was found in one VS/UWS and one MCS+ patient who recovered consciousness (exit-MCS). Six of the seven patients with a favorable outcome showed standard spindles in their recording (Table 4). Eight of the 13 patients with an unfavorable outcome showed no spindles, and the five others showed a low number of standard spindles ( $n < 10$ ).

### Discussion

Patients in a MCS or VS/UWS can show a circadian, ultradian, or uncycled sleep-wake pattern. This is in line with a previous study showing that the sleep cycle can be present or absent in persistent VS patients with no obvious difference in their clinical status.<sup>20</sup> These data suggest that the absence of a sleep-wake cycle might reflect the brainstem damage in DOC. Sleep spindles can possibly be present, slowed, or absent in both MCS and VS/UWS patients with all three etiologies. Patients who clinically improved within 6 months are more prevalent in classes with a high count of standard spindles ( $10 < n < 100$  and  $100 < n < 1000$ ) and fewer in those with a low count ( $n = 0$  and  $1 < n < 10$ ) than patients with persistent or degraded outcome:  $\chi^2 = 12.4$ ,  $p = 0.002$ .

This correlation, however, between the number of standard spindles and outcome 6 months later remains speculative because the number of patients in the different classes is too small. It does, however, highlight the potential prognosis value of sleep spindles in brain-injured patients, which is in line with the preliminary studies of sleep in comatose and vegetative patients.<sup>8</sup> Standard SWS is preserved in trauma patients and in anoxic MCS patients but not in CVA patients, suggesting that this etiology is particularly prone to SWS attenuation.

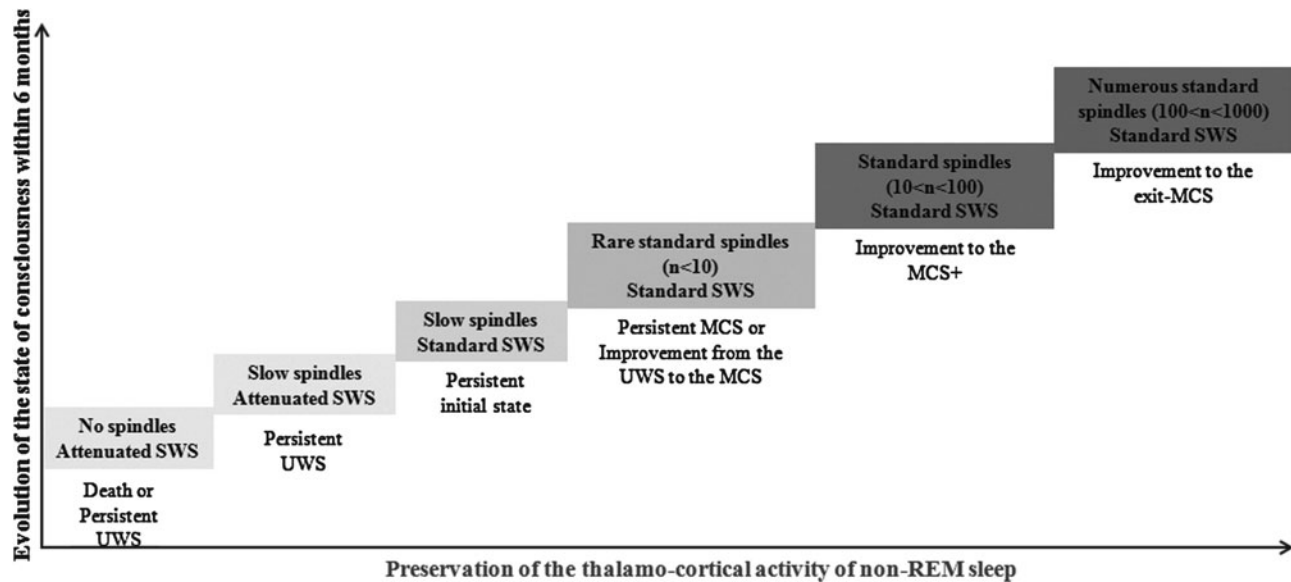
All our MCS patients showed phasic REMS, which is associated with dreaming in healthy subjects. Dreams being by definition a

TABLE 4. OUTCOME OF PATIENTS WITHIN 6 MONTHS ACCORDING TO THE NUMBER OF STANDARD SPINDLES

Number of standard spindles	0	1–10	10–100	100–1000
Number of patients with favorable outcome	1	1	3	2
Number of patients with unfavorable outcome	8	5	0	0

Favorable outcome=behavioral improvement according to the Coma Recovery Scale-Revised.

Unfavorable outcome=persistent or degraded behavior.



**FIG. 3.** Hypothetical model of prediction of outcome according to the quality of non-rapid eye movement sleep in traumatic and anoxic brain-injured patients. UWS, unresponsive wakefulness syndrome; MCS, minimally conscious state; SWS, slow wave sleep.

conscious experience, they have a differential diagnosis value in the VS/UWS. Indeed, it is now well known that some MCS patients are not able to show signs of consciousness on behavioral assessments, so they are evaluated as VS/UWS until fMRI or EEG active paradigms show the contrary.<sup>21–23</sup> Moreover, the three VS/UWS patients who showed REMS were also the only VS/UWS cases having not only a sleep-wake cycle but also some inconsistent conscious features such as food swallowing, facial expressions sometimes congruent with stimulation, or an atypical pattern on positron emission tomography. We therefore support that UWS patients showing REMS should be priority submitted to active paradigms to test the persistence of a minimal consciousness at wake.

Our findings confirm that the operational definitions of wakefulness and sleep are not applicable in DOC.<sup>8,9</sup> Contrary to what several definitions state, the presence of rest periods does not always imply preserved electrophysiological sleep-wake cycles nor sleep stages that should no longer be taken as a distinguishing feature for the definition of UWS or MCS.<sup>24,25</sup> The waking state and sleep stages do not fit the elder standard scoring criteria, which therefore needs to be adapted for polysomnography in DOC.

This study is in line with earlier studies on coma suggesting that the presence of EEG patterns resembling standard sleep may be markers of a favorable outcome.<sup>26–29</sup> Sleep research is of particular interest in brain-injured patients with various etiologies because it can bring to light relationships between sleep patterns and functional neuroanatomy. In particular, the quality and quantity of spindles seem to provide a new index of the severity of the thalamocortical injury in the VS/UWS and MCS (Fig. 3). This would be in line with brain imaging studies showing not only the correlation between the extent of thalamus damage and the behavioral disability and outcome in DOC, but also the restoration of the thalamocortical connectivity during recovery of consciousness.<sup>30–33</sup> Otherwise, REMS is sensitive to cortical injury, so the amount of this stage may be related to the severity of the cortical injury and behavioral impairment in brain-injured patients, but our results don't support this hypothesis.

Finally, although it is still unclear whether they have distinct or sequential roles, sleep is thought to optimize the consolidation

of acquired information in memory and to impact on mental abilities.<sup>34,35</sup> This suggests that the revalidation process may be facilitated in brain-injured patients with preserved sleep compared with those without and stresses the importance of promoting sleep in the clinical routine.

## Conclusion

For the purposes of testing cerebral activity in the VS/UWS, MCS, or intermediary patients who are between these two states, clinicians should keep in mind that arousal and consciousness can be severely impaired and chronobiologically disorganized in these populations. In consequence, a prolonged measure of the brain's spontaneous activity during at least 24 h is of primary interest: first, because it can inform the clinician about the temporal organization of the patient's vigilance states before a multimodal neurological assessment over several days; second, because it can reveal the possible persistence of residual brain activities such as sleep stages and thus provide additional prognosis or differential diagnosis information.

Moreover, 24-h polysomnography is a cheap and ambulatory method that could be adapted to the clinical routine of brain-injured patients in their usual environment contrary to brain scanners or high-density EEG. Further research on sleep-wake architecture in larger samples of patients will improve the clinical evaluation and care of these patients as well as our understanding of the neural correlations of vigilance and consciousness.

## Acknowledgments

The authors thank Pr. Maquet, head of the Sleep Group at the Cyclotron Research Center, for his collaboration. The authors also thank the doctors and nurses of the Centre Neurologique et de Réadaptation Fonctionnelle de Fraiture, the Centre Neurologique William Lennox, and the Neurology Departments of the Centre Hospitalier Universitaire of Liege for their participation in this study. The authors finally thank Mrs. Tina Duvivier for language revision.

This work was supported by the Belgian National Funds for Scientific Research (FNRS/FRIA).

## Author Disclosure Statement

No competing financial interests exist.

## References

- Laureys, S., Owen, A.M., and Schiff, N.D. (2004). Brain function in coma, vegetative state, and related disorders. *Lancet Neurol.* 3, 537–46.
- Lombardi, F., Taricco, M., De Tanti, A., Telaro, E., and Liberati, A. (2002). Sensory stimulation for brain-injured individuals in coma or vegetative state. *Cochrane Database Syst. Rev.* 2, CD001427.
- De Weer, A.S., Da Ros, M., Berré, J., Melot, C., Goldman, S., and Peigneux, P. (2011). Environmental influences on activity patterns in altered states of consciousness. *Eur. J. Neurol.* 18, 1432–1434.
- Candelieri, A., Cortese, M.D., Dolce, G., Riganello, F., and Sannita, W.G. (2011). Visual pursuit: within-day variability in the severe disorder of consciousness. *J. Neurotrauma* 28, 2013–2017.
- Cabello, B., Parthasarathy, S., and Mancebo, J. (2007). Mechanical ventilation: let us minimize sleep disturbances. *Curr. Opin. Crit. Care* 13, 20–26.
- Parthasarathy, S., and Tobin, M.J. (2004). Sleep in the intensive care unit. *Intensive Care Med.* 30, 197–206.
- Drouot, X., Cabello, B., d'Ortho, M.P., and Brochard, L. (2008). Sleep in the intensive care unit. *Sleep Med. Rev.* 12, 391–403.
- Cologan, V., Schabus, M., Ledoux, D., Moonen, G., Maquet, P., and Laureys, S. (2010). Sleep in disorders of consciousness. *Sleep Med. Rev.* 14, 97–105.
- Bekinschtein, T., Cologan, V., Dahmen, B., and Golombek, D. (2009). You are only coming through in waves: wakefulness variability and assessment in patients with impaired consciousness. *Prog. Brain Res.* 177, 171–189.
- Giacino, J.T., Ashwal, S., Childs, N., Cranford, R., Jennett, B., Katz, D.I., Kelly, J.P., Rosenberg, J.H., Whyte, J., Zafonte, R.D., and Zasler, N.D. (2002). The minimally conscious state: definition and diagnostic criteria. *Neurology* 58, 349–353.
- Seel, R.T., Sherer, M., Whyte, J., Katz, D.I., Giacino, J.T., Rosenbaum, A.M., Hammond, F.M., Kalmar, K., Pape, T.L., Zafonte, R., Biester, R.C., Kaelin, D., Kean, J., and Zasler, N. (2010). Assessment scales for disorders of consciousness: evidence-based recommendations for clinical practice and research. *Arch. Phys. Med. Rehabil.* 91, 1795–1813.
- Delorme, A., and Makeig, S. (2004). EEGLAB: an open source toolbox for analysis of single-trial EEG dynamics including independent component analysis. *J. Neurosci. Methods* 134, 9–21.
- Rechtschaffen, A., and Kales, A. (1968). *A Manual of Standardized Terminology, Techniques and Scoring System for Sleep Stages of Human Subjects*. U.S. Dept. of Health, Education, and Welfare: Bethesda, Md.
- Huupponen, E., Väri, A., Himanen, S.L., Hasan, J., Lehtokangas, M., and Saarinen, J. (2000). Optimization of sigma amplitude threshold in sleep spindle detection. *J. Sleep Res.* 9, 327–334.
- Husain, A.M. (2006). Electroencephalographic assessment of coma. *J. Clin. Neurophysiol.* 23, 208–220.
- Blumenfeld, H. (2011). Epilepsy and the consciousness system: transient vegetative state? *Neurol. Clin.* 29, 801–823.
- Bartolomei, F., and Naccache, L. (2011). The global workspace (GW) theory of consciousness and epilepsy. *Behav. Neurol.* 24, 67–74.
- Raichle, M.E., MacLeod, A.M., Snyder, A.Z., Powers, W.J., Gusnard, D.A., and Shulman, G.L. (2001). A default mode of brain function. *Proc. Natl. Acad. Sci. U. S. A.* 98, 676–682.
- Boly, M., Tshibanda, L., Vanhauwenhuyse, A., Noirhomme, Q., Schnakers, C., Ledoux, D., Boveroux, P., Garweg, C., Lambermont, B., Phillips, C., Luxen, A., Moonen, G., Bassetti, C., Maquet, P., and Laureys, S. (2009). Functional connectivity in the default network during resting state is preserved in a vegetative but not in a brain dead patient. *Hum Brain Mapp* 30, 2393–2400.
- Isono, M., Wakabayashi, Y., Fujiki, M.M., Kamida, T., and Kobayashi, H. (2002). Sleep cycle in patients in a state of permanent unconsciousness. *Brain Inj.* 16, 705–712.
- Monti, M.M., Vanhauwenhuyse, A., Coleman, M.R., Boly, M., Pickard, J.D., Tshibanda, L., Owen, A.M., and Laureys, S. (2010). Willful modulation of brain activity in disorders of consciousness. *N. Engl. J. Med.* 362, 579–589.
- Cruse, D., Chennu, S., Chatelle, C., Bekinschtein, T.A., Fernandez-Espejo, D., Pickard, J.D., Laureys, S., and Owen, A.M. (2011). Bed-side detection of awareness in the vegetative state: a cohort study. *Lancet* 378, 2088–2094.
- Rosanova, M., Gosseries, O., Casarotto, S., Boly, M., Casali, A.G., Bruno, M.A., Mariotti, M., Boveroux, P., Tononi, G., Laureys, S., and Massimini, M. (2012). Recovery of cortical effective connectivity and recovery of consciousness in vegetative patients. *Brain* 135, 1308–1320.
- Silva, S., Alacoque, X., Fourcade, O., Samii, K., Marque, P., Woods, R., Mazziotta, J., Chollet, F., and Loubinoux, I. (2010). Wakefulness and loss of awareness: brain and brainstem interaction in the vegetative state. *Neurology* 74, 313–320.
- Landsness, E., Bruno, M.A., Noirhomme, Q., Riedner, B., Gosseries, O., Schnakers, C., Massimini, M., Laureys, S., Tononi, G., and Boly, M. (2011). Electrophysiological correlates of behavioural changes in vigilance in vegetative state and minimally conscious state. *Brain* 134, 2222–2232.
- Chatrian, G.E., White, L.E. Jr., and Daly, D. (1963). Electroencephalographic patterns resembling those of sleep in certain comatose states after injuries to the head. *Electroencephalogr. Clin. Neurophysiol.* 15, 272–280.
- Bergamasco, B., Bergamini, L., Doriguzzi, T., and Sacerdote, I. (1968). The sleep cycle in coma: prognostic value. *Electroencephalogr. Clin. Neurophysiol.* 25, 87.
- Evans, B.M. and Bartlett, J.R. (1995). Prediction of outcome in severe head injury based on recognition of sleep related activity in the polygraphic electroencephalogram. *J. Neurol. Neurosurg. Psychiatry* 59, 17–25.
- Valente, M., Placidi, F., Oliveira, A.J., Bigagli, A., Morghen, I., Proietti, R., and Gigli, G.L. (2002). Sleep organization pattern as a prognostic marker at the subacute stage of post-traumatic coma. *Clin. Neurophysiol.* 113, 1798–1805.
- Uzan, M., Albayram, S., Dashti, S.G., Aydin, S., Hanci, M., and Kuday, C. (2003). Thalamic proton magnetic resonance spectroscopy in vegetative state induced by traumatic brain injury. *J. Neurol. Neurosurg. Psychiatry* 74, 33–38.
- Fernandez-Espejo, D., Junque, C., Bernabeu, M., Roig-Rovira, T., Vendrell, P., and Mercader, J.M. (2010). Reductions of thalamic volume and regional shape changes in the vegetative and the minimally conscious states. *J. Neurotrauma* 27, 1187–1193.
- Lull, N., Noe, E., Lull, J.J., Garcia-Panach, J., Garcia-Marti, G., Chirivella, J., Ferri, J., Sopena, R., de La Cueva, L., and Robles, M. (2010). Thalamic metabolism and neurological outcome after traumatic brain injury. A voxel-based morphometric FDG-PET study. *Neurologia* 25, 174–180.
- Laureys, S., Faymonville, M.E., Luxen, A., Lamy, M., Franck, G., and Maquet, P. (2000). Restoration of thalamocortical connectivity after recovery from persistent vegetative state. *Lancet* 355, 1790–1791.
- Diekelmann, S., and Born, J. (2010). The memory function of sleep. *Nat. Rev. Neurosci.* 11, 114–126.
- Bodizs, R., Kis, T., Lazar, A.S., Havran, L., Rigo, P., Clemens, Z., and Halasz, P. (2005). Prediction of general mental ability based on neural oscillation measures of sleep. *J. Sleep Res.* 14, 285–292.
- Bruno, M.A., Vanhauwenhuyse, A., Thibaut, A., Moonen, G., and Laureys, S. (2011). From unresponsive wakefulness to minimally conscious PLUS and functional locked-in syndromes: recent advances in our understanding of disorders of consciousness. *J. Neurol.* 258, 1373–1384.

Address correspondence to:  
 Victor Cologan, PhD  
 Cyclotron Research Center  
 Allee du 6 Aout 8, B30  
 Liege 4000  
 Belgium

E-mail: victorcologan@gmail.com